

Dual-layer detector spectral computed tomography quantitative parameters for predicting pathological complete remission after neoadjuvant treatment of breast cancer

Shaolan Guo^{1,2}, Dandan Wang³, Qian Zhao⁴, Zhao Bi⁴, Wanhu Li⁴, Jian Zhu^{1,5,6}

¹Department of Radiation Oncology Physics & Technology, Cancer Hospital of Shandong First Medical University, Jinan, China; ²Center of Medical Imaging, Children's Hospital Affiliated to Shandong University, Jinan Children's Hospital, Jinan, China; ³Department of Gynecological Oncology, Zhongnan Hospital of Wuhan University, Wuhan, China; ⁴Department of Medical Imaging, Shandong Cancer Hospital and Institute, Shandong First Medical University and Shandong Academy of Medical Sciences, Jinan, China; ⁵Center of Research in Information BioMedical Sino-France, Nanjing, China; ⁶Shandong Provincial Key Medical and Health Laboratory of Pediatric Cancer Precision Radiotherapy (Shandong Cancer Hospital), Jinan, China

Contributions: (I) Conception and design: S Guo, Q Zhao; (II) Administrative support: J Zhu; (III) Provision of study materials or patients: Z Bi; (IV) Collection and assembly of data: S Guo, W Li; (V) Data analysis and interpretation: S Guo, D Wang; (VI) Manuscript writing: All authors; (VII) Final approval of manuscript: All authors.

Correspondence to: Jian Zhu, MD, PhD. Department of Radiation Oncology Physics & Technology, Cancer Hospital of Shandong First Medical University, Ji-Yan Rd., Jinan 250117, China; Center of Research in Information BioMedical Sino-France, No. 2 Sipailou Rd., Nanjing 210096, China; Shandong Provincial Key Medical and Health Laboratory of Pediatric Cancer Precision Radiotherapy (Shandong Cancer Hospital), Jinan, China. Email: zhujian@sdfmu.edu.cn.

Background: Breast cancer (BC) is a common cancer among women worldwide, and although the use of neoadjuvant therapy (NAT) for BC has become more widespread, there is no standardized prediction of the efficacy of NAT for BC. This study aimed to evaluate the value of quantitative parameters of dual-layer detector spectral computed tomography (DLCT) in predicting whether BC patients can achieve pathological complete response (pCR) after NAT.

Methods: Patients who were first diagnosed with BC in Shandong Cancer Hospital and Institute and received only NAT before surgery were selected for participation in this study. All breast computed tomography (CT) imaging examinations were performed using DLCT, within 1 week before initiating NAT. The gold standard for evaluating the effect of NAT is pathologic response established at surgery. The Miller-Payne grading system was applied to assess the response to NAT. Quantitative parameters were extracted from DLCT, including CT value, normalized CT value, iodine concentration (IC), normalized iodine concentration (NIC), the slope of the spectral Hounsfield unit (HU) curve, effective atomic number, and the normalized effective atomic number. The Mann-Whitney U test was used to compare the distribution differences of DLCT quantitative parameters between the pCR group and the non-pCR group. The diagnostic performance of the quantitative parameters was analyzed by receiver operating characteristic curve. **Results:** In the neoadjuvant chemotherapy group (n=80), compared with the non-pCR group, the slope of the spectral HU curve, IC, effective atomic number, and NIC of arterial phase in the pCR group were higher, and the difference was statistically significant (P<0.05); area under the curve (AUC): 0.768, 0.791, 0.834, and 0.770, respectively. In the neoadjuvant targeted therapy group (n=40), compared with the pCR group, the CT value, IC, effective atomic number, and NIC of the arterial phase in the non-pCR group were higher, and the difference was statistically significant (P<0.05); AUC: 0.844, 0.813, 0.802, and 0.766,

[^] ORCID: 0000-0003-2257-4593.

respectively. There was no significant difference (P>0.05) in DLCT venous phase quantitative parameters between pCR and non-pCR in 70 patients treated with NAT.

Conclusions: The study suggested a possibility that DLCT provided a potential tool to develop a model for predicting pCR to NAT in BC.

Keywords: Breast cancer (BC); dual-layer detector spectral computed tomography (DLCT); neoadjuvant therapy (NAT); pathological complete remission; quantitative parameters

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Introduction

As a common cancer among women around the world, breast cancer (BC) has attracted widespread attention. On 1 February 2024, according to the latest data released by the Agency for Research on Cancer, the number of new cases of BC in the world reached 2.3 million, ranking second among cancers in the world, and becoming the fourth highest cause of cancer-related deaths with 670,000 deaths (1). In contemporary times, the management of BC involves a comprehensive strategy that includes surgical intervention, chemotherapy, radiation therapy, and systemic treatment (2-4). The aim is to combine and sequence these different treatments according to each patient's needs and preferences and to de-escalate treatment whenever possible while preserving oncological safety (5). Neoadjuvant therapy (NAT) has become a treatment option for patients with early-stage BC (6,7). NAT has the potential to decrease tumor size through preoperative intervention, thereby converting inoperable BC to operable BC and non-breastconserving BC to breast-conserving BC. Additionally, it can enhance the likelihood of successful surgical outcomes and provide valuable in vivo drug sensitivity information to guide postoperative treatment (6). NAT is frequently employed in 17-40% of early BC patients (8). The NAT strategy for BC has also continued to develop and evolve. The indication has shifted from being based on stage to comprehensively considering stage and molecular typing (9). The treatment model has been updated from single chemotherapy to chemotherapy combined with anti-human epidermal growth factor receptor 2 (HER2)-targeted therapy, chemotherapy combined with immunotherapy, endocrine therapy, and so on. The present advancement of NAT for BC primarily focuses on HER2-positive BC, triple-negative breast cancer (TNBC), and hormone receptor (HR)-positive BC based on molecular categorization (10). In the case of HER2-positive

