How to design an optimal sensor network for the unfolded protein response

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ABSTRACT Cellular protein homeostasis requires continuous monitoring of stress in the endoplasmic reticulum (ER). Stress-detection networks control protein homeostasis by mitigating the deleterious effects of protein accumulation, such as aggregation and misfolding, with precise modulation of chaperone production. Here, we develop a coarse model of the unfolded protein response in yeast and use multi-objective optimization to determine which sensing and activation strategies optimally balance the trade-off between unfolded protein accumulation and chaperone production. By comparing a stress-sensing mechanism that responds directly to the level of unfolded protein in the ER to a mechanism that is negatively regulated by unbound chaperones, we show that chaperone-mediated sensors are more efficient than sensors that detect unfolded proteins directly. This results from the chaperonemediated sensor having separate thresholds for activation and deactivation. Finally, we demonstrate that a sensor responsive to both unfolded protein and unbound chaperone does not further optimize homeostatic control. Our results suggest a strategy for designing stress sensors and may explain why BiP-mitigated ER stress-sensing networks have evolved.

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INTRODUCTION

The unfolded protein response (UPR) is a multifaceted cellular response to excess unfolded or misfolded proteins within the endoplasmic reticulum (ER) (Liu *et al.*, 2003; Schröder and Kaufman, 2005), a state referred to as ER stress. For moderate stress levels, the cellular response aims to restore protein homeostasis to the ER by up-regulating quality-control enzymes and chaperones, altering ER size and shape, and attenuating translation (Harding *et al.*, 2002). When these responses fail to mitigate stress, the cell initiates apoptosis. Overloading and malfunction of the UPR are associated with many diseases (Kaufman, 2002; Wang and Kaufman, 2012), including diabetes (Scheuner and Kaufman, 2008; Eizirik

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and Cnop, 2010), cancer (Vandewynckel *et al.*, 2013), and neurodegenerative diseases (Scheper and Hoozemans, 2015; Hetz and Saxena, 2017).

A critical aspect of the UPR is the mechanism through which stress in the ER is detected and transduced to the nucleus. In the mammalian UPR, three transmembrane proteins, Ire1 (inositolrequiring enzyme 1), PERK (protein kinase RNA-like ER kinase), and ATF6 (activating transcription factor 6) direct the response through three different pathways (Ron and Walter, 2007; Gardner et al., 2013). Ire1 up-regulates ER-localized chaperones, including the most prevalent ER protein BiP (Kar2 in yeast), and proteins involved in membrane remolding and ER-associated degradation by promoting the splicing of X-box binding protein 1 (XBP-1, Hac1 in yeast), a potent transcription factor. PERK phosphorylates the translation initiation factor eIF2 α , which leads to an overall reduction in mRNA translation, and up-regulates the transcription factor ATF4, which promotes downstream UPR genes, including Chop, a transcription factor gene controlling apoptosis. While both Ire1 and PERK signal through similar mechanisms based on the activation of kinase domains in the cytoplasmic regions, ATF6 signaling is initiated by transport of ATF6 to the Golgi, where it is processed by site-1 and site-2 proteases. The processed amino terminus then diffuses to the nucleus, where it in regulates several UPR target genes, many of which overlap with those controlled by XBP-1. While mammalian

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Abbreviations used: ATF6, activating transcription factor 6; ER, endoplasmic reticulum; Ire1, inositol-requiring enzyme 1; PERK, protein kinase RNA-like ER kinase; UPR, unfolded protein response.

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FIGURE 1: UPR model schematic. (A) Schematic overview of the UPR model. Protein production in the ER lumen is modeled as a chaperone-assisted folding process that returns unfolded proteins to the folding pathway (*F*), which are removed from the system. The basal flux of unfolded proteins into the ER, V_U , is augmented in the case of stress by an additional V_UD flux. The pulsatile stress (top, right box) lasts for duration t_p . Upon increased accumulation of unfolded protein in the ER, the UPR (top, left box) is activated, up-regulating the influx of chaperone into the ER to mitigate the increased folding load. Specific stress-sensing models are shown in B–D. (B) UPR activation model that responds directly to the concentration of unfolded protein in the ER lumen in a piecewise-linear manner with slope proportional to *m*, and activation threshold u_{min} . (C) Chaperone-mediated sensor model that is activated when the concentration of free chaperone decreases below a threshold value $c_{F,max}$. (D) The logic circuit for the AND-switch, which combines the unfolded protein sensor and the free-chaperone sensor.

cells have three interacting signaling pathways associated with the UPR, yeast possesses only the Ire1 pathway (Ron and Walter, 2007; Gardner *et al.*, 2013).

As the downstream responses of the various pathways have become clearer, significant questions regarding the sensory mechanisms of Ire1, PERK, and ATF6 within the ER lumen have been raised. For Ire1 and PERK, early evidence suggested that the chaperone BiP might negatively regulate the activation of the sensory molecules (Kimata et al., 2003). However, a mechanism involving only BiP was shown to be insufficient, because the UPR is inducible in cells with modified Ire1 and PERK that are incapable of binding BiP (Kimata et al., 2004). This led to the hypothesis that the activation of sensory proteins by unfolded protein ligands is buffered by BiP (Kimata et al., 2004, 2007; Pincus et al., 2010). Further support for this hypothesis comes from structural similarities between Ire1 luminal domain dimers and major histocompatibility complexes, which both show a favorable groove for direct peptide binding (Credle et al., 2005). Additional studies have provided evidence of unfolded protein interaction with Ire1 and PERK in yeast (Gardner and Walter, 2011), and more recently with human Ire1 (Karagöz et al., 2017). Other evidence suggests that BiP binding to Ire1 and PERK may be allosterically regulated by unfolded proteins (Carrara et al., 2015), providing an alternative mechanism of activation. Because evidence suggests that Ire1 and PERK bind a set of proteins that overlap with, but are distinct from, those bound by BiP (Karagöz et al., 2017), it seems possible that both of these mechanism are realized in vivo.

