OPEN

Hearing Preservation With the Use of Flex²⁰ and Flex²⁴ Electrodes in Patients With Partial Deafness

*†‡Piotr H. Skarzynski, *Henryk Skarzynski, *Beata Dziendziel, *Joanna J. Rajchel, *Elzbieta Gos, and *Artur Lorens

*World Hearing Center, Institute of Physiology and Pathology of Hearing, Warsaw/Kajetany, Poland; †Heart Failure and Cardiac Rehabilitation Department, Medical University of Warsaw, Warsaw; and ‡Institute of Sensory Organs, Warsaw/Kajetany, Poland

Objective: To evaluate the impact of electrode length on hearing preservation (HP) in Partial Deafness Treatment–Electrical Complement (PDT-EC) subjects.

Study Design: Retrospective case review.

Setting: Tertiary referral center.

Patients: Twenty-three PDT-EC patients (with preoperative air-conduction thresholds \leq 30 dB up to 500 Hz) were divided into two groups: Flex20 electrode (Med-EL GmbH, Innsbruck, Austria) (12 patients) and Flex24 electrode (Med-EL GmbH, Innsbruck, Austria) (11 patients).

Interventions: All participants were subjected to minimally invasive cochlear implantation using the round window approach.

Main Outcome Measure(s): Pure tone audiometry (125–8000 Hz) was performed preoperatively and at 1, 6, 12, and 24 months postoperatively. HP was established using the HEARRING group formula. Speech understanding was assessed preoperatively and at 12 and 24 months postoperatively.

The most important goal of partial deafness treatment (PDT) is to restore the person's hearing ability and speech understanding in complex listening environments (1). The preservation of preoperative functional residual hearing the basis of the most successful auditory rehabilitation (2). To minimize intraoperative cochlear trauma and assist hearing preservation (HP) during

DOI: 10.1097/MAO.000000000002357

Results: Analysis of HP for every individual indicates that more than half the patients with Flex20 and Flex24 had complete HP at 6 months follow-up. None of the patients from either group had complete loss of hearing. At activation, average air-conduction thresholds for low frequencies (125–500 Hz) were slightly better for the short electrode (M=29.03) than for the long (M=39.10) but the difference was not statistically significant (p=0.067). The effect of electrode (Flex20 versus Flex24) was not significant in terms of pure tone audiometry and speech recognition at long-term follow-up.

Conclusions: In the early postoperative period, complete HP was possible in a majority of patients from both groups, but slightly better HP outcomes were achieved by Flex20. In the long term, the length of the electrodes does not affect the degree of HP or speech understanding. **Key Words:** Cochlear implant—Hearing preservation—Med-EL Flex electrodes—Partial deafness treatment.

Otol Neurotol 40:1153-1159, 2019.

cochlear implantation, minimally traumatic surgical technique and the latest electrode design is required (3,4). Atraumatic positioning of the electrode into the cochlear duct is extremely important—any displacement towards scala vestibuli causes damage to the delicate structures of the cochlea, which will have a negative effect on HP (5). O'Connell et al. (6) claim that atraumatic insertion of the electrode into scala tympani (ST) is more likely using lateral wall (LW) electrodes (compared with perimodiolar [MP] or mid-scala electrodes [MS]) and advocate access through the round window or an extended round window (in comparison to cochleostomy).

Quite a few articles have been published on the relationship between the depth of insertion (using the same type of electrode design) and postoperative auditory results (7-9). Most of these studies have a retrospective design. The only prospective study published so far relating electrode length to HP was conducted by Buchman et al. (10); it was closed by the institutional

Copyright © 2019 The Author(s). Published by Wolters Kluwer Health, Inc. on behalf of Otology & Neurotology, Inc.

Address correspondence and reprint requests to Piotr H. Skarzynski, Ph.D., M.D., M.S., Mokra 17 Street, 05-830 Kajetany, Poland; E-mail: p.skarzynski@ifps.org.pl

No other benefits were received.

The authors disclose no conflicts of interest.

Supplemental digital content is available in the text.