BC, NAT has evolved from a singular chemotherapy regimen to a combination of chemotherapeutic agents and targeted medications. Notably, the dual targeting regimen of trastuzumab in conjunction with pertuzumab has emerged as the fundamental approach in NAT for HER2positive BC (11).

Ideally, it could imply an extremely favorable long-term outcome when a pathological complete response (pCR) is achieved after NAT (7,12). Roughly 20% of patients experience pCR following NAT, with variations in rates based on the subtype and stage of BC (13). Registry data shows that 40% of women with HER2-positive BC achieve pCR after NAT, with 23% among triple negative tumors and only 0.3% among luminal A tumors (9,14). Recent studies on dual HER2 blockade and carboplatin regimens in the treatment of triple-negative tumors have shown pCR rates as high as 68% and 80%, respectively, suggesting that pCR rates after NAT may increase further in the next years (13,15).

At present, BC patients who achieve pCR after NAT still have to undergo routine breast surgery without considering the obvious degree of pathological remission. In view of the high pCR rate of some subgroups after NAT, especially when breast-conserving surgery patients receive adjuvant whole breast radiotherapy, it should be questioned whether surgery is a redundant link in the overall management of this part of BC (5). If breast surgery is not performed, however, the standard method of determining response to NAT, being pathological examination of the surgical specimen, is not possible. The main impediments for potential elimination of breast surgery have been the fact that conventional and functional breast imaging techniques are incapable of accurate prediction of residual disease. In addition, a study showed that 10-35% of BCs were insensitive to NAT, and approximately 5% of patients had larger tumors after NAT (16); in these cases, NAT failed

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to exhibit a therapeutic effect and instead delayed surgical treatment. A recent meta-analysis discovered that patients who received NAT had a 15-year local recurrence rate that was 5.5% higher compared to those who received conventional chemotherapy (21.4% vs. 15.9%) (6). The varied outcomes of NAT, based on histopathological and molecular features, further complicate the accurate prediction of pCR prior to treatment (17), which is important for effective treatment planning. The increasing understanding of the variety of BC has led to a growing need for techniques that can help assess the early response to NAT in individual patients. There is a lack of imaging markers that enable noninvasive pretreatment prediction of pCR. Primary breast tumors and axillary lymph node metastases often respond similarly in pattern and degree of response (18). In this article, we mainly focus on the response in the breast to NAT.

Dual-layer detector spectral computed tomography (DLCT) is a new imaging technology offering functional imaging and molecular imaging. DLCT allows for the utilization of a dual-layer detector to capture both lowand high-energy photons within the same imaging beam. It offers energy spectrum analysis in the original data space, resulting in the generation of multi-parameter images. These images, including monoenergetic images and base material images, serve as analytical tools and quantitative indicators for clinical diagnosis. DLCT is capable of quantitatively measuring the concentration and decomposition, as well as inhibiting or enhancing the ability of materials such as iodine, water, calcium, or uric acid (19).

DLCT can provide 12 categories of energy parameters; this article will introduce a few commonly used parameters for breast diseases. By acquiring attenuation values at two different energy levels, it is possible to generate supplementary datasets, including an iodine no water, colorcoded Z-effective images and the spectral Hounsfield unit (HU) curve, alongside conventional computed tomography (CT) images. Its application in the field of breast diseases has begun to receive widespread attention, such as distinguishing tumor lesions, pathological classification, molecular subtypes, analyzing immunohistochemical biomarkers, and determining the stage of lymph nodes (20-25). Thus, we aimed to investigate the value of quantitative multiparametric data, such as iodine concentration (IC), the spectral HU curve, and effective atomic number (Z_{eff}) in predicting pathological complete remission after NAT of BC detected on DLCT. We present this article in accordance with the STARD reporting checklist (available

at https://qims.amegroups.com/article/view/10.21037/ qims-24-511/rc).