While the molecular details of the activation mechanism have yet to be fully resolved, one fact is clear: stress sensing is quite complex. Our aim in this work is to better understand why such a complex system might be beneficial for stress detection, and thereby provide MODEL Model description

To model the UPR (Figure 1), we develop a course model in which we consider only two species explicitly: free unfolded client proteins, U, and the total number of a generic chaperone present in the ER, C_{τ} . Descriptions of the UPR at a similar level of detail have been previously used to investigate the benefits of translational regulation (Axelsen and Sneppen, 2004; Trusina et al., 2008). C_{T} encompasses both free chaperone, C_F , and chaperone forming a folding complex with client proteins, $C \cdot U$, such that $C_T = C_F + C \cdot U$. The unfolded proteins represent those proteins in the ER with a significant number of exposed hydrophobic residues, and hence are highly active and aggregation prone. The chaperones mediate this activity by restoring the proteins to the folding pathway. Proteins returned to this pathway are assumed to fold without incident and are secreted from the ER. The governing-delay differential equations for the reactive unfolded protein and total chaperone levels are

$$\dot{U} = V_U - \frac{k_{\text{cat}}C_T U}{K_{UC} + U} + V_U D \left[1 - H(t - t_p) \right] - k_D U \tag{1}$$

$$\dot{C}_{T} = V_{C} \left(1 + G_{X,\tau} \right) - k_{D} C_{T}$$
⁽²⁾

In Eq. 1, the first term, V_U , represents the basal flux of unfolded proteins into the ER. The second term, $(k_{cat}C_TU)/(K_{UC}+U)$, describes the catalytic activity of the chaperone on the protein. The third term $V_UD[1-H(t-t_p)]$ represents a state of stress, which we model as a square pulse of increased flux starting at t = 0, where the pulse height is D times the basal flux, H is the Heaviside

How do phenotypic features of a sensory network affect the trade-off between accumulation of unfolded proteins and metabolically efficient chaperone production in response to stress? We start from the naïve perspective that the simplest way to detect stress would be to directly count the number of unfolded proteins within the ER. Using a coarse-grained model of the UPR based on direct sensing of unfolded proteins, we determine the optimal shape of response functions for acute and chronic stress conditions. Next, following experimental evidence that chaperones inhibit stress-sensor activation, we determine the optimal response function for acute and chronic stress when sensor activation is negatively regulated by freely available chaperone. Comparing the optimal performance of sensory systems that directly measure unfolded protein concentration with those that respond instead to available chaperone, we show that indirectly measuring stress through free-chaperone concentration leads to a more efficient chaperone use in mitigating stress. Finally, we consider whether further benefits can be obtained by combining both sensing modalities, as is observed experimentally.

insight into the evolutionary forces guiding

stress-sensor design. Specifically, we ask,

Parameter	Value	Units	Source
$k_{\rm cat}$	8.15×10 ⁻⁴	s ⁻¹	Twenty-minute ER residence time (Braakman and Hebert, 2013)
K _{UC}	1.1×10 ⁴	$mol \times V_{ER}^{-1}$	Estimated dissociation constant between BiP and C _{H1} (Carrara <i>et al.</i> , 2015)ª
V _U	200	$mol \times s^{-1}$	In proposed range for protein flux into ER (Vincent <i>et al.,</i> 2014)
V _C	60	$mol \times s^{-1}$	Corresponds with steady-state chaperone level of 3.3×10^5 molecules (Ghaemmaghami et al., 2003) ^b
k _D	1.85×10^{-4}	s ⁻¹	Estimated half-life of chaperone in the ER (Sherman, 2002) ^c
G ₀	5	_	Estimated based on fold-change of <i>Kar2</i> mRNA levels (Kawahara <i>et al.</i> , 1997)
t _{UPR}	9×10 ²	S	Estimated response time of UPR chaperone production (Kawahara <i>et al.</i> , 1997)

^aAssuming ER volume, V_{ER} = 2.15 µm, and that K_{UC} is approximately equal to the dissociation constant of BiP and a client unfolded protein. ^bEstimated copy number of Kar2 (BiP) in *Saccharomyces cerevisiae*.

^cApproximated as the doubling time of yeast.

TABLE 1: Model parameters.

function, and t_p is the pulse duration. The final term, k_DU , captures the decrease in unfolded protein present in the ER due to dilution and degradation, with k_D being the inverse half-life of a protein in the ER. Similarly, in Eq. 2, V_C is the basal influx of chaperone, and the dilution and degradation of chaperone is described by the final term. $G_{X,\tau}$ represents the response function for the feedback response of the UPR. The subscript X denotes the specific model for UPR activation as described in the section *Stress-sensing mechanisms*, and the subscript τ indicates that the response depends on the state of the system at a previous time $t - t_{UPR}$.

A detailed description of the model derivation and assumptions is available in the Supplemental Material. The parameterization of the model is constrained by experimental results from the literature and is presented in Table 1.

