ORIGINAL RESEARCH

Folate receptor-targeted liposomes loaded with a diacid metabolite of norcantharidin enhance antitumor potency for H22 hepatocellular carcinoma both in vitro and in vivo

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Abstract: The diacid metabolite of norcantharidin (DM-NCTD) is clinically effective against hepatocellular carcinoma (HCC), but is limited by its short half-life and high incidence of adverse effects at high doses. We developed a DM-NCTD-loaded, folic acid (FA)-modified, polyethylene glycolated (DM-NCTD/FA-PEG) liposome system to enhance the targeting effect and antitumor potency for HCC at a moderate dose based on our previous study. The DM-NCTD/FA-PEG liposome system produced liposomes with regular spherical morphology, with mean particle size approximately 200 nm, and an encapsulation efficiency >80%. MTT cytotoxicity assays demonstrated that the DM-NCTD/FA-PEG liposomes showed significantly stronger cytotoxicity effects on the H22 hepatoma cell line than did PEG liposomes without the FA modification ($P<0.01$). We used liquid chromatography–mass spectrometry for determination of DM-NCTD in tissues and tumors, and found it to be sensitive, rapid, and reliable. In addition, the biodistribution study showed that DM-NCTD liposomes improved tumor-targeting efficiency, and DM-NCTD/FA-PEG liposomes exhibited the highest efficiency of the treatments ($P<0.01$). Meanwhile, the results indicated that although the active liposome group had an apparently increased tumor-targeting efficiency of DM-NCTD, the risk to the kidney was higher than in the normal liposome group. With regard to in vivo antitumor activity, DM-NCTD/FA-PEG liposomes inhibited tumors in H22 tumor-bearing mice better than either free DM-NCTD or DM-NCTD/PEG liposomes ($P<0.01$), and induced considerably more significant cellular apoptosis in the tumors, with no obvious toxicity to the tissues of model mice or the liver tissue of normal mice, as shown by histopathological examination. All these results demonstrate that DM-NCTD-loaded FA-modified liposomes might have potential application for HCC-targeting therapy.

Keywords: active targeting, PEGylated liposome, diacid metabolite of norcantharidin, hepatic cancer

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Introduction

Hepatocellular carcinoma (HCC) is the sixth-most prevalent cancer and one of the leading causes of cancer-related death worldwide.[1] Unfortunately, only approximately 20% of patients with HCC are eligible for curative treatments that may achieve long-term complete response and improved survival, as most patients present with advanced or unresectable disease and are suitable only for palliative approaches.[2–4] Systemic chemotherapy is commonly used as a palliative treatment to improve survival of patients with HCC.[3]

Among the chemotherapeutic options for HCC are natural products, which have been used in cancer therapy by skilled Chinese practitioners for thousands of years.[5] Norcantharidin (NCTD), a demethylation derivative of cantharidin, obtained from the dried body of the Chinese blister beetle (*Mylabris* spp.), is one such natural anticancer agent.[6–8] In a previous study,[9] we found that NCTD was unstable and subject to ring opening and hydrolysis. The diacid metabolite (DM) of NCTD is a stable form of NCTD.[9,10] Clinical studies have shown that DM-NCTD is effective against HCC as an inhibitor of PP1 and PP2A.[11] Recent studies have also indicated that DM-NCTD administered orally or intravenously has potential applications in cancer chemotherapy.[12,13] Currently, the clinical application of DM-NCTD is limited by its short half-life ($t_{1/2}$), as it is eliminated rapidly. Even high doses of DM-NCTD are unable to maintain a high level of circulating activity,[9] and such doses are prone to causing serious adverse effects, including intense irritation of the urinary organs, leading to nephrotoxicity and inflammation.[14–16] To improve the safety and efficacy of this drug treatment, many new alternative formulations, such as microspheres, microemulsions, and nanoparticles, have been studied.[10,17,18]

Liposomes from naturally occurring phospholipids are biocompatible carriers, and their application in drug-delivery systems is known to reduce drug toxicity and increase therapeutic efficacy.[19] Liposomes are one of the only two families of therapeutic nanocarriers that have been approved for clinical practice.[20] In particular, polyethylene glycolated (PEGylated) liposomes, also known as sterically stabilized liposomes, significantly prolong the circulation time of drugs in vivo by reducing phagocytosis by the reticuloendothelial system and thus improving the efficacy of the cancer therapy.[21–23] Although sterically stabilized liposomes achieve more drug accumulation in the tumor region through an enhanced permeability and retention (EPR) effect,[24–26] a passive targeting effect cannot guarantee increased cellular uptake of the drug(s).[27–29] Therefore, insufficient uptake at tumor sites will decrease the therapeutic benefit of the administered drug dose, and nonspecific association with healthy tissues can lead to toxic adverse effects, limiting the maximum dosage that can be applied safely. This limitation prevents drug-loaded liposomal preparations from achieving their potential therapeutic effects. One strategy to achieve cancer-targeted drug delivery is the utilization of unique molecular markers that are specifically overexpressed within the cancerous tissues.

The folate receptor (FR) is a 38 kDa glycosylphosphatidylinositol membrane-anchored glycoprotein that is overexpressed in various cancers.[30] Conversely, FR expression in normal tissues is considerably reduced compared with tumor tissues. The distinct expression pattern of FR in normal and malignant tissues makes it an ideal target for drug delivery. The natural ligand of FR, folic acid (FA), exhibits highly selective affinity for FR, and has been extensively explored as the targeting ligand for chemotherapeutic nanoparticle delivery because of its inherent high affinity, small size, and nontoxicity.[31–34] Therefore, FA specifically promotes cancer-cell uptake through FR-mediated endocytosis.[35–37]

Therapeutic evaluation of DM-NCTD liposomes in tumors is essential to improving cancer therapy. In a previous study, we confirmed the prolonged circulation characteristics of related parameters and increased the relative bioavailability (F_r) of DM-NCTD liposomes (compared with DM-NCTD as the reference formulation) in Kunming mice at a moderate dose (2 mg/kg) converted from the clinical dosage used in the People's Republic of China (PRC).[9,38] Although the results indicated that a liposomal drug-delivery system could have the potential to overcome the shortcomings of DM-NCTD by improving F_r and increasing therapeutic efficacy, further in vitro and in vivo studies on tumor-targeted FR-mediated DM-NCTD liposome therapy are still needed to confirm these results. Therefore, the aim of this study was to develop tumor-targeted delivery for DM-NCTD and confirm its targeting characteristics at a moderate dose. We prepared DM-NCTD encapsulated in PEG liposomes (DM-NCTD/PEG liposomes) and in FA-PEG liposomes (DM-NCTD/FA-PEG liposomes) to be assessed as tumor-targeting carriers for DM-NCTD. In addition, the DM-NCTD liposomes were characterized, and the characteristics of in vitro DM-NCTD release from the DM-NCTD liposomes were investigated. Furthermore, the biodistribution of DM-NCTD in H22 tumor-bearing mice was assessed to reveal the tumor-targeting effect of DM-NCTD liposomes. Both the in vitro and in vivo antineoplastic activity of DM-NCTD liposomes were studied, including their cytotoxicity against H22 cells in vitro and their tumor inhibition in vivo in H22 tumor-bearing mice. Additionally, tumor-cell apoptosis and the preliminary toxicity of the various formulations in the tissues was assessed by terminal deoxynucleotidyl transferase deoxyuridine triphosphate nick-end labeling (TUNEL) assay and hematoxylin and eosin (H&E) staining.

Materials and methods
Materials

The materials used were the same as those described in our previous study.[38] NCTD (purity >98%) was purchased from J&K Scientific (Beijing, PRC). DM-NCTD was converted

from NCTD (1.11:1, molar ratio). Ribavirin was used as the internal reference standard (IS) (purchased from the National Institutes for Food and Drug Control, Beijing, PRC), while 1,2-distearoyl-*sn*-glycero-3-phosphatidylcholine (DSPC), 1,2-distearoyl-*sn*-glycero-3-phosphoethanolamine-*N*-[methoxy(PEG)-2000] (DSPE-PEG$_{2000}$), and DSPE-PEG$_{2000}$-FA were all purchased from Resenbio (Xi'an, PRC). All other chemicals were analytical grade.

The H22 murine hepatoma cell line was obtained from the Shanghai Cell Center of the Chinese Academy of Medical Science (Shanghai, PRC). Equal numbers of male and female Kunming mice, 20–25 g in weight, were supplied by the Experimental Animal Center, Zhejiang University (Hangzhou, PRC). All animal-handling procedures were performed according to the Guide for the Care and Use of Laboratory Animals of the National Institutes of Health and followed the guidelines of the Animal Welfare Act. All animal experiments were approved by the Ethical Committee of Animal Experimentation of Zhejiang University.

Preparation of DM-NCTD liposomes

DM-NCTD/FA-PEG liposomes were prepared using reverse-phase evaporation.[38] The main procedure was as follows: DSPC, cholesterol, DSPE-PEG$_{2000}$, and DSPE-PEG$_{2000}$-FA (2:1:0.11:0.017 molar ratio) were all dissolved in chloroform. To obtain an emulsion, the lipid solution was mixed with phosphate-buffered saline (PBS) containing DM-NCTD and then homogenized in a sonicator (JY92-II; Ningbo Science Biotechnology Co Ltd, Ningbo, PRC). The obtained emulsion was evaporated by a rotary evaporator (RE-52C; Shanghai Yaguang Instrument Co Ltd, Shanghai, PRC) under negative pressure at 60°C to form the liposome suspensions. The resulting mixture was then homogenized again in a sonicator for 20 minutes to form well-proportioned liposomes. The resulting liposome suspension was successively extruded through a polycarbonate membrane with pore size of 0.22 μm. The DM-NCTD/PEG liposomes were prepared using the same procedure, but without DSPE-PEG$_{2000}$-FA.

