

Comparative analysis between 5 mm and 7.5 mm collimators in CyberKnife radiosurgery for trigeminal neuralgia

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ABSTRACT

Trigeminal neuralgia (TN) is treated in CyberKnife (Accuray Inc, Sunnyvale, USA) with the 5 mm collimator whose dosimetric inaccuracy is higher than the other available collimators. The 7.5 mm collimator which is having less dosimetric uncertainty can be an alternative for 5 mm collimator provided the dose distribution with 7.5 mm collimator is acceptable. Aim of this study is to analyze the role of 7.5 mm collimator in CyberKnife treatment plans of TN. The treatment plans with 5 mm collimators were re-optimized with 7.5 mm collimator and a bi-collimator system (5 mm and 7.5 mm). The treatment plans were compared for target coverage, brainstem doses, and the dose to normal tissues. The target and brainstem doses were comparable. However, the conformity indices were 2.31 ± 0.52 , 2.40 ± 0.87 and 2.82 ± 0.51 for 5 mm, bi-collimator (5mm and 7.5 mm), 7.5 mm collimator plans respectively. This shows the level of dose spillage in 7.5 mm collimator plans. The 6 Gy dose volumes in 7.5 mm plans were 1.53 and 1.34 times higher than the 5 mm plan and the bi-collimator plans respectively. The treatment time parameters were lesser for 7.5 mm collimators. Since, the normal tissue dose is pretty high in 7.5 mm collimator plans, the use of it in TN plans can be ruled out though the treatment time is lesser for these 7.5 mm collimator plans.

Key words: Collimators, CyberKnife, stereotactic radiosurgery, trigeminal neuralgia

Introduction

Trigeminal neuralgia (TN) is the 5th cranial nerve disorder, which results in unbearable facial pain in patients.^[1-3] Radiosurgery is one of the treatment options for TN.^[4,5] Radiosurgery for TN is a very unique procedure as the TN target is the smallest of all known radio surgical targets. Hence, it requires a high degree of precision and accuracy while targeting with a radiosurgical unit. Gamma Knife is one such radiosurgical unit, which is being used

traditionally to treat TN.^[6-8] Gamma Knife radiosurgery is an invasive frame based procedure. However, due to technical advancements in precise targeting, linear accelerator based radiosurgery, and robotic radiosurgery are employed to treat the Trigeminal nerve target as a noninvasive frameless procedure.^[9-14] CyberKnife (Accuray, Sunnyvale, USA) is a robotic radiosurgery unit which is used to treat both intracranial and extracranial lesions stereotactically.

Since TN is the smallest radiosurgical target, the smallest collimator size available in the respective radiosurgical units is used to treat it. In CyberKnife 5 mm collimator is preferred for treating TN while 4 mm is preferred in Gamma Knife. Though, this small collimator sizes are giving reasonable dose distributions in the treatment planning systems, the dosimetric accuracy of such a small radiosurgical fields may not be guaranteed due to the following reasons. According to Pantelis *et al.*,^[15] a diode detector overestimates the output factor of 5 mm collimator of CyberKnife by 5% while a pinpoint ionization chamber underestimates it by 10%. CyberKnife output factor studies by Rah *et al.*,^[16] also shows inaccuracies with the diode and ionization chamber detectors. The diode and ionization chamber detectors are the detectors, which are used traditionally for the relative beam data measurements in classical linear accelerators.

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Since, these detectors are showing uncertainties in output factor measurement of CyberKnife small beams, other non-conventional detectors such as gel dosimeter^[15] and glass rod detector^[16,17] were used to find out the CyberKnife output factors. Though, there are reasons explained by researchers for the inaccuracy in the measurement of output factors, it is an issue with the small collimators and it is predominant for the smallest 5 mm collimator than the other collimator sizes in CyberKnife.^[16-20] Studies by Yu *et al.*,^[18] states that, those uncertainties in output factor measurement increases with a decrease in the collimator size. The dose linearity with monitor unit (MU) is poorer for 5 mm collimator than all other 11 collimator sizes available in CyberKnife.^[21] Since, there is a probable dosimetric inaccuracy with 5 mm collimator; the accurate dose delivery with the 5 mm collimator would be a challenge especially for very tiny targets like the nerve target of TN.

