# **RESEARCH ARTICLE**

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# Ion-pair compounds of diacerein for enhancing skin permeability *in vitro*: the compatibility-permeability relationship of counter ion and diacerein

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#### ABSTRACT

This research aimed to investigate how the relationship between counter ion and diacerein (DCN) exerts an effect on the skin penetration of DCN ion-pair compounds. After the ion-pair compounds were formed by DCN and organic amines with different functional groups, the hydrogen bond of these compounds was confirmed by Fourier-transform infrared (FTIR) spectroscopy and molecular docking. The skin of porcine ears was employed to conduct the *in vitro* skin penetration, DCN – trie-thanolamine was the most potential candidate with the  $Q_{24h}$  of  $7.89\pm0.38 \ \mu g/cm^2$  among organic amines with different functional groups. Whereas among the homologous fatty amine, the most permeable compound was DCN – lauryl amine with the  $Q_{24h}$  of  $11.28\pm0.48 \ \mu g/cm^2$ . Molecular simulation was employed to explore the relationship between counter ion and DCN. It was revealed by the bind energy curve that DCN had the strongest compatibility with triethanolamine among organic amines and laurylamine (N<sub>12</sub>) among fatty amines. It was amazingly found that the *in vitro* permeation fluxes of DCN ion-pair compounds would increase with enhancing the compatibility of counter ion and DCN. These findings broadened our understanding of how the relationship between drug and counter ion affects the skin penetration of ion-pair compounds.

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#### **KEYWORDS**

Diacerein; ion-pair; transdermal; molecular simulation

# 1. Introduction

Diacerein (DCN, Figure 1), a prodrug of rhein, is one of the few drugs that can effectively defer the inflammatory progression of osteoarthritis in the market (Kitadai et al. 2006; Dhaneshwar et al. 2013). It can selectively inhibit the activity of interleukin-1 $\beta$  (IL-1 $\beta$ ) (Mahajan et al., 2006), reduce the expression of matrix metalloproteinases (Domagala et al., 2006) and repair cartilages by stimulating the expression of transforming growth factor  $\beta_1$  (TGF- $\beta_1$ ) and  $\beta_2$  (TGF- $\beta_2$ ) in arthral chondrocytes (Felisaz et al., 1999). Unfortunately, oral administration of DCN has low bioavailability (Walke et al., 2011; Rehman et al., 2015) and gastrointestinal adverse effects (Spencer & Wilde, 1997).

Drugs topically administrated on the skin of joints could be effectively distributed to the subjacent articular cavity of the applied site, which had excellent curative effects on osteoarthritis (Higaki et al., 2005; Shinkai et al., 2008; Tang et al., 2014; Wu et al., 2017). However, the skin is an effective barrier that prevents drugs from entering the body. It is generally accepted that the skin is mainly made up of the lipophilic stratum corneum (SC) and the aqueous viable skin including epidermis and dermis (Delgado-Charro & Guy, 2014). Therefore, it is helpful for drugs having the appropriate solubility to overcome the barrier of skin. Unfortunately, DCN has poor solubility both in water and non-polar solvent. In order to enhance the flux of skin penetration, niosomes (El-Say et al., 2016), bilosomes (Aziz et al., 2018a), elastosomes (Aziz et al., 2018b), and nanoemulsion (Chattopadhyay & Datta, 2018) had been developed for DCN in recent years. But these pharmaceutical methods had some shortcomings, such as instability and complicated preparation process (Table 1).

Without change of drug pharmacologic actions, ion-pair strategy is usually employed to enhance the skin penetration, which can form the hydrogen bond between drug and counter ions (Ogiso & Shintani 1990; Xi et al., 2012a). The skin permeability of the ion-pair compound would be obviously influenced by some factors, such as physicochemical properties (Song et al., 2012, 2016), stability (Xi et al., 2012b), ionizability in viable epidermis (Zhao et al., 2017), and polar surface area (Cui et al., 2015). Although the influence of ion-pair compounds on skin penetration had been summarized in previous reports, it still deserved to investigate the influence of the relationship between drug and counter ion on the skin penetration of ion-pair compounds.