Methods

Patients

The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). This retrospective study was approved by the Ethics Committee of Shandong Cancer Hospital and Institute (approval No. SDTHEC 2023010022) and the requirement for individual consent for this retrospective analysis was waived. The patients who received NAT and underwent surgical treatment between 2019 and 2023 were consecutively enrolled in our study, and we obtained the imaging data and medical records of these patients. The inclusion criteria were as follows: (I) biopsy-verified primary BC without distant metastasis; (II) breast multiparametric DLCT performed before the biopsy; (III) complete NAT with no prior treatment; and (IV) surgery followed by a pathological examination performed after completion of NAT. The exclusion criteria were as follows: (I) combination treatment with multiple NAT regimens (chemotherapy + targeting + immunity); (II) ductal carcinoma in situ, inflammatory BC; (III) history of other malignant tumors; (IV) lack of some images (e.g., lack of arterial phase imaging); (V) low-quality images or the hardly visible lesion rendering difficulty with measurements (e.g., owing to motion artifacts); (VI) neoadjuvant immunotherapy (small sample size); and (VII) surgery was performed at an outside institution.

NAT and classification criteria

All patients received 6–8 cycles of NAT. Although there were some differences among the different patients, the treatment protocol and timeline followed the National Comprehensive Cancer Network guideline (26). All patients had not received any other treatment before or during treatment with NAT, and patients treated with multiple NAT methods in combination (chemotherapy + immunity + targeting) were excluded. Samples that meet the inclusion criteria were divided into two groups based on the treatment method, namely the neoadjuvant chemotherapy group (NC group) and the neoadjuvant targeted therapy group (NT group).

The indication for NAT in the 2023 Chinese Society of Clinical Oncology guidelines for the diagnosis and

Table 1 Quantitative distribution of pCK and non-pCK after neoadjuvant therapy								
Tractment methods	Arteria	l phase	Venous phase					
neament methods	pCR	Non-pCR	pCR	Non-pCR				
Neoadjuvant chemotherapy group	16	64	10	40				
Neoadjuvant targeted therapy group	16	24	8	12				

Table 1 Quantitative distribution of pCR and non-pCR after neoadjuvant therapy

pCR, pathological complete response.

treatment of BC is one of the following conditions: (I) large mass (>5 cm); (II) TNBC; (III) HER2-positive BC; (IV) axillary lymph node metastasis; and (V) the tumor is large and difficult to conserve breast, but there is still a willingness to conserve breast. In addition, the guidelines prioritize HER2-positive BC in recommending treatment options that include single- or dual-targeted drugs. Chemotherapy regimens that include anthracyclines and taxanes are preferred for TNBC. For HR-positive BC, anthracyclines combined with taxanes are recommended.

The NAT regimen of the enrolled patients was determined by two clinicians in Shandong Cancer Hospital and Institute. The grouping criteria were as follows: (I) NC group: a simple chemotherapy regimen containing chemotherapeutic drugs such as anthracyclines and taxanes, such as EC-T, AC-T, TAC, and AT; (II) NT group: chemotherapy combined with anti-HER2 targeted (trastuzumab and pertuzumab) therapy, such as TCbH, TCbHP, AC-THP, and THP.

Pathological assessment of response

All patients who received NAT underwent a comprehensive preoperative evaluation before treatment and the clinical staging of BC according to the American Joint Committee on Cancer (AJCC, 8th edition, 2018) (27), and according to the 2013 International Expert Consensus on the Primary Treatment of Early Breast Cancer in St. Gallen (28,29), BC was subdivided into four molecular subtypes, namely luminal A, luminal B, HER2-rich, and TNBC. The patient's clinical baseline data including menstrual status, estrogen receptor (ER), progesterone receptor (PR), HER2 and Ki-67 status, clinical stage, molecular typing, and so on, were collected.

The conventional histopathological analysis method was employed to assess the response to NAT for pathological evaluation. The Miller-Payne grading system (30) is a common method for assessing the pathological response to NAT in BC. This system evaluates treatment efficacy by categorizing the pathological response into five grades based on the comparison of tumor cell density and morphology between pre-treatment core biopsies and definitive surgical specimens. The Miller-Payne grading system is as follows:

- Grade 1: no change or some minor alteration in individual malignant cells, but no reduction in overall cellularity.
- Grade 2: a minor loss of tumor cells, but overall high cellularity; up to 30% reduction of cellularity.
- Grade 3: between an estimated 30% and 90% reduction in tumor cellularity.
- ✤ Grade 4: a marked disappearance of more than 90% of tumor cells such that only small clusters or widely dispersed individual cells remain (almost pCR).
- Grade 5: no invasive malignant cells identifiable in sections from the site of the tumor (pCR).

In this study, Grade 5 cases were classified as pCR. Grade 1–4 cases were classified as non-pCR. The grouping of this study is shown in *Table 1*.

Spectral CT image acquisition

All breast CT imaging examinations were performed using DLCT (Philips IQon Spectral CT; Philips, Amsterdam, Netherlands), within 1 week before initiating NAT. The imaging sequence included arterial phase iodine density map, color-coded Z-effective images, and the spectral HU curve, and conventional CT images, including venous phase images in some cases. A set of manual sketching examples in Spectral Diagnostic Suite is presented in *Figure 1*.

Image data were acquired on a DLCT unit (Philips IQon Spectral CT) in dual layer detector mode through two layers of detectors to simultaneously collect low- and highenergy data in all patients using standard CT protocols. The settings for the scanners were as follows: tube voltage, 100 kVp; reference tube current time product, 260–350 mAs; pitch, 1.375; reformatted section thickness, 5 mm.

