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Assessing response to neo-adjuvant therapy

Intra-voxel Incoherent Motion modelling by

DWI data and Standardized Index of Shape

in locally advanced rectal cancer using

Abstract

from DCE-MRI

Background: Our aim was to investigate preoperative chemoradiation therapy (pCRT) response in locally advanced rectal cancer (LARC) comparing standardized index of shape (SIS) obtained from dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI) with intravoxel-incoherent-motion-modelling-derived parameters by diffusion-weighted imaging (DWI).

Materials and methods: Eighty-eight patients with LARC were subjected to MRI before and after pCRT. Apparent diffusion coefficient (ADC), tissue diffusion (D_t) , pseudodiffusion (D_p) and perfusion fraction (f) were calculated and percentage changes ΔADC , ΔD_t , ΔD_p , Δf were computed. SIS was derived comparing DCE-MRI pre- and post-pCRT. Nonparametric tests and receiver operating characteristic (ROC) curves were performed.

Results: A total of 52 patients were classified as responders (tumour regression grade; TRG \leq 2) and 36 as not-responders (TRG > 3). Mann–Whitney *U* test showed statistically significant differences in SIS, Δ ADC and Δ D_t between responders and not-responders and between complete responders (19 patients with TRG = 1) *versus* incomplete responders. The best parameters to discriminate responders by nonresponders were SIS and Δ ADC, with an accuracy of 91% and 82% (cutoffs of -5.2% and 18.7%, respectively); the best parameters to detect pathological complete responders were SIS, Δ f and Δ D_p with an accuracy of 78% (cutoffs of 38.5%, 60.0% and 83.0%, respectively). No increase of performance was observed by combining linearly each possible couple of parameters or combining all parameters.

Conclusion: SIS allows assessment of preoperative treatment response with high accuracy guiding the surgeon *versus* more or less conservative treatment. DWI-derived parameters reached less accuracy compared with SIS and combining linearly DCE- and DWI-derived parameters; no increase of accuracy was obtained.

Keywords: assessment response, diffusion parameters change, LARC, neoadjuvant therapy, SIS change

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Introduction

Preoperative radiation therapy and concomitant chemotherapy (pCRT) combined with total mesorectal excision (TME) is the standard of care in locally advanced rectal cancer (LARC).1-7 Recently, conservative surgical approaches are being developed for early rectal cancer and for patients with significant response after pCRT,¹⁻⁴ while a 'wait and see' policy was adopted when a complete clinical response is reached after pCRT reducing morbidity and provides a 'true' organsparing approach.^{5,6} Complete response (CR) was obtained after pCRT with a percentage of 24% of patients.^{8,9} However, several studies report that morphological magnetic resonance imaging (mMRI) alone cannot to detect pCRT changes in the early phase. In fact, in this phase, tumour change induced by pCRT cannot correspond to a visible and appreciable lesion size reduction;¹⁰ it's difficult to differentiate residual tumour by fibrosis.¹¹ Several authors focus their attention on the study of functional quantitative imaging modality¹⁰⁻¹³ such as dynamic contrast-enhanced MRI (DCE-MRI) and diffusion-weighted imaging (DWI). DCE-MRI has proven useful in detecting residual tumour after pCRT.^{10,14} Authors have previously examined DCE-MRI data to assess pCRT response in LARC,¹⁵⁻¹⁷ individuating the standardized index of shape (SIS),¹⁵ a simple semiquantitative parameter capable of detecting significant and CR after CRT in LARC with high accuracy. Moreover, several researchers have proposed functional parameters derived by DWI as potential biomarkers for treatment response.18 Apparent diffusion coefficient (ADC) can be used as an imaging biomarker to reflect biological tumour changes and to monitor tumoural response to pCRT.¹⁰ The intravoxel incoherent motion (IVIM) model for analysing DWI data allows obtaining tissue diffusion and perfusion parameters and can be used to predict therapy response¹⁹⁻²³

The objective of this study is to examine DCE-MRI and DWI diagnostic accuracy in the pathological-response assessment after pCRT in LARC: SIS by DCE-MRI was compared to diffusion parameters derived IVIM model by DWI.

