



# The influence of arm positions on mechanical dyssynchrony measured by gated myocardial perfusion imaging

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**Background:** In routine procedures, patient's arms are positioned above their heads to avoid potential attenuation artifacts and reduced image quality during gated myocardial perfusion imaging (G-MPI). However, it is difficult to achieve this action in the acute period following pacemaker implantation. This study aimed to explore the influence of arm positioning on myocardial perfusion imaging (MPI) in different types of heart disease.

**Methods:** This study was conducted retrospectively. A total of 123 patients were enrolled and underwent resting G-MPI using a standard protocol with arms positioned above their heads and again with their arms at their sides. All individuals were divided into 3 groups: the normal group, the obstructive coronary artery disease (O-CAD) group, and the dilated cardiomyopathy (DCM) group. The G-MPI data were measured by QGS software and Emory Reconstruction Toolbox, including left ventricular ejection fraction (LVEF), end-diastolic volume (EDV), end-systolic volume (ESV), extent, total perfusion deficit (TPD), summed rest score (SRS), scar burden, phase standard deviation (SD), and phase histogram bandwidth (BW).

**Results:** In total, extent, TPD, EDV, ESV, LVEF, systolic SD, systolic BW, diastolic SD, and diastolic BW were all significantly different between the 2 arm positions (all  $P < 0.01$ ). On the Bland-Altman analysis, both EDV and ESV with the arm-down position were significantly underestimated ( $P < 0.001$ ). Meanwhile, TPD, extent, and LVEF with the arm-down position were significantly overestimated ( $P < 0.05$ ). Systolic SD, systolic BW, diastolic SD, and diastolic BW were systematically overestimated ( $P < 0.001$ ). In the DCM group ( $n = 52$ ), EDV, ESV, systolic SD, systolic BW, diastolic SD, and diastolic BW were identified as significantly different by the paired  $t$ -test between the 2 arm positions ( $P < 0.05$ ). In the O-CAD group ( $n = 32$ ), scar burden, ESV, LVEF, and diastolic BW were significantly different between the 2 arm positions ( $P < 0.05$ ).

**Conclusions:** Systolic and diastolic dyssynchrony parameters and most left ventricular (LV) functional parameters were significantly influenced by arm position in both normal individuals and patients with heart failure (HF) with different pathophysiologies. More attention should be given to LV dyssynchrony data during clinical evaluation of cardiac resynchronization therapy (CRT) implantation procedure.

**Keywords:** Gated myocardial perfusion imaging (G-MPI); left ventricular mechanical dyssynchrony (LVMD); phase analysis; heart failure (HF)

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## Introduction

Gated myocardial perfusion imaging (G-MPI) is a widely used, noninvasive, and cost-effective method of imaging that plays an important role in diagnosing, evaluating prognosis, evaluating the viability, and assessing the effectiveness of therapy in heart disease (1). A recent study found that left ventricular mechanical dyssynchrony (LVMD) was more highly correlated with cardiovascular disease (CVD) and all-cause mortality than electrical dyssynchrony (2). Meanwhile, the myocardial perfusion imaging (MPI) phase analysis showed some advantages over other imaging methods with wide availability and excellent reproducibility in valuing global left ventricular (LV) dyssynchrony, such as phase standard deviation (SD), phase histogram bandwidth (BW), and phase entropy (PE). In recent years, nuclear image-guided approaches for cardiac resynchronization therapy (CRT) have shown significant clinical value in assessing LV myocardial viability and mechanical dyssynchrony, recommending the optimal LV lead position, and navigating the LV leading to the target coronary venous site.

Quality control of G-MPI data is a key point to acquiring valid results. However, attenuation artifacts are common in the anterior, inferior, and lateral myocardium, which results in lower diagnostic accuracy. Anterior attenuation has been linked with breast artifacts, whereas inferior attenuation is associated with diaphragm or subdiaphragmatic interference (3). Lateral attenuation and reduced image quality have been related to the left arm during image acquisition. Therefore, MPI is acquired with the left arm positioned above the patient's head in routine procedures (4). However, in the acute period, pacemaker implantation for CRT makes it difficult to achieve such positioning. Additionally, some elderly patients are not able to complete studies in this position. Although new MPI technology has improved the image resolution and quality (5), little data have been obtained about the impact of arm positioning on LV parameters and mechanical dyssynchrony. Therefore, we aimed to explore the influence of arm positioning on MPI in different types of heart disease. We present this article in accordance with

the STROBE reporting checklist (available at <https://qims.amegroups.com/article/view/10.21037/qims-22-1404/rc>).

## Methods

### *Patient population*

This study was conducted retrospectively. This study consecutively enrolled 123 individuals at the First Affiliated Nanjing Medical University Hospital from December 2018 to August 2020. All individuals were divided into 3 groups with the aim to achieve representativeness of the general population: a normal group, an obstructive coronary artery disease (O-CAD) group, and a dilated cardiomyopathy (DCM) group. O-CAD was defined as coronary artery stenosis greater than 50% by coronary angiography or dual-source computed tomography (CT) in at least 1 of the main coronary arteries, previous history of coronary revascularization, or myocardial infarction (6). DCM was diagnosed with the patient's history and exclusion of other etiological factors that might cause heart failure (HF), with LV ejection fraction (LVEF) <45% according to the recent criteria (7). The other individuals were divided into the normal group with the following exclusion criteria: hypertension, diabetes, smoking, hyperlipidemia, other high cardiovascular risk factors, severe arrhythmia, postoperative percutaneous coronary intervention (PCI), HF, and myocardial perfusion abnormalities. This study was approved by the Institutional Ethical Committee of the First Affiliated Hospital of Nanjing Medical University, and informed consent was obtained from all individuals. This study conformed to the provisions of the Declaration of Helsinki (as revised in 2013).