Characterization of DM-NCTD liposomes

Size, zeta potential, and morphology of liposomes

The size and zeta potential of the DM-NCTD liposomes were measured using a Zetasizer 3000HS (Malvern Instruments, Malvern, UK) in accordance with the manufacturer's protocol. Dispersion Technology software, version 4.20 (Malvern Instruments) was used to analyze the effective diameter. The measurements were performed in triplicate.

The vesicle shape of the different liposome formulations was evaluated by high-resolution transmission electron microscopy (Tecnai G2 F20 S-Twin; FEI, Hillsboro, OR, USA).

Determination of the encapsulation efficiency of the DM-NCTD liposomes

Encapsulation efficiency (EE) was determined using a previously reported method.[39] Briefly, 1 mL of the liposome dispersion was eluted with PBS (pH 7.4) through a Sephadex G-50 column (GE Healthcare Bio-Sciences AB, Uppsala, Sweden) to remove the unloaded DM-NCTD. The quantity of entrapped drug was determined by disrupting the liposome dispersion with methanol. The drug concentration in the liposomes was measured by high-performance liquid chromatography (HPLC; Agilent 1200; Agilent Technologies, Santa Clara, CA, USA). The EE of DM-NCTD was estimated as follows:

$$EE\% = \frac{W_{columns}}{W_{total}} \times 100 \qquad (1)$$

where $W_{columns}$ is the measured amount of DM-NCTD in the liposome suspension after separation in the column and W_{total} is the measured amount of DM-NCTD in an equal volume of the liposome suspension before separation in the column.

The amount of DM-NCTD in the liposomes was measured using HPLC at room temperature. A Zorbax SB-C18 column (4.6×250 mm, 5 μm) was employed. The mobile phase was methanol and 0.025 M potassium dihydrogen phosphate (11:89 v/v), and the pH of the aqueous phase was adjusted with H_3PO_4 to 3. The flow rate was 1.0 mL/min. The wavelength of the ultraviolet detector was 210 nm. The injection volume was 20 μL.

In vitro drug-release assay

Drug release from the DM-NCTD liposomes was measured by dialysis. Briefly, 10 mL of DM-NCTD liposomes was placed into a dialysis bag (2,000 Da molecular weight cutoff), which was then placed into a beaker containing 50 mL of medium and stirred for 48 hours at 37°C±0.5°C. At various time points, aliquots were withdrawn from the beaker and replaced with equal volumes of the medium. Aliquots (10 mL) of the DM-NCTD liposomes were mixed with the same amount of medium as the total dosage, which was determined by disrupting the liposome dispersions with methanol. The DM-NCTD concentrations were then measured by HPLC, as described in the previous section. To allow comparison with DM-NCTD, the release medium was PBS (pH 7.4).

EE and particle-size stability in vitro

Liposome stability under in vitro storage conditions is an important criterion for both in vitro and in vivo biomedical applications. To investigate the EE and particle-size stability of DM-NCTD liposomes in PBS (pH 7.4) at 4°C in the dark, three batches of DM-NCTD liposomes (DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes) were assessed at various time points (1, 7, 15, and 30 days) by the methods described in previous sections.

In vitro cytotoxicity of the DM-NCTD liposomes

The in vitro antineoplastic activity of the DM-NCTD liposomes was determined by their cytotoxicity to H22 cells, using the 3-(4,5-dimethylthiazol-2-yl)-2, 5-diphenyltetrazolium bromide (MTT) assay. Cells in logarithmic growth were seeded into 96-well plates at a density of 10^4 cells per well and incubated for 24 hours, then the medium was exchanged for fresh medium. The cells were then treated with 100 µL of sterile samples (DM-NCTD, DM-NCTD/PEG liposomes, and DM-NCTD/FA-PEG liposomes) at a range of concentrations (0.8, 4, 20, 100, and 500 µg/mL). Next, the cells were incubated for 24 and 48 hours. After incubation, 20 µL of a 5 mg/mL MTT solution in PBS was added to each well, and the plate was incubated for an additional 4 hours. The supernatant was then carefully removed, and 100 µL of dimethyl sulfoxide was added to each well. After the formazan crystals had dissolved completely, optical density at 490 nm (A_{490}) was determined with a model 680 Microplate Reader (Bio-Rad Laboratories Inc, Hercules, CA, USA). The inhibition rate (IR) of the treated cells was defined as follows:

$$IR\% = \left[1 - \frac{A_{490}(treated)}{A_{490}(untreated)}\right] \times 100 \qquad (2)$$

with A_{490} values for the treated and untreated cells.

Validation of analytical method in vivo

A Sciex 4000 Q-Trap tandem quadrupole mass spectrometer, equipped with an electrospray ionization source (Thermo Fisher Scientific, Waltham, MA, USA), a Paradigm MS4B series for HPLC (Bruker Corporation, Billerica, MA, USA), and an HTC PAL autosampler (CTC Analytics AG, Zwingen, Switzerland), was used for the liquid chromatography tandem mass spectrometry (LC-MS/MS) analysis. The apparatus and LC-MS/MS conditions were the same as those described in our previous study.[9]

Whole tissues and tumor samples were collected from the mice and stored at −80°C until use. The samples were homogenized in saline (tissue or tumor:water ratio of 1:4, w/v). A 100 µL aliquot of each sample was combined with 57 µL of 1 M hydrochloric acid and 43 µL of IS (100 µg/mL), followed by the addition of 300 µL of acetone and vortexing for 5 minutes. Finally, the mixture was centrifuged at 12,000 rpm for 25 minutes at 4°C. A 200 µL aliquot of the supernatant was transferred to a 2 mL polypropylene centrifuge tube and evaporated using a condensation dryer. The residue was reconstituted with the appropriate amount of water containing 0.1% formic acid and then centrifuged at 12,000 rpm for 15 minutes at 4°C. Finally, 5 µL of the supernatant was injected for analysis. A thorough and complete validation method for assaying the DM-NCTD mouse samples was performed in accordance with the US Food and Drug Administration (FDA) guidelines.[40]

Biodistribution study

Preparation of the H22 tumor-bearing mouse model

The in vivo antineoplastic study was performed as previously described, with a few modifications.[41,42] Briefly, after serial subcultivation of the H22 cells for 7 days, mice with viable H22 ascites tumors were killed by cervical dislocation under sterile conditions. The ascites were withdrawn and mixed with physiological saline to dilute the cell density to 1×10^7/mL. The tumor-cell ascites were injected subcutaneously into the right hind limb of each mouse at a dose of approximately 0.1 mL/10 g.

Biodistribution study in H22 tumor-bearing mice

When the tumor volume reached approximately 300 mm³, the H22 tumor-bearing mice were randomly assigned to one of three groups: group 1 received DM-NCTD, group 2 received DM-NCTD/PEG liposomes, and group 3 received DM-NCTD/FA-PEG liposomes. All groups were injected with 2 mg/kg DM-NCTD through the tail vein. The dose was converted from the clinical dosage used in the PRC (10–30 mg/60 kg per single dose for adults, and the ratio of adult to mice 1:9.01), and has been reported previously in a therapeutic anticancer study.[43]

After drug administration, the H22 tumor-bearing mice were killed at 1, 2, 4, and 8 hours. The tumors or excised tissues (heart, liver, spleen, lung, and kidney) were collected, blotted with a paper towel, rinsed in saline, blotted again to remove excess fluid, weighed, and homogenized as described in the "Validation of analytical method in vivo" section. Meanwhile, the concentration of DM-NCTD in each sample was measured by LC-MS/MS as described in the same section.

The area under the curve (AUC) from 0 to 8 hours and peak concentration (C_{max}) in the tissues and tumors were calculated using a noncompartment model with PK Solver version 2.0 (China Pharmaceutical University, Nanjing, People's Republic of China). Based on the AUC and C_{max} values, four targeting parameters – relative intake rate (R_e), tissue/tumor-targeting efficacy (T_e), relative targeting efficiency (R_{Te}), and peak concentration ratio (C_e) – were calculated to evaluate the tissue or tumor-specific targeting of the DM-NCTD liposomes, as per the equations below:[44]

$$R_e = \frac{AUC_{DM-NCTD/liposomes}}{AUC_{DM-NCTD}} \qquad (3)$$

$$T_e\% = \frac{AUC_{tissue\ or\ tumor-targeted}}{\sum AUC_{tissue\ or\ tumor-targeted} + \sum AUC_{untargeted}} \times 100 \qquad (4)$$

$$R_{Te} = \frac{T_{e\ (DM-NCTD/liposomes)}}{T_{e\ (DM-NCTD)}} \qquad (5)$$

$$C_e = \frac{C_{max\ (DM-NCTD/liposomes)}}{C_{max\ (DM-NCTD)}} \qquad (6)$$

In vivo antineoplastic activity and preliminary toxicity of the DM-NCTD liposomes

After the preparation of the H22 tumor-bearing mouse model described, the model mice were randomly assigned to one of the four different experimental groups: the control group (PBS) or the groups that were administered DM-NCTD, DM-NCTD/PEG liposomes, or DM-NCTD/FA-PEG liposomes. Moreover, to investigate the preliminary toxicity of the DM-NCTD and DM-NCTD liposomes on normal liver tissue, Kunming mice were randomly assigned to the same four experimental groups mentioned.