Materials and methods

Patient selection

Eighty-eight consecutive patients with median age of 64.6 years (range 44–84 years) were enrolled in this prospective study, from March 2013 to

December 2016. All patients had rectal adenocarcinoma, histologically proven. Inclusion criteria were: clinical T4-3 or nodal involvement. Exclusion criteria were: inability to give informed consent, previous rectal surgery, and contraindications to MRI. The present study was approved by the National Cancer Institute of Naples local ethical committee (institutional deliberation n. 357 of 20.04.2010). All participants provided written informed consent for inclusion in the present study. In this protocol, sample size is obtained using the one-sided t test in a one-sample proportion condition. The significance level of the test was targeted at 0.50. Group sample size of at least 82 cases achieves 80% power to detect a difference between the response accuracy rate of 0.6, considering a known success proportion of 89% (accuracy of SIS reported by Petrillo and colleagues¹⁶), an expected success proportion of sample of 95% and a true difference of response accuracy rate $\delta = 0$.

Table 1 reports patient characteristics.

Neoadjuvant therapy and surgical approach

External radiation therapy was executed using one posterior–anterior and two lateral fields or intensity-modulated radiation therapy (IMRT) system. Standard fractions of 1.8 Gy/day were given, five times a week up to a total dose of 50.4 Gy in 28 fractions. Treatment planning details have been previously reported.^{24–26} Planning target volume (PTV) for IMRT was produced according to the 83 recommendations of the International Commission for Radiation Units.²⁷ Each patient received the standard treatment with capecitabine at a dose of 825 mg/m² twice daily, 5 days a week, for 5 weeks.

Patients underwent TME 8 weeks \pm 1 week after the end of pCRT.

Magnetic resonance imaging data acquisition

DCE-MRI was performed before and after pCRT (84–95 days as the range for two MRI exams) with a 1.5T scanner (Magnetom Symphony, Siemens Medical System, Erlangen, Germany) and phased-array body coil. Precontrast coronal T1-weighted two-dimensional (2D) turbo spinecho (TSE) images, sagittal and axial T2 weighted (T2w) 2D TSE images were acquired. Axial DW images were obtained with spin-echo diffusion-weighted echo-planar sequence (SE-DW-EPI) at *b* values equal to 0, 50, 100, 150, 300, 600, 800 s/
 Table 1. Patient characteristics and histopathological findings.

Characteristics	All patients <i>n</i> = 88 (%)	TRG 1-2 n = 52	TRG 3-4 n = 36	<i>p</i> *
Sex				>0.05
Male/female	62 (71)/9 (29)	35/17	27/9	
Median age (range)	66 (44–84)	69 (47–84)	63 (44–81)	
Gunderson risk				>0.05
Intermediate: T3N0	7 (6.8)	5	2	
Moderately high: T3N1, T4N0	35 (38.6)	20	15	
High: T3N2, T4N1-2	46 (47.7)	27	19	
Distance from anal verge				>0.05
≪5 cm	43 (49)	26	17	
>5 cm	45 (51)	26	19	
Circumferential resection margin				>0.05
>2mm	28 (32)	15	13	
≤2mm	21 (24)	15	6	
≤1mm	38 (43)	22	16	
Not measurable	1* (1)	0	1	
Pathological T				< 0.01
T0-2	73 (83)	50	23	
Т3-4	15 (17)	2	13	
Pathological N				< 0.05
NO	71 (81)	46	25	
N1-2	17 (19)	6	11	

*Not measurable for intraperitoneal lesion.