### *Single-photon emission CT (SPECT) MPI assessment*

All individuals underwent resting electrocardiogram (ECG)-SPECT MPI with their arms positioned above their heads and again with their arms at their sides. MPI was performed approximately 60 minutes after injection using 740–1,110 MBq of <sup>99m</sup>Tc-sestamibi. The SPECT images

were acquired in a dual-headed camera (CardioMD; Philips Medical Systems, Eindhoven, Netherlands) with a standard protocol with a 20% energy window of approximately 140 KeV, 180° orbit, 32 steps with 25 seconds per step, 8-bin gating, and 64 planar projections per gate. After MPI data acquisition was completed, reconstruction processing was performed using QPS/QGS software to obtain short-axis, vertical long-axis, and horizontal long-axis tomographic images and then obtain left cardiac function parameters, including LVEF, end-diastolic volume (EDV), end-systolic volume (ESV), total perfusion deficit (TPD), extent, summed rest score (SRS), and scar burden.

Meanwhile, image reconstruction and reorientation were performed by Emory Reconstruction Toolbox (ERTtoolbox; Atlanta, GA, USA) for mechanical dyssynchrony, including phase distribution of LV systolic dyssynchrony (LVSD) and LV diastolic dyssynchrony (LVDD). The MPI images were reconstructed by ordered subset expectation maximization (OSEM) with 3 iterations and 10 subsets and then filtered by a Butterworth low-pass filter with an order of 10 subsets and a cutoff frequency of 0.3 cycles/cm.

The resulting gated short-axis MPI images were sent to an interactive tool for automatized access to LV contour parameters by an automatic myocardial sampling algorithm that searched 3-dimensionally (3D) for the maximal count circumferential profiles in each cardiac frame. Subsequently, the onset of mechanical contraction and relaxation throughout the cardiac cycle were obtained based on multi-harmonic Fourier approximations (8). Then, the LVMD was represented by the phase distribution of LVSD and LVDD for the entire left ventricle, and quantitative parameters of LVMD were calculated as the SD and BW, respectively (8,9).

### Statistical analysis

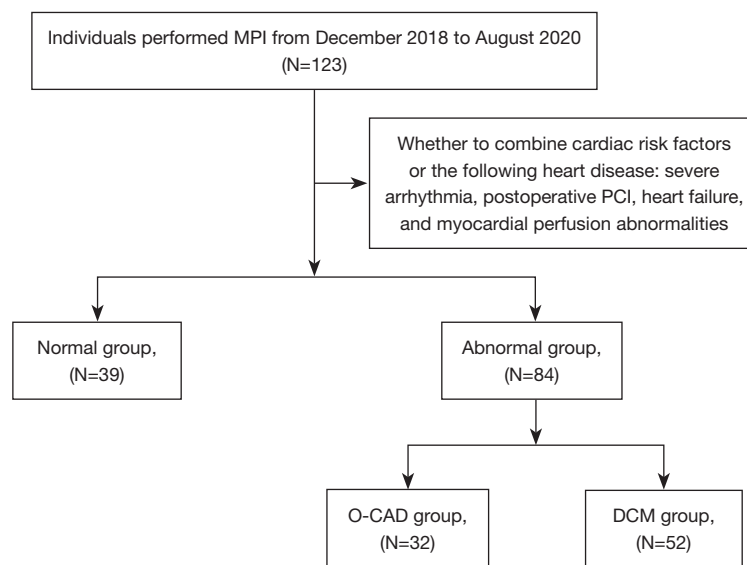
Continuous variables were expressed as the mean  $\pm$  standard deviation, and categorical variables were expressed as numbers and percentages. Comparisons between arms-up and arms-down were performed using Student's *t*-test for paired data. One-way analysis of variance (ANOVA) was performed for continuous variables, including baseline characteristics and LV parameters. Pearson's correlation analysis was applied to assess the association between arms up and arms down in left cardiac parameters. The Bland-Altman analysis of agreement was used to compare the average absolute difference in LV measurements between the 2 groups (10). Additionally, the Kruskal-Wallis H-test was employed to assess the differences in baseline characteristics among the 3 groups, which

encompassed variables such as hypertension, diabetes, body mass index (BMI), alcohol consumption, and smoking (11). A 2-tailed  $P < 0.05$  was considered statistically significant. Statistical analysis was performed with the software SPSS 22.0 (IBM Corp., Armonk, NY, USA).