This is an open access article distributed under the terms of the Creative Commons Attribution-Non Commercial-No Derivatives License 4.0 (CCBY-NC-ND), where it is permissible to download and share the work provided it is properly cited. The work cannot be changed in any way or used commercially without permission from the journal.

bioethics committee after recruiting only 13 patients: six in a group with shorter electrodes (medium, 20.9 mm) and seven in a group with longer (standard, 26.4 mm) electrodes. The reason was that the results of a preliminary statistical analysis 6 months postoperatively revealed that the use of the longer electrodes was associated with significantly better speech understanding. The authors suggested that deeper insertion angles with the standard arrays produced greater degrees of cochlear coverage in the apical regions and a better or more natural tonotopic place representation during stimulation. However, it should be noted that the authors did not specify the precise hearing thresholds of their patients, saying just that they were "standard candidates for cochlear implantation" and "had moderate to profound hearing loss and poor speech perception ability" in the preoperative period (without precisely specifying the hearing thresholds in both groups).

The methodological diversity of research conducted in the area of HP—particularly in terms of reporting initial hearing status—creates difficulties in comparing results and drawing conclusions based on appropriate meta-analyses (11). To assess the impact of electrode length on HP outcomes, it is necessary to conduct a study in a homogeneous group of PDT patients in terms of their preoperative residual hearing. This is particularly important in patients with normal or nearly normal hearing (\leq 30 dB HL) up to 500 Hz and severe-to-profound hearing loss above 500 Hz. According to the classification of Skarzynski et al. (12,13), these patients qualify as Partial Deafness Treatment– Electrical Complementation (PDT-EC).

The aim of this study was to evaluate the impact of electrode length on HP in a selected group of adults with PDT-EC receiving one of two kinds of flexible electrodes: the longer 24 mm electrode array or shorter 20 mm electrode array.

MATERIALS AND METHODS

Eligibility Criteria

Records of all cochlear implantation conducted in our center were carefully studied to make sure that the participants complied with the following eligibility criteria:

- 1) implanted at age 18 years or older;
- 2) postlingual onset of deafness;
- 3) preoperative hearing loss qualifying a patient into the PDT-EC group according to Skarzynski et al. (12) (i.e., air-conduction thresholds \leq 30 dB up to 500 Hz and severe-to-profound hearing loss above 500 Hz);
- 4) full medical and audiometric documentation of pre- and postoperative (minimum 24 mos) hearing results;
- use of a minimally invasive surgical approach through the round window according to the Skarzynski six-step procedure (13,14) and a fully inserted Flex²⁰ or Flex²⁴ electrode set.

Participants

The evaluated group consisted of 23 patients with PDT-EC. Subjects were implanted unilaterally with a Med-EL cochlear

Otology & Neurotology, Vol. 40, No. 9, 2019

implant (CI) (Med-EL GmbH, Innsbruck, Austria) between August, 2014 and July, 2016. The participants were divided into two groups based on the electrode length.

One group (n = 11) received the longer Flex²⁴ electrode. This is a 24-mm electrode array featuring Flex-Tip technology and designed for combined Electric Acoustic Stimulation (EAS) with insertion of less than 1.5 turns. It has 19 platinum electrode contacts with an active stimulation length of 20.9 mm. Diameter at the basal end is 0.8 mm and dimensions at the apical end are 0.5×0.3 mm.

The second group (n = 12) received the shorter Flex²⁰ electrode. This 20-mm electrode array also features Flex-Tip technology and has a diameter at the basal end of 0.8 mm and dimensions at the apical end of 0.5×0.3 mm. However, its 19 platinum electrode contacts have a shorter active stimulation length of 15.4 mm, designed for cases of partial deafness or other specific needs or surgical preferences.

The decision to use the shorter or longer electrode was based on preoperative air-conduction thresholds. In both groups of PDT-EC patients, the results of pure-tone audiometry confirmed hearing thresholds of less than or equal to 30 dB HL up to 500 Hz. However, the Flex²⁰ was offered to patients with more residual hearing (\leq 75 dB HL) at 750 and 1000 Hz. If subjects had less residual hearing, they were assigned the longer electrode.

One month postoperatively, 22 subjects were programmed with electric stimulation only, due to well-preserved low-frequency hearing thresholds. The acoustic unit (system Duet) was activated 1 month postoperatively in one patient with the $Flex^{24}$ who had postoperatively air-conduction thresholds of 60 to 75 dB HL for low frequencies (125–500 Hz). This patient also used hearing aid in the non-CI ear. Additionally, after 12 months follow-up, we observed a significant deterioration of hearing thresholds (to 30–85 dB HL) at low frequencies in one subject with $Flex^{20}$, so the acoustic unit was also activated in this case.