TRG, tumour regression grade; T0-4, size and extent of tumour; N0-2, extent of lymph node spread.

 mm^2 . Axial dynamic contrast-enhanced T1-weighted fast low angle shot three-dimensional gradient-echo images were obtained: 1 sequence before and 10 sequences, after intravenous injection of 0.1 mmol/kg of a positive, gadolinium-based paramagnetic contrast agent (Gd-DOTA, Dotarem, Guerbet, Roissy-CdG-Cedex, France) at 2 ml/s of flow rate, followed by a 10 ml saline flush at the same rate. Sagittal, axial and coronal postcontrast T1-weighted 2D TSE images, with and without fat saturation were also acquired. Table 2 reports MR sequence parameters. In order to reduce respiratory artefacts, each patient received bowel preparation and antispasmodic medication.

Magnetic resonance image data analysis

Image evaluation was done by consensus of two radiologists with 25 years and 10 years of experience in abdominal MRI reading and assessing.

Radiologists, using precontrast T1-weighted images,²⁸ drawn manually regions of interests

Sequence	Orientation	TR/TE/FA (ms/ms/degree)	FOV (mm × mm)	Pixel spacing	ST/gap (mm/mm)
T1w 2D TSE	Coronal	499/13/150	450 imes 450	0.87×0.87	3/0
T2w 2D TSE	Sagittal	4820/98/150	250 imes 250	0.78 imes 078	3/0
T2w 2D TSE	Axial	3970/98/150	250 imes 250	0.78 imes 0.78	3/0
SE-DW-EPI	Axial	2700/83	270 imes 230	1.70×1.70	4/0
T1w FLASH 3D	Axial	9.8/4.76/25	330 imes 247	0.59 imes 0.59	3/0
T1w FLASH 3D	Axial	9.8/4.76/25	330 imes 247	0.59 imes 0.59	3/0
T1w 2D TSE	Sagittal	538/13/150	250 imes 250	0.48×0.48	3/0
T1w 2D TSE	Coronal	538/13/150	250 imes 250	0.48×0.48	3/0
T1w 2D TSE	Axial	450/12/150	270 × 236	0.52×0.52	3/0

Table 2. Pulse sequence parameters on magnetic resonance studies.

AT, acquisition time; DW, diffusion weighted; EPI, echo-planar sequence image; FA, flip angle; FLASH, fast low angle shot; FOV, field of view; SE, spin echo; ST, slice thickness; TE, echo time; TF, turbo factor; T1w, T1 weighted; TSE, turbo spin echo; T2w, T2 weighted; TR, repetition time; 2D, two dimensional; 3D, three dimensional.

(ROIs) along tumour contours, covering the whole lesion with exclusion of peripheral fat, avoiding artefact and blood vessels. For DW-MRI, the radiologists, using DWI with the highest *b* value, manually drew ROIs along tumour contours to obtain DW-MR volume of interest (VOI). No image coregistration was used: we took care to avoid slices where motion artefacts were visible; moreover, a volumetric analysis in order to estimate functional parameters was done to minimize voxel misalignment errors.

In order to perform SIS analysis, an OsiriX (Pixmeo SARL, Bernex, Switzerland) plugin has been developed by the authors.²⁹ For each VOI using the time intensity, curves were calculated using the median value of two dynamic parameters: the maximum signal difference (MSD) and the washout slope (WOS).³⁰ Then, the percentage changes were calculated before and after pCRT (Δ MSD = (MSD₁ – MSD₂)/MSD₁ × 100 and Δ WOS = (WOS₁ – WOS₂)/WOS₁ × 100), and their combination as defined by Petrillo and colleagues.¹⁵

ADC was calculated using the mono-exponential model,^{19,20} while IVIM-derived parameters^{19,20,23,31-34} were calculated by means of variable projection (VARPRO) algorithm.³⁵ In a previous study we reported that the VARPRO algorithm is superior to the conventional Levenberg–Marquardt algorithm for nonlinear curve fitting in the IVIM method for DW-MRI data analysis.³⁶

All analyses were performed using Matlab R2007a (The MathWorks Inc., Natick, MA).