To facilitate analysis, we nondimensionalize the model by choosing the degradation time k_D^{-1} to be a characteristic timescale and V_C / k_D to be a characteristic concentration. This leads to a normalized form of the model:

$$\dot{u} = v - \frac{\alpha c_T u}{\beta + u} + v D \Big[1 - H(t - \tau_p) \Big] - u \tag{3}$$

$$\dot{c}_T = 1 + G_{X,\tau} - c_T$$
 (4)

In addition to the normalized times for the pulse duration $\tau_p = t_p k_D$ and UPR response time $\tau_{UPR} = t_{UPR} k_D$, we have introduced three dimensionless parameters:

$$v = V_U / k_D, \qquad \alpha = \frac{k_{cat}}{k_D}, \qquad \beta = \frac{K_{UC}k_D}{V_C}$$
 (5)

where v is the dimensionless influx rate of unfolded protein into the ER, α is the dimensionless catalytic constant for chaperone-assisted folding, and β is the dimensionless K_m for the chaperone–unfolded protein interaction.

Stress-sensing mechanisms

In yeast, the level of stress in the ER is sensed by the transmembrane protein Ire1, which then facilitates the splicing of the transcription factor Hac1. Hac1 up-regulates the transcription of *Kar2*, among other genes, increasing the translation of the ER chaperone Kar2

(BiP). We capture this process through a phenomenological model governing the level of activation of Ire1. Because there is a finite amount of time required for splicing, transcription, and translation, the increased flux of chaperone depends on the level of activity of Ire1 a time τ_{UPR} before. We incorporate this lag time as a time delay on the state variables u and c_T in the response function and denote $def_{u_T} = u(t - \tau_{UPR})$ and $c_{T,\tau} = c_T(t - \tau_{UPR})$. We consider three different response functions, each representing a different stress-sensing mechanism.

Unfolded protein sensor

In the first mechanism, activation is directly related to the concentration of unfolded protein in the ER (Figure 1B). In this case, the activation function, $G_{u,\tau}$, is

$$\frac{G_{u,\tau}}{G_0} = \begin{cases} 0 & \text{for } u_{\tau} \le u_{\min} \\ (u_{\tau} - u_{\min})m & \text{for } u_{\min} < u_{\tau} < u_{\min} + \frac{1}{m} \\ 1 & \text{for } u_{\tau} \ge u_{\min} + \frac{1}{m} \end{cases}$$
(6)

where G_0 the maximal gain, u_{min} is the level of unfolded protein for which the UPR first activates, and *m* is the slope of the response function. The inverse of *m* can be interpreted as the width of the active range of the sensor. The response function resembles common sigmoidal responses found in biology but has the advantage of having the same steady state for any parameterization of the response function so long as the steady state is below the activation threshold. We refer to this mechanism as the "U-switch" mechanism.

Chaperone sensor

The second mechanism we consider is one in which activation of the UPR is inhibited by free chaperones in the ER (Figure 1C). In this case, the activation function, $G_{c,\tau'}$ is

$$\frac{G_{c,\tau}}{G_0} = \begin{cases} 1 & \text{for } c_{F,\tau} \le c_{F,\max} - \frac{1}{m} \\ (c_{F,\max} - c_{F,\tau})m & \text{for } c_{F,\max} - \frac{1}{m} < c_{F,\tau} < c_{F,\max} \\ 0 & \text{for } c_{F,\tau} \ge c_{F,\max} \end{cases}$$
(7)

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where $c_{F,\tau}$ is the concentration of free chaperone at time $t - \tau_{UPR'}$ which is given by

$$c_{F,\tau} = c_{T,\tau} \left(1 - \frac{u_{\tau}}{\beta + u_{\tau}} \right) \tag{8}$$

(see the Supplemental Material for a detailed derivation). $c_{F,\max}$ is the threshold concentration of free chaperone above which there is no activation, and *m* is the slope of the response. We refer to this mechanism as the " C_F -switch" mechanism.

Unfolded protein-AND-chaperone sensor

The final mechanism consists of a combination of the previous two mechanisms such that both the unfolded protein–sensing function and the chaperone-sensing function must be active, that is, *u* concentration must be high and c_F concentrations low, for the UPR to respond (Figure 1D). The activation function for this case, $G_{AND,T'}$ is

$$G_{AND,\tau} = G_{u,\tau}G_{c,\tau} \tag{9}$$

We refer to this mechanism as the "AND-switch" mechanism, as it becomes a logical AND function in the case that the unfolded protein and chaperone sensors become discrete on–off switches.

Fitness measures and Pareto optimization

It is often the case that the fitness of a phenotype is a function of several independent quantities. While the UPR influences cellular fitness in a wide-ranging set of interactions and functions that remain to be fully understood, we choose to focus on two measures of fitness that are central to UPR function: 1) the amount of excess unfolded protein present in the ER while the cell is under stress and 2) the total excess production of chaperone in response to an impulse of stress. The first measures how effectively the UPR is able to mitigate the negative effects of high concentrations of highly reactive protein species (such as aggregation and misfolding) in the ER. The second measures the metabolic cost associated with rapidly reducing stress through chaperone production. When dealing with multiple fitness functions, one option is to choose a weighting for each and use the weighted sum of the individual fitness functions as a scalar measure of overall fitness. However, this often requires an ad hoc choice of weights, making the results somewhat subjective. An alternative approach is to use Pareto optimization, which seeks to determine Pareto-efficient solutions in fitness space. The set of Pareto-efficient solutions, also called the Pareto front, is the set of points in fitness space for which any improvement in one fitness measure can only be achieved by a decline in another fitness measure. Any specific weighting scheme in a scalar weighted-sum fitness measure corresponds to a point on the Pareto front. This technique has been used to probe phenotype space distributions in general (Savir et al., 2010; Shoval et al., 2012) and has been applied to several biological problems in particular, including gene regulatory networks (Warmflash et al., 2012) and homeostatic control (Szekely et al., 2013).