### Results

A total of 123 individuals who underwent SPECT MPI were included in this study (*Figure 1*). The baseline characteristics of high cardiovascular risk factors are listed in *Table 1* including age, gender, hypertension, diabetes, BMI, smoking, and alcohol consumption. Besides, in O-CAD patients, there were 24 cases of stable angina and 8 cases of myocardial infarction. For all individuals, the age was  $61.27 \pm 10.87$  years, and 74.80% ( $n=92$ ) of patients were male. There were statistically significant differences in age, hypertension, BMI, alcohol consumption, and smoking between the normal group, O-CAD group, and DCM group (all  $P < 0.05$ ) (*Table 1*). In total, Pearson's correlation analysis revealed that there were high correlations for SRS, extent, scar burden, TPD, EDV, ESV, LVEF, systolic SD, systolic BW, diastolic SD, and diastolic BW between the arm-up and arm-down positions in all variables (all  $P < 0.01$ , *Table 2*). *Figure 2* and *Figure 3* illustrate the G-MPI obtained from a normal individual (58-year-old male, 63 kg, BMI 23.9 kg/m<sup>2</sup>). A noticeable finding in the images is that the perfusion in the inferior-lateral and inferior walls appears to be decreased in the images with the arms down when compared to the images with the arms up. However, apart from SRS and scar burden, several parameters including extent, TPD, LVEF systolic SD, systolic BW, diastolic SD, and diastolic BW exhibited significantly higher values in the arm-down position group compared to the arm-up position group, as determined by the paired *t*-test (all  $P < 0.05$ ) (*Table 2*). Conversely, the arm-down position group showed significantly lower values for EDV and ESV compared to the arm-up position group, as determined by the paired *t*-test. Additionally, in both the arm-up and arm-down position groups, the cardiac function parameters were higher in males compared to females except for LVEF values, as indicated in *Table 3*.

In the Bland-Altman analysis (*Figure 4*), both EDV and ESV with the arm-down position were significantly underestimated by a mean of 5.0 ( $P < 0.001$ ) and 7.5 ( $P < 0.001$ ), respectively, compared with EDV and ESV with the arm-up position. Meanwhile, LVEF, extent, scar burden, and TPD with the arm-down



**Figure 1** Study flow diagram. MPI, myocardial perfusion imaging; PCI, percutaneous coronary intervention; O-CAD, the obstructive coronary artery disease; DCM, dilated cardiomyopathy.

**Table 1** Baseline characteristics of the enrolled patients

Variables	All (n=123)	DCM group (n=52)	O-CAD group (n=32)	Normal group (n=39)	P value
Age (years)	61.27±10.87	62.46±11.14	64.13±11.14	57.10±11.47	0.013
Male	92	40	28	24	0.179
Hypertension	42	22	20	0	<0.001
Diabetes	8	4	4	0	0.059
BMI (kg/m <sup>2</sup> )	24.14±2.60	23.32±2.97	25.51±1.71	24.28±1.83	0.025
Smoking	28	16	12	0	<0.001
Alcohol	12	8	4	0	<0.001

Data are expressed as mean ± standard deviation or number. DCM, dilated cardiomyopathy; O-CAD, obstructive coronary artery disease; BMI, body mass index.

position were overestimated compared with those with the arm-up position by a mean of 2.3 ( $P<0.001$ ), 0.8 ( $P=0.02$ ), 0.6 ( $P=0.27$ ), and 1.0 ( $P=0.005$ ), respectively (Figures 5,6). Furthermore, to analyze the influence of arm position on LV phase analysis parameters, we examined the difference between BW and SD in both LV systolic and diastolic parameters (Table 2). There was a high correlation for systolic SD, systolic BW, diastolic SD, and diastolic BW between the arm-up and arm-down positions in all 3 groups (all  $P<0.01$ ). Moreover, systolic SD, systolic BW, diastolic SD, and diastolic BW were all higher in the arm-down positions (all  $P<0.05$ ). Meanwhile, as suggested by the Bland-Altman plot in

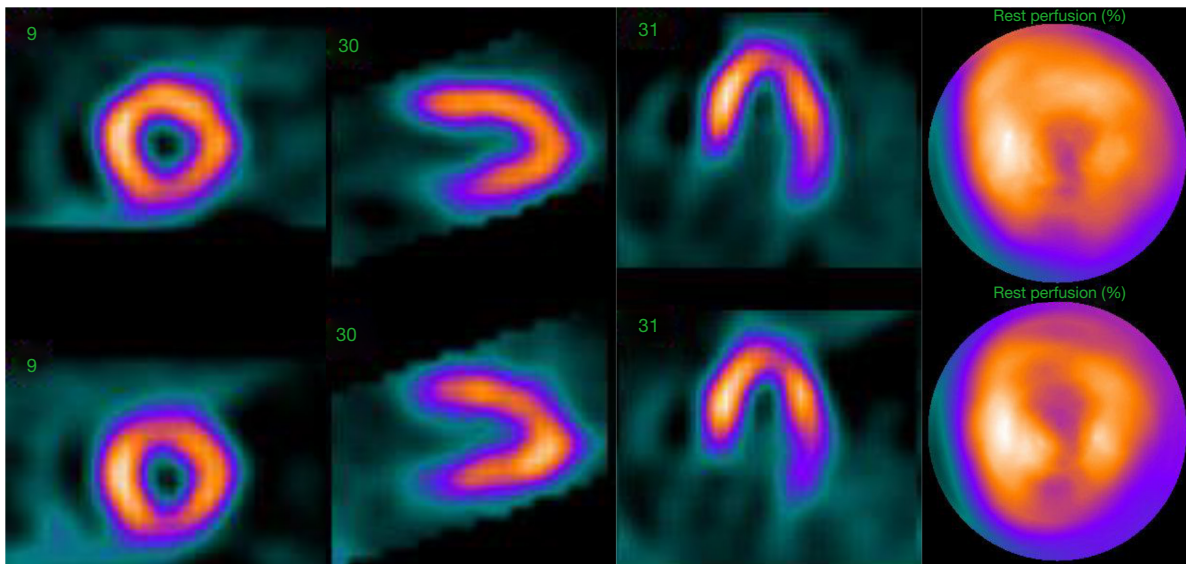
Figure 7 and Figure 8, systolic SD, systolic BW, diastolic SD, and diastolic BW were systematically overestimated by a mean of 5.6 ( $P<0.001$ ), 24.1 ( $P<0.001$ ), 7.4 ( $P<0.001$ ), and 22.6 ( $P<0.001$ ), respectively.