Evaluation of pathologic response

Pathologic response evaluation was effected using the procedure described by both Avallone and colleagues²⁴ and Andreola and colleagues,³⁷ considering the TRG used by Mandard and colleagues,³⁸ assessed by two experienced pathologists; patients with TRG 1 or 2 were classified as major responders, while the remaining patients (TRG 3, 4, or 5) were considered as nonresponders. Patients with TRG 1 were categorized as complete responders.

Statistical analysis

Data were expressed as median \pm standard deviation values. Percentage changes of perfusion and diffusion parameters among responders and nonresponders and among pathological complete responders and incomplete responders were analysed using the Mann–Whitney nonparametric test. Receiver operating characteristic (ROC) curves were calculated to obtain diagnostic performance of SIS and diffusion parameters. Area under the ROC curve (AUC) was considered and

		AADC %	Δf %	ΔD _p %	ΔD _t %	SIS %
Nonresponders	Median value	15.53	-14.77	-8.17	20.04	-34.57
	Standard deviation	13.14	111.30	106.83	53.70	79.72
Responders	Median value	28.18	-33.16	-19.19	29.09	60.31
	Standard deviation	11.45	139.86	144.47	97.46	48.66
All	Median value	24.65	-31.18	-16.98	25.78	25.18
	Standard deviation	15.45	101.27	125.82	45.74	81.09
p value*		<<0.001	0.91	0.48	<<0.001	<<0.001

Table 3. Standardized index of shape change and diffusion parameter change median values for responders and nonresponders groups.

*Mann-Witney U test.

ADC, apparent diffusion coefficient; f, perfusion fraction; D_p , pseudodiffusion; D_t , tissue diffusion; SIS, standardized index of shape.

optimal thresholds were obtained maximizing the Youden index. Sensitivity, specificity, positive predictive value (PPV) and negative predictive value (NPV) were performed. Fisher's exact tests were used to assess if the results were statistically significant. McNemar tests were used in order to compare diagnostic performance for each modality and derived parameters. Moreover, a linear classifier was used to assess diagnostic performance of the parameters' couple combinations, using percentage change of each single parameter and of all derived parameters obtaining sensitivity, specificity, PPV, NPV and accuracy.

A p value < 0.05 was considered significant for all tests. All analyses were performed using Statistics Toolbox of Matlab R2007a.

Results

Each patient had rectal adenocarcinomas; after pCRT and TME, 19 patients had TRG 1, 33 had TRG 2, 21 had TRG 3, 15 had TRG 4, while there were none with TRG 5. Consequently, 52 patients were responders and 19 complete responders by TRG.

Table 1 reports patient characteristics, SIS, ΔADC , ΔD_{t} , ΔD_{p} , Δf and histopathological findings.

Mann–Whitney nonparametric test showed statistically significant differences in SIS, ΔADC and ΔD_t median values between responder patients and nonresponders (Table 3). Table 4 reports SIS

and diffusion parameters performance, while Table 5 shows the performance of each parameter's couple combination (Δf and ΔD_p , Δf and ΔD_t , ΔD_{p} and and ΔD_{t} , SIS and ΔADC , SIS and Δf , SIS and ΔD_t , SIS and ΔD_p , ΔADC and Δf , ΔADC and ΔD_t , ΔADC and ΔD_p) to differentiate responders from nonresponders and to detect complete responders versus incomplete responders. Results were statistically significant for each parameter (Fisher's exact test p < 0.01). SIS diagnostic performance to assess pCRT response was statistically powerful compared with $\triangle ADC$, $\triangle f$, $\triangle D_t$ and $\triangle D_p$ performance, resulting in an increase of values of sensitivity and specificity (p < 0.05 at McNemar test). Conversely, in the discrimination of complete pathological responders, SIS obtained the same accuracy (78%) of Δf and ΔD_p . However, Δf and ΔD_p had a very low sensitivity.

Couple parameter combinations and linear combinations of all MR-extracted parameters did not increase diagnostic performance compared with SIS, both to discriminate responders *versus* nonresponders and to detect pathological complete responders.