The fitness landscape guiding the evolution of the cellular stress response very likely has many competing factors, such as the response time or noise reduction, in addition to the accumulation of unfolded proteins in the ER lumen and the production of mitigating chaperones. Here, we focus only on the trade-off between unfolded protein concentration and chaperone production, as these are two fundamental features of homeostatic UPR control. We note that this trade-off is only one of many possible guiding principles in stresssensor design. The function measuring the cost of excess unfolded protein accumulation in the ER is given by

$$\mu_U = \frac{1}{u_{ss}T} \int_0^T \max\{u, u_{ss}\} dt$$
(10)

where *T* is the duration of the simulation, max $\{u, u_{ss}\}$ is the maximum between the unfolded protein level and the steady-state unfolded protein concentration at each time, and the prefactor to the integral is a normalization constant. Note that we seek to minimize a cost function. The corresponding fitness function would be the negative of the cost function and is maximized. μ_U measures the time average of the excess unfolded protein in the ER, normalized by the steady-state unfolded protein concentration. The cost function for chaperone production is computed by

$$\mu_C = \frac{1}{T} \int_0^T (1 + G_{X,\tau}) dt \tag{11}$$

 μ_C gives the time average of the chaperone production rate. Together, the measures $\left(\mu_U,\mu_C\right)$ form the two-dimensional fitness space for the UPR.

In the case of the *U*-switch and C_F -switch, the Pareto fronts are computed using a brute-force method by calculating the objective functions over a 100-by-100 grid of logarithmically spaced points in the ranges $m \in [0.1, 1000]$, $u_{\min} \in [0.01u_{ss}, 1000u_{ss}]$, and $c_{F,\max} \in [0.001c_{F,ss}, 0.999c_{F,ss}]$. We found that using a brute-force method provides efficient coverage of the extreme points on the Pareto front. For the AND-switch, in which the number of independent parameters is four as opposed to two, the Pareto front is calculated using the nondominated sorting algorithm II (Deb et al., 2002) as implemented in the Python software platypus (Hadka, 2015).

RESULTS

Any effective stress-sensing network must be sensitive to the concentration of unfolded proteins in the ER lumen. However, the efficiency with which a sensor controls the UPR will depend on the time course of the stress. With this in mind, we consider the response of sensory networks to two types of characteristic stress time courses: 1) a sustained chronic stress, in which the system adjusts to a new steady state at a larger-than-usual protein influx, and 2) acute stresses of varying amplitude and duration, in which the on and off dynamics of the UPR become important. For each stress type, we determine the set of Pareto-optimal sensor designs for the unfolded protein sensor and the free-chaperone sensor and compare their features and efficiency. Finally, we compare the U-switch and C_{r} -switch sensor models individually with the combined ANDswitch model. Results from the response of these three sensing strategies to different stresses provide insights into the potential evolutionary benefits of sensor network design.

Optimal design of a sensor for chronic stress

We initially consider a cell subjected to a sustained pulse of increased unfolded protein translocation rate into the ER. The stimulus, which we call chronic stress, is a step increase of influx rate that continues indefinitely, allowing the system to fully acclimate to the stressed state. For this stress signal, we have computed the Paretooptimal parameterizations of both the unfolded protein–sensing and the free chaperone–sensing mechanisms (Figure 2A). In the case of chronic stress, both objective functions are determined by the new steady state reached by the UPR-activated system. Both mechanisms can reach the same set of steady states, and hence have the same Pareto fronts. Additionally, for each mechanism, the switching function that produces a steady state is not unique. In fact,



FIGURE 2: Pareto front for chronic stress response. (A) The Pareto front (blue stars) for a sustained stress, where the system adapts to an increased stress level. The insets provide representative activation functions for the point on the Pareto front marked by a red triangle for the *U*-switch (top inset) and C_F -switch (bottom inset). (B) The steady-state unfolded protein level as a function of influx rates. The black lines show the steady states of the system when there is no UPR activation (left) and full UPR activation (right). The solid and dashed sections of the lines correspond to stable and unstable fixed points, respectively. The blue lines show the analytically determined fixed points for intermediate activation of the UPR. The shaded regions show the range of oscillations of numerically simulated solutions. The numbers in the top center of each panel correspond to the activation functions shown as insets in A.

many combinations of slope and threshold will lead to the same steady state in response to chronic stress, as shown schematically in Figure 2A (insets). This can be readily seen by considering two-switch parameterization $(u_{\min,1}, m_1)$ and $(u_{\min,2}, \alpha m_1)$, in which the slope of the second response function is related to the slope m_1 through a linear scaling α . In the linear regime of the response, the steady-state chaperone and unfolded protein levels, c_T^* and u^* are related through the equations

$$c_{T}^{*} = m_{1}G_{0}(u^{*} - u_{\min,1}) + 1$$

$$= \alpha m_{1}G_{0}(u^{*} - u_{\min,2}) + 1$$
(12)

which leads to the linear relationship between $u_{\min,1}$ and $u_{\min,2}$ in terms of α

$$u_{\min,2} = u^* \left(1 - \frac{1}{\alpha} \right) + u_{\min,1}$$
 (13)

Hence, infinitely many combinations of (u_{\min}, m) will lead to the same steady state and the same efficiency in dealing with a specific state of chronic stress. The same is true for the chaperone-based sensor.

