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A simple and rapid colorimetric detection of serum IncRNA biomarkers for diagnosis of pancreatic cancer[†]

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A colorimetric assay is developed for detection of lncRNA HOTTIP by one-step reverse transcription-loopmediated isothermal amplification (RT-LAMP) coupled with positively-charged gold nanoparticles ((+) AuNP) for diagnosis of pancreatic cancer. This assay allows simple, rapid, and sensitive quantification of lncRNA down to 50 copies.

1. Introduction

Pancreatic ductal adenocarcinoma (PDAC), accounting for 95% of pancreatic cancer cases, is one of the most common malignancies with a high mortality-to-incidence ratio of 98% in 2018.^{1,2} PDAC patients are often diagnosed at an advanced stage due to the lack of displayed symptoms, leading to poor prognosis with an overall survival of 6 months after diagnosis only.³ Available treatments remained ineffective with the majority of patients developing metastatic diseases eventually.^{4,5} Meanwhile, the most common circulating PDAC biomarker in blood, carbohydrate antigen 19-9 (CA-19-9), is not applicable for diagnosis due to limited specificity and sensitivity.⁶ This high-lights an urgent demand for alternative biomarkers suitable for diagnosis of PDAC with high accuracy, simplicity and cost-effectiveness.

Non-coding RNA (ncRNA) has emerged to be a new hallmark for cancer. Short and long ncRNAs play essential roles in regulating gene expression and cellular mechanisms associated with cancer initiation and progression. However, detection of short ncRNA like microRNA (miRNA) remains challenging due to the short sequence and high homology among family members.⁷ Long non-coding RNA (lncRNA) accounting for more than 80% of ncRNA has higher sequence specificity as well as tissue specificity.⁷ lncRNAs are capable of resisting RNase digestion and circulate in body fluids with enhanced stability.⁸ Therefore, these emphasize the significance of lncRNAs as promising biomarkers for cancer diagnosis and prognosis. lncRNA HOXA distal transcript antisense RNA (HOTTIP) plays an important role in PDAC by promoting cell proliferation and migration.⁹ Studies reported abnormal upregulation of HOTTIP in PDAC tumours and importantly in body fluids,¹⁰ suggesting HOTTIP as a competent circulating biomarker for diagnosis of PDAC.

Few approaches have been developed to detect lncRNA. Microarrays and RNA sequencing are well-established methods while requiring expensive instrumentation.¹¹ Currently, quantitative reverse transcription PCR (RT-qPCR) remains the standard for lncRNA detection.7 However, RT and qPCR must be performed separately in two steps which are prone to contamination. Sample isolation and purification are often required for RT-qPCR, making the procedures complicated, costly and timeconsuming. Such an approach is also less reliable for detection in body fluids due to a lack of standardized reference genes for normalization.⁷ Droplet digital PCR (ddPCR) has emerged as a new generation of PCR technology for quantification of miRNA and circular RNA (circRNA), with improved precision, sensitivity and reproducibility compared to RT-qPCR.12,13 Nevertheless, requirements of sample purity and quality, thermocycling conditions and relatively high cost of ddPCR limit its application for early detection. A novel cyclic enzymatic repairing-mediated signal amplification has been reported recently for fluorescent detection of lncRNA HOTAIR in cancer cells.14 Therefore, it is necessary to develop direct method for detection of lncRNAs in patient samples. Here, we applied a novel and simple approach for lncRNA detection using reverse transcription-coupled loop-mediated isothermal amplification (RT-LAMP), which functions at low temperature for rapid and highly sensitive detection.¹⁵ LAMP utilizes a set of multiple primers targeting 6 to 8 regions which enhances sensitivity and specificity for detection. Comparing to traditional RT-qPCR, one-step RT-LAMP takes 30-60 min at constant low temperature of 50-65 °C for reaction to proceed, without using sophisticated equipment.¹⁶ More importantly, LAMP provides another advantage of amplifying crude biological sample such as detergent-treated cerebrospinal fluid, heat-treated blood and