Figure 1(a) reports ROC analysis for SIS and diffusion-derived parameters differentiating responders from nonresponders. Figure 1(b) shows ROC analysis for SIS and diffusionextracted parameters to detect complete pathological response.

Figure 2(a), (c) and (e) show DCE-MRI images and SIS evaluation for a responder patient with

	AUC	Sensitivity	Specificity	PPV	NPV	Accuracy	Cutoff	
Performance to discriminate responders by nonresponders group								
AADC	0.79	0.87	0.75	0.83	0.79	0.82	18.74	
Δf	0.49	0.19	0.92	0.77	0.44	0.49	46.41	
ΔD_p	0.46	0.08	0.97	0.80	0.42	0.44	76.98	
ΔD_{t}	0.76	0.63	0.83	0.85	0.61	0.72	27.76	
SIS	0.90	0.96	0.83	0.89	0.94	0.91	-5.16	
Performance to discriminate complete pathological response versus not complete response								
AADC	0.69	0.89	0.46	0.31	0.94	0.56	18.74	
Δf	0.45	0.21	0.94	0.50	0.81	0.78	56.95	
ΔD_p	0.41	0.11	0.97	0.50	0.80	0.78	80.49	
ΔD_t	0.69	0.68	0.68	0.37	0.89	0.68	29.00	
SIS	0.86	0.89	0.74	0.49	0.96	0.78	38.46	

Table 4. Performance of standardized index of shape and diffusion parameters' change.

 Δ , change in parameter; ADC, apparent diffusion coefficient; AUC, area under curve; f, perfusion fraction; D_p, pseudodiffusion; D_t, tissue diffusion; SIS, standardized index of shape; NPV, negative predictive value; PPV, positive predictive value.

TRG 2 and SIS = 13.34%. For the same patient, Figure 2(b) and (c) show the ADC map pre- and post-treatment. \triangle ADC value was 38.79%.

Figure 3(a), (c) and (e) show DCE-MRI images and SIS evaluation for a nonresponder patient with TRG 4 and SIS = -75.19%. For the same patient, Figure 3(b) and (c) show the ADC map pre- and post-treatment. \triangle ADC value was 8.92%.

Figure 4(a), (c) and (e) show DCE-MRI images and SIS evaluation for a complete pathological responder patient with TRG 1 and SIS = 117.64%. For the same patient, Figure 4(b) and (c) show the ADC map pre- and post-treatment. Δ ADC value was 54.86%.

Discussion and conclusion

Recently, there has been emergent interest in functional imaging to improve treatment-response assessment allowing detection of treatmentinduced changes before morphological changes are visible.¹⁰ DCE-MRI and DWI have emerged as powerful tools for predicting pCRT response in several types of tumours and also in rectal cancer. The objective of this study was to examine DCE-MRI and DWI diagnostic accuracy in the pathological-response assessment after pCRT in LARC: SIS by DCE-MRI was compared with the diffusion-parameter-derived IVIM model by DWI.

To the best of our knowledge, there are no other studies that compare DCE-MRI and DWI data in LARC and their combination for therapyresponse assessment after pCRT. There are several studies that with a single modality examine capability of evaluating therapy respo the nse.11-16,39,40 We demonstrated the ability of SIS to detect complete and significant response after pCRT in LARC15 and the strength of SIS compared with fluorodeoxyglucose positron-emission tomography (¹⁸F-FDG-PET) examination.41 Some studies demonstrated the role of DWI in LARC for assessing therapy response^{39,40} and several studies evaluated the use of the IVIM model for extracting DWI data by both perfusion and diffusion parameters in different types of tumours.^{32,33,42} In our previous study,¹⁰ we compared SIS with diffusion parameters and their combination after short-course radiotherapy in LARC, demonstrating that no accuracy increase was obtained combining linearly each possible perfusion and diffusion parameter couple

