



Original Article

Lower trunk muscle activity-induced alignment and cop position during single-leg standing

TETSUYA NAKAO, PT, MS^{1)*}, KENICHI MASUDA, MD¹⁾, SHIGEYUKI KANAI, MD¹⁾, JUNZO TSUJITA, BS²⁾, KAZUFUMI HIRAKAWA, PhD³⁾, SHUICHI OKADA, PhD⁴⁾

¹⁾ Sports Medical and Science Institutes, Kansai University of Health Sciences: 2-11-1 Wakaba, Kumatori, Sennan, Osaka 590-0482, Japan

²⁾ Institute of Health and Sport Medical Sciences, Japan

³⁾ Faculty of Health and Medical Sciences, Kyoto Gakuen University, Japan

⁴⁾ Graduate School of Human Development and Environment, Kobe University, Japan

Abstract. [Purpose] The purpose of this study was to clarify fundamental changes induced by lower trunk muscle contraction during single-leg standing. [Subjects and Methods] Ten healthy normal males participated in this study. All subjects could accurately perform lower trunk muscle contraction-type Abdominal Expansion (AE), Abdominal Bracing (AB), and Abdominal Cave-in (AC). The alignment and position of the center of foot pressure (COP) during single-leg standing with SLR and step position after rotating the body from single-leg standing with maximum SLR were measured in each lower trunk muscle contraction type. [Results] When AC was performed during single-leg standing with SLR, the SLR angle increased, COP shifted backward, and the posterior tilt angle of the trunk and cross step distance decreased. [Conclusion] It was assumed that AC during wind-up increases the angle of lower limb elevation and decreases the posterior tilt angle of the trunk and cross step distance.

Key words: Abdominal Cave-in, Cross step, Posterior tilt angle of the trunk

(This article was submitted Feb. 15, 2017, and was accepted Mar. 20, 2017)

INTRODUCTION

To safely and effectively perform body movement, such as throwing, induction of an appropriate kinetic chain by utilizing gravity and ground reaction force is essential to improve performance and prevent damage¹⁾. Pitching motion in baseball starts with shifting the center of gravity of the body from the base of support in wind-up, which is standstill single-leg standing, toward pitching direction by abductor and external rotator muscle forces of the hip joint of the supporting leg. The speed of movement increases with an increase in the force of these muscles in wind-up. This increase in the speed augments the ground reaction force upon grounding the stepping foot in the late-cocking phase²⁻⁴⁾. This ground reaction force doesn't produce ascending kinetic chain unless the force is effectively linked to pelvic rotation.

It is difficult to directly change problematic phenomena in various motions. To improve the problematic phenomena, it is necessary to approach factors causing the problems.

Unconscious cross stepping in the late-cocking phase has to be corrected, but correction in the early-cocking phase during step motion is difficult. Since the cause of cross step may be present in wind-up, setting a proper alignment in wind-up is necessary. It is important to move the trunk from the back inclination to the upright direction and the foot pressure from the front inside to the center during windup⁵⁾. Lower trunk muscle contraction changes alignment of single-leg standing⁶⁾, but there has been no report on the relation between lower trunk muscle contraction and pitching motion during wind-up.

The objective of this study was to clarify lower trunk muscle contraction-induced fundamental changes during SLR

*Corresponding author. Tetsuya Nakao (E-mail: nakao@kansai.ac.jp)

©2017 The Society of Physical Therapy Science. Published by IPEC Inc.

This is an open-access article distributed under the terms of the Creative Commons Attribution Non-Commercial No Derivatives (by-nc-nd) License <<https://creativecommons.org/licenses/by-nc-nd/4.0/>>.



Fig. 1. SLR angle on single-leg standing

The subject stood in the upright posture with both hands placed on the hip and contracted the lower trunk muscles. The subject stood so as to align the acromion, greater trochanter, and lateral epicondyle in a vertical straight line and then raised one leg to the maximum level while retaining knee extension.