Each mouse was injected with 2 mg/kg DM-NCTD through the tail vein. For the model mice, tumor growth was investigated in H22 tumor-bearing mice injected with DM-NCTD or DM-NCTD liposomes on days 1–9 after H22 cells were injected on day 0 (n=10). The normal mice were each injected on days 1–9 with DM-NCTD or DM-NCTD liposomes as planned (2 mg/kg, n=10). The mice were killed by cervical dislocation on day 10, and then subcutaneous tumors of the model mice were carefully collected and weighed. The IR on tumor weight (IR_w) was assessed as follows:

$$IR_W\% = \left(1 - \frac{W_{drug}}{W_{control}}\right) \times 100 \qquad (7)$$

where W_{drug} and $W_{control}$ are the tumor weights of the drug-administered and control groups, respectively. Tumor size was measured every day on days 1–10 with a Vernier caliper, and the individual tumor volumes (V) were calculated by the following formula:

$$V = \frac{Length \times Width^2}{2} \qquad (8)$$

The mice were also weighed every day.

Finally, the mice were killed and the major organs (heart, liver, spleen, lung, and kidney) and tumors were harvested and fixed in a 4% formaldehyde solution for 24 hours at room temperature. Paraffin wax sections were prepared from the harvested tissues. Tumor-cell apoptosis was detected by TUNEL assay according to the manufacturer's protocol.[45] The sections were treated with proteinase K and 0.3% H_2O_2 for 10 minutes, then the sections were incubated in the TUNEL reaction mixture. Finally, the sections were stained with a diaminobenzidine solution for 10 minutes at room temperature. Photographs were captured under a microscope (Olympus, ×200; Tokyo, Japan). The tissues were stained with H&E according to the manufacturer's instructions and observed under bright-field microscopy (Olympus, ×200).

Statistical analysis

Data are expressed as mean ± standard deviation. Statistical significance was set at $P < 0.05$.

Results and discussion
Dose of DM-NCTD

In our previous study, we confirmed the pharmacokinetic profiles of different-level doses of DM-NCTD in normal saline solution after administration to beagles, which could be helpful in identifying a rational dose range for DM-NCTD in the preclinical study.[9] The pharmacokinetic study revealed that the risk of DM-NCTD intoxication may increase at high doses, and these results were consistent with the reported adverse effects for adults administered the high clinical dosage in the PRC. It is precisely because of these reasons that our study focused on increasing the $t_{1/2}$ and decreasing the potential adverse effects of DM-NCTD when the drug was used at a moderate dose. In the current study, we confirmed that the liposome groups exhibited an apparently longer circulation time following intravenous administration to mice (2 mg/kg), while the F_r of DM-NCTD increased.[38] We also investigated the tumor-targeting efficiency, antineoplastic activity, and preliminary toxicity evaluation at the moderate

Table 1 Evaluation results of DM-NCTD liposomes (n=3)

Group	Particle size (nm)	PDI	Zeta potential (mV)	EE (%)
DM-NCTD/PEG liposomes	203.5±1.2	0.14±0.01	5.9±0.2	82.3±0.5
DM-NCTD/FA-PEG liposomes	205.7±1.1	0.10±0.01	6.9±1.6	80.1±0.6

Note: Data presented as mean ± standard deviation.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; PDI, polydispersity index; EE, encapsulation efficiency; PEG, polyethylene glycol; FA, folic acid.

dose on the basis of previous research, and our results provide a reference for further research into evaluating the risk of the high dose of DM-NCTD liposomes in further studies.

Characterization of the DM-NCTD liposomes

Size, zeta potential, and morphology

The average sizes of the DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes were approximately 203 and 205 nm, respectively; these sizes are preferable for tumor accumulation via the EPR effect.[24–26] Moreover, the zeta potential (5.9 and 6.9 mV, respectively) analyses demonstrated that both types of drug-loaded liposome exhibited approximately neutral surface charge, which would minimize undesirable nonspecific protein adsorption (Table 1).[27]

No significant changes were observed in any of the characteristics following the addition of FA to the liposomes. The particle-size distribution and zeta potential of the DM-NCTD/FA-PEG liposomes are presented in Figure 1A and B, while transmission electron microscopy (Figure 1C) demonstrates the regular spherical morphology of the DM-NCTD/FA-PEG liposomes. The EE values were both >80% (Table 1).

In vitro drug release

In vitro DM-NCTD-release data are presented in Figure 1D. DM-NCTD was quickly and completely released into PBS (pH 7.4). The release of DM-NCTD from the liposomes demonstrated that DM-NCTD liposomes released DM-NCTD in a sustained manner within 48 hours compared with DM-NCTD.
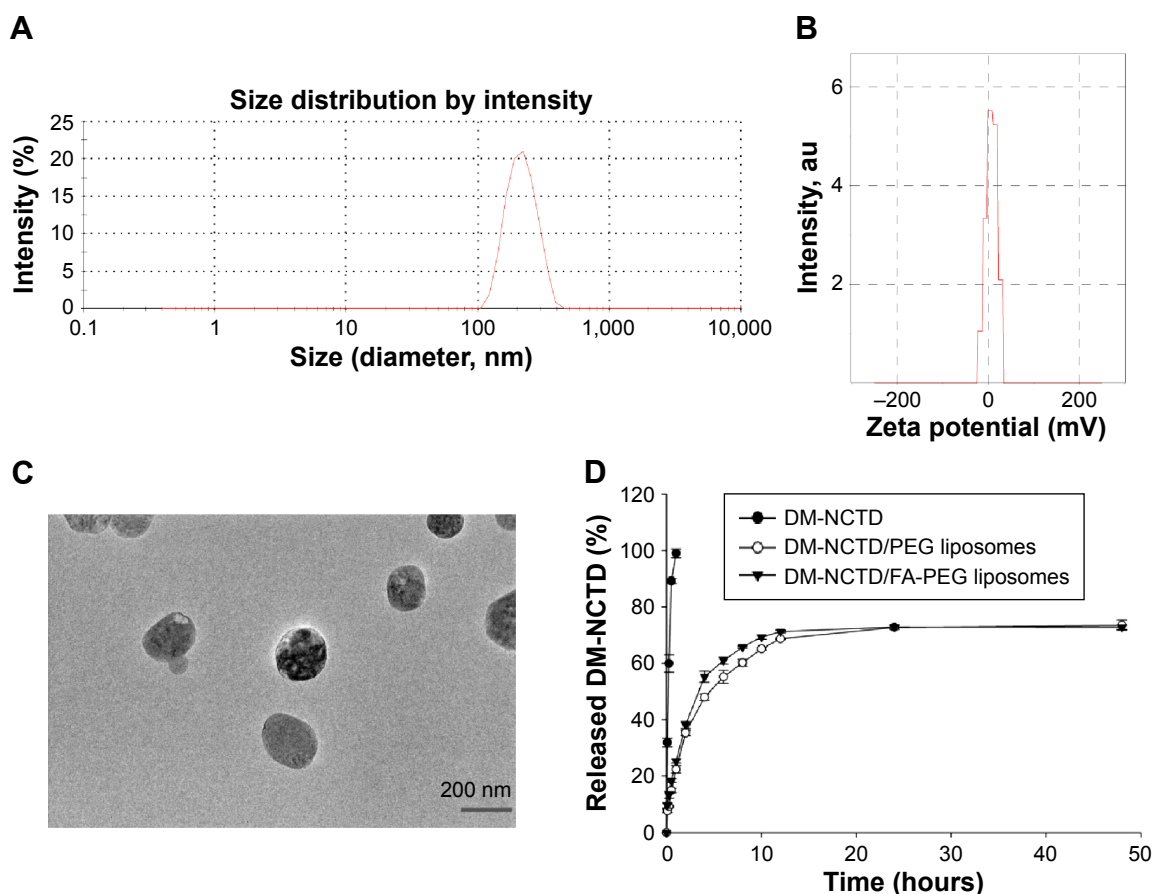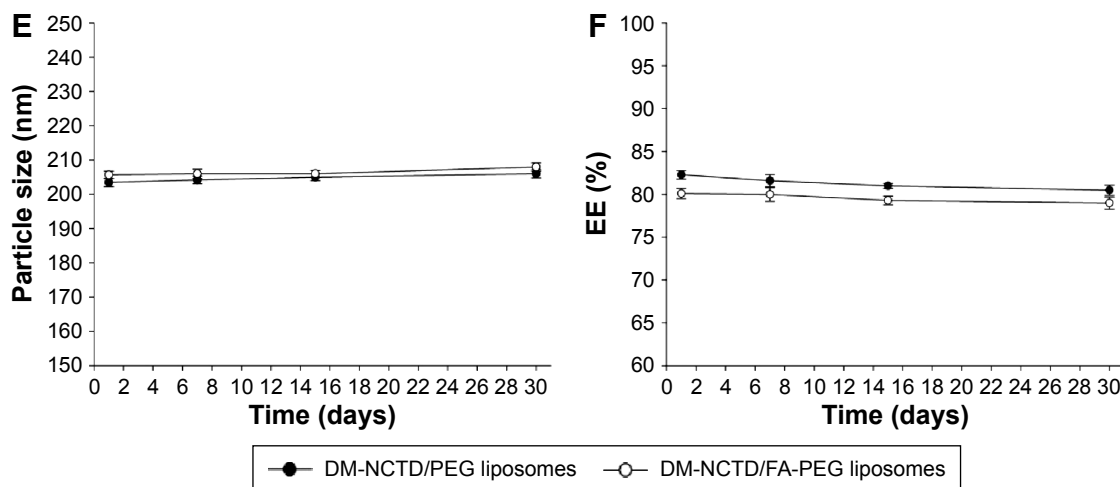
Figure 1 (*Continued*)

Figure 1 Characterization of DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes.