	Sensitivity	Specificity	PPV	NPV	Accuracy		
Performance to discriminate responders by nonresponders group							
SIS and AADC	0.92	0.86	0.91	0.89	0.90		
SIS and ∆f	0.87	0.83	0.88	0.81	0.85		
SIS and ΔD_p	0.87	0.86	0.90	0.82	0.86		
SIS and ΔD_t	0.90	0.83	0.89	0.86	0.88		
ΔD_p and Δf	0.56	0.42	0.58	0.39	0.50		
ΔD_t and Δf	0.71	0.75	0.80	0.64	0.73		
ΔD_t and ΔD_p	0.73	0.64	0.75	0.62	0.69		
ΔADC and Δf	0.79	0.72	0.80	0.70	0.76		
ΔADC and ΔD_{p}	0.83	0.75	0.83	0.75	0.80		
ΔADC and ΔD_t	0.81	0.72	0.81	0.72	0.77		
All parameters	0.90	0.83	0.89	0.86	0.88		
Performance to discrim	inate complete patho	ological response vers	s <i>us</i> not comple	te response			
SIS and AADC	0.79	0.74	0.45	0.93	0.75		
SIS and ∆f	0.79	0.75	0.47	0.93	0.76		
SIS and ΔD_p	0.74	0.72	0.42	0.91	0.73		
SIS and ΔD_t	0.79	0.74	0.45	0.93	0.75		
ΔD_p and Δf	0.26	0.78	0.25	0.79	0.67		
ΔD_t and Δf	0.58	0.70	0.34	0.86	0.67		
ΔDt and ΔD_p	0.58	0.77	0.41	0.87	0.73		
ΔADC and Δf	0.58	0.52	0.25	0.82	0.53		
ΔADC and ΔD_{p}	0.58	0.61	0.29	0.84	0.60		
ΔADC and ΔD_t	0.63	0.68	0.35	0.87	0.67		
All narameters	0 74	0 74	0.44	N 91	0 74		

Table 5. Performance of combinations of standardized index of shape with the diffusion parameters' change.

 Δ , change in parameter; ADC, apparent diffusion coefficient; AUC, area under curve; f, perfusion fraction; D_p, pseudodiffusion; D_t, tissue diffusion; SIS, standardized index of shape; NPV, negative predictive value; PPV, positive predictive value.

extracted by DCE-MRI and DWI or combining all functional MR-derived parameters with respect to SIS alone.

Our results showed that there were statistically significant differences between responders and nonresponder patients for SIS, Δ ADC and Δ D_t (p < 0.001 with Mann–Whitney *U* test). The best

parameters for classifying responder and nonresponder patients were \triangle ADC and SIS, with a sensitivity of 87% and 96%, a specificity of 75% and 83% and an accuracy of 82% and 91%, respectively, using cutoffs of 18.74% and -5.16%, respectively. SIS diagnostic performance to assess pCRT response was statistically significant compared with \triangle ADC, \triangle f, \triangle D_t and \triangle D_p performance,



Figure 1. Receiver operating characteristic analysis for the standardized index of shape and diffusion parameters by intravoxel incoherent motion.

This analysis discriminates responders from nonresponders (a), and complete pathological response *versus* noncomplete pathological response (b).





Figure 2(a), (c) and (e) show DCE-MRI images and SIS analysis for a responder patient with TRG 2 and Δ SIS = 13.34%. For the same patient, Figure 2(b) and (d) show the ADC map pre- and post-treatment. Δ ADC value was 38.79%. ADC, apparent diffusion coefficient; DCE, dynamic contrast enhanced; MRI, magnetic resonance imaging; SIS, standardized

index of shape; TRG, tumour regression grade; MSD, maximum signal difference; ROI, region of interest; STD, standard deviation; TTP, time to peak; WII, wash in intercept; WIS, wash in slope; WOI, wash out intercept; WOI_WII, wash out intercept rate; WOS, wash out slope; WOS_WIS, wash out slope on wash in slope rate.



