Anti-inflammatory Effect of Abciximab-Coated Stent in a Porcine Coronary Restenosis Model

The aim of this study was to examine the anti-inflammatory effect of abciximab-coated stent in a porcine coronary overstretch restenosis model. Ten abciximab-coated stents, ten sirolimus-eluting stents (SES), and ten paclitaxel-eluting stents (PES) were deployed with oversizing (stent/artery ratio 1.3:1) in porcine coronary arteries, and histopathologic analysis was done at 28 days after stenting. There were no significant differences in the neointima area normalized to injury score and inflammation score among the three stent groups $(1.58 \pm 0.43 \text{ mm}^2, 1.57 \pm 0.39 \text{ mm}^2)$ in abciximab-coated stent group vs. 1.69±0.57 mm², 1.72±0.49 mm² in the SES group vs. 1.92±0.86 mm², 1.79±0.87 mm² in the PES group, respectively). In the neointima, most inflammatory cells were lymphohistiocytes. Significant positive correlations were found between the extent of inflammatory reaction and the neointima area (r=0.567, p<0.001) and percent area stenosis (r=0.587, p<0.001). Significant correlations were found between the injury score and neointimal area (r= 0.645, p < 0.001), between the injury score and the inflammation score (r=0.837, p < 0.001), and between the inflammation score and neointimal area (r=0.536, p =0.001). There was no significant difference in the inflammatory cell counts normalized to injury score among the three stent groups $(75.5 \pm 23.1/\mu L)$ in abciximabcoated stent group vs. $78.8 \pm 33.2/\mu$ L in the SES group vs. $130.3 \pm 46.9/\mu$ L in the PES group). Abciximab-coated stent showed comparable inhibition of inflammatory cell infiltration and neointimal hyperplasia with other drug-eluting stents in a porcine coronary restenosis model.

Key Words : Stents; Inflammation; Blood Platelets

INTRODUCTION

Although the implantation of coronary stents can prevent vessels from post-interventional elastic recoil and appears to limit adverse remodeling, the problem of restenosis and the need for consecutive reinterventions remains the major limitation of stent implantation (1-3). The mechanism of instent restenosis (ISR) after stent implantation is principally neointimal hyperplasia (4-8). It has been reported that there is a strong correlation between the degree of vascular inflammation and neointimal formation (9, 10). The pathological process of ISR is characterized by an inflammatory healing process after stretch and damage of the vessel wall (10-12).

Based on observations that ISR is a consequence of inflammation and smooth muscle cell proliferation, several immunosuppressive and anti-proliferative therapies have been investigated to inhibit these processes. Sirolimus is a potent immunosuppressive agent with anti-inflammatory and anti-proliferative effects. Previous studies of sirolimus-eluting stent (SES) have shown a range of biological effects on inflammaYoung Joon Hong, Myung Ho Jeong, Sang Rok Lee, Seo Na Hong, Kye Hun Kim, Hyung Wook Park, Ju Han Kim, Weon Kim, Youngkeun Ahn, Jeong Gwan Cho, Jong Chun Park, Jung Chaee Kang

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tion and neointimal growth (13-15). Paclitaxel suppresses neointimal formation accompanied by persistent fibrin deposition, macrophage infiltration, and an overall decrease in smooth muscle cells after implantation (16-18).

Abciximab is a potent inhibitor that block the final pathway of platelet aggregation and decreases short- and longterm event rates after percutaneous coronary intervention (19-21). Besides blocking effect for platelet aggregation, abciximab reacts to $\alpha V\beta 3$ receptor of vascular smooth muscle cell and to Mac-1 of macrophage and inhibits proliferation of vascular smooth muscle cells and inflammatory reaction (22-26). Our previous study showed that abciximabcoated stent reduced stent restenosis by inhibition of cell proliferation and extracellular matrix synthesis compared with bare-metal stent in a porcine coronary restenosis model (27-29).