Notes: (**A**) Particle-size distribution of DM-NCTD/FA-PEG liposomes. (**B**) Zeta potential of DM-NCTD/FA-PEG liposomes. (**C**) TEM of DM-NCTD/FA-PEG liposomes. (**D**) In vitro release of DM-NCTD liposomes with comparison to DM-NCTD (37°C, PBS, pH 7.4, n=3). (**E**) Particle-size stability of DM-NCTD liposomes in 30 days (4°C, in dark, PBS, pH 7.4, n=3). (**F**) EE stability of DM-NCTD liposomes in 30 days (4°C, in dark, PBS, pH 7.4, n=3).

Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol; TEM, transmission electron microscopy; PBS, phosphate-buffered saline; EE, encapsulation efficiency; au, arbitrary unit.

EE and particle-size stability in vitro

Previous studies have shown that DM-NCTD is a stable form of NCTD both in vitro and in vivo,[7,9,10] and retains the main structure–activity relationships of NCTD.[7,38] However, investigations into the stability of DM-NCTD liposomes are essential, because liposomal stability is a prerequisite for achieving long circulation time and tumor-targeted delivery, which is strongly influenced by the hydrophilic stealth layer, zeta potential, lipid composition, particle size, and distribution.[46] In the current study, DSPE-PEG$_{2000}$ was used as the definitive functional phospholipid in the liposomal formulation to maintain a long circulation time and specific stability. This compound is also used in the FDA-approved PEGylated liposomal doxorubicin.[46,47]

In the stability studies, the results demonstrated that the particle size of the liposomes ranged from 203.5 to 206 nm in the DM-NCTD/PEG liposome group and from 205.7 to 208 nm in the DM-NCTD/FA-PEG liposome group (Figure 1E). In addition, the EE values ranged from 82.3% to 80.5% in the DM-NCTD/PEG liposome group and from 80.1% to 79% in the DM-NCTD/FA-PEG liposome group (Figure 1F). No significant changes were observed in the two groups, indicating that the liposomes were stable for 1 month at 4°C in the dark.

In vitro cytotoxicity of the DM-NCTD liposomes

First, the cytotoxicity of the blank liposomes was investigated. The concentration of the blank liposomes was equal to the concentration of the drug-loaded liposomes used in the cytotoxicity assay. The blank liposomes were incubated with H22 cells for 24 and 48 hours. Over 95% of the cells survived during the incubation period, indicating that the blank liposomes did not exhibit cytotoxicity against H22 cells.

H22 cells were incubated with DM-NCTD, DM-NCTD/PEG liposomes, or DM-NCTD/FA-PEG liposomes for 24 and 48 hours to analyze the cytotoxicity of these treatments, as depicted in Figure 2. The DM-NCTD concentrations in the liposomes were equal to those of the free DM-NCTD (0.8, 4, 20, 100, and 500 µg/mL). Both dose-dependent and time-dependent cytotoxicity were observed. All of the groups exhibited cytotoxicity against H22 cells, as shown in Figure 2. In this study, half-maximal inhibitory concentration values revealed that free DM-NCTD was the most efficacious among the three treatments in vitro at 24 and 48 hours ($P<0.01$) (Table 2). The results demonstrated that the cytotoxicity of DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes increased more rapidly compared with DM-NCTD from 24 to 48 hours. Figure 2 shows that the DM-NCTD/PEG liposome group exhibited the lowest cytotoxicity of the three groups, and that the unmodified liposomes displayed very little cytotoxicity at doses of 4 and 20 µg/mL at 24 hours and no cytotoxicity at a dose of 0.8 µg/mL at both 24 and 48 hours. However, the FA-modified liposomes performed better than the unmodified liposomes, particularly at low doses at 24 hours (4 or 20 µg/mL at 24 hours, $P<0.01$).

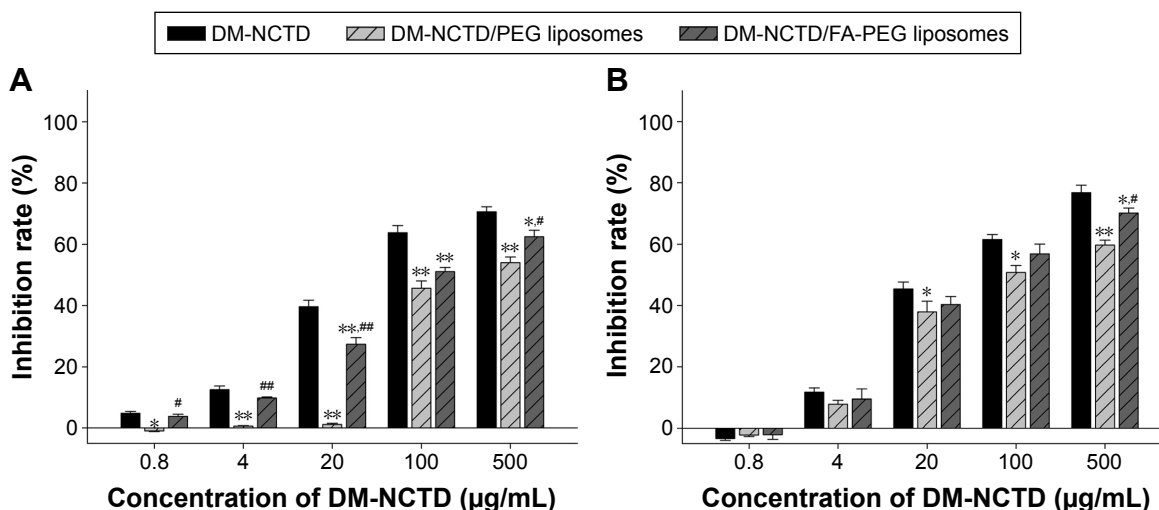In the different dose groups at 24 and 48 hours, the free drug exhibited the greatest antitumor effect of the three

Figure 2 In vitro cytotoxicity of DM-NCTD and DM-NCTD liposomes on H22 cell lines for 24 hours (**A**) and 48 hours (**B**), respectively (n=3).
Notes: **$P<0.01$, *$P<0.05$ vs DM-NCTD group; ##$P<0.01$, #$P<0.05$ vs DM-NCTD/PEG liposome group.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol.

groups, and the FA-modified group was better than the unmodified group, indicating that DM-NCTD accumulated more easily than the other groups in H22 cells, owing to its intracellular antitumor role, as previously described.[48–51] We believe that the cellular internalization mechanism of the free drug and drug-loaded liposomes contributed to this phenomenon. For the free drug, the low molecular weight (186.16 Da) of DM-NCTD might assist in its internalization into cells by direct diffusion, thus explaining why the free drug accumulated more quickly than the liposomes in the cells. For the unmodified group, the low IR is related to its sustained drug release. Reports indicate that PEGylation significantly reduces the cellular uptake and endosomal/lysosomal escape of liposomes and interferes with the tumor retention and antitumor efficacy of liposome-based drug-delivery systems,[27–29] indicating that encapsulated DM-NCTD may be internalized via diffusion after extracellular release from liposomes. Finally, with regard to the FA-modified liposomal group, FA is an active targeting moiety and natural element that specifically promotes uptake of these liposomes by cancer cells

through FR-mediated endocytosis.[35–37] Although the results for cytotoxicity of the FA-modified liposomal drug-delivery system are consistent with the previous reports mentioned, the hypothesized cellular internalization mechanism of DM-NCTD liposomes still needs to be confirmed.

Validation of the analytical method in vivo

LC-MS/MS methods may overcome the disadvantages that have been reported with the current DM-NCTD analytical methods, including low resolution of HPLC ultraviolet,[52] instability of gas chromatography–MS,[53] high lower limit of quantification, and long chromatography run times.[54] In the current study, an LC-MS/MS method with multiple reaction monitoring was developed and validated for the determination of DM-NCTD in mouse tissues and tumor, using ribavirin as the IS.

Specificity was assessed by analyzing three different samples of the blank matrix with and without DM-NCTD and IS, as well as the in vivo samples. No endogenous interference was noted from the tumor homogenates or from the tissue homogenates of heart, liver, spleen, lung, and kidney, thus ensuring the high specificity of the LC-MS/ MS method. In this study, we used the tumor homogenates as an example (Figure S1). The retention times of DM-NCTD and the IS were approximately 2.8 and 1.4 minutes, respectively. Inter- and intraday precision, matrix effect, and extraction recovery for three quality-control samples from five replicates are presented in Table S1. The stability of DM-NCTD was within 15%, as indicated by the relative standard deviation for the quality-control samples (n=5).