Surgical Procedure

The decision on qualifying the PDT-EC patient for cochlear implantation was made on the basis of a lack of sufficient benefits from conventional hearing aids (obtaining a score of $\leq 60\%$ in the monosyllabic word test in the best-aided condition) and appropriate motivation to undergo treatment. All procedures were conducted by the same senior surgeon from our tertiary referral center. In all cases, a minimally invasive surgical approach through the round window according to the Skarzynski 6-step procedure (14) with full insertion of CI electrode was used. Steroids were given in all patients with PDT: 0.1 mg/kg of body mass per day of dexamethasone administered intravenously in two equal doses per day (about 0.5 h before cochlear implantation and 3 h after). Dosing with steroids was continued for 3 to 4 days (15).

Audiometric Assessment and Hearing Preservation

Hearing threshold measurements were conducted on all patients five times: preoperatively, 1 month after the operation (at activation), 6 months after the operation, 12 months after the operation, and 24 months after the operation. HP was calculated based on pure-tone audiometry at 11 audiometric frequencies (0.125, 0.25, 0.5, 0.75, 1, 1.5, 2, 3, 4, 6, and 8 kHz) and was calculated using the Skarzynski et al. (16) formula:

$$HP = \left(1 - \frac{PTApost - PTApre}{PTAmax - PTApre}\right) * 100 [\%]$$

1

In this equation, PTApre is the pure tone average measured preoperatively, PTApost is the pure tone average measured postoperatively, and PTAmax is the maximum level generated by a standard audiometer (provided in detail on the HEAR-RING Internet site (17)). The HP values can be divided into: loss of hearing (no detectable hearing), minimal HP (range, 1-25%), partial HP (26–75%), and complete HP (>75%).

Speech Understanding Evaluation

The Pruszewicz monosyllabic word test was conducted in free-field at the preoperative period under unaided and aided configurations (with hearing aids) under the best conditions. The test was conducted in quiet and in noise at a signal-to-noise ratio of +10 dB. The signals were presented at 65 dB SPL. The Pruszewicz monosyllabic word test in free-field was also used to assess auditory benefits after cochlear implantation at the 12 and 24 months follow-up.

Ethical Considerations

All procedures were in accordance with the ethical standards of the responsible institutional review board (approval KB.IFPS:12/2018) and of the Helsinki Declaration. The first author of the current work was the principal investigator. Due to the retrospective nature of the study, no informed consent was obtained from the participants.

Statistical Analyses

Mixed-design analysis of variance (ANOVA) was conducted to determine the impact of electrode length on audiometric results:

- air-conduction thresholds for all audiometric frequencies (125-8000 Hz)
- air-conduction thresholds for low audiometric frequencies only (125–500 Hz)
- 3) word recognition in quiet and noise.

The level of statistical significance was established at p < 0.05. For statistical analysis, IBM SPSS Statistics v.24 software (IBM, New York, U.S.A.) was used.

TABLE 1. Characteristics of study participants according to
group ($Flex^{20}$ and $Flex^{24}$ electrodes)

Patient Characteristics	Flex ²⁰	Flex ²⁴	
Sex, n (%)			
Male	4 (33.3)	5 (45.5)	
Female	8 (66.7)	6 (54.5)	
Implantation site, n (%)			
Right	5 (41.7)	5 (45.5)	
Left	7 (58.3)	6 (54.5)	
Etiology of hearing loss, n (%)			
Idiopathic SNHL	10 (83.3)	7 (63.6)	
Acoustic trauma	2 (16.7)	2 (18.2)	
Ototoxic drug	0	1 (9.1)	
Mumps	0	1 (9.1)	
Age at implantation, M (SD)	49.6 (15.5)	52.8 (15.2)	
Duration of hearing loss, M (SD)	16.6 (5.4)	23.4 (15.6)	

SD indicates standard deviation; SNHL, sensorineural hearing loss.

RESULTS

Characteristics of the study participants (sex, operated ear, etiology of hearing loss, age at operation, and age at diagnosis) according to group (shorter or longer electrodes) are presented in Table 1.