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stool samples while eliminating the need for nucleic acid extraction. $^{\scriptscriptstyle 17,18}$

Gold nanoparticles characterized by their optical properties and sensitivity are widely used for a range of biomedical applications, including genetic therapy, drug delivery and biosensors. Properties of the gold nanoparticles including sizes, shapes, charges and functionalities are dependent on the method of synthesis using various reducing and stabilizing agents.¹⁹ Gold nanoparticles are commonly applied for detection of nucleic acids, proteins and pathogens based on the redshift effect upon reaction with aggregation of particles, leading to a color change from red to purple.²⁰ However, such color shift is also induced by self-aggregation of nanoparticles in the absence of target molecules, which may affect reliability and clarity for colorimetric sensor detection.

Herein, we proposed a colorimetric assay combining LAMP amplification with aggregation of positively-charged gold nanoparticles ((+)AuNPs) for detection of HOTTIP, as shown in Fig. 1. HOTTIP in serum is first amplified by LAMP assay. Negatively-charged double-stranded DNA (dsDNA) synthesised during LAMP precipitate (+)AuNPs, leading to a distinctive color change from red to colorless due to increased gravitational force of the AuNP-nucleic acid structure. Such decolorization process is triggered by increasing lncRNA concentration, so we hypothesized that upregulation of lncRNA biomarker in cancer samples would result in significant color change compared to normal samples.

2. Materials and methods

2.1 Materials and reagents

Bst3.0 polymerase, magnesium sulfate and $10 \times$ isothermal amplification buffer were purchased from New England Biolabs

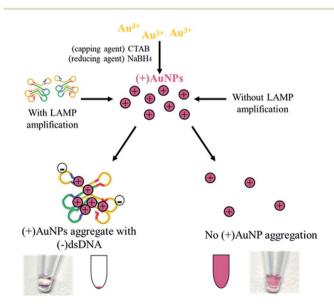


Fig. 1 Schematic illustration of colorimetric LAMP-(+)AuNP assay. First, one-step RT-LAMP is performed to amplify HOTTIP in serum. Subsequently, (+)AuNPs are added leading to decolorization depending on HOTTIP expression level.

(Ipswich, MA, USA) while reverse transcriptase was ordered from Thermo Fisher Scientific (Vilnius, Lithuania). Six oligonucleotide primers for loop-mediated isothermal amplification of HOTTIP were designed through the PrimerExplorer V5 software available online (http://primerexplorer.jp/lampv5e/ index.html), which includes forward inner primer (FIP), backward inner primer (BIP), forward outer primer (F3), backward outer primer (B3), loop forward primer (LF) and loop backward primer (LB) (Table S1†). Chloroauric acid (HAuCl₄), cetyltrimethyl ammonium bromide (CTAB) and sodium borohydride (NaBH₄) were obtained from Sigma-Aldrich (St. Louis, MO).

2.2 Cell lines and mouse serum samples

PDAC cell lines PANC-1 and CFPAC-1 were obtained from American Type Culture Collection (Manassas, VA) and cultured in Dulbecco's Modified Eagle's Media (DMEM) containing 10% fetal bovine serum and 100 units per mL of penicillin and streptomycin. Total RNA from cell lines and genomic DNA were isolated using TRIzol-chloroform extraction and salt extraction respectively. Male BALB/c nude mice aged 4 to 6 weeks were obtained from Laboratory Animal Services Centre of the Chinese University of Hong Kong. All animal procedures were performed in accordance with the Guidelines for Care and Use of Laboratory Animals of Chinese University of Hong Kong and approved by the Animal Ethics Committee of Chinese University of Hong Kong.

For *in vivo* mice xenograft model, CFPAC-1 cells were orthotopically injected into the pancreas of the mice. The tumor was allowed to grow for at least 8 weeks for tumor development before serum collection. For serum isolation, blood was allowed to clot for 30 minutes after collection at room temperature, followed by centrifugation at 2000*g* for 10 minutes.