Holland Philips IQon Spectral CT machine was used for chest biphasic enhanced scanning. The entire chest



Figure 1 A set of manual sketching examples in Spectral Diagnostic Suite. (A) Conventional computed tomography images; (B) effective atomic number; (C) the slope of the spectral HU curve. Ar, area; Av, average; SD, standard deviation; perim, perimeter; ROI, region of interest; HU, Hounsfield unit; A, anterior; P, posterior; L, left; R, right; F, female; WL, window level; WW, window width.

was examined from the superior opening of the thorax to the lower border of the costophrenic angle while taking a deep breath, encompassing the breast and armpit area. For contrast-enhanced scanning, an iodinated nonionic contrast media (ioversol, 320 mg/mL iodine; HENGRUI Medicine, Jiangsu, China) was administered through the right or left ulnar vein by a dual-head injector. The dosage was 1.5 mL/kg with a flow rate of 2.5 mL/s, followed by a bolus injection of 30 mL of saline given at the same flow rate. The ulnar vein on the opposite side of the suspected breast lesion was chosen for injection to prevent a beam hardening artifact in the axillary vein. Following the injection, the arterial phase scans began using a bolus-tracking method with a threshold of 250 HU in the descending aorta. The venous phase scanning was delayed by 45 seconds after the arterial phase scanning was completed.

DLCT image analysis

All the images were analyzed by using viewer software on a workstation (Intelli Space Portal version 10.0). DLCT quantitative parameters were measured by two radiologists (W.L., with 10 years of experience in breast and chest diagnostic imaging, and S.G., with 2 years of experience in post-reconstruction imaging, Philips) who were blinded to the immune histochemical results of invasive BC, by placing a circular region of interest (ROI), excluding any area of obviously gross necrosis, calcification, or large vessels. The immunohistochemical results of the puncture were unknown, and consistency analysis was performed by intraclass coefficient correlation (ICC), with the average of the two taken as the final result. The ROI region was selected according to the arterial phase image, and the ROI region was pasted on iodine density map and atomic number image using the copy function to ensure that the size and position of the ROI region are completely consistent. The CT value, IC, and Z_{eff} of the ROI were divided by the value of the aorta in the same layer, respectively, to obtain the normalized CT value (NCT), normalized iodine concentration (NIC), and normalized effective atomic number (NZ_{eff}). The slope of the spectral HU curve (λ_{HU}) was calculated as follows (23):

$$\lambda_{\rm HU} = \left(\rm HU_{40keV} - \rm HU_{70keV}\right) / 30$$
^[1]



Figure 2 The flowchart of this study, from initial retrieval to final study cohort.

Statistical analysis

Statistical analyses were performed using the commercially available statistical software SPSS 22.0 (IBM Corp., Armonk, NY, USA). The ICC was used to evaluate the consistency of the two readers in the measurement of quantitative parameters of DLCT, and an ICC >0.75 indicated good consistency. In addition to age, clinical baseline data were selected based on sample size characteristics for Fisher's exact Chi-squared test. Age was used to analyze the significance of differences by *t*-test. The Mann-Whitney *U* test was used to compare the distribution differences of DLCT quantitative parameters between the pCR group and the non-pCR group. Receiver operating characteristic (ROC) curve analysis was used to evaluate the diagnostic capacity of DLCT quantitative parameters, and the corresponding sensitivity and specificity were obtained. The level of significance was defined as P<0.05. The Mann-Whitney U test was a two-tailed analysis and the ROC curve analysis was a one-tailed analysis.

Results

Clinical baseline characteristics of patients

A total of 120 patients were enrolled in our study; all participants in this study are female. A flowchart of the study population is shown below (*Figure 2*). The patients' pathological results were verified by the pathology department of Shandong Cancer Hospital and Institute to meet the enrollment criteria. The pathological type of the patients was invasive cancer, and the clinical tumor node metastasis (cTNM) stages were all I–III. Detailed patient statistics are summarized in *Table 2*. The results of

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Clinical characteristics —	Neo	Neoadjuvant chemotherapy			Neoadjuvant targeted therapy			
	pCR	Non-pCR	P value	pCR	Non-pCR	P value		
Age (years)	50.1±10.7	47.5±10.7	0.153	49.3±11.7	48.9.1±10.6	0.223		
Menstrual status			0.833			0.833		
Non-menopausal	9 (56.3)	37 (57.8)		8 (50.0)	11 (45.8)			
Menopausal	7 (43.7)	27 (42.2)		8 (50.0)	13 (54.2)			
ER			0.573			0.272		
(+)	1 (6.3)	6 (9.4)		2 (12.5)	7 (29.2)			
()	15 (93.7)	58 (90.6)		14 (87.5)	17 (70.8)			
PR			0.655			0.261		
(+)	1 (6.3)	5 (7.8)		3 (18.8)	8 (33.3)			
()	15 (93.7)	59 (92.2)		13 (81.2)	16 (66.7)			
HER2			0.833			0.212		
(+)	0	2 (3.1)		15 (93.7)	19 (79.2)			
()	16 (100.0)	62 (96.9)		1 (6.3)	5 (20.8)			
Ki-67			0.028			0.165		
High expression (>20)	14 (87.5)	48 (75.0)		12 (75.0)	20 (83.3)			
Low expression (≤20)	2 (12.5)	16 (25.0)		4 (25.0)	4 (16.7)			
Clinical TNM stage			0.642			0.146		
I/II	11 (68.8)	40 (62.5)		9 (56.2)	6 (25.0)			
III	5 (31.2)	24 (37.5)		7 (43.8)	18 (75.0)			
Molecular typing			0.629			0.629		
Luminal A	0	3 (4.7)		0	1 (4.2)			
Luminal B	1 (6.3)	1 (1.6)		2 (1.3)	6 (25.0)			
HER2-rich	0	2 (3.1)		14 (8.7)	17 (70.8)			
Triple negative	15 (93.7)	58 (90.6)		0	0			