In the subgroup of normal individuals ( $n=39$ , Table 4), SRS, extent, TPD, ESV, LVEF, systolic SD, systolic BW, and diastolic SD were shown to be significantly different by the paired  $t$ -test between the 2 arm positions (all  $P<0.05$ ). However, there were no differences in scar burden, diastolic BW, and EDV in the normal group (all  $P>0.05$ ). In the DCM group ( $n=52$ , Table 5), EDV, ESV, systolic SD, systolic BW, diastolic SD, and diastolic BW were shown to be significantly different by the paired  $t$ -test between the

**Table 2** Left ventricular functional parameters and the correlations in all groups (n=123) with two arm positions

Variables	Arm-down position	Arm-up position	R value	P value
SRS	5.98±7.28	6.04±7.80	0.928	0.805
Extent	10.15±10.77	8.80±12.05	0.950	0.023
Scar burden	19.82±10.32	9.33±12.30	0.871	0.340
TPD	8.63±8.55	7.65±9.75	0.952	0.001
EDV (mL)	157.57±104.57	162.95±112.58	0.990	0.001
ESV (mL)	93.59±99.45	101.31±109.47	0.986	<0.001
LVEF (%)	52.76±25.83	50.50±24.97	0.978	<0.001
Systolic SD	34.37±19.03	28.76±17.43	0.705	<0.001
Systolic BW	144.33±86.13	120.47±84.21	0.725	<0.001
Diastolic SD	60.67±16.33	53.58±20.04	0.425	<0.001
Diastolic BW	199.67±66.25	177.91±67.80	0.504	<0.001

R values (correlation coefficient), indicate a statistically significant relationship ( $P<0.01$ ) between the 2 arm positions in all variables. Data are expressed as mean  $\pm$  standard deviation. SRS, summed rest score; TPD, total perfusion deficit; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; SD, phase standard deviation; BW, phase histogram bandwidth.

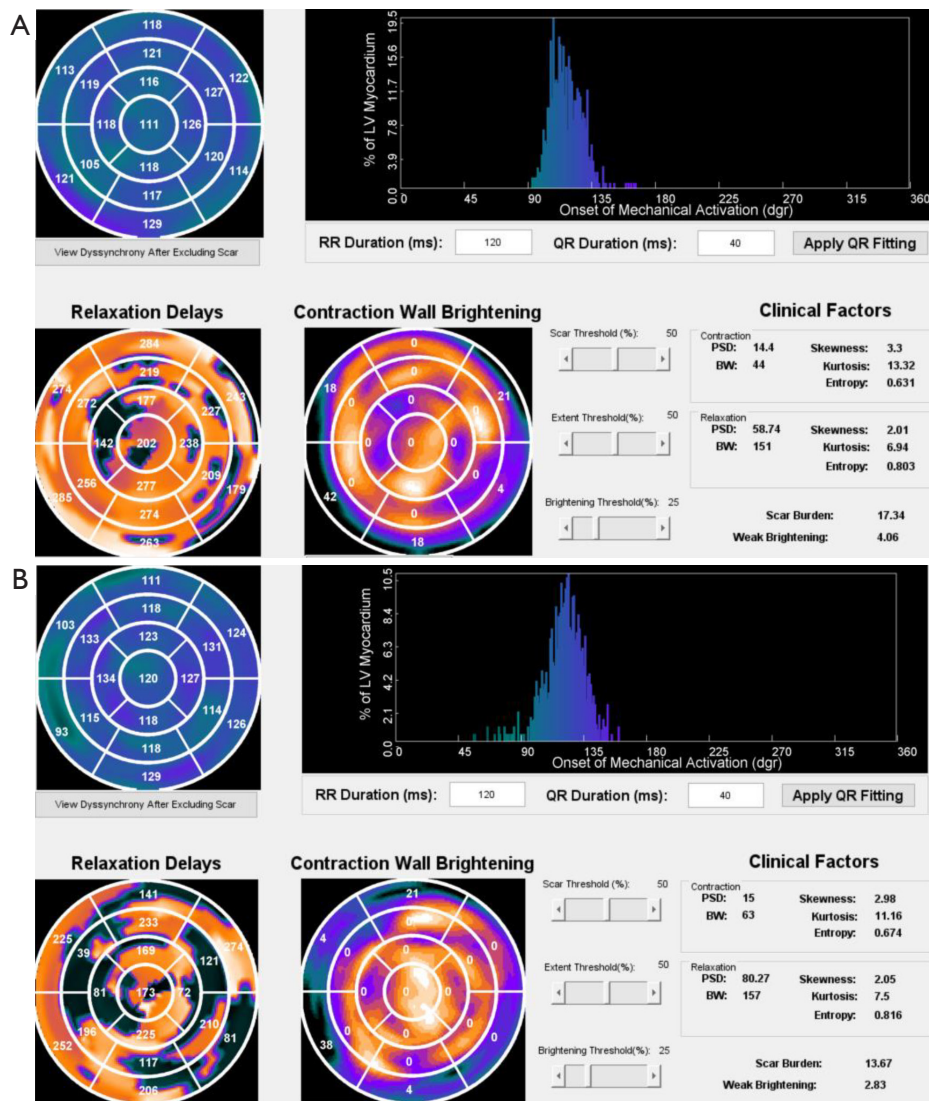


**Figure 2** A G-MPI obtained from a normal individual (58-year-old male, 63 kg, BMI 23.9 kg/m<sup>2</sup>). The top row represents the images captured with the arms up, while the bottom row shows the images obtained with the arms down. From left to right, the images correspond to the short axis, vertical axis, horizontal axis, and a parametric bull's eye plot. A noticeable finding in the images is that the perfusion in the inferior-lateral and inferior walls appears to be decreased in the images with the arms down when compared to the images with the arms up. G-MPI, gated myocardial perfusion imaging; BMI, body mass index.