Figure 3. Dynamic contrast-enhanced magnetic resonance imaging and standardized index of shape analysis for a nonresponder patient.

Figure 3(a), (c) and (e) show DCE-MRI images and SIS analysis for a nonresponder patient with TRG 4 and Δ SIS = -75.19%. For the same patient, Figure 3(b) and (d) show the ADC map pre- and post-treatment. Δ ADC value was 8.92%. ADC, apparent diffusion coefficient; DCE, dynamic contrast enhanced; MRI, magnetic resonance imaging; SIS, standardized index of shape; TRG, tumour regression grade; MSD, maximum signal difference; ROI, region of interest; STD, standard deviation; TTP, time to peak; WII, wash in intercept; WIS, wash in slope; WOI, wash out intercept; WOI_WII, wash out intercept on wash in intercept rate; WOS, wash out slope; WOS_WIS, wash out slope on wash in slope rate.



Figure 4. Dynamic contrast-enhanced magnetic resonance imaging and standardized index of shape analysis for a complete pathological responder patient.

Figure 4 (a), (c) and (e) show DCE-MRI images and SIS analysis for a complete pathological responder patient with TRG 1 and Δ SIS = 117.64%. For the same patient, Figure 4(b) and (d) show the ADC map pre- and post-treatment. Δ ADC value was 54.86%.

ADC, apparent diffusion coefficient; DCE, dynamic contrast enhanced; MRI, magnetic resonance imaging; MSD, maximum signal difference; ROI, region of interest; SIS, standardized index of shape; STD, standard deviation; TRG, tumour regression grade; TTP, time to peak; WII, wash in intercept; WIS, wash in slope; WOI, wash out intercept; WOI_WII, wash out intercept on wash in intercept rate; WOS, wash out slope; WOS_WIS, wash out slope on wash in slope rate.

resulting in an increase both of sensitivity and specificity (p < 0.05 with McNemar test).

Patients with pathological CR have a favourable long-term outcome with very good local control and disease-free survival.38 Adopting a 'wait and see' policy for clinical complete responders helps prevent surgical morbidity and mortality risks.43-⁴⁵ Choi and colleagues³⁹ reported that ADC low percentile values have significant difference between pathological CR and nonpathological CR groups. Our findings showed that the best parameter for detecting complete responders was SIS, with a sensitivity of 86% and a specificity of 74%, with a cutoff of 38.46%. SIS showed the same accuracy (78%) as IVIM-derived Δf and ΔD_p . However, Δf and ΔD_p had a very low sensitivity, probably due to major complexity in the IVIM-derived parameter calculation which is more influenced by image noise. Combining different functional imaging techniques could increase the specificity of therapy response. Lambrecht and colleagues⁴⁶ demonstrated that combining ¹⁸F-FDG PET/computed tomography (CT) with DWI may further increase the response assessment specificity. In our study, instead, each parameter couple combination and the linear classifier of all MR-extracted parameters did not determine an increase of the diagnostic performance compared with SIS alone, both in detecting significant and complete responders.

There are some possible limits in our study: two radiologists evaluated the MR images by consensus in a single session, therefore intraobserver variability was not evaluated. IVIM-extracted parameter reproducibility was not assessed; however the use of median values for VOI for each DCE and DW parameter allows obtaining more robust measures. In this study, our aim was to assess pathological complete and significant response after neoadjuvant therapy. Other modalities having an important role in clinical diagnosis (CT, endoscopy and endoscopic ultrasound) were not included, however, these could be added in a future study for patient stratification.

SIS is an encouraging DCE-MRI semiquantitative functional biomarker suitable for assessing and predicting pCRT response guiding surgeon *versus* more or less conservative treatment. SIS allows assessment of preoperative treatment response with high accuracy while DWI-derived parameters reached less accuracy compared with SIS. Moreover, in combining linearly DCE- and DWI-derived parameters, no increase in accuracy was obtained.

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Conflict of interest statement

The authors declare that there is no conflict of interest.

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