Table 2 Characteristics of patients treated with neoadjuvant therapy

Data are presented as mean \pm standard deviation or n (%). (+) = positive, (-) = negative. pCR, pathological complete response; ER, estrogen receptor; PR, progesterone receptor; HER2, human epidermal growth factor receptor 2; TNM, tumor node metastasis.

Chi-squared test showed that the efficacy of NAT was not correlated with clinical factors such as menstrual status, ER, PR, HER2, cTNM stage, and molecular typing (P>0.05). However, the results of Chi-squared test showed that the efficacy of NC was correlated with Ki-67 (P=0.028).

Comparison of DLCT quantitative parameters of pathological pCR and non-pCR in BC patients after NAT

The ICC value measured by the two physicians for arterial

phase DLCT quantitative parameters was 0.942 (range, 0.801 to 0.979), indicating that the quantitative parameters measured by the two doctors have strong consistency. In the NC group, the pCR group tended to display higher arterial phase $\lambda_{\rm HU}$, IC, $Z_{\rm eff}$, and NIC compared with the non-pCR group, and the difference was statistically significant (P<0.05). In the NT group, the non-pCR group tended to display higher arterial phase CT value, IC, $Z_{\rm eff}$, and NIC compared with the difference was statistically significant (P<0.05), and the difference was statistically significant (Table 3).

Parameters -	Neoadjuvant chemotherapy			Neoadjuvant targeted therapy			
	pCR	Non-pCR	P value	pCR	Non-pCR	P value	
Arterial phase λ_{Hu} (HU/keV)	2.35±0.387	1.37±0.107	0.018	1.725±0.336	2.199±0.137	0.057	
Arterial phase CT value (HU)	64.148±19.117	54.264±11.382	0.496	53.150±3.909	65.889±2.013	0.010	
Arterial phase NCT (HU)	0.260±0.035	0.214±0.012	0.517	0.199±0.016	0.243±0.011	0.057	
Arterial phase IC (mg/mL)	1.346±0.256	0.732±0.065	0.010	0.805±0.112	1.173±0.091	0.020	
Arterial phase NIC	0.178±0.042	0.089±0.009	0.018	0.085±0.132	0.122±0.009	0.047	
Arterial phase Z_{eff}	8.056±0.106	7.700±0.035	0.003	7.757±0.065	7.944±0.039	0.025	
Arterial phase NZ _{eff}	0.765±0.023	0.712±0.017	0.088	0.711±0.010	0.725±0.007	0.343	

Table 3 Correlation of dual-layer detector spectral computed tomography arterial phase quantitative parameters with pCR after neoadjuvant therapy of breast cancer

Data are presented as mean \pm standard deviation. pCR, pathological complete response; λ_{Hu} , the slope of the spectral HU curve; HU, Hounsfield unit; CT, computed tomography; NCT, normalized CT value; IC, iodine concentration; NIC, normalized iodine concentration; Z_{eff} , effective atomic number; NZ_{eff}, normalized effective atomic number.

Analysis of diagnostic efficiency of DLCT quantitative parameters

The quantitative parameters with statistically significant differences between pCR and non-pCR in BC patients after NAT were included in the ROC curve (Figure 3 and Table 4). In the NC group, the results showed that the area under the curve (AUC) of λ_{HU} , IC, Z_{eff} , and NIC were 0.768, 0.791, 0.834, and 0.770, respectively, and the difference was statistically significant (P<0.05). Taking the arterial phase Z_{eff} of 7.97 as the diagnostic threshold, it had the highest diagnostic efficiency in differential diagnosis of pCR versus non-pCR (AUC of 0.834, sensitivity of 62.50%, specificity of 90.63%). In the NT group, the results showed that the AUC of CT value, IC, Z_{eff}, and NIC were 0.844, 0.813, 0.802, and 0.766, respectively, and the difference was statistically significant (P<0.05). Taking the arterial phase CT value of 57.3 as the diagnostic threshold, it had the highest performance in differential diagnosis of pCR versus non-pCR (AUC of 0.844, sensitivity of 75.00%, specificity of 91.67%).