However, the sensitivity of the response to changes in stress and the damping of oscillations depend on the particular parameterization of the switching function. As the response becomes steeper, Figure 2B shows that the mean level of unfolded protein changes less in response to the increases in influx. However, this comes at the cost of oscillations. Thus, while tighter control over the mean value of protein concentration can be achieved with a more abrupt response, a more graded response allows the system to adjust to a range of different levels of chronic stress without oscillations.

Efficient sensor design for acute stress

In the case of chronic stress, the quality of a response depended on the steady-state behavior of the stressed system. The dynamics of the system were not important, except in regard to oscillations in systems with steep responses. In contrast, for shorter stress events in which a new steady state may not be reached, the dynamics of the UPR are essential in determining the efficiency of the response. To investigate this, we consider the response of the system to stress pulses of different shape. Owing to the nonlinear coupling and delays, analytical solutions are either unavailable or uninformative for the transient pulse response. Hence, we numerically determine the Pareto fronts for each mechanism across a range of pulse shapes. Figure 3, A-E, shows Pareto fronts for a set of pulses in which the total protein influx is conserved (i.e., $D\tau_p = \text{constant}$), and the amplitude and duration of the pulse is modulated. For small-amplitude, long-duration pulses, the unfolded protein-based switch is slightly more efficient when excess unfolded protein accumulation is the primary cost. However, the magnitude of the difference between the two mechanisms is small relative to the difference seen for other pulses. Similarly, for very short pulses of larger amplitude, the two mechanisms are essentially equivalent. However, for intermediate pulse shapes, the chaperone-based switch can be substantially more efficient. To quantify this, we divide the area under the Pareto front of the C_{F} -switch by the area under the U-switch Pareto front

$$\Delta_{P} = \frac{\int \mu_{U}^{C} d\mu_{C}}{\int \mu_{U}^{U} d\mu_{C}} \tag{14}$$

where μ_U^U is μ_U of the unfolded protein–based mechanism and μ_U^C is μ_U of the chaperone-based mechanism and the integrals are computed over the range of the μ_C on the Pareto fronts. When $\Delta_P > 1$, the chaperone-based mechanism provides a more efficient response across parameterizations, while the unfolded protein–based



FIGURE 3: Pareto front for acute pulse. (A–E) The Pareto fronts corresponding to the *U*-switch sensor (blue circles) and the C_F -switch sensor (red squares) for different pulse shapes. The total excess protein in each pulse is 1, with the pulse height and duration changing. (F) The normalized area between the Pareto fronts of each mechanism as a function of pulse amplitude (with total pulse influx conserved). The black dashed line delineates the pulse shapes for which the *U*-switch is superior (left) from those for which the C_F -switch is superior (right).

mechanism is more efficient when $\Delta_P < 1$. We note that the ability of this metric to quantify the degree to which one mechanism is superior to another depends on the Pareto fronts not crossing. Observation of the calculated Pareto fronts indicates that, in the small range where the Pareto fronts do cross, the C_F -switch is superior when the more dominant cost is the mitigation of stress (see Figure 3, A and B). Figure 3F shows Δ_P for the cases $D\tau_p = 1$. There is a large range of intermediate pulses for which the chaperone-based switch is significantly more efficient for any choice of parameterization.

The added efficiency of the C_F -switch can be understood by examining the phase-plane trajectories of each mechanism (Figure 4B). The projection of the unfolded protein sensor threshold into the $c_{\tau} - u$ plane is a horizontal line, while the freechaperone sensor threshold projects onto a line with a positive slope (see the Supplemental Material for derivation). Whereas the horizontal threshold of the unfolded protein sensor threshold means that the UPR will turn on and off at identical levels of stress, the slope of the free-chaperone sensor means that the on and off thresholds are no longer symmetric with regard to stress. This imparts three advantages to the free chaperone-sensing system. First, it allows for earlier activation when a stress arises, thereby reducing the maximum concentration of unfolded protein that occurs during the stress event (shown as a heat map on the Pareto fronts in Figure 4A). Additionally, the gradient of the slope with respect to unfolded protein concentration is maximal at the onset of stress for the C_F -switch, allowing an initially strong response (see heat map in Figure 4C). Finally, the system is able to deactivate the response sooner when the level of stress begins to

subside, thereby preventing the excess production of unneeded chaperone, as seen in the corresponding time courses shown in Figure 4C.

While the cost function μ_U measures the integrated excess protein accumulation with the ER over the time course of the stress, the maximal level of unfolded protein may also be an important physiological measure of fitness. In Figure 4A, the Pareto fronts for each mechanism are colored corresponding to the peak unfolded protein concentrations experienced during the stress pulse. For the same amount of excess chaperone production, the chaperone-based sensor leads to both less integrated excess unfolded protein and lower peak unfolded protein for nearly the entire Pareto front, except where the two mechanisms provide equivalent responses.