Table 2 IC_{50} of various groups against H22 cells for 24 hours and 48 hours in vitro (n=3)

Group	IC_{50} on H22 cell lines (µg/mL)	
	24 hours	**48 hours**
DM-NCTD	39.6±1.20	30.0±1.73
DM-NCTD/PEG liposomes	164.0±1.57**	92.5±1.31**
DM-NCTD/FA-PEG liposomes	95.3±1.52**,##	50.1±1.04**,##

Notes: **$P<0.01$ vs DM-NCTD group; ##$P<0.01$ vs DM-NCTD/PEG liposome group. Data presented as mean ± standard deviation.
Abbreviations: IC_{50}, half-maximal inhibitory concentration; DM, diacid metabolite; NCTD, norcantharidin; PEG, polyethylene glycol; FA, folic acid.

As shown in Tables S2–S4, no significant difference was observed under the different stability conditions, indicating that DM-NCTD was stable under the storage, disposition, and analysis conditions used. The method was sufficiently sensitive for biodistribution analysis of DM-NCTD in H22 tumor-bearing mice.

In vivo biodistribution in H22 tumor-bearing mice

FA-modified liposomes were used as biocompatible carriers to reduce the potential toxicity of DM-NCTD, prolong its retention time,[38] and increase its tumor-targeting ability.[31–34] In the current study, the tissue- and tumor-targeting characteristics of DM-NCTD and DM-NCTD liposomes were evaluated through biodistribution. Figure 3 presents the results of tissue- and tumor-distribution in samples obtained at 1, 2, 4, and 8 hours after injection of DM-NCTD, DM-NCTD/ PEG liposomes, or DM-NCTD/FA-PEG liposomes into the

mouse tail vein (2 mg/kg, n=6). Free DM-NCTD was present in the tissues and tumors, with particularly high levels noted in the liver, spleen, and kidney. The highest concentrations were achieved at 2 hours. However, the concentration in the tumor was very low and was rapidly eliminated. Compared with DM-NCTD, DM-NCTD liposomes improved the tumor-targeting efficiency, and DM-NCTD/FA-PEG liposomes exhibited the highest efficiency of the three treatments (Tables 3 and 4).

The noncompartment parameters of AUC_{0-8}, $t_{1/2}$, and C_{max} for DM-NCTD liposomes and free DM-NCTD in the tissues and tumors of H22 tumor-bearing mice after intravenous administration are presented in Table 3. R_e, T_e, R_{Te}, and C_e were calculated using AUC_{0-8} and C_{max}, and the results are presented in Table 4. The DM-NCTD/ PEG liposome and DM-NCTD/FA-PEG liposome groups exhibited excellent tumor-targeting efficiency (R_e 4.86 and 9.25, T_e 12.81% and 24.44%, R_{Te} 2.36 and 4.50, and C_e
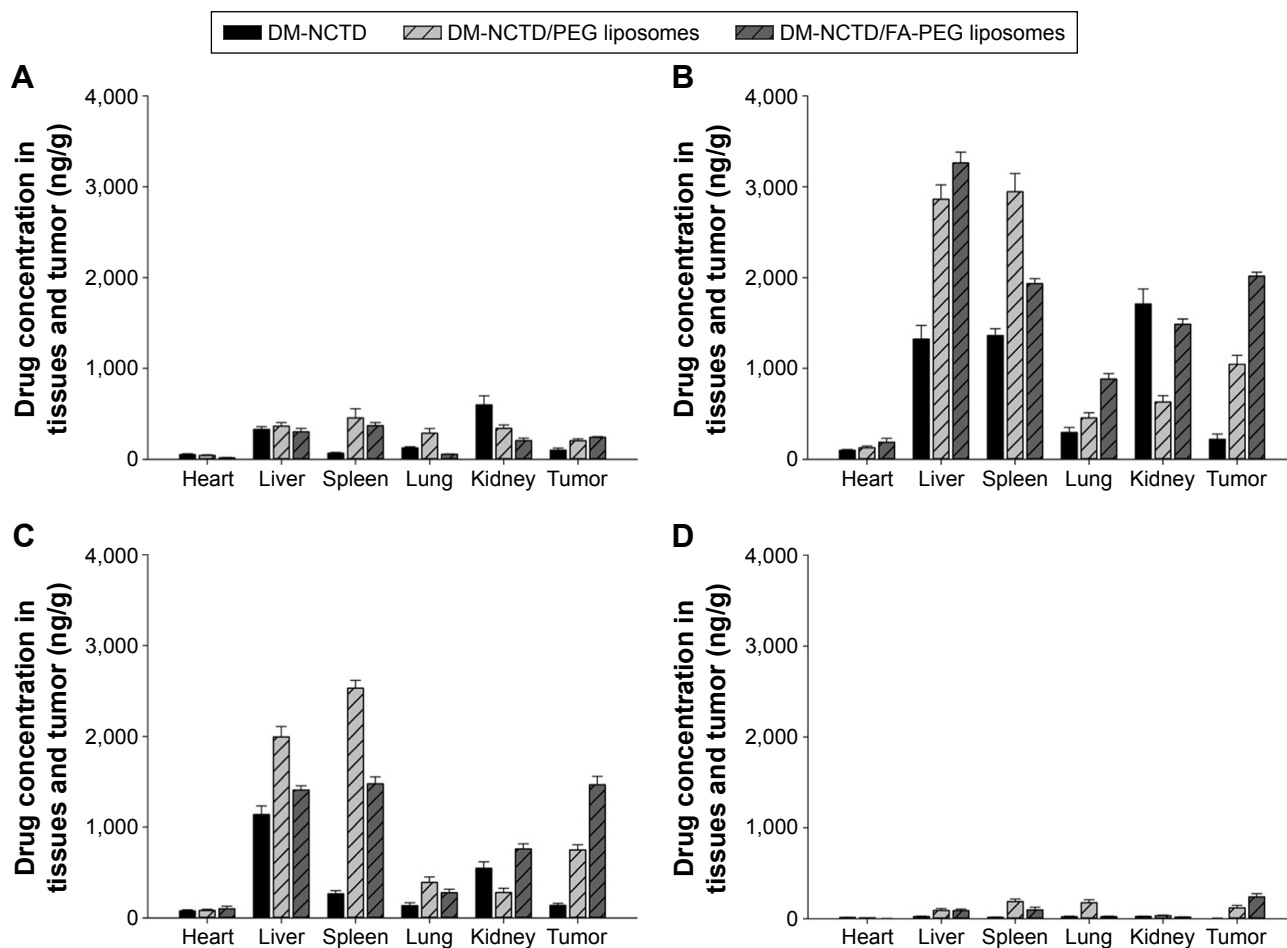

Figure 3 Tissues and tumor distribution.
Notes: DM-NCTD and DM-NCTD liposomes at 1 (**A**), 2 (**B**), 4 (**C**), and 8 hours (**D**) after intravenous administration in H22 tumor-bearing mice, while the tumor volume reached approximately 300 mm³ (2 mg/kg, n=6).
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol.

Table 3 Pharmacokinetic parameters of DM-NCTD and DM-NCTD liposomes in tissues and tumors of H22 tumor-bearing mice after intravenous administration while tumor volume reached approximately 300 mm³ (2 mg/kg, n=6)

Tissue/tumor sample	$AUC_{0-\infty}$ (ng·h/mL)			$t_{1/2}$ (hours)			C_{max} (ng/mL)		
	DM-NCTD	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes	DM-NCTD	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes	DM-NCTD	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes
Heart	116.98±10.63	126.20±18.05	151.65±12.71**,##	1.84±0.25	1.38±0.21**	0.92±0.17**,##	24.08±2.39	31.40±7.96*	46.57±5.63**,##
Liver	1,481.15±51.3	2,750.35±97.53**	2,435.63±88.34**,##	0.94±0.22	1.14±0.02	1.12±0.23	330.15±13.96	715.65±15.84**	815.56±21.3**,##
Spleen	740.09±25.16	3,266.03±113.56**	2,017.28±54.26**,##	0.89±0.02	1.42±0.24**	1.30±0.28**	340.11±17.74	736.57±30.95**	483.29±17.16**,##
Lung	266.17±13.55	657.45±37.57**	569.54±31.39**,##	1.51±0.32	4.16±1.29**	1.09±0.23**,##	73.43±6.17	113.40±4.68**	220.19±15.55**,##
Kidney	1,283.72±66.1	586.98±29.48**	1,209.74±36.17##	0.94±0.28	1.34±0.29**	0.88±0.12##	427.14±20.81	157.23±13.25**	371.35±16.1**,##
Tumor	223.18±17.56	1,085.67±99.4**	2,064.84±41.32**,##	1.02±0.14	1.83±0.26**	1.87±0.21**	54.57±9.21	260.95±36.85**	504.37±17.56**,##

Notes: **$P<0.01$, *$P<0.05$ vs DM-NCTD group; ##$P<0.01$ vs DM-NCTD/PEG liposome group. Data presented as mean ± standard deviation.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; AUC, area under the curve; $t_{1/2}$, half-life; C_{max}, peak concentration; PEG, polyethylene glycol; FA, folic acid.