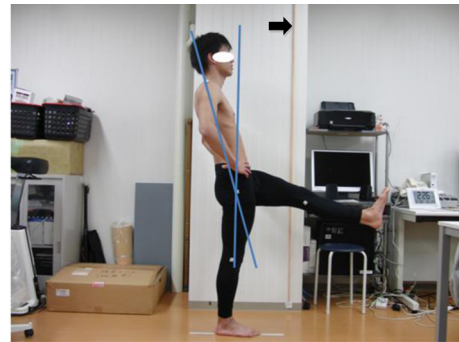


Fig. 2. Maximum posterior tilt angle of the trunk after SLR on single-leg standing

Keen extension on the support side was maintained. The posterior tilt angle was measured regarding a vertical line drawn from the greater trochanter as a baseline axis and a line connecting the greater trochanter and acromion as a moving axis. Vertical line (➡) was drawn on the wall.

on single-leg standing, focusing on its posture control at the time of lower limb lifting with knee extension caused from wind-up to early-cocking. So, SLR alignment and COP position during single-leg standing and step position after SLR on single-leg standing were measured in different lower trunk muscle contraction types. Lower trunk muscle contraction types were Abdominal Expansion (AE), Abdominal Bracing (AB), and Abdominal Cave-in (AC)⁷⁾.

SUBJECTS AND METHODS

Ten healthy normal males participated in this study (age: 20.9 ± 1.6 years old, height: 174.5 ± 3.6 cm, body weight: 68.6 ± 8.5 kg). All subjects could accurately perform lower trunk muscle contraction types AE, AB, and AC.

The lower trunk muscle contraction types were classified into three types, because of importance to synchronize the timing of exercise and respiration⁷⁾. In AE, the abdominal circumference increases from that in resting expiration due to inhalation of air, and abdominal lateral muscle activity is observed. In AB, abdominal lateral muscle activity is observed without a change in the abdominal circumference from that in resting expiration. In AC, the abdominal circumference is decreased from the resting expiratory position by exhalation and physiological lumbar lordosis, and muscle thickness increases due to concentric contraction of the abdominal lateral muscles⁸⁻¹¹⁾.

The breathing types were confirmed using a respiration wave sensor (DL-230, S&M Co., Ltd.), and the abdominal circumference was measured using a measure. The muscle contraction types and muscle thickness were determined using a diagnostic ultrasound imaging system (LOGIQ e, GE Healthcare Japan) and electromyogram analysis system (Biolog DL-3100, S&M Co., Ltd.)^{12, 13)}.

The maximum SLR angle and COP position during single-leg standing with SLR were measured. The subjects stood on both legs placing their hands on the bilateral hips in order to fix their scapulars and contracted the lower trunk muscles. They stood so as to align the acromion, greater trochanter, and lateral malleolus in a vertical line. Then, they raised one leg to the maximum level while retaining knee extension. The COP position (shift of the mean center of anteroposterior sway) at the maximum level of SLR on single-leg standing was measured using a lower limb gravimeter (G-620, Anima Corp.). The measurement time and sampling frequency were set at 10 seconds and 20 Hz, respectively. The SLR angle was measured using an image analysis system (Dartfish software 5.5, DARTFISH) (Fig. 1). Measurement was initiated with SLR from standing on both legs with AE, followed by SLR from standing on both legs with AB and then SLR from standing on both legs with AC.

The maximum posterior tilt angle and COP position were measured after maximum SLR on single-leg standing. The trunk was tilted backward from the standing SLR posture while contracting the lower trunk muscles, and the posterior tilt angle of the trunk and COP position were measured during posterior tilting. The knee of the supporting leg was kept extended. The posterior tilt angle was measured regarding a vertical line drawn from the right greater trochanter as a baseline axis and a line connecting the right greater trochanter and right acromion as a moving axis. The measurement devices and order of measurement were the same as described above (Fig. 2).