Hearing Preservation in PDT-EC Groups

The average pre- and postoperative air-conduction hearing thresholds in each group of $Flex^{20}$ and $Flex^{24}$ electrodes are shown in Figure 1. Exact descriptive statistics of pre- and postoperative air-conduction thresholds are presented in the supplementary table, http://links.lww.com/MAO/A821. The HP outcomes for each postoperative follow-up period (activation to 24 months follow-up) are presented separately for patients with $Flex^{20}$ and $Flex^{24}$ electrodes in Table 2.

The analysis of HP results for each individual indicates that in the short-term (up to 12 months follow-up), all

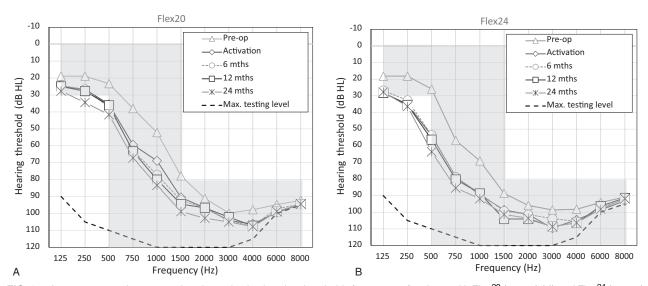


FIG. 1. Average pre- and postoperative air conduction hearing thresholds for groups of patients with Flex^{20} (n = 12) (A) and Flex^{24} (n = 11) electrodes (B).

Hearing Preservation Evaluation

Period	Complete HP n (%)		Partial HP n (%)		Minimal HP n (%)		Loss of Hearing n (%)	
	Flex ²⁰	Flex ²⁴	Flex ²⁰	Flex ²⁴	Flex ²⁰	Flex ²⁴	Flex ²⁰	Flex ²⁴
At activation	8 (66.7)	8 (72.7)	4 (33.3)	3 (27.3)	0 (0)	0 (0)	0 (0)	0 (0)
Result 6 months	6 (50.0)	7 (63.6)	6 (50.0)	4 (36.4)	0 (0)	0 (0)	0 (0)	0 (0)
Result 12 months	5 (41.7)	6 (54.5)	7 (58.3)	5 (45.5)	0 (0)	0 (0)	0 (0)	0 (0)
Result 24 months	5 (41.7)	5 (45.5)	6 (50.0)	6 (54.5)	1 (8.3)	0 (0)	0 (0)	0 (0)

TABLE 2. Hearing preservation outcomes for groups of patients with $Flex^{20}$ and $Flex^{24}$ electrodes at each follow-up

patients with Flex²⁰ and Flex²⁴ had complete or partial HP. Importantly, none of the patients from either group had complete loss of hearing in the long term (up to 24 months follow-up). In one patient with Flex²⁰, complete HP was observed up to 6 months postsurgery, and then a gradual, substantial deterioration of hearing occurred to reach a minimal HP at the long-term (24month) follow-up.

The average pre- and postoperative air-conduction thresholds across all audiometric frequencies (125-8000 Hz) and low-frequencies (125-500 Hz) for both groups of patients are summarized in Table 3.

Average Air-Conduction Threshold Across All Frequencies (125-8000 Hz)

Overall, there was a significant effect of time on the mean audiometric thresholds: F = 28.79; p < 0.001; $e^2 = 0.578$. For both sets of electrodes, mean air-conduction threshold across all frequencies was the smallest before implantation but remained stable from activation until 24 months postoperatively. The effect of electrode was nonsignificant: F = 1.93; p = 0.179; $e^2 = 0.084$. There was no significant interaction effect (time \times electrode):

 $F = 0.60; p = 0.597; e^2 = 0.028$, but it was noticed that there was a difference between sets of electrodes at the activation period (1 month after implantation). The overall mean air-conduction thresholds were better for the short electrode (M = 74.34) than for the long electrode (M=81.03), but only at activation (p=0.029).