2.3 In vitro transcription of HOTTIP transcripts

HOTTIP expression plasmid was obtained from abm and was digested with XhoI to generate linearized DNA template. *In vitro* transcription of HOTTIP RNA was performed by MEGAscript T7 Transcription Kit according to the manufacturer's protocol.

2.4 Loop-mediated isothermal amplification

Reactions were prepared on ice in Eppendorf PCR tubes. Standard LAMP was performed in incubator at 60 °C for one hour. Typical LAMP reaction volume was 5 μ L, which contained 0.2 μ M of F3 and B3 primers, 1.6 μ M of FIP and BIP primers, 8 mM MgSO₄, 12.5 U reverse transcriptase and 1.6 U Bst3.0 polymerase (NEB). 500 ng of PANC-1 DNA was used in positive reactions. For detection in serum sample, top-up water volume was replaced by diluted serum. After reaction, 1 μ L of amplification products were analysed in 2% agarose gel electrophoresis stained in GelRed stain (IO Rodeo) under UV transilluminator.

2.5 Preparation of positively-charged gold nanoparticles

(+)AuNPs were prepared according to Li's approach.²¹ Briefly, 1 mM of chloroauric acid (HAuCl₄) and 10 mM of cetyltrimethyl ammonium bromide (CTAB) (Sigma-Aldrich) were mixed in

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a 17 mL solution to produce a yellowish solution, and the mixture was allowed to stirred in a shaker for 15 minutes. Then, 100 mM sodium borohydride (NaBH₄) (Sigma-Aldrich) in 2 mL was added drop by drop with stirring. The mixture was stirred for another 8 min until there was a permanent color change to a reddish-purple solution. Subsequently, the (+)AuNP solution was filtered and stored at -4 °C before use.

2.6 Characterization of gold nanoparticles

Size and shape of gold nanoparticles were characterized under transmission electron microscope (TEM, Hitachi, H-7700, Tokyo, Japan). Size distribution and zeta potential analysis were investigated using particle size analyser (Zetasizer Nano ZS90, Malvern Panalytical Ltd, England). Interaction between AuNP and LAMP was demonstrated by Fourier Transform Infrared Spectroscopy (FTIR) (Thermo Nicolet, Nexus). Data were presented as mean \pm SD from three independent experiments.

2.7 Optimization of absorbance wavelength for AuNP detection

Optimization of wavelength was conducted using PANC-1 gDNA in 1 μ L reacting with 10 μ L of (+)AuNP. Absorbance in the range of 400 nm to 700 nm were recorded after 1 hour using Nano-Drop 2000 Spectrophotometer (Thermo Fisher Scientific, Wilmington, DE).

2.8 LAMP-(+)AuNP colorimetric detection of lncRNA HOTTIP in mice serum

Serum samples from 29 healthy mice and 13 mice xenografts were analysed. LAMP reaction in 5 μ L was prepared in optimized conditions. Top-up water volume was replaced by diluted serum samples while 0.6 μ L of serum was needed for each reaction. After LAMP, 1 μ L of solution was added to 20 μ L of (+) AuNP particles for decolorization at room temperature. Absorbance at 520 nm was measured after 30 min.

2.9 Statistical analysis

Statistical analysis was performed by GraphPad Prism 6 and difference between two groups were analysed using one-way analysis of ANOVA. Statistical significance was considered when *p*-value (two-sided) smaller than 0.05.

3. Results and discussion

3.1 Optimization of LAMP conditions

The combination and concentration of primers for LAMP was first determined (Fig. S1, ESI[†]). The optimal primer sets included 0.2 μ M of outer F3 and B3 primers and 1.6 μ M of inner FIP and BIP primers (Fig. S2, ESI[†]). With optimal primer conditions, experimental parameters including temperature, time, concentration of magnesium sulfate, reverse transcriptase and Bst3.0 polymerase were optimized systematically (Fig. S3, ESI[†]). Subsequent reactions were carried out using 8 mM MgSO₄, 12.5 U reverse transcriptase, 16 U Bst3.0 polymerase at 60 °C for 60 min.