The position of the left heel grounded after leftward rotation of the body from SLR on single-leg standing was measured using a carpenter's square ruler. The baseline was set to a vertical line drawn from a line drawn along the lateral side of the right foot. The distance between the grounded left heel and baseline was measured as the cross step distance. A distance of the step position on the right side of the baseline was judged as cross step+. The order of measurement was the same as described above (Fig. 3).

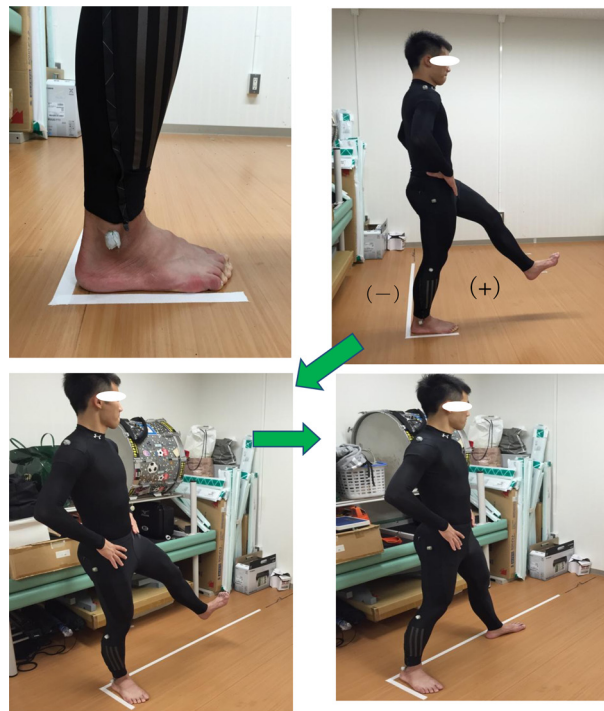


Fig. 3. Step position after rotating the body from SLR on single-leg standing

The step position was measured at the front heel grounded site after forward rotation of the body from SLR on single-leg standing using a carpenter's square ruler. The baseline was set to a vertical line drawn from a line drawn along the lateral side of the rear foot. The distance between the grounded front heel and baseline was measured. The distance of the step position on the right side of the baseline was regarded as cross step+.

Table 1. Body alignment of single leg standing

	AE	AB	AC	AE-AB	AE-AC	AB-AC
Single leg standing SLR						
F-B position of COP (cm)	1.61 ± 1.02	0.69 ± 1.23	-0.41 ± 1.36	*	*	*
Angle of SLR (°)	58.4 ± 9.3	61.6 ± 9.9	69.6 ± 9.5	*	*	*
From single leg stanging SLR						
F-B position of COP (cm)	-0.03 ± 1.25	-0.9 ± 1.51	-2.02 ± 1.33	*	*	*
Angle of trunk posterior tilt (°)	19.4 ± 4.4	17.5 ± 3.4	14.4 ± 3.6	*	*	*
Instep distance	12.5 ± 8.7	7.3 ± 8.7	-8.1 ± 14.5	*	*	*

Values are mean ± standard deviation (SD).

*Significant differences ($p < 0.05$)

F-B position of COP: The forward and backward position shift of the foot pressure

The COP (-) means backward position from line of navicular and cuboid.

Normality was confirmed in all measurement data using Shapiro-Wilk (analysis software, IBM SPSS Statistics 19), but homogeneity could not be confirmed. Thus, the significance of differences among groups was confirmed using Friedman's nonparametric test, and between-group comparison was performed using Wilcoxon signed-rank test after confirming the significance of difference ($p < 0.05$).

This study was approved by Kansai University of Health Sciences Ethics Committee, and informed consent was obtained from the subjects after explaining risks and safety.

RESULTS

The SLR angle significantly decreased on single-leg standing with AE ($58.4 \pm 9.3^\circ$) compared with those with AB ($61.6 \pm 9.9^\circ$) and AC ($69.6 \pm 9.5^\circ$), and it significantly decreased on single-leg standing with AB compared with that with AC ($p < 0.05$) (Table 1).