Average Air-Conduction Threshold for Low Frequencies (125–500 Hz)

For low frequencies, the effect of time on audiometric thresholds was statistically significant: F = 14.27; p < 0.001; $e^2 = 0.405$. For both sets of electrodes, mean air-conduction threshold across low frequencies was the smallest before implantation but remained stable from activation to 24 months postoperatively. The effect of electrode was nonsignificant: F = 1.07; p = 0.312; $e^2 = 0.049$. There was no significant interaction effect (time × electrode): F = 0.83; p = 0.451; $e^2 = 0.038$, but at activation mean air-conduction thresholds for low frequencies were slightly better for short electrodes (M=29.03) than for long electrodes (M=39.10) but the difference was not statistically significant (p = 0.067).

Period	Range of Frequencies Tested									
	125-8000 Hz					125–500 Hz				
	Min	Max	M	SD	Me	Min	Max	М	SD	Me
$Flex^{20}$ (n = 12)										
Preoperative	54.55	79.32	64.13	7.09	62.27	5.00	30.00	19.86	7.29	20.00
At activation	57.73	85.45	74.34	7.56	76.13	11.67	56.67	29.03	10.88	26.66
Result 6 months	64.09	91.36	75.61	7.95	74.09	6.67	66.67	30.00	16.22	25.83
Result 12 months	61.82	97.73	78.03	10.32	75.68	6.67	71.67	33.47	19.42	27.50
Result 24 months	61.82	104.55	81.44	13.06	75.63	6.67	81.67	40.14	25.17	28.33
$Flex^{24}$ (n = 11)										
Preoperative	49.09	81.82	68.59	68.59	67.72	10.00	30.00	20.76	6.47	21.66
At activation	73.18	92.50	81.03	81.03	80.45	25.00	73.33	39.09	14.05	38.33
Result 6 months	70.91	88.64	80.02	80.02	79.54	21.67	63.33	37.72	11.29	35.00
Result 12 months	68.18	97.27	81.79	81.79	79.53	21.67	73.33	40.00	16.55	35.02
Result 24 months	71.82	100.00	83.18	83.18	80.45	21.67	75.00	42.58	17.82	33.33

TABLE 3. Average pre- and postoperative air-conduction thresholds across all audiometric frequencies (125–8000 Hz) and for low

SD indicates standard deviation.

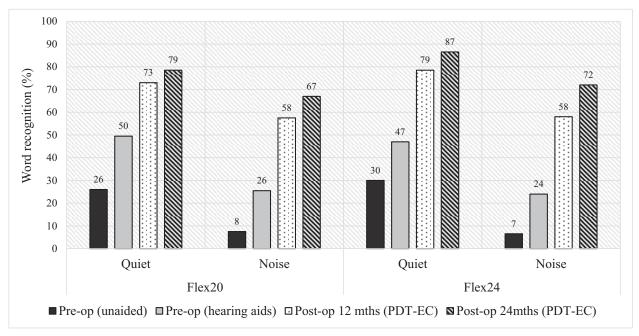


FIG. 2. Average word recognition scores on the Pruszewicz monosyllabic word test in free field for quiet and noise before and after cochlear implantation for groups of patients using Flex^{20} (n = 12) and Flex^{24} (n = 11).

Speech Understanding in PDT-EC Groups

Before surgery all patients reported a lack of benefit from conventional hearing aids. Ten of 23 patients used a unilateral hearing aid before surgery of which only two reported regular use of the prosthesis. Only one patient used bilateral hearing aids before surgery. After cochlear implantation, this patient (with Flex²⁴) continued to use bilateral stimulation (electroacoustic stimulation in the implanted side and a hearing aid in the non-CI ear). The others 22 of 23 patients used monaural electrical stimulation (including one patient using electroacoustic stimulation).

The results of the Pruszewicz monosyllabic word test conducted preoperatively and at 12 and 24 months after surgery are shown in Figure 2.

The results showed a steady improvement over time in speech understanding in quiet and noise for both groups of patients. A significant improvement in speech understanding was also observed in the single patient using $Flex^{20}$ in whom a minimal HP was observed at the 24-month follow-up. In this patient (with electroacoustic stimulation in the operated ear), understanding of monosyllabic words increased from 5 to 90% in quiet and 0 to 75% in noise at the 24-month follow-up.