This research aimed to how the relationship between counter ion and DCN exerts an effect on the skin penetration of DCN ion-pair compounds. First, the organic amines with

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Figure 1. The FTIR spectra of (a) organic amine; (b) DCN and its ion-pair compounds.

different functional groups were selected to form ion-pair compounds with DCN, and the hydrogen bond of these compounds was confirmed by FTIR and molecular simulation. Subsequently, the *in vitro* skin permeation experiments of these compounds were investigated. In order to avoid different functional groups of ion-pair compounds influencing on skin permeability, a series of homologous fatty amines were

Table 1. The chemical structure of DCN and counter ion.



also selected to form ion-pair compounds with DCN, and then the *in vitro* permeation experiments of these compounds with the same functional groups were also conducted. Finally, the relationship of DCN and counter ion was further explored by blends module in the Material Studio 8.0 software (Accelrys, San Diego, CA).

# 2. Materials and methods

# 2.1. Materials

Diacerein was obtained from Xi'an Tianfeng Biotechnology Co., Ltd. (Xi'an, China). Aminoethane (ea), diethyl amine (Dea), triethyl amine (Tea), aminoethyl alcohol (eta), diethanol amine (Deta), triethanol amine (Teta), and isopropyl myristate (IPM) were purchased from Chemical Reagent Co., Ltd. (Shanghai, China). Aminohexane (N<sub>6</sub>), n-octyl amine (N<sub>8</sub>), decyl amine (N<sub>10</sub>), lauryl amine (N<sub>12</sub>), tetradecyl amine (N<sub>14</sub>), cetyl amine (N<sub>16</sub>), and n-octadecyl amine (N<sub>18</sub>) were supplied by Shanghai McLaren Biochemical Technology Co., Ltd. (Shanghai, China). HPLC grade acetonitrile was provided by Tianjin Comio Chemical Reagent Co., Ltd. (Tianjin, China). All other chemicals were of analytical grade.

# 2.2. Preparation of DCN ion-pair complexes

DCN and equimolar of organic amines were dissolved in acetone, and then mixed by magnetic stirrer bars for 24 h at room temperature. Subsequently, the mixture was filtered and washed with anhydrous ethanol to remove excess organic amines. Finally, the obtained DCN ion-pair compounds were dried by vacuum drying.

# 2.3. FTIR spectroscopy studies

An appropriate amount of DCN and its ion-pair complexes were mixed with KBr. After that the mixtures were ground, dried and then pressed as tablets. An appropriate amount of amine was directly painted on the infrared window slice of potassium bromide (Tianjin Tianpu Instrument, Tianjin, China). The FTIR spectra was recorded on a Nicolet 6700 spectrometer (Thermo Fisher Scientific, Waltham, MA) with the scanning range of 4000–400 cm<sup>-1</sup> and a resolution of 4 cm<sup>-1</sup>.

# 2.4. DSC experiments

SDT Q600 instrument (TA Instruments, New Castle, DE) was used to characterize the melting point of DCN and its ionpair complexes. About 4 mg of drugs were placed in a standard aluminum crucible with a heating range of 25–350 °C and a heating rate of  $10 \,^{\circ}\text{C}\cdot\text{min}^{-1}$ . All samples were tested under the protection of 50 mL·min<sup>-1</sup> of nitrogen flow.

#### 2.5. Solubility experiments

The excess DCN and its ion-pair complexes were separately added to 2.0 mL solvent in a sealed polypropylene microvials. The obtained complexes were vibrated by ultrasonic for 10 min then continuously shaken in a water bath at 32 °C until equilibrium. At predetermined time interval 48 h, 0.3 mL sample was withdrawn, the samples were determined by HPLC after being filtered through the membrane of 0.45  $\mu$ m and diluted if necessary.

#### 2.6. Apparent distribution coefficient studies

The classic shake-flask method was used to determine the apparent distribution coefficient (Log *P*). DCN and its ion-pair complexes were added into n-octanol, then mixed with equal volume distilled water. The samples were shaken for 48 h at  $32^{\circ}$ C and centrifuged at 10,000 rpm for 10 min. After phase separation, the concentrations of each drug in both water and n-octanol layer were analyzed by HPLC.