Table 4 Tissue and tumor-targeting parameters of DM-NCTD and DM-NCTD liposomes in H22 tumor-bearing mice after intravenous administration while tumor volume reached approximately 300 mm³ (2 mg/kg, n=6)

Tissue/tumor sample	R_e		T_e (%)			R_{Te}		C_e	
	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes	DM-NCTD	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes	DM-NCTD/PEG liposomes	DM-NCTD/FA-PEG liposomes
Heart	1.08	1.3	2.85	1.79	1.49	0.52	0.63	1.3	1.93
Liver	1.86	1.64	36.03	28.83	32.46	0.9	0.8	2.17	2.47
Spleen	4.41	2.73	18	23.88	38.55	2.14	1.33	2.17	1.42
Lung	2.47	2.14	6.47	6.74	7.76	1.2	1.04	1.54	3
Kidney	0.46	0.94	31.22	14.32	6.93	0.22	0.46	0.37	0.87
Tumor	4.86	9.25	5.43	24.44	12.81	2.36	4.50	4.78	9.24

Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; R_e, relative intake rate; T_e, tumor-targeting efficacy; R_{Te}, relative targeting efficiency; C_e, peak concentration ratio; PEG, polyethylene glycol; FA, folic acid.

4.78 and 9.24, respectively) compared with the DM-NCTD group. Given that liposomes have passive targeting ability owing to their small size (approximately 200 nm), an EPR effect is achieved, and the particles accumulate relatively easily into well-vascularized tumors through vascular fenestrations.[24–26] The results in Table 3 show that the AUC_{0-8}, $t_{1/2}$, and C_{max} of tumor tissue were significantly prolonged in both the unmodified and FA-modified liposomal groups ($P<0.01$), which indicates that the EPR effects might be helpful for this kind of liposomal group loaded with DM-NCTD-targeting tumors. In addition, the FA-modified group exhibited increased tumor-targeting efficiency compared with the other groups, owing to its active targeting mechanism (Table 4).[35–37]

Overall, in comparison with DM-NCTD, we found that both DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes were able to decrease the efficiency of kidney-specific targeting (R_e 0.46 and 0.94, T_e 6.93% and 14.32%, R_{Te} 0.22 and 0.46, and C_e 0.37 and 0.87, respectively), as shown in Table 4, which helped to decrease the potential nephrotoxicity of DM-NCTD. Meanwhile, with regard to DM-NCTD/PEG liposomes and DM-NCTD/FA-PEG liposomes, it should be noted that not only did tumor-targeting efficiency increase but the efficiency of kidney-specific targeting was also improved (AUC_{0-8} ranged from 586.98±29.48 to 1,209.74±36.17 ng·h/mL, and C_{max} from 157.23±13.25 to 371.35±16.10 ng/mL), as shown in Table 3 ($P<0.01$). The results revealed that although the active liposome group had an apparent increase in the tumor-targeting efficiency of DM-NCTD, the risk of DM-NCTD intoxication to kidneys was higher than in the normal liposome group, which is consistent with our previous report.[38]

In the future, we will need to perform a comprehensive and thorough safety evaluation of FA-modified liposome-loaded DM-NCTD. Based on the results of the current study, we will perform a further study on the antineoplastic activity and preliminary toxicity of DM-NCTD and its liposomes.

In vivo antineoplastic activity and preliminary toxicity of the DM-NCTD liposomes

To provide in vivo evidence for the antitumor potential of the DM-NCTD liposomes, their antitumor efficacy was investigated using H22 tumor-bearing mice. Tumor growth was measured using a Vernier caliper, and the growth curve is presented in Figure 4A. All of the experimental formulations were effective in preventing tumor growth compared with PBS treatment. Mice treated with the DM-NCTD/FA-PEG liposomes displayed stronger tumor inhibition compared with those treated with either DM-NCTD or DM-NCTD/PEG liposomes ($P<0.01$).

The IR_w in response to the treatments was also determined (Table 5). DM-NCTD liposomes exhibited excellent antitumor activity, with an IR_w of 40.41% and 67.81% for unmodified and FA-modified liposomes, respectively, which was considerably enhanced compared with free DM-NCTD. Figure 4B demonstrates a similar weight-change range of the mice during the experiment. Therefore, none of the treatments influenced the weight of the model mice as a result of the tumor-specific toxicity of DM-NCTD liposomes.
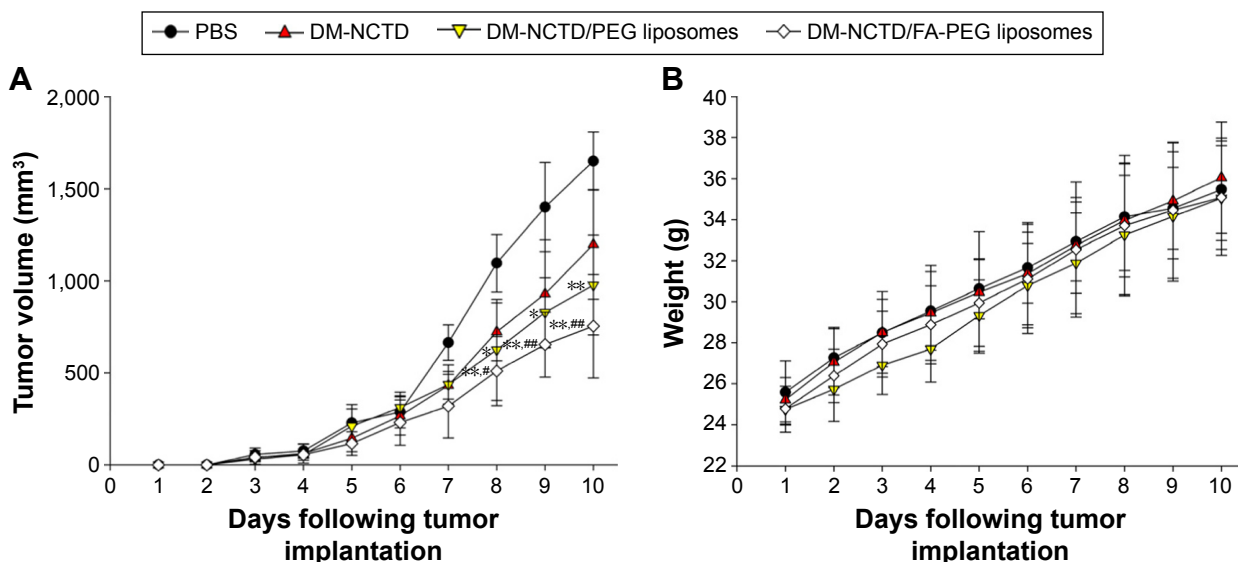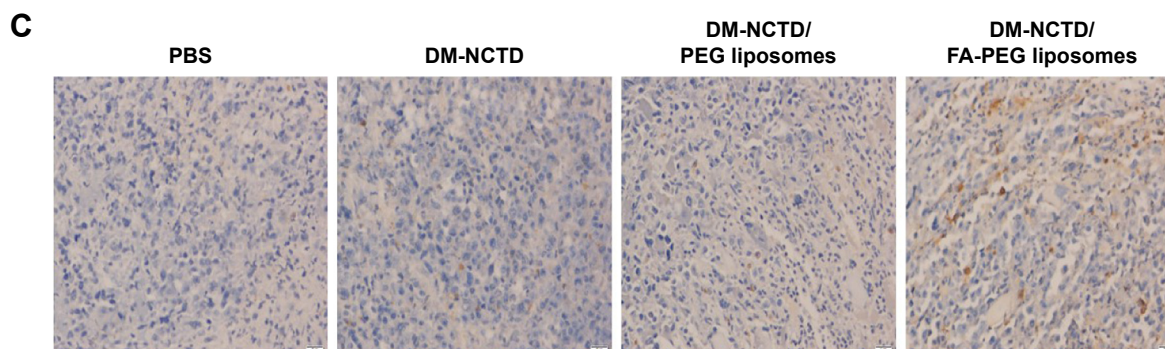

Figure 4 (Continued)

C

Figure 4 Anti-tumor study in H22 tumor-bearing mice.
Notes: (**A**) Tumor growth in H22 tumor-bearing mice of DM-NCTD and DM-NCTD liposome groups after H22 cells were injected at day 0 (2 mg/kg per day, administered on days 1–9, and killed on day 10; n=10); (**B**) H22 tumor-bearing mice weight change of DM-NCTD and DM-NCTD liposome groups after H22 cells were injected at day 0 (2 mg/kg per day, administered on days 1–9, and killed on day 10; n=10); (**C**) tumors of H22 tumor-bearing mice stained with TUNEL after in vivo antineoplastic activity study (bar 20 μm). ******$P<0.01$, *****$P<0.05$ vs DM-NCTD group; ##$P<0.01$, #$P<0.05$ vs DM-NCTD/PEG liposome group.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol; PBS, phosphate-buffered saline; TUNEL, terminal deoxynucleotidyl transferase deoxyuridine triphosphate nick-end labeling.

We conclude that delivery of DM-NCTD in the FA-PEG liposomes improves tumor inhibition in vivo.