Word Recognition in Quiet

The effect of time was statistically significant: F = 106.58; p < 0.001; $e^2 = 0.856$. For the short electrodes, mean speech recognition in quiet was 26% before implantation and improved to 73% at 12 months and to 78.5% at 24 months postoperatively. For the long electrodes, mean speech recognition in quiet was 30% before

implantation and improved to 78.5% at 12 months and to 86.5% at 24 months postoperatively. The effect of electrode was nonsignificant: F = 0.75; p = 0.398; $e^2 = 0.040$. There was no significant interaction effect (time × electrode): F = 0.84; p = 0.428; $e^2 = 0.045$. Word recognition in quiet was similar for both electrodes in each period.

Word Recognition in Noise

The effect of time was statistically significant: F = 95.59; p < 0.001; $e^2 = 0.839$. For the short electrodes, mean speech recognition in noise was 7.5% before implantation and improved to 57.5% at 12 months and to 67% at 24 months postoperatively. For the long electrodes, mean speech recognition in noise was 6.5% before implantation and improved to 58% at 12 months and to 72% at 24 months postoperatively. The effect of electrode was nonsignificant: F = 0.02; p = 0.885; $e^2 = 0.001$. There was no significant interaction effect (time × electrode): F = 0.25; p = 0.754; $e^2 = 0.014$. Word recognition in noise was similar for both electrodes at each period.

DISCUSSION

Ongoing scientific and clinical studies on preserving cochlear structure and potentially preserving residual low-frequency hearing have resulted in the development of thinner, shorter, and more flexible LW electrodes (18). According to the manufacturer, both the Flex²⁰ and Flex²⁴ LW electrodes, with insertion depths of less than 1.5 turns, makes it possible to reduce trauma and increase the chance of HP. A special

tapered tip and ultra-flexible wave-shaped wires have been developed to increase mechanical flexibility. We found that at the first follow-up (at activation), slightly better HP outcomes were seen in PDT-EC patients which used the short, flexible 20 mm electrodes. At longer follow-up, electrode length was not associated with degree of HP.

When evaluating HP after CI, a limitation of our study is lack of information about the location of the electrode within the cochlea. A CT scan is not routinely performed on all patients undergoing cochlear implantation. It is widely accepted that to limit trauma during electrode insertion, the electrode array should be positioned entirely within the ST (6). Some evidence has suggested that LW electrodes are more likely to reside solely within the ST than other array designs (3,4,6). Wanna et al. (19) compared outcomes between LW and PM electrodes and found that more LW electrodes (89%) resided completely within the ST than did their PM counterparts (58%). When they compared three surgical approaches, the authors concluded that both enlarged RW and standard RW procedures had higher rates of complete ST insertion than did cochleostomies, and this pattern held true regardless of the electrode type. Mady et al. (4) assessed whether electrode type (LW and PM) with full-length arrays produced by the same manufacturer affects HP. At short-term (1 mo) follow up, LW electrodes were associated with significantly better HP than MP electrodes. At long-term (1 yr) follow-up, electrode type was not associated with HP or outcomes of speech perception. However, the authors note that at a long-term follow-up, less patients in the LW group had audiometric testing data than did patients in the PM group. Surgical approach also differed by electrode type, and insertion of the electrode via the round window was more frequently performed in the group of patients who received the LW electrode. Achieving an improvement in speech understanding is an important goal in the treatment of deafness and partial deafness. The better that preoperative hearing can be preserved, the greater the benefits reported by the CI user (20,21). Preoperatively, even when there is a good level of low frequency hearing in patients with PDT-EC, relatively poor speech understanding is present, despite the use of hearing aids. After surgery, all subjects had a significant improvement in speech perception in quiet and in noise. However, the length of the electrode did not affect speech understanding. These observations differ from previously reported results. According to Büchner et al. (7), who studied the speech comprehension scores among ES-only users (residual hearing less than 75 dB at 250 Hz), the patients with longer (Flex²⁸) electrodes had better scores than patients with shorter electrodes (Flex²⁰ and Flex²⁴). Similar results were found with the Bruce et al. (9) study: longer electrode insertions (Standard, 26.4 mm) gave better speech perception in the early postactivation period compared with shorter electrodes (medium, 20.9 mm). However,

no quality of life or music perception differences were found between the groups.