We examined the anti-inflammatory effect of abciximabcoated stent and compared with that of SES and with that of paclitaxel-eluting stent (PES) in a porcine coronary overstretch restenosis model.

MATERIALS AND METHODS

Animal study protocol

The animal study was approved by the Ethical Committee of the Chonnam National University Hospital in Gwangju, Korea. Study animals were female swine weighing 22-35 kg. To decrease acute thrombosis after stenting, premedication with aspirin 100 mg and clopidogrel 75 mg per day was given for 5 days before procedure. On the day of the stent implantation, pigs were anesthetized with ketamine (20 mg/ kg intramuscularly) and xylazine (2 mg/kg intramuscularly). They received 3 L/min of supplemental oxygen continuously through oxygen mask. After subcutaneous lidocaine 2% at the cut-down site was administered, left carotid artery was surgically exposed, and a 7-8F sheath was inserted. Continuous hemodynamic and surface electrocardiographic monitoring was maintained throughout the procedure. After Heparin 10,000 uints was administered intravenously as a bolus prior to the procedure, the target coronary artery was engaged using standard 7-8F guide catheters, and control angiograms of the both coronary arteries were performed using nonionic contrast agent in two orthogonal views.

Method of coating abciximab into stents

A plasma polymerization reaction was performed to attach amine radical to MAC stent (AMG, Munich, Germany) surface. A stent was fixed in tubular reactor, which was made by pyrex glass tube, and then the pressure was dropped to less than 5 mtorr by vacuum pump. For attachment of amine radical to stent surface, diaminocyclohexane monomer was drifted to tubular reactor a constant dose (0.96 SCCM), and plasma was generated using at a radiofrequency power generator. The power for polymerization of plasma was 100 W for 5 min and then 60 W for 15 min. The used abciximab is a human-murine chimeric antibody Fab fragment (c7E3 Fab) and blocks glycoprotein IIb/IIIa receptor directly. A 7 cm-long, 1 cm-wide glass tube was boiled in 100°C water for 5 min and then taken out and allowed to dry in an incubator. Then 2 mL of abciximab solution was delivered to this glass tube, and the stent was immersed in this solution. The carboxy radical of abciximab was introduced to amine radical attached to stent to achieve covalent bond and improved attachment power between stent and abciximab. This reaction was performed for 1 hr and then stent was taken out and allowed to dry for more than 24 hr. For release kinetics of abciximab from the stent, the stent was placed in glass vial and immersed in 100 mL of phosphate-buffered saline. We confirmed coating of abciximab onto the surface of the stent by scanning electron microscopy. The amount of coating of abciximab onto the surface of the stent was 90 µg/stent, and the median thickness of coating was 1 μ m. The amount of abciximab release to buffer solution was measured using absorbance test for ultraviolet at 278 nm. The amount of abciximab release increased with the time and remained on the stent surface 1 month after coating of abciximab to the stent.

Stent- induced stenosis

Besides abciximab-coated stent, we used two commercially available U.S. Food and Drug Administration-approved drug-eluting stent platforms Sirolimus (Cypher stent, Cordis, Johnson and Johnson, Miami Lakes, FL, U.S.A.) and Paclitaxel (Taxus stent, Boston Scientific, Boston, MA, U.S.A.). The used size and length of stents were 3.0×17 mm abciximab-coated stents, 3.0×18 mm SES, and 3.0×16 mm PES. The stent was deployed by inflating the balloon to nominal pressure at injury site, and the resulting stent-toarterv ratio was 1.3:1. Repeated angiograms were obtained immediately after stent implantation. Then, all equipments were removed, and the carotid artery was ligated. All animals received 100 mg of aspirin and 75 mg of clopidogrel orally daily until death. Twenty-eight days after stenting, the animals underwent repeated angiography in the same orthogonal views before death, and 20 mL of potassium chloride intracoronary injection was done. The hearts were removed, and the coronary arteries were pressure-perfusion fixed at 70 mmHg in 10% neutral-buffered formalin overnight. Arteries were step-sectioned, processed routinely for light microscopy, and stained with hematoxylin-eosin stain for histological analysis.