Average volume of a TN target is about 40 mm³.^[14] The thickness of the nerve target is about 2 mm and the length is about 6 mm. Because of such small dimensions of the nerve target 5 mm collimator is preferred in CyberKnife. However, the immediately next collimator size of 7.5 mm, which is having less dosimetric uncertainty than the 5 mm collimator may perhaps be a choice for the CyberKnife treatment of TN. There are evidences available in the literature for selecting larger collimator sizes. Fraioli *et al.*^[10] used 10 mm collimator in a dedicated linear accelerator and Kanner *et al.*^[22] used concentric 4 mm and 8 mm collimators in Gamma Knife. Similarly, Smith *et al.*^[23] used 5 mm and 7.5 mm collimators in a dedicated linear accelerator set up to treat TN.

Dose distribution with 7.5 mm collimator should be analyzed before considering it for the treatment of TN. In the present study, an attempt is made to find out the role of 7.5 mm collimator in the CyberKnife treatment plans of TN.

Materials and Methods

Randomly selected 11 TN patients were taken for this retrospective study. Multiplan treatment planning system (Accuray, Sunnyvale, USA) was used to generate the CyberKnife radiosurgery treatment plans. The nerve target and the organs at risks (OARs) were delineated in computed tomography images (1 mm slice thickness) after fusing with the special magnetic imaging sequence called T2 drive. The initial treatment plans were generated and executed with 5 mm collimators. The prescribed dose was 60 Gy in a single fraction to the nerve target. Usually, this 60 Gy is prescribed to 75-85% isodose with respect to the maximum point dose. The maximum point dose to the brain stem was a constraint dose of 40 Gy. Retrospectively, the treatment plans for 7.5 mm collimator were generated by keeping the same optimization goals. However, the optimization was

rerun. In a similar way, treatment plans were generated with 5 mm and 7.5 mm bi-collimator system as well.

The target doses were analyzed and compared for volume doses, dose conformity, and homogeneity. In the target volume doses, $D_{98\%}$, $D_{90\%}$, $D_{75\%}$, $D_{50\%}$, $D_{30\%}$, and $D_{10\%}$ were taken for the analysis. Conformity index was calculated using the Paddick^[24] and Nakamura *et al.*,^[25] formula. Conformity Index = $(V_{RI} \times TV)/(TV_{RI})^2$, where V_{RI} is the overall volume receiving the prescription dose, TV is the Trigeminal nerve target volume, and TV_{RI} is the target volume, which receives the prescription dose. Homogeneity index was calculated using the following formula. Homogeneity index = D_{max}/D_{RI} ,^[26] where D_{max} is the maximum point dose, D_{RI} is the prescription dose. P values were calculated using the two tailed Student's T test and tabulated.

The dose spillage outside the target was calculated instead of the organ specific doses except the maximum doses of the brainstem. Brain stem is the critical OAR, which is in closer vicinity to the trigeminal nerve target.^[14] Hence, brainstem is the OAR, which is prone to get very high dose when compared to all other OARs drawn for the CyberKnife treatment planning of TN. Keeping this in mind the brain stem dose and the dose to soft-tissue, which is surrounding the nerve target, were also analyzed in this study. In brainstem the maximum dose was estimated by using the volume dose indices $D_{1\%}$, $D_{2\%}$ and the maximum point dose. The dose indices $D_{5\%}$ and $D_{10\%}$ were also taken for analysis. Dose to the normal tissue, which is surrounding the nerve target, was analyzed in terms of the dose volumes $V_{100\%}$, $V_{90\%}$, $V_{75\%}$, $V_{50\%}$, $V_{25\%}$, and $V_{10\%}$. Here, $V_{100\%}$ indicates the overall volume excluding the target, which receives the prescription dose of 60 Gy.

The treatment parameters, such as the number of beams, number of nodes, and the total number of MUs were also compared between the treatment plans. Nodes are the virtual points in space where the robot places the miniature linear accelerator for different beam orientations. Several nodes constitute a path. For TN, a dedicated treatment path is available in CyberKnife radiosurgery.

Results

The mean volume of the trigeminal nerve target was 36.9 ± 3.4 mm³. The mean prescription volume, which is nothing but the $V_{100\%}$ was $71.7 \pm 7.8\%$ volume of the nerve target. Dose distribution comparison between the treatment plans by 5 mm collimator, 5 mm and 7.5 mm collimators and 7.5 mm collimator for a sample case is shown in Figure 1.