Comparison of our results with previous reports on the effect of electrode length on HP outcome is difficult due to methodological differences and the degree of residual hearing. Suhling et al. (8) reported that HP is possible with both short (20-24 mm array length) and long (28 mm) electrodes in a group of patients with preoperative air-conduction thresholds better than or equal to 80 dB between 125 and 1500 Hz. However, shorter electrodes provide smaller hearing losses for up to 1 year after the operation. It is noteworthy that the authors did not use any HP classification but evaluated it as the median difference pre- and postoperatively for frequencies 125 to 1500 Hz. On the basis of a group of patients with only electric stimulation (ES) from the same center published 1 year later, the authors confirm that the preoperative residual hearing at low frequencies (125-1000 Hz) in patients receiving Flex²⁰ and Flex²⁴ electrodes was significantly better than for patients who received a longer Flex^{28} electrode (7). However, the best HP results were obtained in the group of patients with electric-acousticstimulation (EAS) who received Flex²⁰ and Flex²⁴. Nevertheless, preoperative hearing thresholds for these four groups of patients differed appreciably. On the other hand, evidence that hearing can be preserved using deep insertion of the CI electrode array was confirmed in the study by Bruce et al. (22). In this case it should be emphasized that HP was evaluated in a group of 13 patients who used a deep insertion electrode array (Med-EL Flex^{SOFT}, 31.5 mm), and their preoperative residual hearing was outside the criteria for EAS stimulation.

There are many factors determining the success of a CI operation, and one is the use of specially designed electrodes with different lengths and mechanical properties which match the patient's preoperative residual hearing (6). In addition, the results of HP need to take into account surgical technique, electrode array design, insertion speed of the electrode, and use of corticosteroids (23–25). In the most recent publication reporting the results of a meta-analysis, there was no significant effect of electrode array length on HP outcome (23). It was suggested, however, that the round window approach with a straight electrode array might result in a better HP outcome.

Suhling et al. (8) emphasize that to achieve the best result for each subject, decision-making should take into account the individual's cochlear anatomy, level of preoperative residual hearing, and medical history. When deciding on the choice of electrode length in patients with partial deafness, it is necessary to take into account the natural course of progressive hearing loss (25,26). Most of our PDT-EC patients had progressive hearing loss, which was confirmed by audiometric testing. Our observation that residual hearing may worsen over time following CI is in line with previous reports (4,27). In the light of these findings, we suggest that using the longer $Flex^{24}$ electrode in PDT-EC patients may be a better choice, especially in the long-term. However, to make a firm conclusion on this, we need additional studies. Due to the small sample size of our study, its power was not adequate to detect statistical significance (it was lower than 80%). To have a sample size adequate for detecting a difference between the $Flex^{20}$ and $Flex^{24}$ electrodes 24 months after implantation, it be necessary to set up an inter-center collaboration and collect results from a large group of PDT-EC patients.

CONCLUSION

In early postoperative observations, complete HP was possible in the majority of patients from both groups, although slightly better HP outcomes were achieved by the Flex²⁰. In the long-term, however, the electrode length (20 or 24 mm) does not affect the degree of HP or speech understanding, at least in the hands of an experienced otosurgeon. Considering that HP is also possible using a deeply inserted long electrode array, and that most patients have progressive hearing loss, the use of a longer, flexible electrode seems to be a better choice.

REFERENCES

- Gantz BJ, Turner C, Gfeller KE, Lowder MW. Preservation of hearing in cochlear implant surgery: advantages of combined electrical and acoustical speech processing. *Laryngoscope* 2005;115:796–802.
- Gifford RH, Davis TJ, Sunderhaus LW, et al. Combined electric and acoustic stimulation with hearing preservation: effect of cochlear implant low-frequency cutoff on speech understanding and perceived listening difficulty. *Ear Hear* 2017;38:539–53.
- Jolly C, Garnham C, Mirzadeh H, et al. Electrode features for hearing preservation and drug delivery strategies. *Adv Otorhinolaryngol* 2010;67:28–42.
- Mady LJ, Sukato DC, Fruit J, et al. Hearing preservation: does electrode choice matter? *Otolaryngol Head Neck Surg* 2017;157:837–47.
- Fabie JE, Keller RG, Hatch JL, et al. Evaluation of outcome variability associated with lateral wall, mid-scalar, and perimodiolar electrode arrays when controlling for preoperative patient characteristics. *Otol Neurotol* 2018;39:1122–8.
- O'Connell BP, Hunter JB, Wanna GB. The importance of electrode location in cochlear implantation. *Laryngoscope Investig Otolar*yngol 2016;1:169–74.
- Büchner A, Illg A, Majdani O, Lenarz T. Investigation of the effect of cochlear implant electrode length on speech comprehension in quiet and noise compared with the results with users of electroacoustic-stimulation, a retrospective analysis. *PLoS One* 2017;12: e0174900.
- Suhling M-C, Majdani O, Salcher R, et al. The impact of electrode array length on hearing preservation in cochlear implantation. *Otol Neurotol* 2016;37:1006–15.