Statistical analysis of DLCT venous phase quantitative parameters

Our study included 120 patients, among whom 70 included venous phase images as well as arterial phase images. The ICC value of the quantitative parameters measured by the two physicians for venous phase DLCT was 0.878 (range, 0.791 to 0.970), indicating that the quantitative data measured by the two physicians had strong consistency. We obtained the quantitative parameters of DLCT venous phase according to the same method, and statistical analysis was performed using the Mann-Whitney U test. The results showed that there was no significant difference (P>0.05) in DLCT venous phase quantitative parameters between pCR and non-pCR (*Table 5*).

Discussion

Currently, there is still no standard method to predict responses to NAT, and which diagnostic tools can accurately confirm or rule out residual disease in the breast after NAT remains to be determined. At present, there are a variety of imaging methods available to predict the feasibility of NAT for BC, but they all have some limitations. Multiple small prospective and retrospective trials have produced varying but generally mediocre results in terms of the diagnostic accuracy of imaging in determining residual disease after NAT (31,32). Diagnostic accuracy might also depend on tumor biology (33). Dynamic contrastenhanced magnetic resonance imaging (DCE MRI) of the breast offers the highest diagnostic accuracy in primary tumor therapy response assessment among the currently established methods (physical examination, mammography, and ultrasound) (31). Based on DCE MRI feature analysis, combined with intratumoral and peri-tumor dynamic enhanced magnetic resonance imaging texture features can accurately predict the pCR, with a reported AUC value of 0.74 after NAT (34). In a combined analysis of six studies,



Figure 3 ROC curve analysis of dual-layer detector spectral computed tomography quantitative parameters for the differential diagnosis of neoadjuvant treatment in breast cancer. (A) Neoadjuvant chemotherapy group; (B) neoadjuvant targeted therapy group. λ_{HU} , the slope of the spectral Hounsfield unit curve; IC, iodine concentration; Zeff, effective atomic number; NIC, normalized iodine concentration; CT, computed tomography; ROC, receiver operating characteristic.

Table 4 Receiver operating	characteristic curve a	analysis of dual-lay	er detector spectra	l computed	l tomography	⁷ quantitative	parameters for	the
differential diagnosis of neoad	ljuvant treatment in l	breast cancer						

Parameters	AUC (95% CI)	Threshold of parameter	Sensitivity (%)	Specificity (%)	P value			
Neoadjuvant chemotherapy pCR vs. non-pCR								
Arterial phase $\lambda_{\rm Hu}$ (HU/keV)	0.768 (0.5914–0.9438)	1.27	100.00	50.00	0.021			
Arterial phase IC (mg/mL)	0.791 (0.6314–0.9506)	0.66	100.00	50.00	0.012			
Arterial phase Z_{eff}	0.834 (0.6803–0.9877)	7.97	62.50	90.63	0.004			
Arterial phase NIC	0.770 (0.5747–0.9644)	0.15	50.00	96.88	0.020			
Neoadjuvant targeted therapy pCR vs. non-pCR								
Arterial phase CT value (HU)	0.844 (0.6403–1.0472)	57.3	75.00	91.67	0.011			
Arterial phase IC (mg/mL)	0.813 (0.6248–1.0002)	1.09	87.50	66.67	0.021			
Arterial phase Z_{eff}	0.802 (0.6097–0.9944)	7.92	100.00	58.33	0.025			
Arterial phase NIC	0.766 (0.5567–0.9746)	0.13	100.00	50.00	0.049			

pCR, pathological complete response; λ_{Hu} , the slope of the spectral HU curve; HU, Hounsfield unit; IC, iodine concentration; Z_{eff} , effective atomic number; NIC, normalized iodine concentration; CT, computed tomography; AUC, area under the curve; CI, confidence interval.

the positive predictive value (ability to correctly predict the presence of residual disease at final pathologic examination) was high at 93%. The negative predictive value (the ability to correctly predict disease at the final pathological examination) was only 65%, which reduced the overall diagnostic accuracy to 84% (35). In addition, changes in pharmacologic kinetic model parameters have been investigated in BC patients undergoing NC. Two published systematic reviews suggest that the volume transfer constant

(K^{trans}) is a promising parameter for early identification of treatment response (36,37). Although clinical DCE MRI is routinely performed in accordance with the standards of the American Society of Radiology, the use of DCE MRI for pharmacokinetic analysis is still in the research stage (31).

Despite these promising data, DCE MRI is currently not reliable enough to allow patients to avoid surgical resection after a complete imaging response (31); limitations remain in detecting small tumor foci scattered after NAT (34,38).

 Table 5 Statistical analysis of dual-layer detector spectral computed tomography venous phase quantitative parameters in differential diagnosis of neoadjuvant therapy for breast cancer

Parameters –	Neoadjuvant chemotherapy			Neoadjuvant targeted therapy			
	pCR	Non-pCR	P value	pCR	Non-pCR	P value	
Venous phase λ_{Hu} (HU/keV)	3.206±0.698	2.611±0.788	0.148	2.960±0.934	3.593±0.931	0.352	
Venous phase CT value (HU)	71.712±8.157	72.061±14.649	0.921	74.825±13.532	88.838±15.070	0.067	
Venous phase NCT (HU)	0.518±0.098	0.521±0.120	0.921	0.510±0.136	0.628±0.097	0.171	
Venous phase IC (mg/mL)	1.512±0.314	1.320±0.370	0.336	1.508±0.443	1.807±0.449	0.476	
Venous phase NIC	0.388±0.087	0.328±0.104	0.216	0.373±0.139	0.433±0.094	0.610	
Venous phase $Z_{_{eff}}$	8.134±0.158	8.037±0.203	0.303	8.138±0.216	8.275±0.216	0.476	
Venous phase NZ_{eff}	0.890±0.021	0.871±0.032	0.272	0.880±0.036	0.892±0.020	0.762	