Tumor-cell apoptosis and the preliminary tissue toxicity of the various formulations was assessed by TUNEL assays and H&E staining. DM-NCTD/FA-PEG liposomes induced more significant increases in the levels of tumor-cell apoptosis compared with DM-NCTD/PEG liposomes and free drug (Figure 4C), and none of the groups exhibited obvious toxicity to the tissues of model mice (Figure 5) or to the liver tissue of normal mice (Figure 6). The investigations also revealed that the moderate dose used did not result in any obvious adverse effects on kidneys or other tissues of the model mice, including the groups treated with DM-NCTN or DM-NCTD liposomes. However, although there were no obvious adverse effects on kidneys during the in vivo antineoplastic activity in this study in mice administered the moderate dose, it remains unclear whether the liposomes could decrease the adverse effects of DM-NCTD when used

at high doses, which requires further study. Meanwhile, histopathological examination alone is not enough to evaluate toxicity to kidney function; there still needs to be further evaluation of the toxicity to kidneys and other tissue function after the in vivo study.

Conclusion

The current study describes a novel method using DM-NCTD-loaded FA-modified liposomes as a tumor-targeted drug-delivery system. The liposomes exhibited excellent stability and showed sustained drug release. The LC-MS/MS method used to determine the concentrations of DM-NCTD in tissues and tumors is sensitive, rapid, and reliable. In addition, the biodistribution study showed that DM-NCTD liposomes improved tumor-targeting efficiency, and DM-NCTD/FA-PEG liposomes exhibited the highest efficiency of the treatments ($P<0.01$). Meanwhile, the results revealed that although the active liposome group had an apparent increase in the tumor-targeting efficiency of DM-NCTD, the risk of DM-NCTD intoxication to kidneys was higher than in the normal liposome group ($P<0.01$). Compared with DM-NCTD/PEG liposomes, DM-NCTD/FA-PEG liposomes exhibited enhanced cytotoxicity toward H22 cells ($P<0.01$) and a significant antitumor effect in H22 tumor-bearing mice ($P<0.01$), with more significant tumor-cell apoptosis and no obvious toxicity to the tissues of model mice or to the liver tissue of normal mice, as demonstrated by the results of histopathological examination. The results of this research demonstrate that DM-NCTD-loaded FA-modified liposomes might be a potential tumor-targeting drug-delivery system for HCC treatment.

Table 5 Tumor weight and IR$_w$ in H22 tumor-bearing mice after H22 cells injected at day 0 (2 mg/kg per day, administered on days 1–9, killed and measured on day 10, n=10)

Group	Tumor weight (g)	IR$_w$ (%)
PBS	1.46±0.21	–
DM-NCTD	1.02±0.3	30.14
DM-NCTD/PEG liposomes	0.87±0.1*	40.41
DM-NCTD/FA-PEG liposomes	0.47±0.16**,##	67.81

Notes: **$P<0.01$, *$P<0.05$ vs DM-NCTD group; ##$P<0.01$ vs DM-NCTD/PEG liposome group. Data presented as mean ± standard deviation.
Abbreviations: IR$_w$, inhibition rate on tumor weight; PBS, phosphate-buffered saline; DM, diacid metabolite; NCTD, norcantharidin; PEG, polyethylene glycol; FA, folic acid.
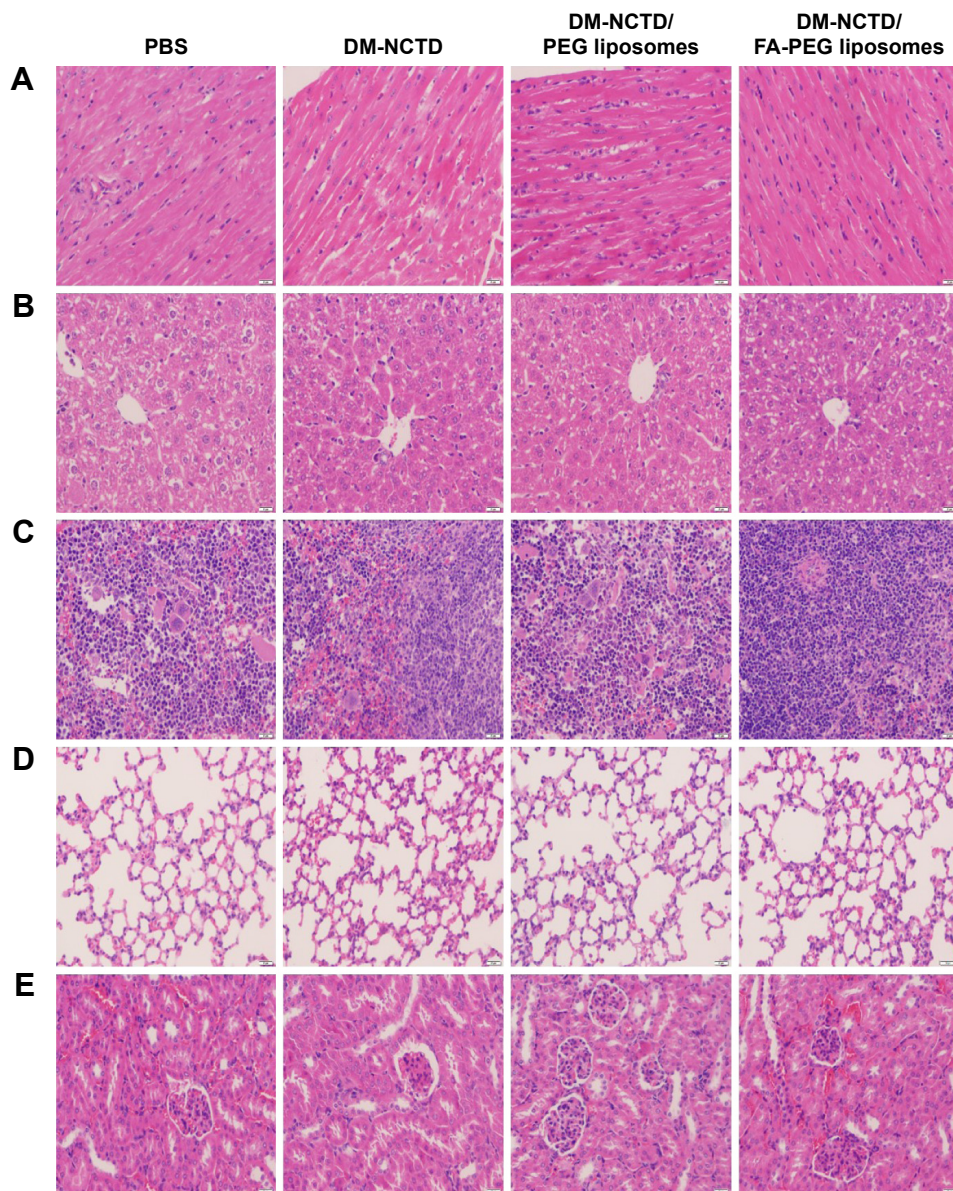
Figure 5 Tissues of H22 tumor-bearing mice stained with hematoxylin and eosin after in vivo antineoplastic activity study.
Notes: (**A**) Heart; (**B**) liver; (**C**) spleen; (**D**) lung; (**E**) kidney. Bar 20 μm.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol; PBS, phosphate-buffered saline.
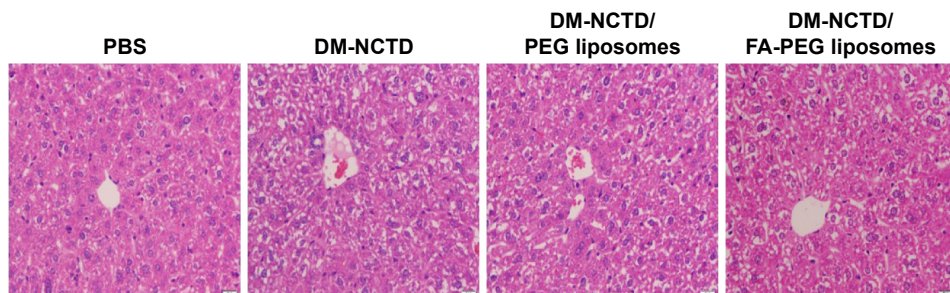

Figure 6 Liver tissue of normal Kunming mice stained with hematoxylin and eosin (2 mg/kg per day, administered on days 1–9, and killed on day 10; bar 20 μm).
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; FA, folic acid; PEG, polyethylene glycol; PBS, phosphate-buffered saline.

Acknowledgments

Disclosure

The authors report no conflicts of interest in this work.