2 arm positions ( $P<0.05$ ). In the O-CAD group (n=32, Table 6), scar burden, ESV, LVEF, and diastolic BW were shown to be significantly different by the paired *t*-test between the 2 arm positions ( $P<0.05$ ).

## Discussion

This study investigated the influence of arm position on LVMD parameters in normal individuals and HF patients



**Figure 3** In this normal individual, systolic SD, systolic BW, diastolic SD and diastolic BW were different by the paired *t*-test in arms up (A) compared with arms down (B) (systolic SD: 14.4 vs. 15.0; systolic BW: 44.0 vs. 63.0; diastolic SD: 58.74 vs. 80.27; diastolic BW: 151.0 vs. 157.0). SD, phase standard deviation; BW, phase histogram bandwidth.

with different pathophysiologies. The main finding was that systolic and diastolic dyssynchrony parameters and most LV function and perfusion parameters were significantly influenced by arm position in both normal individuals and HF patients with different pathophysiologies.

Gated SPECT (G-SPECT) has been widely used in evaluating the clinical outcome of heart disease and the CRT response. Quantitative analysis of G-SPECT images is becoming an increasingly common tool in the field of nuclear cardiology. Therefore, quality control in acquiring gated MPI data is very important to achieve valid

results (12). The Cedars-Sinai QGS program and Emory cardiac toolbox (13), which are commonly used commercially available MPI analysis software packages, can produce reliable computations of LV perfusion and function parameters from G-SPECT MPI data.

However, some potential artifacts and pitfalls should also be paid close attention to. LV segmentation, including precise assignment of LV contours by determining the endocardial and epicardial surfaces, is essential for MPI SPECT quantification. The presence of extracardiac activity can also cause inaccuracy by including adjacent

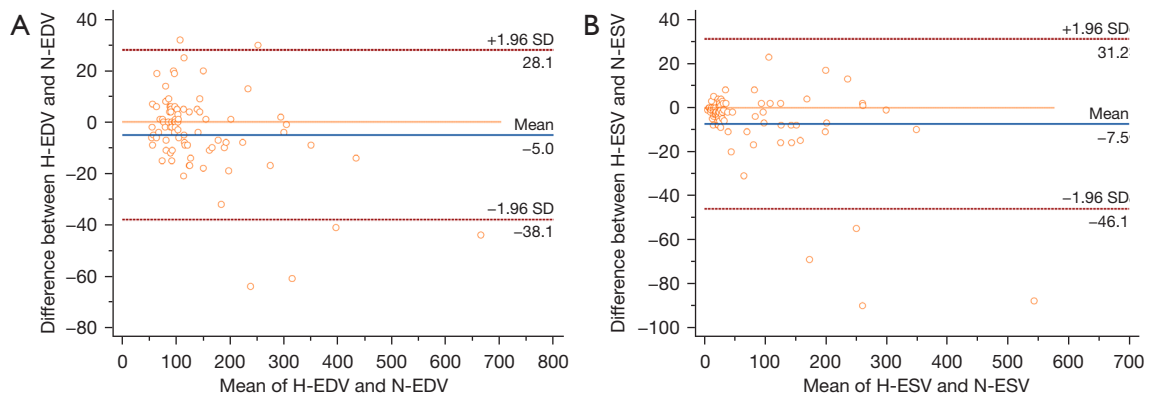
**Table 3** Left ventricular functional parameters in male and female (n=123) with both arm-up and arm-down positions

Variables	Male	Female	P value
<b>SRS</b>			
Arm down	6.24±7.93	5.19±4.90	0.491
Arm up	6.76±8.60	3.90±4.17	0.078
<b>Extent</b>			
Arm down	11.67±11.63	5.65±5.77	0.007
Arm up	11.11±13.51	5.65±5.77	0.005
<b>Scar burden</b>			
Arm down	21.43±11.27	16.72±7.00	0.031
Arm up	21.48±12.55	14.62±5.06	0.004
<b>TPD</b>			
Arm down	9.89±9.24	4.87±4.43	0.004
Arm up	9.03±10.73	3.55±3.74	0.006
<b>EDV (mL)</b>			
Arm down	166.67±107.60	130.55±91.31	0.096
Arm up	172.96±116.54	133.26±95.54	0.090
<b>ESV (mL)</b>			
Arm down	100.79±102.27	72.23±88.68	0.168
Arm up	109.80±114.18	76.10±91.16	0.139
<b>LVEF (%)</b>			
Arm down	51.00±25.45	57.97±26.67	0.195
Arm up	48.54±24.87	56.32±24.76	0.134
<b>Systolic SD</b>			
Arm down	36.73±19.86	27.34±14.44	0.017
Arm up	31.08±18.46	21.89±11.71	0.011
<b>Systolic BW</b>			
Arm down	154.08±88.50	115.39±72.48	0.030
Arm up	133.15±89.32	82.84±51.78	0.004
<b>Diastolic SD</b>			
Arm down	62.36±15.82	55.65±17.04	0.047
Arm up	55.61±20.62	47.54±17.11	0.052
<b>Diastolic BW</b>			
Arm down	208.75±64.39	172.71±65.34	0.008
Arm up	187.67±69.40	148.94±54.07	0.005