Data are presented as mean \pm standard deviation. pCR, pathological complete response; λ_{Hu} , the slope of the spectral HU curve; HU, Hounsfield unit; CT, computed tomography; NCT, normalized CT value; IC, iodine concentration; NIC, normalized iodine concentration; Z_{eff} , effective atomic number; NZ_{eff}, normalized effective atomic number.

It may overestimate or underestimate the residual lesions, and its accuracy is also closely related to the morphology, histology, atrophy pattern, and molecular subtypes of the tumor (39,40). In diffuse cell loss, tumors degenerate in a more uneven manner, leaving multiple scattered foci of single tumor cells after chemotherapy, often with little or no change in overall tumor size (41).

Positron emission tomography has a sensitivity of 84.0% and a specificity of 66.0% in predicting pCR after NAT. It can be used to identify non-remission lesions and replace non-cross-resistant NAT regimens in the early stage of NAT (42). Formation of tumor fibrosis occurs after NAT, residual intraductal carcinoma, and tumor remaining after the disappearance of invasive cancer components. The change in density leads to inaccurate evaluation of residual tumors by mammography and ultrasound (43).

Minimally invasive image-guided biopsy has demonstrated potential in detecting residual disease in the breast following NAT (44). Nonetheless, conflicting concerns emerge: for instance, the sensitivity and specificity of image-guided biopsy may be influenced by factors such as molecular subtypes, tumor heterogeneity, and the dimensions of both initial and residual imaging abnormalities, which may present challenges in terms of ease and accuracy of sampling (45).

Future clinical trials may explore the incorporation of biomarkers alongside image-guided biopsies to predict pCR without necessitating surgical intervention, as this approach has the potential to enhance diagnostic precision. Early research has shown that the alpha- and gamma-adaptin binding protein monotherapy biomarker can predict pCR in small samples with an accuracy of 78–100% (46). Other studies have shown that higher levels of tumor-infiltrating lymphocytes and anti-HER2 CD4⁺ T-helper type 1 are associated with higher polymerase chain reaction ratios (47,48). However, these biomarkers have not yet been clinically confirmed.

Considering there is still no standard method to predict responses to NAT, this study aimed to evaluate the value of quantitative parameters of DLCT for pretreatment prediction of pCR to NAT for BC.

The recognized imaging method for NAT evaluation is DCE MRI; however, it still has some shortcomings and many contraindications. CT examination is convenient, fast, affordable, and can be "one-stop" scanning. It cannot only observe breast lesions, but also understand lymph node and lung metastases. As a new technology for CT examination, DLCT is increasingly being used and has been shown to be useful in tumor imaging across multiple organ systems (49-51). Based on the concept that biomedical images contain information that may reflect underlying pathophysiology, and that their relationships could be revealed through quantitative image analyses, quantitative parameters of DLCT turn medical images into minable data to improve diagnostic, prognostic, and predictive accuracy, thereby bridging the gap between medical imaging and personalized medicine. Iodine density maps provide quantitative information about tissue vascularity and perfusion. Virtual monoenergetic images at lower keV allow enhancement

of iodine and could lead to a better delineation of breast lesions that contain iodine, thus increasing their visibility and detectability (49,52). Some studies have found that quantitative parameters of dual energy CT may allow estimating the benign or malignant nature of breast masses, such as NIC, λ_{HU} , and NZ_{eff} (21,25,53). Using colorcoded Z_{eff} images is more efficient than comparing HU values on traditional CT scans for differentiating between various tissues based on their effective atomic number (49,52). Wang et al. (54) found that venous phase NIC, as well as arterial and venous phase NZ_{eff}, can distinguish between the luminal A and non-luminal A subtypes. Some researchers have shown that it can be used to distinguish between positive benign focal findings that do not require further clarification and suspicious or positive malignant focal findings, thus helping to avoid unnecessary followup examinations (21,53,54). Dual energy CT can predict the pathological classification, molecular subtype, and immunohistochemical classification of BC (24,25,54,55). To the best of our knowledge, our study is the first to predict breast pCR of NAT using quantitative parameters of DLCT. No invasive procedure was needed in our study. Therefore, we evaluated the value of DLCT quantitative parameters in predicting pCR before NAT for BC. Our research shows that DLCT can provide useful value in predicting the efficacy of NAT in BC patients.