As far as the target dose coverage is concerned, all the three plans were yielding similar results. The mean value of the $D_{98\%}$ was 48.8 ± 3.8 Gy, 50.1 ± 4.0 Gy, and

49.7 ± 3.9 Gy respectively for 5 mm collimator plan, 5 mm and 7.5 mm collimators plan and 7.5 mm collimator plan. Similarly, D_{10%} values were 72.1 ± 2.1 Gy, 70.4 ± 2.6 Gy and 69.1 ± 2.9 Gy respectively for 5 mm, 5 mm and 7.5 mm, 7.5 mm collimator plans. The graph between the volume dose index and the target doses are shown in Figure 2. The maximum, minimum and the mean target doses along with the conformity index and homogeneity index are given in Table 1. The conformity index for the 5 mm plan is found to be the smallest when compared to the other two plans. The mean conformity indices were 2.31 ± 0.52, 2.40 ± 0.87 and 2.82 ± 0.51 for 5 mm, 5 mm and 7.5 mm, 7.5 mm collimator plans respectively. However, the 7.5 mm plan is more homogeneous than the other two plans.

The mean values of D_{1%} of the brain stem were 10.1 ± 2.4 Gy, 10.4 ± 2.2 Gy and 10.6 ± 2.1 Gy for 5 mm, 5 mm and 7.5 mm, 7.5 mm collimator plans respectively. Similarly, the maximum point doses were 37.4 ± 2.2 Gy, 38.1 ± 5.1 Gy and 38.8 ± 5.5 Gy for 5 mm, 5mm and 7.5 mm, 7.5 mm collimator plans respectively. The graph between the brainstem volume dose index and the corresponding brainstem dose is plotted in Figure 3.

The dose spillage outside the target was considerably higher for the 7.5 mm plan than the other two plans. Specifically, the 6 Gy volume (V_{10%}) was 15.2cc for 7.5 mm plan while it was 11.3cc for 5 mm and 7.5 mm plan and 9.9cc for 5 mm plan. The graph between the dose volume index and the soft-tissue volume is shown in Figure 4.

As far as the treatment parameters (Number of beams, Nodes and MU) are concerned the 7.5 mm collimator plan was yielding the lesser values than 5 mm collimator plan

and the 5 mm and 7.5 mm collimator plan. The comparison between the collimator plans in terms of the number of nodes and beams are shown in Figure 5. The total numbers of MUs for all the 11 cases in all the three collimator plans are compared in Figure 6.

Discussion

From the results, it is noticeable that the target dose coverage is almost the same in all the three plans. However, the maximum brain stem doses are higher for the 7.5 mm collimator plans than the bi-collimator (5 mm and 7.5 mm) plans and 5 mm collimators. Dose spillage outside the target including the brainstem is again higher for the 7.5 mm collimator plans. This dose spillage is a major drawback with the 7.5 mm collimator. This is a critical point as these higher doses are delivered in a single fraction. Specifically, the 6 Gy volumes in 7.5 mm collimator plans are about 1.53 times higher than 5 mm collimator plans and about 1.34 times higher than the bi-collimator plans. Similarly, the dose volume V_{50%} (volume receiving 30 Gy dose) is 3.3cc, 4.1cc, and 5.3 cc respectively for 5 mm collimator plan, 5 mm and 7.5 mm collimators plan, and 7.5 mm collimator plan. This shows the degree of dose spillage in 7.5 mm collimator plans than the other two plans.

On the other hand, the bi-collimator plans are yielding results in between the 7.5 mm collimator plans and 5 mm collimator plans. As far as the dose spillage is concerned, these bi-collimator plans are also poorer than the 5 mm collimator plans. Furthermore, restriction or addition of 7.5 mm collimators or 5 mm collimators in the bi-collimator system is not in the hands of the planner.