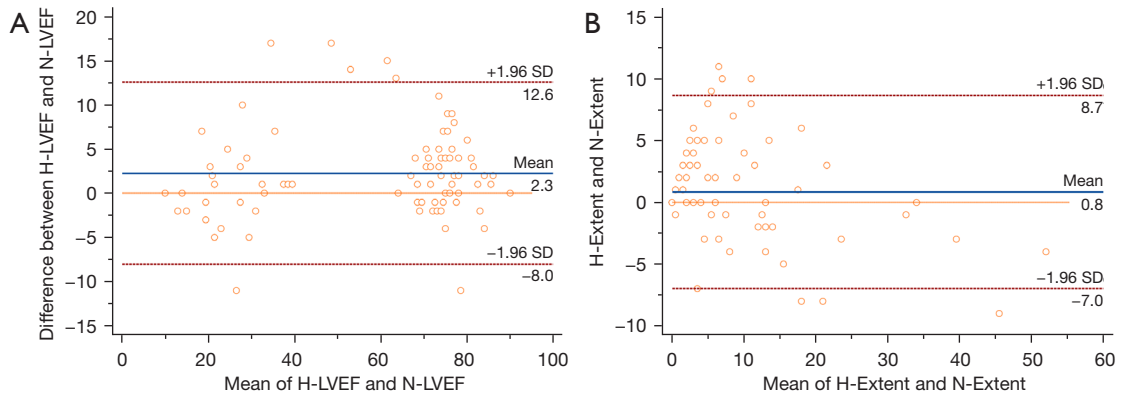
Data are expressed as mean ± standard deviation. SRS, summed rest score; TPD, total perfusion deficit; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; SD, phase standard deviation; BW, phase histogram bandwidth.

extracardiac activity in the LV boundary due to activity related to subdiaphragmatic organs, including the liver and bowel. Besides, weight, BMI, chest circumference, breast attenuation, and bra cup size are better parameters to predict count rate loss, which relates to the quantification of cardiac perfusion and MPI parameters (3,14). A reasonable speculation is that left arm positioning influences the uptake of regional myocardial technetium-99m MPI. Then, the LV boundary region of interest (ROI) was changed according to the location of the maximum pixel count, leading to the inappropriate determination of the point of normalization. However, the current attenuation correction method in the QPS software can effectively compensate for attenuation using the normal limits database. Nonetheless, clinicians may not pay close attention to the subtle variations between patients with their arms up and arms down, as this difference is only present in a small subset of patients. The standard protocol of SPECT is positioning the arms up to maintain the best image quality. Nevertheless, patients with fractures or dislocations of their shoulders or arms may not be able to elevate their arms, especially in patients with pacemaker implantation for CRT during the acute period (15). In a previous study, Toma *et al.* reported that arm positioning did not influence regional myocardial distribution on technetium-99m sestamibi MPI (4). However, Prvulovich *et al.* found that arm positioning influences reconstructed tomographic images depicting regional 201Tl distribution, particularly anterolaterally (16). The different findings in the 2 studies could be explained by the insensitivity of cardiac emission data to truncation, and attenuation correction was not performed in all studies. Furthermore, using a large field of view (FOV) gamma camera might have reduced truncation artifacts in their study. In our study, the normal patients showed higher SRS, extent, and TPD, especially in the lateral wall and anterior lateral wall, which could be explained by the lower uptake of regional myocardial technetium-99m MPI.

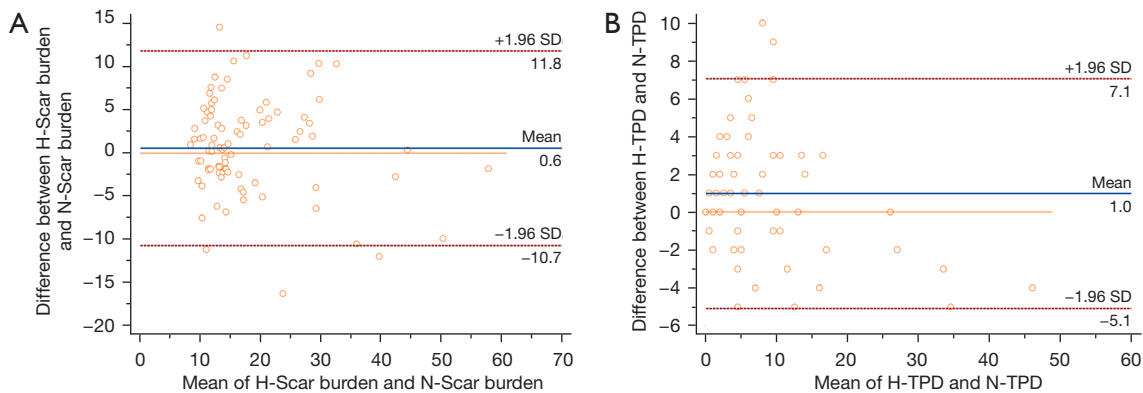
Phase analysis provides a new tool to assess LVMD without any additional radiation dose to the patients (17). Mechanical dyssynchrony can be widely present in HF patients, as observed in our research (18). Our previous study and the literature have shown that LVMD is an independent predictor of cardiac complications in patients with DCM and coronary artery disease (19,20). Furthermore, phase analysis can help in identifying potential candidates for CRT, and a study has shown that assessment of mechanical left ventricular dysfunction (LVD)



**Figure 4** Bland-Altman plots between the arm-down position and the arm-up position for measurement of left ventricular parameters. EDV (A) and ESV (B) were underestimated by a mean of 5.0 ( $P<0.001$ ) and 7.5 ( $P<0.001$ ). EDV, end-diastolic volume; ESV, end-systolic volume; H, arm-down position; N, arm-up position.