We explored the potential reasons for the significant differences in arterial phase DLCT parameters between pCR and non-pCR groups. The DLCT iodine uptake value is used to calculate the actual IC of the contrast agent in the enhanced image, which more accurately reflects the blood supply and enhancement characteristics of the tissue than the CT value. The iodine map is the distribution map that the DLCT reflects the iodine uptake (49,56). In this study, there were differences in IC and NIC between the pCR and non-pCR groups. This may have been due to the different number of new blood vessels in the lesion and the inflammatory reaction caused by tumor cell degeneration and necrosis leading to changes in vascular permeability, resulting in different IC in the lesion. The arterial and venous phase energy spectrum curves of BC patients showed a downward trend. As the keV level rises to about 70 keV, the energy spectrum curves tend to be parallel, so the slope of the 40-70 keV range was selected for analysis in this study. The richer the blood vessels in the tumor tissue, the more the iodine uptake, and the more obvious the attenuation of the energy spectrum curve. Therefore, the λ_{HU} can indirectly reflect the tumor by reflecting the blood

supply. As an important parameter of DLCT, the principle of $Z_{\rm eff}$ is to add the information of material composition to each pixel and present it in the form of color quantization. In this study, the difference of $Z_{\rm eff}$ value between pCR and non-pCR groups reflects the difference of material composition between the two groups.

In this study, our results showed that there is a correlation between DLCT arterial phase quantitative parameters and BC pCR of NAT, which can provide a reference value for the clinical prediction of breast pCR of NAT. In addition, we obtained a total of seven sets of arterial phase data. Each group only screened out four parameters with statistically significant differences (P<0.05). After pairwise combination of other parameters (P>0.05), we further explored the potential value of DLCT quantitative parameters. Among the arterial phase parameters of DLCT in the NC group, a good diagnostic efficiency can also be achieved by combining arterial phase CT with NCT and NZ_{eff}. The AUC was 0.762 (sensitivity of 50.00%, specificity of 96.88%, P=0.23). But in the group NT, the diagnostic effect of the combination of parameters with P>0.05 was poor. This study has several limitations. Firstly, the number of cases was limited, the data of pCR and non-pCR distribution was unbalanced. Clinically, the number of BC patients who received a preoperative DLCT scan and completed NAT was relatively small. pCR of NAT was encountered less frequently, which is consistent with clinical observation. Nonetheless, the ROC curves exhibited sensitivity to imbalanced datasets, which may have impacted the interpretations drawn from the findings. Therefore, it is recommended that additional research involving larger sample sizes be conducted to corroborate the results of the current study through the application of thresholding techniques. Secondly, we focused only on two therapeutic methods in NAT, because the number of cases for other treatments was too small and there are no further studies. The quantity of data obtained from the venous phase images in these cases was limited, which could have led to significant errors in data analysis. Therefore, it is important to further explore the potential of quantitative parameters in the venous phase DLCT. Additional research utilizing larger sample sizes and a broader range of NATs for BC is necessary.

- (I) Predicting response to radiotherapy and chemotherapy:
 - Current limitation: currently, the application of DLCT in assessing the efficacy of radiotherapy and chemotherapy for cancer is limited. This is

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primarily because DLCT technology is still in its developmental phase and its full potential in this area has not been fully explored.

- Future research: future research should focus on developing and validating DLCT-based biomarkers that can predict the response of tumors to radiotherapy and chemotherapy. This could involve using DLCT to measure changes in tumor blood flow, perfusion, and metabolic activity, which are known to be affected by these treatments. By identifying such biomarkers, clinicians could potentially tailor treatment plans to individual patients, improving outcomes and reducing unnecessary toxicity.
- (II) Combining DLCT imaging with radiomics:
 - Current potential: in the era of personalized medicine, radiomics—the extraction of quantitative features from medical images—holds great promise for enhancing various aspects of BC management, including diagnosis, prognosis, prediction, monitoring, image-guided interventions, and evaluation of treatment response.
 - Integration with DLCT: by combining DLCT imaging with radiomics, researchers can potentially unlock new insights into BC biology and behavior. DLCT provides additional spectral information that can be used to differentiate tissues based on their iodine content and other material properties. This spectral information, combined with radiomic features, could lead to more accurate and personalized assessments of BC.
 - Future research: future research should explore the integration of DLCT and radiomics in BC management. This could involve developing and validating radiomic models that incorporate DLCT-derived features to improve diagnostic accuracy, predict prognosis, and monitor treatment response. Additionally, studies should investigate the potential of these models to guide personalized treatment decisions, such as selecting the most appropriate therapy based on an individual patient's tumor characteristics.

Conclusions

The present preliminary study suggested a possibility that DLCT provided a potential tool to predict pCR to NAT in BC. The early prediction of the efficacy of NAT offers the

opportunity to modify preoperative treatments or aids in determining surgical options.

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Footnote

Reporting Checklist: The authors have completed the STARD reporting checklist. Available at https://qims.amegroups.com/article/view/10.21037/qims-24-511/rc

Conflicts of Interest: All authors have completed the ICMJE uniform disclosure form (available at https://qims. amegroups.com/article/view/10.21037/qims-24-511/coif). The authors have no conflicts of interest to declare.

Ethical Statement: The authors are accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved. The study was conducted in accordance with the Declaration of Helsinki (as revised in 2013). The study was approved by ethics committee of Shandong Cancer Hospital and Institute (approval No. SDTHEC 2023010022) and individual consent for this retrospective analysis was waived.

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