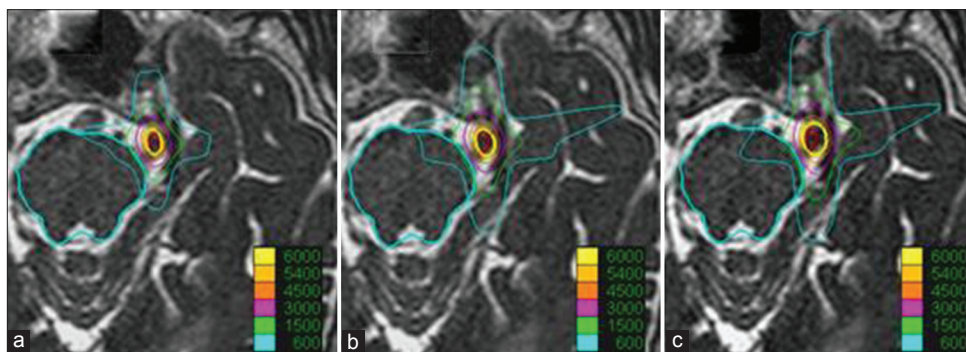


Figure 1: An axial dose distribution comparison between 5 mm collimator plan (a), 5-7.5 mm bi-collimator plan (b), and 7.5 mm collimator plan (c)

Table 1: Target dose distribution analysis for all the three collimator plans

Index	5 mm plan	5 mm and 7.5 mm plan	7.5 mm plan
Minimum dose	47.92±4.10 Gy (P=0.0816)	49.36±4.43 Gy (P=0.0971)	48.95±4.24 Gy (P=0.0824)
Maximum dose	74.03±1.79 Gy (P=0.0000)	72.47±3.32 Gy (P=0.0054)	70.80±2.83 Gy (P=0.0017)
Mean dose	63.52±1.07 Gy (P=0.0000)	63.27±1.85 Gy (P=0.0002)	62.78±1.41 Gy (P=0.0000)
Conformity index	2.31±0.52 (P=0.4750)	2.40±0.87 (P=0.6039)	2.82±0.51 (P=0.4556)
Homogeneity index	1.23±0.03 (P=0.0000)	1.21±0.06 (P=0.0053)	1.18±0.05 (P=0.0015)

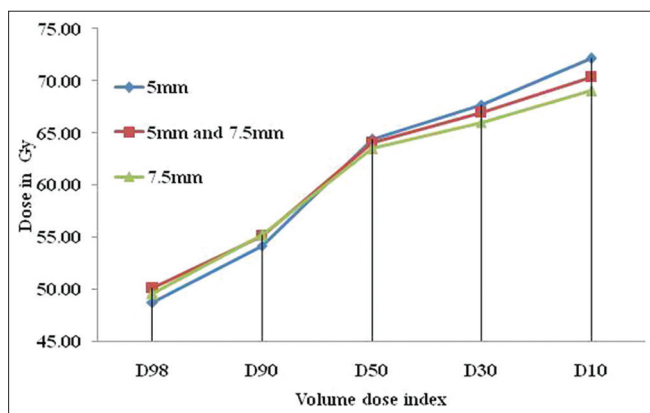


Figure 2: The graph between the volume dose index and the corresponding target doses in all the collimator plans

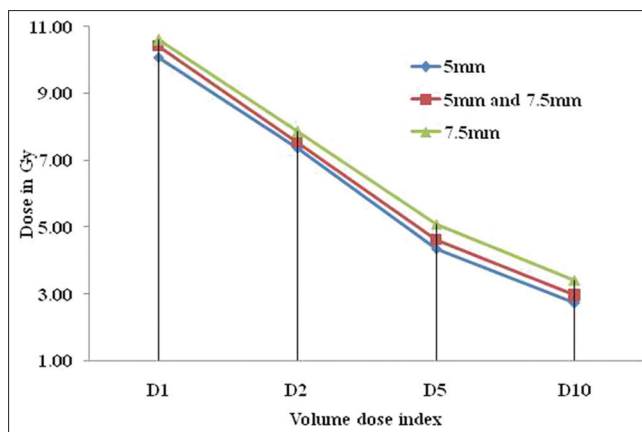


Figure 3: The graph between the brainstem volume dose index and the corresponding brainstem doses all the three collimator plans