#### 2.7. In vitro permeation experiments

According to the description in our previous report (Xu et al., 2011), the porcine ears immediately obtained from the killed pig were supplied by local slaughterhouse (Xiangtan, China). The hair of porcine ears was carefully cut off with animal hair clippers. Then, skin grafting knife (Medical Equipment

Factory of Shanghai Medical Instruments Co., Ltd., Shanghai, China) was employed to separate the skin and subcutaneous fat, and the skin of thickness in range of  $0.6 \pm 0.1$  mm was obtained. The skin was kept frozen at -20 °C no more than 2 weeks.

Two-chamber Franz diffusion cells (receiver volume of 6.5 mL, effective diffusion area of 2.8 cm<sup>2</sup>) were used for the in vitro transdermal experiments. The prepared skin was placed between the cell halves with the SC facing the donor cell. The receptor compartment was filled with phosphate buffered saline (pH 7.4), which was put in a water bath at  $32 \pm 0.5$  °C and stirred with a magnetic bar at 300 rpm. The saturated solution of DCN and its ion-pair compounds in isopropyl myristate was filled in the donor cell, and a glass sheet was employed to cover the supply chamber during the in vitro permeation experiments. Since the experiment started, 1.0 mL sample was withdrawn from the receptor compartment at predetermined time interval 2, 4, 6, 8, 10, 12, 14, and 24 h. Subsequently, the equal volume of fresh PBS was replenished. These investigations were performed with different individual skin at least in triplicate.

# 2.8. HPLC analysis

The samples were determined by an LC-20A HPLC system (SHIMADZU, Kyoto, Japan). The separation was achieved on an InertSustain C18 column (4.6 mm  $\times$  250 mm, 5  $\mu$ m, SHIMADZU, Kyoto, Japan) with the flow rate keeping at 1.0 mL/min, the column temperature maintaining at 40 °C and mobile phase consisting of methanol:water (25:75, v/v) with 0.4% phosphoric acid in water. Injection volume for each run was 50  $\mu$ L, and detection wavelength was 254 nm.

#### 2.9. Molecular simulation

At first smart algorithm (cascade of steepest descent, quasi-Newton methods, and conjugate gradient) was employed to obtain the optimal geometry of Str ion-pair compound and the organic amine. Molecular docking was performed in blends module using Materials Studio Version 8.0 (Accelrys, San Diego, CA), and COMPASS force field was conducted throughout the whole simulation processes (Cui et al., 2015; Zhao et al., 2017).

Binding energy curves of two components in blends simulation is an effective tool to distinguish their compatibility (Wang et al., 2016). The role property of the components can be distinguished in evaluating binding energies: one component acts as a base role ( $E_{\rm bb}$ ) and the other serve as a screen role ( $E_{\rm ss}$ ). In order to investigate the compatibility of Str and its ion-pair compounds with skin, molecular simulation was carried out in blends module of Materials Studio Version 7.0 (Accelrys Inc., San Diego, CA), and COMPASS force field was performed throughout the whole simulation processes.



Figure 2. Minimum energy of DCN ion-pair compounds forming with A (a) EA, (b) DEA, (c) TEA, (d) ETA, (e) DETA, and (f) TETA.

# 3. Results

# 3.1. FTIR spectra

FTIR spectroscopy could offer the evidence of the proton transfer from the carboxylic acid of DCN to the amine. The FTIR spectra of DCN and its ion-pair complexes are shown in Figure 2. The stretching vibration of the N-H group was among  $3500-3200 \text{ cm}^{-1}$  (Silverstein et al., 2014). After DCN formed ion-pair compounds with organic amine, a new conbroad absorption peak tinuous appeared among  $3300-2000 \text{ cm}^{-1}$ . DCN has the strong narrow peak at 1693.44 cm<sup>-1</sup>, which belongs to the C=O of the carboxyl group (Arunan et al., 2011). But this strong narrow peak of DCN ion-pair compounds had red shift.