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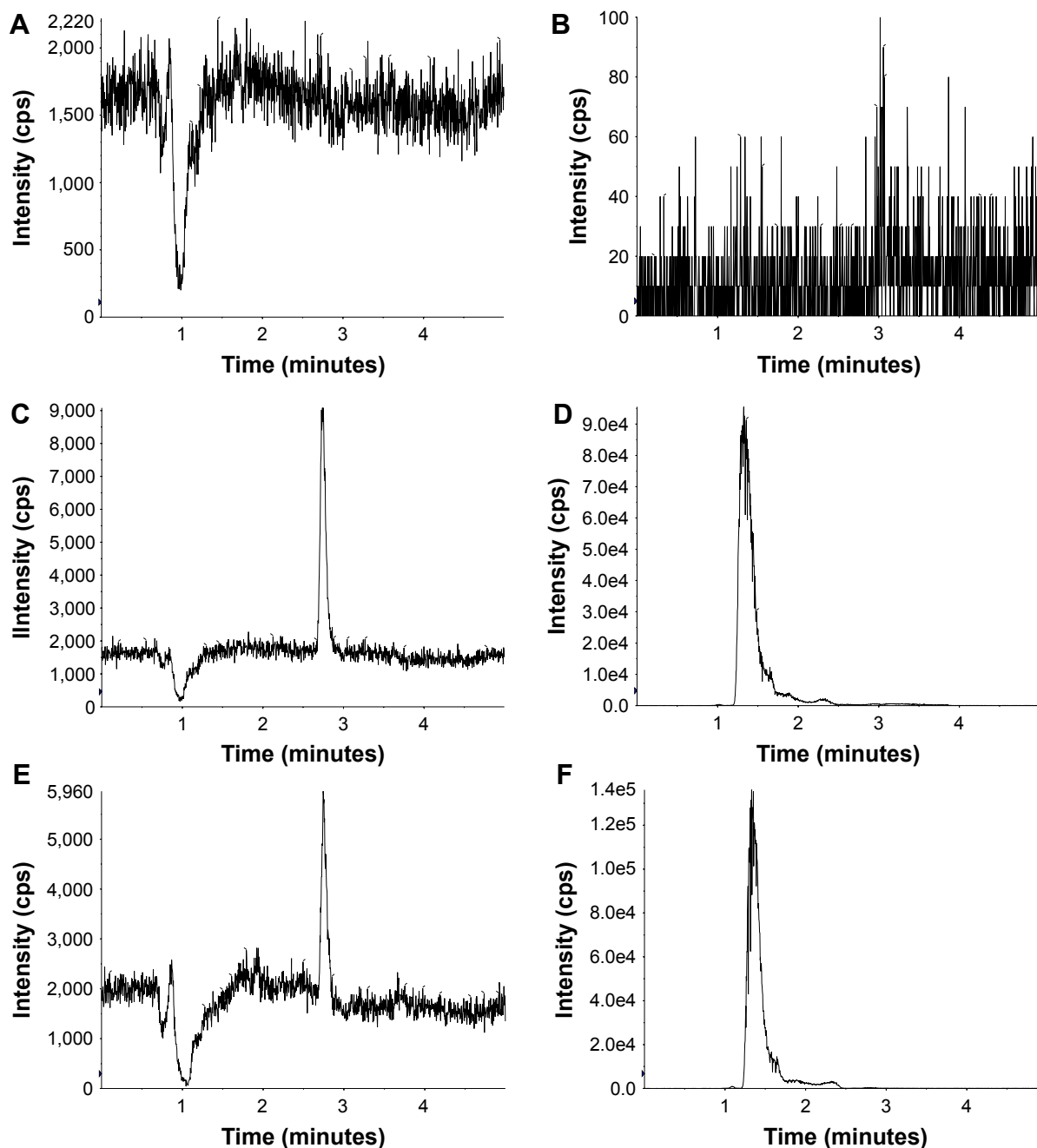
Supplementary materials

Figure S1 Chromatograms of DM-NCTD and IS.
Notes: Chromatograms of DM-NCTD in blank tumor homogenates (**A**); chromatograms of IS in blank tumor homogenates (**B**); chromatograms of DM-NCTD in tumor homogenates spiked with DM-NCTD (0.1 μg/ml) and IS (100 μg/ml) (**C**); chromatograms of IS in tumor homogenates spiked with DM-NCTD (0.1 μg/ml) and IS (100 μg/ml) (**D**); chromatograms of DM-NCTD in an extracted tumor homogenates sample from H22 tumor-bearing mice 1 hour after intravenous administration of 2 mg/kg DM-NCTD spiked with IS (**E**); chromatograms of IS in an extracted tumor homogenates sample from H22 tumor-bearing mice 1 hour after intravenous administration of 2 mg/kg DM-NCTD spiked with IS (**F**).
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; IS, internal standard; cps, counts per second.

Table S1 Precision, matrix effect, and extraction recovery of DM-NCTD in biological matrix (n=5)

Biological matrix	Nominal concentration (µg/mL)	Interday[a] RSD (%)	Intraday[b] RSD (%)	Matrix effect[c] (%) DM-NCTD	IS[d]	Extraction recovery (%) DM-NCTD/IS
Heart	0.1	11.1	11.1	88.3±7.7	83.4±9.5	88.1±11.3
	1	11.1	12.5	89.3±5.4	85.7±10.4	86.1±7.5
	5	9.7	1	96.7±11.3	87.7±6.4	85.2±6.7
Liver	0.1	11.1	11.1	89.5±8.5	95.3±7.2	101±11
	1	11.1	11.1	102±10	87.5±10.3	103±13
	5	6.4	0.4	97.4±8.3	92.4±9.3	88.4±9.5
Spleen	0.1	11.1	11.1	86.1±10.3	92.5±8.3	93.8±10.2
	1	11.1	12.5	98.5±3.8	95.2±9.3	88.7±11.2
	5	10.7	2.4	93.7±9.3	98.4±11.3	106±9
Lung	0.1	11.1	12.5	102±9	85.3±7.8	96.2±6.7
	1	11.1	11.1	86.3±4.7	88.4±7.3	84.5±8.4
	5	3.0	5.5	90.2±7.7	85.2±7.4	95.3±10.8
Kidney	0.1	11.1	11.1	105±12	95.7±8.7	85.1±5.9
	1	11.1	11.1	99.6±5.2	82.4±5.3	86.2±7.3
	5	7.3	2.9	100±9	93.0±5.5	101±10
Tumor	0.1	11.1	11.1	88.1±10.4	98.1±9.7	85.3±8.9
	1	11.1	11.1	91.3±4.9	84.6±8.8	82.6±9.1
	5	6.7	5.7	96.2±8.1	96.5±10.1	90.0±7.8

Notes: [a]Three plasma samples were run on each of 2 validation days; [b]three plasma samples were analyzed five times on the same day; [c]matrix effect % = B/A ×100, where A is the peak area of the DM-NCTD standard solution and B is the peak area of the DM-NCTD standard spiked after extraction; [d]concentration of the IS was 100 µg/mL in the acetone to precipitate protein of three-level quality-control samples; extraction recovery % = C/B ×100, where C is the peak area of the DM-NCTD standard spiked before extraction. Matrix effect and Extraction recovery data are presented as mean ± standard deviation.
Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; RSD, relative standard deviation; IS, internal standard; A, the peak area of the DM-NCTD standard solution; B, the peak area of the DM-NCTD standard spiked after extraction; C, the peak area of the DM-NCTD standard spiked before extraction.

Table S2 Stability test of DM-NCTD in different conditions (n=5)

Sample	RSD (%) 4°C, 1 week (µg/mL) 0.1	1	5	25°C, 4 hours (µg/mL) 0.1	1	5	−20°C, 1 week (µg/mL) 0.1	1	5
Heart	11.3	6.7	8.2	10.3	5.8	10.4	12.5	9	8.3
Liver	6.8	12.4	7.5	10.2	8.1	4.6	8.2	9.3	10.6
Spleen	10.3	7.4	5.9	11.8	8.7	11.4	12.4	8.3	6.4
Lung	6.3	8.9	10.2	3.5	12.4	10.7	8.4	7.2	5.9
Kidney	12.1	8.4	6.9	11.2	10.4	7	11.2	10.3	9.3
Tumor	8.2	11.6	8.7	7.7	11	12.1	12.9	8.4	9.8

Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; RSD, relative standard deviation.

Table S3 Repeated freeze–thaw stability test of DM-NCTD (n=5)

Sample	RSD (%) One cycle (µg/mL) 0.1	1	5	Two cycles (µg/mL) 0.1	1	5	Three cycles (µg/mL) 0.1	1	5
Heart	4.3	8.1	5.7	6	10.3	11.5	8.3	12.4	6.2
Liver	5.2	9.5	10.1	6.3	8.3	8	7.3	10.4	7
Spleen	8.9	5.3	8.2	10.6	7.3	5.7	8	12.4	5.6
Lung	10.7	9.4	10.1	5.3	8.5	7.4	9.2	12.8	8.1
Kidney	7.9	5.8	3.9	11.4	8.2	7.8	8.3	10.7	4.6
Tumor	12.6	10.9	11.4	12.7	9.8	7.8	9.8	10.5	13.6

Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; RSD, relative standard deviation.

Table S4 The auto-sampler placed stability test of DM-NCTD (n=5)

Sample	RSD (%)								
	25°C, 6 hours (µg/mL)			25°C, 12 hours (µg/mL)			25°C, 24 hours (µg/mL)		
	0.1	1	5	0.1	1	5	0.1	1	5
Heart	7.3	8	10.2	10.7	5.4	3.9	5	9.4	11.3
Liver	8.8	11.3	8.4	5.1	9.7	6.3	8.8	10.7	7.9
Spleen	11.3	7.2	11.7	5.3	8.6	6.7	11.4	7.8	5.4
Lung	6.4	3.8	5.9	9.1	11.3	10.2	6	8.2	12.5
Kidney	8.4	3.2	11.5	13.2	5.7	6.1	10.4	9.3	5.2
Tumor	9.3	5.6	9	8.8	9.2	12.6	8.9	11.8	10.3

Abbreviations: DM, diacid metabolite; NCTD, norcantharidin; RSD, relative standard deviation.