Under the optimized conditions, specificity and sensitivity of LAMP for detection of HOTTIP were then evaluated. Since the outer primers (F3 and B3) create the basis of the loop structure for amplification in LAMP, we validated the specificity of these primers. PCR was carried out using outer F3 and B3 primers. Analysis of PCR product by agarose gel electrophoresis showed a single band with expected size (Fig. 2a). Sanger sequencing of the PCR product also confirmed the specificity of primers for HOTTIP (Fig. 2b). We then evaluated the sensitivity of the LAMP assay over a range from 10¹⁰ to 0 copies of HOTTIP. As low as 50 copies of HOTTIP could be detected in our assay (Fig. 2c). Since components in serum such as amino acids or salts may inhibit LAMP assay by binding to essential magnesium ions and polymerase enzymes,22 we next determined the optimal dilution of serum for HOTTIP detection. Four-fold dilution of serum could achieve the highest efficiency of HOTTIP detection (Fig. 2d).

3.2 Characterization of (+)AuNPs and interaction with LAMP products

Size and shape of (+)AuNPs after synthesis were characterized under transmission electron microscopy (TEM), showing spherical

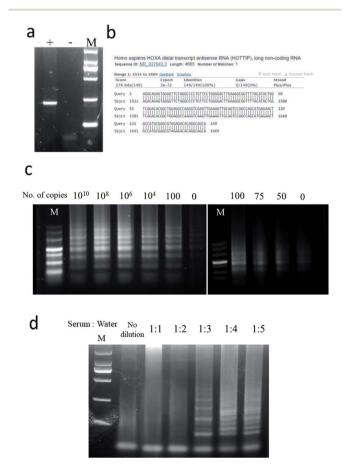


Fig. 2 Specificity, sensitivity and performance of detecting HOTTIP by LAMP in serum. Specificity of LAMP F3 and B3 primers to HOTTIP were validated under (a) agarose gel electrophoresis and (b) Sanger sequencing; +: positive control; -: negative control. (c) Evaluation of sensitivity of LAMP over a range from 10^{10} to 0 copies of HOTTIP. (d) Optimization of LAMP in serum with different dilution.

gold nanoparticles with estimated average size of 10 \pm 1.5 nm (Fig. 3a). Dynamic light scattering (DLS) revealed size distribution of nanoparticles with hydrodynamic diameter of 29 \pm 3.4 nm (Fig. 3b), while TEM would provide a more accurate measurement of the particle hard core size.²³ Polydispersity index (PDI) of 0.33 \pm 0.04 under DLS analysis demonstrated uniformity and monodispersity of the gold nanoparticles.

After incubation of gold nanoparticles with LAMP reaction products, there was a rightward shift of increase in average particles size distribution from 29 nm to 401.6 \pm 52.1 nm estimated by DLS, with large aggregates observed under TEM (Fig. 3c). Two size distribution patterns were shown, with a major peak indicating large aggregation between LAMP products and nanoparticles, while unreacted particles or smaller aggregates contributed to the lower peak. This suggested that aggregation of gold nanoparticles occurred as a result of interaction between AuNP and LAMP products.

Zeta potential analysis of the gold nanoparticles confirmed positive nature (+34.5 \pm 2.5 mV) of particles (Fig. 4a). There was a reduction in zeta potential to +22.9 \pm 4.6 mV after incubation with LAMP components due to neutralization of positive charges of gold nanoparticles by negatively-charged primers and dNTPs (Fig. 4b). Moreover, the zeta potential further reduced to +15.8 \pm 1.6 mV in the presence of LAMP reaction products due to absorption of negatively-charged nucleic acid polymers formed in LAMP to positive-charged gold nanoparticles (Fig. 4c).