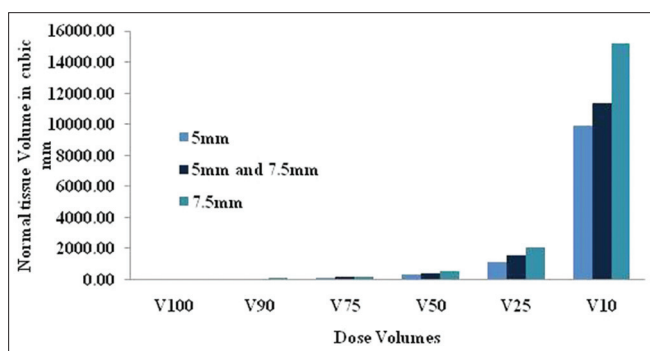


Figure 4: Comparison of the normal tissue doses in terms of dose volume indices

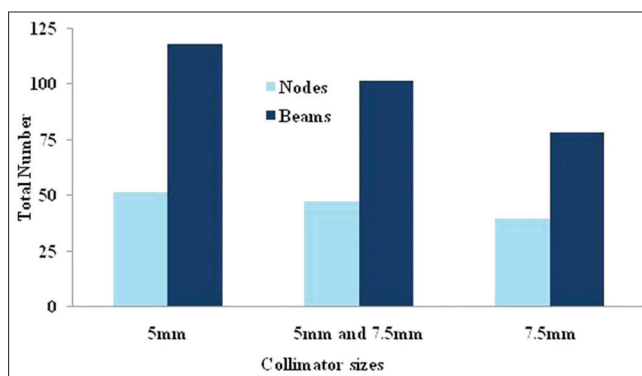


Figure 5: Comparison of the number of nodes and beams between the three collimator plans

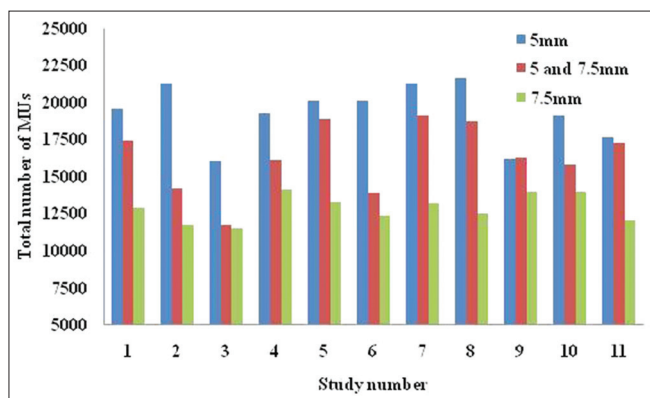


Figure 6: The MU spread in all the three collimator plans for all the 11 cases taken in the present study

From the present study, it is evident that the treatment parameters are having the least values for the 7.5 mm collimator. The number of beams and nodes are about 1.28 and 1.51 times higher for 5 mm collimator plans than the 7.5 mm collimators. Similarly, the bi-collimator plans are about 1.18 and 1.29 times higher than the 7.5 mm collimator plans. This reduction of treatment parameters encourages the fact of faster treatment delivery. In bi-collimator plans the mixing ratio of 5 mm beams and 7.5 mm beams is not consistent. Though this bi-collimator plan is better than the 7.5 mm collimator,

they are not showing any superiority over 5 mm collimator plans.

According to Flickinger *et al.*,^[27] increased treatment volume in TN may result in complications. Ma *et al.*^[28] emphasize the same while comparing the linear accelerator based radiosurgery and Gamma knife radiosurgery for TN. Based on this clinical fact, 7.5 mm collimator can be avoided in radiosurgical plans of TN as it irradiates more normal tissue than 5 mm collimators though it can yield lower treatment time parameters.

Conclusion

The TN nerve target dose coverage with 7.5 mm collimator is similar to that of the bi-collimator plans and 5 mm collimator plans. Brainstem doses are slightly higher for the 7.5 mm collimator. The bi-collimator plans are also inferior to 5 mm collimator plans in this respect. The treatment parameters are lower for 7.5 mm collimator plan than the other two plans. However, the normal tissue irradiated by 7.5 mm collimator is much higher than 5 mm collimator and 5 mm and 7.5 mm bi-collimator plans. Since the volume of irradiated normal tissue is critical in radiosurgery of TN, the role

of 7.5 mm collimator in CyberKnife radiosurgery for TN can be ruled out.

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