# 3.2. The physicochemical properties of DCN ion-pair compounds with organic amines

The physicochemical properties of DCN ion-pair compounds including melt point, solubility and Log *P* value are presented in Table 2. After the DCN ion-pair compounds were formed by DCN and six organic amines, the melt point decreased obviously. The Log *P* value of the DCN was 1.50, while the Log *P* value of those DCN ion-pair compounds decreased to -0.4 to -0.1. The solubility of DCN in water was no more than 10 µg/mL; however, the solubility of DCN

ion-pair compound in water increased to more than 3000  $\mu$ g/mL. These indicated that the polarity of DCN ionpair compounds increased significantly. Isopropyl palmitate is a lipophilic solvent with low dielectric constant ( $\varepsilon_r$ =3.18), which is frequently used as a vehicle solution in transdermal research of ion-pair compounds (Xi et al., 2012a,b; Cui et al., 2015). Thus, isopropyl myristate was selected as the donor solution in this experiment.

# 3.3. The skin permeation of DCN ion-pair compounds with organic amines

After the ion-pair compounds were formed by DCN and organic amines with different groups, the *in vitro* penetration experiments of DCN and these compounds were conducted. As shown in Table 3, the transdermal permeation rate of DCN ion-pair compounds was significantly higher than that of DCN, and the  $Q_{24h}$  of DCN ion-pair compounds with alkanolamine was higher than those compounds with alkylamines. Among six DCN ion-pair compounds, DCN-Teta has the highest transdermal permeation rate. The different skin permeability of DCN ion-pair compounds with organic amines was perhaps caused by the hydrogen-bonding potential of the intercellular lipid and ion-pair compounds because of the counter ion with different types and numbers of organic amine (Cui et al., 2015).

Table 2. Physicochemical properties of DCN and DCN ion-pair compounds.

	Melt point (°C)	Log P	Equilibrium solubility (µg/mL)		
			IPM	PBS (pH 7.4)	Water
DCN	260.84	$1.50 \pm 0.01$	83.59 ± 18.05	1441.87 ± 5.58	$8.29 \pm 0.27$
DCN-ea	243.05	$-0.39 \pm 0.007$	$92.80 \pm 14.10$	12155.69 ± 81.21	$6928.52 \pm 4.80$
DCN-Dea	176.57	$-0.32 \pm 0.007$	$410.37 \pm 20.56$	18473.86 ± 91.09	5453.36 ± 27.84
DCN-Tea	172.47	$-0.27 \pm 0.006$	1385.02 ± 13.68	8187.55 ± 44.36	3232.52 ± 12.61
DCN-eta	148.83	$-0.25 \pm 0.005$	121.56 ± 1.20	6099.91 ± 24.71	3059.63 ± 35.77
DCN-Deta	149.10	$-0.22 \pm 0.006$	115.89 ± 16.60	$11105.50 \pm 18.51$	3998.30 ± 12.50
DCN-Teta	153.92	$-0.13 \pm 0.005$	99.38 ± 12.80	$2514.24 \pm 10.27$	$6374.94 \pm 14.60$

Table 3. Skin permeation data of DCN and its ion-pair compounds with different groups.

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Samples	$Q_{24h}^{a}$ (µg/cm <sup>2</sup> )	$J_{ss}^{b}$ (µg/cm <sup>2</sup> ·h <sup>-1</sup> )	T <sub>lag</sub> <sup>c</sup> (h)			
DCN	$1.83 \pm 0.22$	0.06 ± 0.01	$2.68 \pm 0.78$			
DCN-ea	$2.17 \pm 0.30$	$0.08 \pm 0.02$	$1.79 \pm 0.66$			
DCN-Dea	$2.82 \pm 0.49$	$0.10 \pm 0.01$	$4.12 \pm 1.14$			
DCN-Tea	$2.85 \pm 0.64$	$0.11 \pm 0.04$	$3.39 \pm 0.55$			
DCN-eta	$3.04 \pm 0.67$	$0.09 \pm 0.04$	$1.41 \pm 0.56$			
DCN-Deta	$4.03 \pm 0.71$	$0.11 \pm 0.02$	$2.16 \pm 0.55$			
DCN-Teta	$7.89\pm0.38$	$0.17\pm0.05$	$1.52 \pm 0.48$			

 ${}^{a}Q_{24h}$ , the cumulative amount of drug permeated per unit area at 24 h.

 $b^{J_{sin}}_{J_{ssr}}$  the steady-state flux obtained from the slope of the linear portion of the plots.