To further validate the interaction between LAMP and AuNP, FTIR spectra of purified LAMP products, AuNP, and LAMP/ AuNP reaction complexes were collected (Fig. 4d). From the LAMP product spectrum, two distinct peaks observed at approximately 1040 cm⁻¹ and 1080 cm⁻¹ were representative of C-C bond vibration in DNA ribose sugar and phosphate group (P-O) respectively.^{24,25} Aggregates formed after incubation of AuNP with LAMP products demonstrated a broader peak with

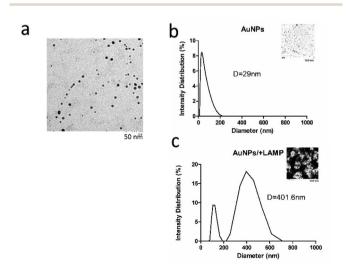


Fig. 3 Characterization of gold nanoparticles and interaction with LAMP products. AuNPs were observed under (a) TEM and (b) DLS image. (c) TEM and DLS analysis after incubation of AuNPs with LAMP reaction product.

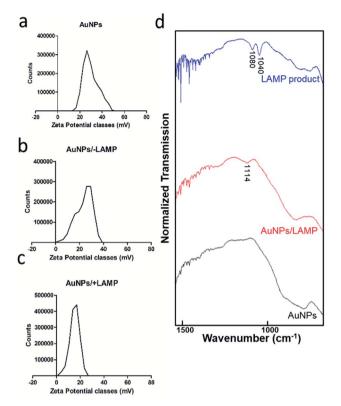


Fig. 4 Validation of interaction between LAMP and AuNP by zeta potential analysis of (a) AuNP alone, (b) after incubation with LAMP components, (c) after incubation with LAMP reaction products; and (d) FTIR spectrum of LAMP product, AuNP and LAMP/AuNP reaction complexes.

a shift to 1114 cm⁻¹, which was combination of the two DNA bands. The bands indicative for DNA were absent in AuNP alone, confirming the interaction between LAMP products and nanoparticles.

3.3 Optimization and sensitivity of the colorimetric (+) AuNPs detection

The analytical performance of positively-charged gold nanoparticles on detection of LAMP products were evaluated. Using genomic DNA ranging from 0 to 1600 ng reacting with 10 µL of (+)AuNP, the optimal wavelength at 520 nm was determined for DNA detection (Fig. 5a). Since the (+)AuNP would precipitate with negatively-charged LAMP components including dNTP and primers, aggregation with LAMP product and decolorization of the (+)AuNP reaction mixture would be interfered. This may potentially lead to false positive results (Fig. S4a in the ESI⁺). Therefore, LAMP components to (+)AuNPs ratio was optimized to minimize background decolorization. 20 µL of (+)AuNPs per µL of LAMP reaction mixture could overcome the interference brought by the negatively-charged dNTP and primers in LAMP (Fig. S4b in the ESI[†]). We then coupled (+)AuNPs with LAMP over a range from 10¹⁰ to 100 copies of HOTTIP as input for detection. As expected, there was a negative correlation between HOTTIP copy number and absorbance measured (Fig. 5b).

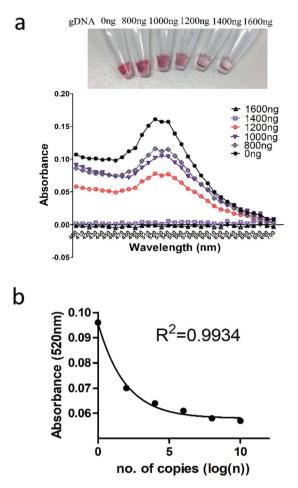


Fig. 5 Optimization and analysis of performance of (+)AuNP detection. (a) Absorption spectra of (+)AuNP over a range of DNA from 0 to 1600 ng. (b) High sensitivity of AuNP illustrated by detection of LAMP products with different copies of input HOTTIP transcripts ranging from 10¹⁰ to 100 copies.