Logical AND-switch sensor combining chaperone and unfolded protein concentrations

Experimental evidence supports a model for UPR activation that relies on both the dissociation of BiP from the sensory protein and the binding of an unfolded protein to sensor oligomers (Oikawa et al., 2007; Pincus et al., 2010; Karagöz et al., 2017). To investigate how a sensor integrating both the concentration of unfolded protein and the concentration of free chaperone (which serves as an indirect measure of chaperone-sensor binding), we combine the models for the *U*-switch with the C_F -switch by multiplying the two activation functions (see Eq. 9) to form the AND-switch (shown in Figure 1D). The AND-switch is zero everywhere that either the *U*-switch or the C_F -switch are zero and fully activated only when both individual switches are also fully activated. In this way, as the two slope



FIGURE 4: Comparison of Pareto fronts for *U*-switch and C_F -switch. (A) The Pareto fronts for the UPR activated by the level of unfolded protein directly (circles) and by the level of free chaperone (squares). The chaperone-sensing system performs more efficiently than the unfolded protein–sensing system in all cases. The coloring of the markers corresponds to the maximum unfolded protein concentration reached during the stress event. (B) The time courses for unfolded protein (top) and total chaperone (bottom) during the stress event for the two Pareto-optimal models indicated by the arrows (and green triangles) in A. (C) The phase-plane trajectories (black curves) for the same two parameterizations in B. The background coloring indicates the activation level for the UPR in each model. Owing to the slanted activation threshold of the C_F -switch, the UPR deactivates at a higher level than the *U*-switch. Parameter values for the stress pulses are: D = 2.15, $\tau_p = 0.46$.

parameters, m_u and m_c , become large, the AND-switch approximates a logical AND gate for the two input signals.

Figure 5 shows a comparison between the Pareto sets for the AND-switch and the two individual switching functions for a pulse with amplitude D = 1.0 and duration $\tau_p = 0.5$. At low values of μ_C on the Pareto fonts, the AND-switch coincides with the U-switch, while at higher values of μ_C on the Pareto front, the AND-switch and the C_F -switch coincide. For all cases, the AND-switch aligns with the better of the U-switch and the C_F -switch, but never outperforms them. This suggests that, when the trade-off between chaperone production and unfolded protein buildup favors greater chaperone production, the optimal sensing strategy is to monitor the free chaperone, as demonstrated by the C_F -switch results. In this case, the unfolded protein concentration does not directly control UPR activation, although it may still influence the system in ways not considered here, such as stabilizing the signal or reducing noise. When the trade-off places a premium on chaperone efficience.

ciency (low μ_c), the Pareto front more closely follows that of the *U*-switch than the C_F -switch. However, this effect is only present for pulses in which there is a portion of the Pareto front for which the *U*-switch is superior, which occur only for relatively small-amplitude pulses (Figure 3).

The preference for the AND-switch to coincide with either the *U*- or *C*_F-switch can be understood by considering the large *m* limit at which both the *U*-switch and *C*_F-switch become approximately binary. Then, the fully active region of the UPR in phase space is where $u > u_{min}$ and $c_F < c_{F,max}$. Three scenarios are then possible for the control of activation (shown schematically in Figure 6), each of which depends on where the two activation thresholds intersect in the phase plane. First, if the intersection occurs at a value of c_T that is less than the steady state, then both the activation and deactivation thresholds will be determined by the c_F condition. In the second case, if the intersection occurs at a c_T that is greater than the steady-state chaperone concentration (because no change in total



FIGURE 5: Comparison of Pareto fronts for AND-switch, *U*-switch, and C_F -switch. (A) The Pareto fronts for the *U*-switch, C_F -switch, and the AND-switch. The AND-switch coincides with the better of either the *U*-switch or the C_F -switch in all cases, but does not outperform the individual mechanisms. (B, C) The phase-plane trajectories and activation levels for sets of points on the Pareto fronts for which the AND-switch coincides with the *U*-switch (downward-pointing triangles in panel A) and the C_F -switch (upward-pointing triangles in panel A). The left-most panels are for the *U*-switch, the center panels are for the C_F -switch, and the right-most panels are for the AND-switch. The pulse parameters are D = 1.0, $\tau_P = 0.5$.

chaperone occurs until after the UPR is activated), but less than the maximal value reached during the stress event, the activation threshold will be determined by u_{\min} , and the deactivation threshold will be determined by $c_{F,\max}$. In the third case, if the intersection is located at a c_T value greater than the maximal level encountered by the system, then the control of both activation and deactivation depends only on u_{\min} . The first and third scenarios correspond to the C_F -switch and U-switch, respectively, while the second scenario

used both conditions of the AND-switch's logic to separately control the thresholds for turning the UPR on and off. However, under the conditions shown in Figure 5, the optimal AND-switch always is of the type described in the first case. Yet, even though the activation threshold is set by the C_{F^-} switch, the slope of the response allows the activation surface (heat map in Figure 5B, right panel) to closely mimic that of the *U*-switch (left panel).

Taken as a whole, these results suggest that a sensing mechanism that incorporates both chaperone sequestration and direct unfolded protein binding does not improve the efficiency of the feedback response beyond what can be achieved by either mechanism individually. Therefore, optimization of the trade-off between chaperone production and stress mitigation can rationalize the observation of a chaperone-based sensor, as discussed in the preceding section, but not the combination of this mechanism with direct unfolded protein activation, suggesting that the combined mechanism observed in both yeast and higher eukaryotes serves another purpose.