The COP position significantly shifted forward on single-leg standing with AE (1.61 ± 1.02 cm) compared with those with AB (0.69 ± 1.23 cm) and AC (-0.41 ± 1.36 cm), and it was significantly shifted forward on single-leg standing with AB compared with that with AC ($p < 0.05$) (Table 1).

The posterior tilt angle of the trunk significantly increased on single-leg standing with AE ($19.4 \pm 4.4^\circ$) compared with those with AB ($17.5 \pm 3.4^\circ$) and AC ($14.4 \pm 3.6^\circ$), and it significantly increased on single-leg standing with AB compared with that with AC ($p < 0.05$) (Table 1).

The COP position in posterior tilt of the trunk with AE (-0.03 ± 1.25 cm) significantly shifted forward compared with those with AB (-0.9 ± 1.51 cm) and AC (-2.02 ± 1.33 cm), and it significantly shifted forward in posterior tilt of the trunk with AB compared with that with AC ($p < 0.05$) (Table 1).

The cross step distance significantly increased after rotation with AE (12.5 ± 8.7 cm) compared with those with AB (7.3 ± 8.7 cm) and AC (-8.1 ± 14.5 cm), and it significantly increased after rotation with AB than that with AC ($p < 0.05$) (Table 1).

DISCUSSION

When the lower trunk muscles are contracted to perform AE and AB, the abdominal organs are lowered while increasing the abdominal circumference and the external sphincter of the anus is relaxed similarly to that in defecation¹⁴). In AB and AE not using pelvic floor muscle contraction, stabilization of the lumbosacral region by pelvic floor muscle action may be lacking^{15–18}). In AC, since the thoracolumbar fascia is tensed by concentric contraction of the transverse abdominal and pelvic floor muscles, it becomes the lower trunk muscle contraction type stabilizing the lumbosacral region^{15–18}).

It has been clarified that muscle forces of the four limbs and trunk significantly decrease in AB compared with those in AC⁷), suggesting that securing stability of the lumbosacral region was difficult in AB, which may have resulted in the reduction of the SLR angle on single-leg standing with AE and AB compared with that with AC. It was assumed that since the COP position was already shifted forward by AE or AB, the center of gravity of the raised leg could not be shifted forward and increasing the SLR angle was difficult. When AC was performed during SLR on single-leg standing, the COP position shifted backward, and the SLR angle on single-leg standing with AC was larger than those with AE and AB, suggesting that posterior tilting of the trunk and augmentation of lower limb elevation after SLR on single-leg standing were difficult.

It has been clarified that performing AE and AB on single-leg standing shifts COP anteromedially and makes the pelvis face the elevation side⁶), trunk tilts backward when loading anteromedially of the foot induced cross step⁵). Also, it was clarified that the posterior tilt angle of the trunk was increased during SLR on single-leg standing with AE and AB compared with that with AC in this study. So that increasing of posterior tilt angle during SLR on single leg standing may have extended the anterior soft tissue of the hip joint and increased the cross step distance. When the pelvis was rotated toward the elevated side from this state, the anterior surface soft tissue of the hip joint may have tensed from the early phase and limited the pelvic rotatory movement, increasing the cross step distance. Accordingly, it is assumed that performing AC in wind-up increases the left leg elevation angle, decreases the posterior tilt angle of the trunk, and decreases the cross step distance. We are planning to clarify the relationship between lower trunk muscle contraction in wind-up and the cross step distance in the late-cocking phase in pitching motion.

ACKNOWLEDGEMENT

We are grateful to Mr. Ilseong Song and members of the study group of kinetic chain & injury prevention for their participation in this study.