3.4 LAMP-AuNP colorimetric detection of lncRNA HOTTIP in normal and cancer mice serum

To investigate the capability of the LAMP-(+)AuNP assay in detecting HOTTIP in PDAC serum, the assay was applied for detection in mice serum with PDAC. CFPAC-1 cells were orthotopically injected to the pancreas in BALB/c nude. Mice serum was collected when tumour was developed. LAMP was carried out using diluted normal and PDAC mice serum samples with gold nanoparticles added subsequently. Absorbance was measured after 30 min. In general, reaction mixture turned colorless for tumor samples while remained red for normal samples (Fig. 6a). In addition, color changes were quantified by measuring the absorbance at 520 nm. The LAMP-(+)AuNP assay for HOTTIP detection in PDAC had sensitivity of 69% and specificity of 83% at a cut-off value of 0.06 (Fig. 6b). Area under the receiver operating characteristic (ROC) curve confirmed the good performance of this diagnostic assay (Fig. 6c). Collectively, our results demonstrated the utility of LAMP-(+)AuNP assay for diagnosis of PDAC by detection of lncRNA HOTTIP in diluted serum.

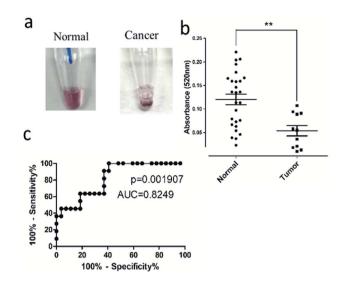


Fig. 6 LAMP-AuNP colorimetric detection in mice serum with PDAC. (a) Representative images of color change of (+)AuNP solution after LAMP assay in normal and cancer mice serum. (b) Quantitative measurement of the (+)AuNP solution after LAMP assay at A_{520} . At a cut-off value of 0.06, LAMP-(+)AuNP assay had sensitivity of 69.2% and specificity of 82.8%. ***p*-Value < 0.001. (c) Area under the receiver operating characteristic (ROC) curve showing good performance of the LAMP-AuNP assay.

4. Conclusions

In summary, our study proposed a rapid colorimetric approach for detection of lncRNA HOTTIP in diluted serum for diagnosis of PDAC using the LAMP-(+)AuNP assay. A major advantage of this assay is its feasibility in diluted serum without the need of RNA extraction and purification. The reaction includes two steps carried out in single tube under isothermal condition for one hour with high simplicity and cost-effectiveness. LAMP detection has high sensitivity down to 50 copies of HOTTIP with enhanced specificity using multiple primers without complicated probe design. Decolorization induced by aggregation of nanoparticles is distinctive between normal and cancer samples and which can be further validated by quantitative measurement, confirming reliability of the assay. Therefore, the LAMP-(+)AuNP assay has great potential for clinical screening of PDAC based on lncRNA detection. Multiple biomarkers may be utilized to improve accuracy of detection. Regarding to identification of urine-based and saliva-based biomarkers in cancer diagnosis,²⁶⁻²⁸ we aim at developing a completely non-invasive diagnostic approach using alternative biological fluids which would be investigated in the future.

Conflicts of interest

There are no conflicts to declare.

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Notes and references

- 1 M. Ilic and I. Ilic, World J. Gastroenterol., 2016, 22, 9694–9705.
- 2 E. B. Andrew, G. H. Yasmin, F. Harold and L. L. Aimee, *World J. Gastroenterol.*, 2014, **20**, 11182–11183.
- 3 D. F. Megan, A. A. Melissa, I. L. Christopher, J. D. R. Anneclaire and J. B. Deborah, *Cancer Epidemiol.*, *Biomarkers Prev.*, 2005, **14**, 1766–1773.
- 4 P. E. Oberstein and K. P. Olive, *Ther. Adv. Gastrointest. Endosc.*, 2013, **6**, 321–337.
- 5 C. L. Wolfgang, J. M. Herman, D. A. Laheru, A. P. Klein, M. A. Erdek, E. K. Fishman and R. H. Hruban, *Ca-Cancer J. Clin.*, 2013, **63**, 318–348.
- 6 K. E. Poruk, D. Z. Gay, K. Brown, J. D. Mulvihill,
 K. M. Boucher, C. L. Scaife and S. J. Mulvihill, *Curr. Mol. Med.*, 2013, 13, 340–351.
- 7 T. Shi, G. Gao and Y. Cao, Dis. Markers, 2016, 2016, 1-10.
- 8 L. Bolha, M. Ravnik-Glavač and D. Glavač, *Dis. Markers*, 2017, **2017**, 1–14.
- 9 Y. Cheng, I. Jutooru, G. Chadalapaka, J. C. Corton and S. Safe, *Oncotarget*, 2015, **6**, 10840–10852.
- Y. Wang, Z. Li, S. Zheng, Y. Zhou, L. Zhao, H. Ye, X. Zhao,
 W. Gao, Z. Fu, Q. Zhou, Y. Liu and R. Chen, *Oncotarget*, 2015, 6, 35684–35698.
- 11 S. Uchida, *High-Throughput*, 2017, 12, DOI: 10.3390/ ht6030012.
- 12 F. E. Ahmed, N. C. Ahmed and M. M. Gouda, *Integr. Cancer Sci. Ther.*, 2018, **5**, 1–7.
- 13 C. Wang, Q. Ding, P. Plant, M. Basheer, C. Yang, E. Tawedrous, A. Krizova, C. Boulos, M. Farag, Y. Cheng and G. M. Yousef, *Clin. Biochem.*, 2019, 67, 54–59.
- 14 Y. Zhang, X. Wang, X. Su and C. Zhang, *Chem. Commun.*, 2019, **55**, 6805–6952.