 ${}^c\!T_{\rm lagr}$  the extrapolated value of the linear portion of the permeation curve to the abscissa.

Table 4. Skin permeation data of DCN and its ion-pair compounds with fatty amines.

Samples	$Q_{24h}^{a}$ (µg/cm <sup>2</sup> )	$J_{ss}^{b}$ (µg/cm <sup>2</sup> ·h <sup>-1</sup> )	$T_{\text{lag}}^{c}$ (h)
DCN	$1.83 \pm 0.22$	$0.06 \pm 0.01$	$2.68 \pm 0.78$
DCN-N <sub>6</sub>	$3.86 \pm 0.21$	$0.10 \pm 0.02$	$1.52 \pm 0.36$
DCN-N <sub>8</sub>	$4.30 \pm 0.63$	$0.14 \pm 0.03$	$2.15 \pm 0.22$
DCN-N <sub>10</sub>	$6.41 \pm 0.23$	$0.20 \pm 0.03$	$1.38 \pm 0.14$
DCN-N <sub>12</sub>	$11.28 \pm 0.48$	$0.34 \pm 0.02$	$2.50 \pm 0.18$
DCN-N <sub>14</sub>	$7.03 \pm 1.56$	$0.24 \pm 0.05$	$1.31 \pm 0.11$
DCN-N <sub>16</sub>	$6.44 \pm 0.36$	$0.22 \pm 0.01$	$1.28 \pm 0.23$
DCN-N <sub>18</sub>	5.97 ± 1.25	$0.20\pm0.01$	$1.42 \pm 0.52$

 ${}^{a}Q_{24h}$ , the cumulative amount of drug permeated per unit area at 24 h.

 $b^{J_{cont}}_{J_{ss}}$  the steady-state flux obtained from the slope of the linear portion of the plots.

 ${}^c\!T_{\text{lag}\prime}$  the extrapolated value of the linear portion of the permeation curve to the abscissa.

# 3.4. The skin permeation of DCN ion-pair compounds with fatty amines

In order to avoid different functional groups introducing to DCN ion-pair compounds, a series of homologous fatty amines were selected to form ion-pair compounds with DCN. The results of the *in vitro* transdermal penetration for DCN and those results are presented in Table 4. As the number of carbon atoms increased, the transdermal permeation rate of DCN ion-pair compounds would increase slowly, then decrease gradually, and attain the peak value at 12 carbon atoms. It was also found that the  $Q_{24h}$  of DCN-N<sub>12</sub> was higher than that of DCN-Teta.

# 3.5. Molecular simulation

The optimal geometry of DCN and counter ions was obtained by smart algorithm. Then molecular docking was employed to confirm the hydrogen bond of DCN ion-pair compounds. As shown in Figure 3, the hydrogen bond of DCN ion-pair compounds was formed between DCN and all counter ions. In detail, the formation of the hydrogen bond was the proton transfer from the deprotonated acids anion ( $RCOO^{-}$ ) of DCN to the protonated cation (<sup>+</sup>HNR) of counter ions.

Usually, the compatibility of two components can be judged by their binding energy curves: one component acts as a base role  $(E_{\rm bb})$  and the other component serves as a screen role ( $E_{ss}$ ). In the progress of molecular simulation, DCN and counter ions are set to a base role ( $E_{\rm bb}$ , red line) and a screen role (Ess, other colors line), respectively. The binding energy curves of the two substances were relatively similar, the compatibility of the two substances was better (Wang et al., 2016). Among organic amines with different functional groups, the binding energy curve of triethanolamine was most similar to that of DCN, as shown in Figure 3(a). Thus it could be concluded that triethanolamine had the best compatibility with DCN. As shown in Figure 3(b), it could also be concluded that laurylamine (N12) had the best compatibility with DCN among selected fatty amine. As shown in Figure 3(c), it was also found that binding energy distribution curves of laurylamine and DCN was more similar, which indicated that laurylamine  $(N_{12})$  had stronger compatibility with DCN than triethanolamine.