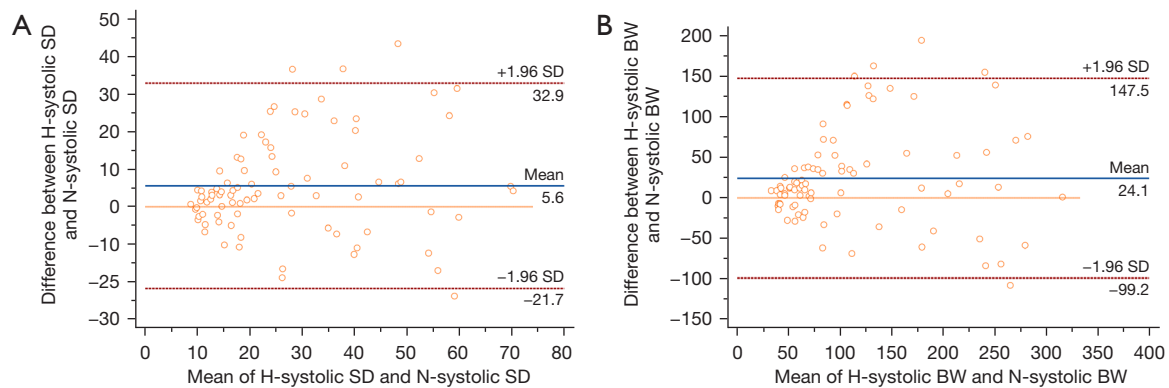


**Figure 5** Bland-Altman plots between the arm-down position and the arm-up position for measurement of LV parameters. LVEF (A) and extent (B) were overestimated by a mean of 2.3 ( $P<0.001$ ) and 0.8 ( $P=0.02$ ). LV, left ventricular; LVEF, LV ejection fraction; H, arm-down position; N, arm-up position.

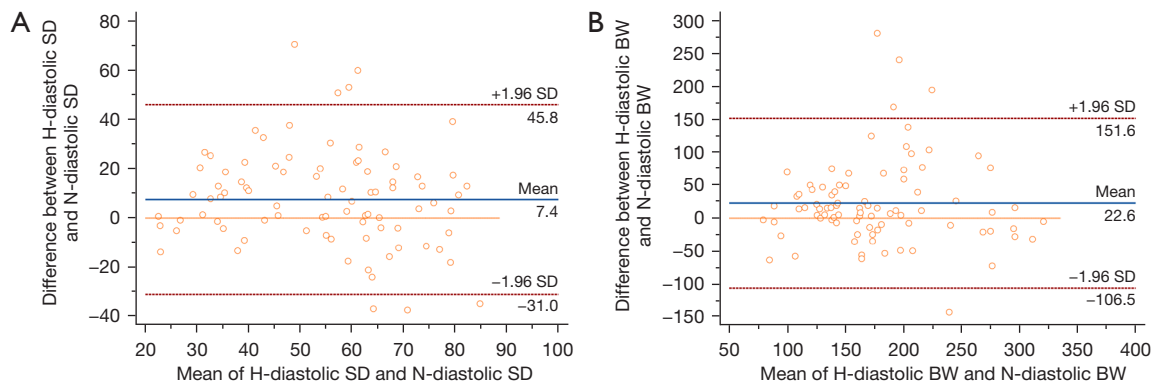


**Figure 6** Bland-Altman plots between the arm-down position and the arm-up position for measurement of left ventricular parameters. Scar burden (A) and TPD (B) were overestimated by a mean of 0.6 ( $P=0.27$ ) and 1.0 ( $P=0.005$ ). H, arm-down position; N, arm-up position; TPD, total perfusion deficit.





**Figure 7** Bland-Altman plots between the arm-down position and the arm-up position for measurement of LV systolic and diastolic dyssynchrony. Systolic SD (A) and systolic BW (B) were overestimated by a mean of 5.6 ( $P < 0.001$ ) and 24.1 ( $P < 0.001$ ). H, arm-down position; N, arm-up position; SD, phase standard deviation; BW, phase histogram bandwidth; LV, left ventricular.



**Figure 8** Bland-Altman plots between the arm-down position and the arm-up position for measurement of LV systolic and diastolic dyssynchrony. Diastolic SD (A), and diastolic BW (B) were overestimated by a mean of 7.4 ( $P < 0.001$ ), and 22.6 ( $P < 0.001$ ). H, arm-down position; N, arm-up position; SD, phase standard deviation; BW, phase histogram bandwidth; LV, left ventricular.

could predict clinical outcomes in patients undergoing CRT (21). Phase analysis is a further extension of wall thickening, which is related to the time interval in the 3D LV myocardial wall (9). Phase analysis depends heavily on the myocardial counts at the base of the heart. Therefore, the parameters of phase analysis can be influenced by the heart rate histogram, the gated cine display, and the phase polar map artifact. In our study, the myocardial counts may be partly impaired by the arm, and thus, the LV boundaries cause a mild change in phase analysis. Besides, Kortelainen *et al.* (22) reported that LVMD were sensitive to changes in acquisition time and the increase of noise in myocardial perfusion imaging. Mukherjee *et al.* (23) revealed that low-dose stress images had higher dyssynchrony parameters as compared to high-dose rest images. So, exploring a proper

acquisition time and right dosage of radiotracer would be a substantial way to address the influence of arm position in these individuals.