DISCUSSION

Only with the appropriate design can a sensor network for the UPR efficiently regulate protein homeostasis in the cell. We developed a minimal model of the UPR that incorporates the stress of increased protein influx or increased protein misfolding within the ER, the role of folding chaperones in mitigating that stress, and the sensory network that controls the magnitude and timing of the transcriptional feedback. This model was then used in a genetic multi-objective optimization algorithm to determine the Pareto-optimal set of signal-transducing functions mapping the stress levels in the ER to response levels of chaperone transcription. Pareto optimization provides a useful structure for the analysis of regulatory mechanisms within the cell that must strike a balance between a few (or many) competing measures of fitness. In particular, it removes the subjectivity often required when choosing weights for different fitness functions to generate a single scalar fitness variable. Instead, calculation of the Pareto front allows for a clear

understanding of the trade-offs constraining the fitness space of a phenotype.

In this work, we have applied this technique to the problem of maintaining protein homeostasis in the ER through the activation (and deactivation) of the UPR. Optimality was assessed with regard to two metrics: 1) the integrated level of unfolded protein over the course of the stressing event and 2) the excess production of chaperone over the course of the stress.



FIGURE 6: Schematic depiction of AND-switch phase-plane geometry. In the binary-switch limit, the intersection of the activation thresholds for the U-switch (dashed blue line) and the C_F -switch (solid blue lines) with the phase-plane trajectory of the system (solid black curve) mark the points at which the UPR activates and deactivates. The shaded regions above the u_{min} line and to the left of the $c_{F,max}$ lines demarcate the area of phase space for which the UPR is activated under the control of the AND-switch. Line 1 shows a case for which $c_{F,max}$ dictates both the on and off transitions for the UPR. In the case of line 2, the on transition is determined by u_{\min} , and the off transition is controlled by $c_{F,max}$. Finally, line 3 shows a case for which the on and off transitions are set by u_{min} . The arrows labeled ΔC mutation and ΔU mutation show the predicted change to the activation thresholds for a mutant in which the interaction between chaperone and sensor is disrupted (ΔC) and a mutant in which the unfolded protein-sensor affinity is decreased (ΔU). We emphasize that this picture is schematic, and for any real system, the dynamics (black curve) will necessarily depend on the threshold values for the UPR.

What makes a good sensor network?

Analysis of the model provided insight into desirable traits for stress-sensing networks. First, for chronic stress, in which the system has time to reach a new steady state (or limit cycle), the steepness of the activation function has two opposing effects: a greater slope suppresses oscillations of the feedback, but at the cost of looser overall control of the unfolded protein level across the operational range of the homeostat. Because experiments of UPR activation show nonoscillatory, dose-dependent responses to stress (Pincus et al., 2010), it seems as though a more graded response that suppresses oscillations and allows for stable intermediate UPR levels has been selected.

Second, the model helped to identify a benefit of sensing stress through the concentration of free chaperone, as opposed to the concentration of unfolded proteins directly. A BiP-mediated activation was initially proposed for Ire1-based stress sensing due to the clear connection between BiP-Ire1 coimmunoprecipitation and suppression of the UPR with BiP overexpression (Dorner *et al.*, 1992; Bertolotti *et al.*, 2000; Okamura *et al.*, 2000). The analysis presented here provides a possible reason that a BiP-based mechanism would evolve. Sensing the level of free chaperone can both provide a sharper response during increasing stress and increase the deactivation threshold as the system returns to basal functioning. Hence, it provides both faster on and off responses, allowing for a more efficient use of excess chaperone. The notion that one function of BiP is to accelerate the deactivation of the UPR is supported by experiments: yeast with an Ire1 mutant that does not bind BiP exhibits delayed deactivation of the UPR upon the removal of stress compared with wild type (Pincus *et al.*, 2010). Interestingly, it has been demonstrated in yeast (Pincus *et al.*, 2010), and more recently in human (Karagöz *et al.*, 2017), that unfolded proteins within the ER lumen interact directly with Ire1 and are essential for full UPR activation. It has been proposed that unfolded proteins act as a ligand for activating the UPR, while BiP plays the role of a buffer (Oikawa *et al.*, 2007; Pincus *et al.*, 2010). Our analysis shows that the AND-switch logic requiring both inputs can decouple the threshold for activating the UPR from the point at which the UPR deactivates, but this does not enhance the efficiency of the response with regard to the tradeoff between chaperone production and stress mitigation. Hence, the combined sensory mechanism is likely the result of another factor such as noise reduction or ligand selectivity.

Effect of sensor mutations on signaling

Our model provides qualitative predictions regarding the impact mutations to Ire1 will have on the sensor activation and sensitivity to stress. An Ire1 mutant that does not bind BiP effectively increases $c_{F,max}$ such that the C_F -switch would always be active (Figure 6). In the case of the AND-switch, this means the activation and deactivation are both controlled by the unfolded protein threshold, u_{min} . The early shutoff provided by the chaperone-sensing portion of the AND-switch is lost. In support of this, time-course experiments for UPR activation using an Ire1 mutant that does not bind BiP show an increased lag time between the removal of stress and deactivation of the UPR compared with wild-type Ire1 (Pincus et al., 2010). Similar to more detailed UPR models (Pincus et al., 2010), our minimal model predicts precisely this effect. Furthermore, our model shows that the origin of the BiP-mediated deactivation lies in the differing dependence on unfolded protein concentration of the U-switch and C_{F} -switch. The fact that this has been experimentally observed in yeast lends credence to the idea that cells have evolved to take advantage of the enhanced efficiency of a BiP-mediated stress response.