# 4. Discussion

Ion-pair compounds have a special type of hydrogen bond with a proton transferring between drug and counter ion (Xi et al., 2012a,b). Organic amines could offer a pair lone electron, and the proton would be provided by the carboxyl group of DCN. The DCN ion-pair compound of the C=O on carboxyl group had a red shift. For that reason, it was concluded that the hydrogen bond was formed at the carboxyl position of DCN. A continuous broad absorption peak appeared among  $3300-2000 \text{ cm}^{-1}$ , which was attributed to the tunneling effect of intermolecular hydrogen bonds during the transfer of protons. The hydrogen bond of DCN ionpair compounds at the carboxyl position of DCN was further confirmed by molecular docking.

The Log P value of ion-pair compounds is a pivotal factor that influences the skin permeation fluxes (Song et al., 2016; Zhao et al., 2017). However, the Log P could not always reflect the results of permeation fluxes. After DCN formed the ion-pair compounds with organic amines possessing different functional groups, the Log P value of these compounds decreased obviously. The correlation between skin permeability fluxes of DCN compounds and Log P was



Figure 3. The binding energy distributions curves of DCN and (a) organic amines with different functional groups; (b) fatty amines; (c) triethanolamine and lauryl amine.

consistent with some literature reports (Song et al., 2012; Xi et al., 2012b). However, as for some drugs with appropriate Log P value, the skin permeability fluxes of the ion-pair compounds had negative relationship with their Log P value (Song et al., 2012, 2016).

The penetrant diffusion coefficient of SC would be obviously affected by the hydrogen bond of the intercellular lipids and penetrant (Hadgraft, 2001). The intercellular lipids is the main barrier of skin, which have many donors and receptors of hydrogen bond (Hadgraft, 2001; Gary et al., 2012). It was reported that the counter ions with lower hydrogenbonding potential tended to achieve the better effect of skin permeability (Cui et al., 2015). The skin permeability of DCN and organic amine ion-pair compounds maybe affected by the different hydrogen bond of the intercellular lipids and the ion-pair compounds due to the counter ion with different types and numbers of organic amine. As for the ion-pair compounds of DCN and fatty amines, their skin permeability should not be influenced by the different hydrogen bond of the intercellular lipids and their ion-pair compounds. However, the transdermal permeation rate of these compounds increased slowly, then decreased gradually with the carbon atoms of counter ion increasing.

The properties of ion pairs are affected not only by the properties of drugs, but also by the properties of counter ions. It is worth exploring how the relationship between counter ion and DCN effect on the skin penetration of DCN ion-pair compounds. It was found by the bind energy curve that DCN had the strongest compatibility with triethanolamine among organic amines with different functional groups and laurylamine (N<sub>12</sub>) among fatty amines. Laurylamine had stronger compatibility of with DCN than triethanolamine. Among organic amines with different functional groups, DCN-Teta was the most potential candidate. The transdermal permeation rate of DCN-fatty acid compounds would increase slowly with the carbon atoms of counter ion increasing, attain the peak at 12, then decreased gradually. The skin permeation rate of DCN-N<sub>12</sub> was higher than that of DCN-Teta. It was amazingly found that the in vitro permeation fluxes of DCN ion-pair compounds would increase with enhancing the compatibility of counter ion and DCN.

lon-pair compounds pass through SC more easily than individual ions because the central ion and an oppositely charged ion behave as a single-unit behavior via the electrostatic interactions (McNaught & Wilkinson, 1997; Cavallari et al., 1998; Fini et al., 1999; Cristofoli et al., 2021). However, these electrostatic interactions of the hydrogen bond are very weak, the hydrogen bond of ion-pair compounds breaks and forms on an extremely short timescale (Song et al., 2016). It was reported that the longer the ion-pair lifetime, the higher the skin permeation flux (Xi et al., 2012b). Perhaps the life time of DCN ion-pair compounds would be extended because the electrostatic interaction of counter ion and DCN would increase with their compatibility enhancing (Song et al., 2016; Cristofoli et al., 2021).

# 5. Conclusions

The hydrogen bond of DCN ion-pair compounds formed at the carboxyl position of DCN, and the skin permeation fluxes of DCN ion-pair compounds would increase with the enhancement of the compatibility of counter ions and DCN. These findings broadened our knowledge of how the relationship of drug and counter ion affects percutaneous penetration of ion-pair compounds.

# **Disclosure statement**

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