The present research confirms the influence of arm positioning on MPI in different types of heart disease, so physicians should be cautious when applying results from different arm positions. The selection of SPECT combined with CT might be an optional method for minimizing attenuation (24). A preliminary study has demonstrated the potential of utilizing deep learning algorithms for coregistration of attenuation correction maps in MPI (25). Furthermore, artificial intelligence (AI) shows promise for applications in the field of attenuation correction (26). Shi *et al.* (27) developed a deep convolutional neural network that successfully generated accurate attenuation maps to

**Table 4** Left ventricular functional parameters in normal groups (n=39) with different arm positions

Variables	Arm-down position	Arm-up position	P value
SRS	1.05±1.64	0.54±1.00	0.037
Extent	2.95±3.48	0.97±1.72	<0.001
Scar burden	13.53±3.60	12.40±3.08	0.115
TPD	3.26±3.04	1.36±1.65	<0.001
EDV (mL)	94.49±24.34	94.54±22.01	0.976
ESV (mL)	23.85±11.31	25.72±12.49	0.006
LVEF (%)	75.67±5.93	73.90±7.73	0.024
Systolic SD	20.36±11.00	14.66±5.20	0.002
Systolic BW	80.31±45.96	55.69±19.38	0.003
Diastolic SD	52.07±19.05	43.48±19.09	0.011
Diastolic BW	157.62±52.94	138.54±45.94	0.071

Data are expressed as mean ± standard deviation. SRS, summed rest score; TPD, total perfusion deficit; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; SD, phase standard deviation; BW, phase histogram bandwidth.

**Table 5** Left ventricular functional parameters in DCM groups (n=52) with different arm positions

Variables	Arm-down position	Arm-up position	P value
SRS	9.88±6.08	10.23±6.25	0.483
Extent	14.15±9.53	14.38±11.44	0.698
Scar burden	26.29±9.49	25.00±11.38	0.185
TPD	11.38±7.16	11.15±8.48	0.584
EDV (mL)	242.50±112.76	255.04±120.87	<0.001
ESV (mL)	183.62±93.97	196.81±109.02	0.002
LVEF (%)	25.54±8.93	24.65±7.89	0.223
Systolic SD	49.41±15.65	41.43±15.03	0.001
Systolic BW	211.62±70.28	180.08±77.90	0.006
Diastolic SD	68.11±12.22	59.48±17.08	0.005
Diastolic BW	239.15±58.52	214.08±70.67	0.028

Data are expressed as mean ± standard deviation. DCM, dilated cardiomyopathy; SRS, summed rest score; TPD, total perfusion deficit; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; SD, phase standard deviation; BW, phase histogram bandwidth.

**Table 6** Left ventricular functional parameters in O-CAD groups (n=32) with different arm positions

Variables	Arm-down position	Arm-up position	P value
SRS	5.63±9.39	5.94±10.33	0.573
Extent	12.44±13.96	11.31±15.55	0.140
Scar burden	18.61±12.32	20.20±13.52	0.01
TPD	10.69±11.76	9.63±13.34	0.098
EDV (mL)	96.44±20.59	96.69±24.60	0.901
ESV (mL)	32.31±25.49	38.25±28.76	0.001
LVEF (%)	69.06±16.57	64.00±16.77	<0.001
Systolic SD	26.99±13.82	25.36±16.13	0.450
Systolic BW	113.00±68.65	102.56±76.76	0.214
Diastolic SD	59.06±13.05	59.29±21.43	0.353
Diastolic BW	186.75±56.49	167.13±54.98	0.018

Data are expressed as mean ± standard deviation. O-CAD, obstructive coronary artery disease; SRS, summed rest score; TPD, total perfusion deficit; EDV, end-diastolic volume; ESV, end-systolic volume; LVEF, left ventricular ejection fraction; SD, phase standard deviation; BW, phase histogram bandwidth.

enhance attenuation correction for SPECT-only scanners. However, further research is required to establish an additional training sample with a validation dataset, which would enable the selection of optimal parameters for model training and the implementation of AI-based algorithms in future studies.

### Limitations

Some limitations should be noted in our study. First, the population of our retrospective study was relatively small for establishing a reference range. Second, not all of the patients underwent stress myocardial perfusion SPECT imaging, so the difference between stress and rest imaging is still needed in further studies. Additionally, cardiac magnetic resonance imaging (MRI) or positron emission tomography (PET) was not performed in our study; therefore, the cardiac functional parameters were not compared with other imaging modalities. Finally, more information on the arm position in different software algorithms for G-MPI remains to be determined.

## Conclusions

Systolic and diastolic dyssynchrony parameters and most LV functional parameters were significantly influenced by arm position in both normal individuals and HF patients with different pathophysiologies. More attention should be focused on LV dyssynchrony perfusion data during clinical evaluation of CRT implantation procedure.

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## Footnote

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*Ethical Statement:* The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by the Institutional Ethical Committee of the First Affiliated Hospital of Nanjing Medical University, and informed consent was provided by all the patients.

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