Similarly, our model predicts that mutations causing a decrease in the affinity between Ire1 and unfolded proteins, effectively raising u_{\min} , could have one of two effects. If the mutation is severe enough to prevent the interaction altogether, the threshold for activation for the AND-switch would increase to an unsustainable level of stress, and the UPR would never activate. Alternatively, if the mutation raised u_{min} by a smaller amount, but enough so that the intersection of the U threshold and C_F threshold moved from either case 1 or case 2 to case 3 in Figure 6, then both activation and deactivation would be set by the unfolded protein concentration. In this case, we would again expect that the early shutoff provided by the BiP-Ire1 interaction would be lost. Mutational experiments disrupting the proposed unfolded protein binding site on Ire1 have shown that the UPR is diminished for given drug-induced stress levels (Credle et al., 2005), indicating that the affinity of Ire1-unfolded protein interaction can be modulated. It would be interesting to see whether certain mutations also remove the BiP-controlled early shutoff by increasing the threshold of unfolded protein required for activation to a level that renders the Ire-BiP interaction irrelevant.

Other features can affect the fitness of stress signaling

While our model is far simpler than the many-faceted response of the true UPR, it captures essential aspects of the ER stress response and allows for clear analysis of a subset of the evolutionary constraints governing the sensing mechanism of Ire1. Our model also provides novel insight into the role played by the stress-detecting network in optimizing the UPR. Of course, there are several questions that require further inquiry. For one, we have only considered isolated incidents of stress in this work. In reality, cells experience a dynamic continuum of different unfolded protein loads on the ER folding machinery. It remains to be established how switch design might be altered when the evolutionary driver is a distribution of protein fluxes into the ER. In this scenario, it is tempting to speculate that a graded response would be even more valuable, as it would allow for greater specificity in response over a range of stress levels. In a similar vein, the relatively small copy number of Ire1 molecules in the cell (\approx 200; Ghaemmaghami *et al.*, 2003) implies that there will be significant noise in any signal transmitted from the ER lumen to the nucleus. Further work will examine how noise and information transmission effect fitness of stress signaling.

Finally, we note that the model presented here is not limited to describing the feedback of the UPR. It can readily be extended to any feedback control mechanism of enzymatic reactions in which either the substrate or enzyme act as a positive or negative regulator of enzyme production.

Conclusions

In summary, we developed a minimal model of the UPR to understand optimal design of the ER stress-sensor network. The most important results of our analysis are as follows: 1) A graded response will, in general, suppress oscillations in chronic stress conditions, at the expense of looser regulation of unfolded protein concentration in the ER. 2) Sensors whose activity is down-regulated by the amount of free chaperone can improve fitness by activating and deactivating at different levels of stress. 3) Integrating signals from freechaperone levels and unfolded proteins imbues the stress signaling network with an additional degree of freedom for tuning control of the UPR. However, this extra degree of freedom does not enhance the fitness of the controller with regard to the trade-off considered here. By unraveling the advantages gained by indirect regulation of the ER stress sensor, our approach helps in understanding homeostatic controllers in other biological contexts and can guide synthetic biology sensor design.

MATERIALS AND METHODS

Numerical solution of delay differential equations

To simulate Eqs. 3 and 4, we use the Python software pydelay, which implements the Bogacki-Shampine method to compute trajectories of systems of delay differential equations (Flunkert and Schoell, 2009). Solutions to delay differential equations require the specification of a time history for each variable for at least as long as the longest delay present in the system. Here, we use the steady state of the unfolded protein and chaperone levels for the time history, such that our perturbations due to stress are deviations from the steady functioning of the ER folding machinery. The steady states are found by setting Eqs. 3 and 4 equal to zero under the assumption that the UPR is operating at a basal level below the threshold for activation, which leads to

$$c_{T,ss} = 1 \tag{15}$$

$$u_{ss} = \frac{1}{2} \left[\nu - \alpha - \beta + \sqrt{\left(\nu - \alpha - \beta\right)^2 + 4\nu\beta} \right]$$
(16)

These equations are valid only so long as they are consistent with the assumption that the UPR is inactive at the steady state, that is, $u_{ss} < u_{min}$ for the *U*-switch and $c_{F,ss} > c_{F,max}$ for the *C*_F-switch and both conditions for the AND-switch. This requirement places constraints on the values taken by u_{min} and $c_{F,max}$ for a given parameterization. For the optimization procedure described in

Fitness measures and Pareto optimization, we ensure that the steady state for the baseline influx does not activate the UPR for all simulations. Additionally, if the slope of the activation function, m, for the C_F -switch is small enough, the activation function can be less than G_0 when $c_F = 0$, effectively lowering the maximum possible response. To avoid this, we also ensure that both the C_{F} and ANDswitches can reach maximum activation for positive c_F . If the amplitude of the stress is small enough, the existing (steady-state) chaperone concentration is sufficient to maintain a new steady-state concentration of unfolded protein that is still below the activation threshold for the UPR (see the Supplemental Material). Conversely, for a fixed stress amplitude, D, a maximal value of the activation threshold can be determined, beyond which no response will occur. This provides a boundary constraint for the Pareto optimization procedure. Despite the simulations being started with a history at the steady state, numerical artifacts can occasionally lead to small fluctuations at the onset of the simulations. To ensure that these do not interact with the prescribed perturbations we seek to analyze, each simulation is allowed to relax for a period of $30 au_{\it UPR}$ before the pulse of stress is applied. Following the equilibration period, each model is simulated for time of τ_{p} + 30 τ_{UPR} . This allows all simulations, regardless of pulse shape and response function parameterization to return to a steady state following the stress response.

Code availability

Python scripts used to simulate the model and calculate Pareto sets can be found at https://bitbucket.org/schnell-lab/upr_feedback_ control/src/master. All codes were run using Python, version 2.7.

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