REFERENCES

- 1) Kneighbaum E, Berthelsk M: Biomechanics A qualitative approach for studying human movement, 4th ed. Benjamin Cummings, 1995, pp 335–354.
- 2) MacWilliams BA, Choi T, Perezous MK, et al.: Characteristic ground-reaction forces in baseball pitching. *Am J Sports Med*, 1998, 26: 66–71. [[Medline](#)]
- 3) Hirashima M, Yamane K, Nakamura Y, et al.: Kinetic chain of overarm throwing in terms of joint rotations revealed by induced acceleration analysis. *J Bio-mech*, 2008, 41: 2874–2883. [[Medline](#)] [[CrossRef](#)]
- 4) Kageyama M, Sugiyama T, Kanehisa H, et al.: Difference between adolescent and collegiate baseball pitchers in the kinematics and kinetics of the lower limbs and trunk during pitching motion. *J Sports Sci Med*, 2015, 14: 246–255 eCollection. [[Medline](#)]
- 5) Morihara T, Matsui T, Takashima M: Pitching disorder thinking from kinetic chain. Tokyo: Zen-nihonbyoinshuppankai, 2014. (in Japanese)
- 6) Nakao T, Masuda K, Kanai S, et al.: Pelvic rotation angle and center of foot pressure with the lower trunk muscular contractions on single stance. *Jpn J Phys Fit Sport Med*, 2011, 60: 352 (in Japanese).
- 7) Nakao T, Tsujita J, Yamashita Y, et al.: Influences on motor function caused by the lower trunk muscular contractions. *Jpn J Physiol Anthropol*, 2015, 20: 135–145 (in Japanese).
- 8) Grenier SG, McGill SM: Quantification of lumbar stability by using 2 different abdominal activation strategies. *Arch Phys Med Rehabil*, 2007, 88: 54–62. [[Medline](#)] [[CrossRef](#)]
- 9) Richardson C, Jull G, Toppenberg R, et al.: Techniques for active lumbar stabilisation for spinal protection: a pilot study. *Aust J Physiother*, 1992, 38: 105–112.

[\[Medline\]](#) [\[CrossRef\]](#)

- 10) O'Sullivan PB, Phytz GD, Twomey LT, et al.: Evaluation of specific stabilizing exercise in the treatment of chronic low back pain with radiologic diagnosis of spondylolysis or spondylolisthesis. *Spine*, 1997, 22: 2959–2967. [\[Medline\]](#) [\[CrossRef\]](#)
- 11) Barnett F, Gillear W: The use of lumbar spinal stabilization techniques during the performance of abdominal strengthening exercise variations. *J Sports Med Phys Fitness*, 2005, 45: 38–43. [\[Medline\]](#)
- 12) Hodges PW, Pengel LH, Herbert RD, et al.: Measurement of muscle contraction with ultrasound imaging. *Muscle Nerve*, 2003, 27: 682–692. [\[Medline\]](#) [\[Cross-Ref\]](#)
- 13) Marshall P, Murphy B: The validity and reliability of surface EMG to assess the neuromuscular response of the abdominal muscles to rapid limb movement. *J Electromyogr Kinesiol*, 2003, 13: 477–489. [\[Medline\]](#) [\[CrossRef\]](#)
- 14) DeLancey JO: Anatomy and biomechanics of genital prolapse. *Clin Obstet Gynecol*, 1993, 36: 897–909. [\[Medline\]](#) [\[CrossRef\]](#)
- 15) Richardson AC, Edmonds PB, Williams NL: Treatment of stress urinary incontinence due to paravaginal fascial defect. *Obstet Gynecol*, 1981, 57: 357–362. [\[Medline\]](#)
- 16) Tajiri K, Huo M, Maruyama H: Effects of co-contraction of both transverse abdominal muscle and pelvic floor muscle exercises for stress urinary incontinence: a randomized controlled trial. *J Phys Ther Sci*, 2014, 26: 1161–1163. [\[Medline\]](#) [\[CrossRef\]](#)
- 17) Tajiri K: An approach to assessment of female urinary incontinence risk using the thickness of the transverse abdominal muscle. *J Phys Ther Sci*, 2012, 24: 43–46. [\[CrossRef\]](#)
- 18) Smith MD, Coppieters MW, Hodges PW: Postural response of the pelvic floor and abdominal muscles in women with and without incontinence. *Neurorol Urodyn*, 2007, 26: 377–385. [\[Medline\]](#) [\[CrossRef\]](#)