- 15 D. J. Grab, O. V. Nikolskaia, N. Inoue, O. M. Thekisoe, L. J. Morrison, W. Gibson and J. S. Dumler, *PLoS Neglected Trop. Dis.*, 2011, 5, e1249.
- 16 D. G. Wang, J. D. Brewster, M. Paul and M. Peggy, *Molecules*, 2015, **20**, 6048–6059.
- 17 D. J. Grab, O. V. Nikolskaia, N. Inoue, O. M. Thekisoe, L. J. Morrison, W. Gibson and J. S. Dumler, *PLoS Neglected Trop. Dis.*, 2011, 5, e1249.
- 18 Z. K. Njiru, PLoS Neglected Trop. Dis., 2012, 6, e1572.
- 19 Y. C. Yeh, B. Creran and V. M. Rotello, *Nanoscale*, 2012, 4, 1871–1880.
- 20 D. Vilela, M. C. González and A. Escarpa, *Anal. Chim. Acta*, 2012, **751**, 24–43.
- 21 Z. Li, X. Miao, K. Xing, A. Zhu and L. Ling, *Biosens. Bioelectron.*, 2015, 74, 687-690.
- 22 H. Kaneko, T. Kawana, E. Fukushima and T. Suzutani, J. Biochem. Biophys. Methods, 2007, 70, 499–501.
- 23 F. D. Sikkema, M. Comellas-Aragones, R. G. Fokkink, B. J. M. Verduin, J. J. L. M. Cornelissen and R. J. M. Nolte, *Org. Biomol. Chem.*, 2007, 5, 54–57.
- 24 T. Rolim, J. Cancino and V. Zucolotto, *Biomed. Microdevices*, 2015, **17**, 1–9.
- 25 B. R. Wood, Chem. Soc. Rev., 2016, 45, 1980-1998.
- 26 A. Øverbye, T. Skotland, C. J. Koehler, B. Thiede, T. Seierstad,
 V. Berge, K. Sandvig and A. Llorente, *Oncotarget*, 2015, 6, 30357–30376.
- 27 O. E. Bryzgunova, M. M. Zaripov, T. E. Skvortsova,
 E. A. Lekchnov, A. E. Grigor'eva, I. A. Zaporozhchenko,
 E. S. Morozkin, E. I. Ryabchikova, Y. B. Yurchenko,
 V. E. Voitsitskiy and P. P. Laktionov, *PLoS One*, 2016, 11, e0157566.
- 28 T. Machida, T. Tomofuji, T. Maruyama, T. Yoneda, D. Ekuni,
 T. Azuma, H. Miyai, H. Mizuno, H. Kato, K. Tsutsumi,
 D. Uchida, A. Takaki, H. Okada and M. Morita, *Oncol. Rep.*, 2016, 36, 2375–2381.