- Bruce IA, Felton M, Lockley M, et al. Hearing preservation cochlear implantation in adolescents. *Otol Neurotol* 2014;35:1552–9.
- Buchman CA, Dillon MT, King ER, Adunka MC, Adunka OF, Pillsbury HC. Influence of cochlear implant insertion depth on performance: a prospective randomized trial. *Otol Neurotol* 2014;35:1773–9.
- Adunka OF, Gantz BJ, Dunn C, Gurgel RK, Buchman CA. Minimum reporting standards for adult cochlear implantation. *Otolar*yngol Head Neck Surg 2018;159:215–9.
- Skarzynski H, Lorens A, Skarżyński PH. Electro-Natural Stimulation (ENS) in partial deafness treatment: a case study. *J Hear Sci* 2015;4:CS67–71.
- Skarzynski H, Lorens A, Piotrowska A, Skarzynski PH. Hearing preservation in partial deafness treatment. *Med Sci Monit* 2010;16:CR555–62.
- Skarzynski H, Matusiak M, Piotrowska A, Skarzynski PH. Surgical techniques in partial deafness treatment. J Hear Sci 2012;2:9–13.
- Skarżyńska MB, Skarżyński PH, Król B, et al. Preservation of hearing following cochlear implantation using different steroid therapy regimens: a prospective clinical study. *Med Sci Monit* 2018;24:2437–45.
- Skarzynski H, van de Heyning P, Agrawal S, et al. Towards a consensus on a hearing preservation classification system. *Acta Otolaryngol Suppl* 2013;3–13.
- Towards a consensus HEARRING. HEARRING. Available at: https://www.hearring.com/news-posts/towards-consensus/. Accessed November 30, 2018.
- Risi F. Considerations and rationale for cochlear implant electrode design - past, present and future. J Int Adv Otol 2018;14:382–91.
- Wanna GB, Noble JH, Carlson ML, et al. Impact of electrode design and surgical approach on scalar location and cochlear implant outcomes. *Laryngoscope* 2014;124 (suppl):S1–7.
- Mahmoud AF, Massa ST, Douberly SL, Montes ML, Ruckenstein MJ. Safety, efficacy, and hearing preservation using an integrated electro-acoustic stimulation hearing system. *Otol Neurotol* 2014;35:1421–5.
- Derinsu U, Serin GM, Akdaş F, Batman Ç. Cochlear implantation: is hearing preservation necessary in severe to profound hearing loss? J Craniofac Surg 2011;22:520–2.
- Bruce IA, Bates JE, Melling C, Mawman D, Green KM. Hearing preservation via a cochleostomy approach and deep insertion of a standard length cochlear implant electrode. *Otol Neurotol* 2011;32:1444–7.
- Snels C, IntHout J, Mylanus E, Huinck W, Dhooge I. Hearing preservation in cochlear implant surgery: a meta-analysis. *Otol Neurotol* 2019;40:145–53.
- Skarzynski H, Matusiak M, Furmanek M, et al. Radiologic measurement of cochlea and hearing preservation rate using slim straight electrode (CI422) and round window approach. *Acta Otorhinolaryngol Ital* 2018;38:468–75.
- Causon A, Verschuur C, Newman TA. A Retrospective analysis of the contribution of reported factors in cochlear implantation on hearing preservation outcomes. *Otol Neurotol* 2015;36: 1137–45.
- Usami SI, Moteki H, Tsukada K, et al. Hearing preservation and clinical outcome of 32 consecutive electric acoustic stimulation (EAS) surgeries. *Acta Otolaryngol (Stockh)* 2014;134:717–27.
- Fraysse B, Macías AR, Sterkers O, et al. Residual hearing conservation and electroacoustic stimulation with the nucleus 24 contour advance cochlear implant. *Otol Neurotol* 2006;27:624–33.