Histopathological analysis

Histopathologic evaluation of each artery was performed by an experienced cardiovascular pathologist. The specimens were embedded in methylmethacrylate, and sections were cut with the low-speed diamond wafer mounted to the Buehler Isomet saw (Buehler Ltd., Lake Bluff, IL, U.S.A.), leaving the stent wires intact in the cross sections to minimize potential artifacts from removal of stent wires. Sections of 50- to 100- μ m thickness were obtained at about 1 mm apart and stained with hematoxylin-eosin for histological analysis. Measurements of the histopathologic sections were performed using a calibrated microscope, digital video imaging system, and microcomputer program (Visus 2000 Visual Image Analysis System, IMT Tech., CA, U.S.A.). Borders were manually traced for lumen area, area circumscribed by the internal elastic lamina, and the innermost border of the external elastic lamina (external elastic lamina area). Morphometric analysis of the neointimal area for a given vessel was calculated as the measured internal elastic lamina area minus lumen area. The measurements were made on five cross-sections from the proximal and distal ends and the three midpoints of each stented segment. Histopathologic stenosis was calculated as $100 \times (1-$ [lesion lumen area/lesion internal elastic lamina area]).

Evaluation of arterial injury

Arterial injury at each strut site was determined by the anatomic structures penetrated by each strut. A numeric value was assigned, as previously described by Schwartz et al.: 0=no injury; 1=break in the internal elastic membrane; 2=perforation of the media; 3=perforation of the external elastic membrane to the adventitia (30). The average injury score for each segment was calculated by dividing the sum of injury scores by the total number of struts at the examined section.

Evaluation of inflammation scores and neointimal reaction

With regard to the inflammation score for each individual strut, the grading was as follows: 0=no inflammatory cells surrounding the strut; 1=light, noncircumferential lymphohistiocytic infiltrate surrounding strut; 2=localized, moderate to dense cellular aggregate surrounding the strut noncircumferentially; and 3=circumferential dense lymphohistiocytic cell infiltration of the strut. The inflammation score for each cross section was calculated by dividing the sum of the individual inflammation scores by the total number of struts at the examined section. Inflammatory cell counts were normalized to injury score in neointima and compared among three stent groups.

Statistical analysis

Statistical analysis was performed with the aid of the commercially available software (SPSS Version 11, Chicago, IL, U.S.A.). The data were presented as mean value \pm SD. Unpaired Student's t test was used for the comparison of inflammatory cell counts normalized to injury score of the two stent groups. Analysis of variance (ANOVA) was used for comparisons of the three stent groups. To examine the correlations between the measured histologic variables, regression analysis was applied for each set of measured variables. A value of p<0.05 was considered statistically significant.

RESULTS

Procedural characteristics

Two stents were placed for two coronary arteries per one pig. A total of thirty stents including ten abciximab-coated setnts, ten SESs, and ten PESs, were placed in the proximal



Fig. 1. The hematoxylin-eosin stain of the low- and high-power fields (magnitude, ×20, ×400) of neointimal hyperplasia and inflammatory cell infiltration in abciximab-coated stent (A, B), sirolimus-eluting stent (C, D), and paclitaxel-eluting stent (E, F).

left anterior descending, proximal circumflex, and proximal right coronary artery for fifteen pigs (Table 1). Mortality for this study was zero. Quantitative coronary angiography before and after stent implantation established the stent-to-artery diameter ratio as 1.336 ± 0.061 for all 30 stented arteries. There was no significant difference in stent-to-artery ratio among three stent groups.

Neointimal response to injury

The lumen area, neointima area, and percent area stenosis at 28 days after stent implantation were not different significantly among three stent groups (Fig. 1, Table 2). Although there was a trend that the average injury score for each segment was higher in the PES group, this was not statistically significant (Table 2). There were no significant differences in the neointima area normalized to injury score and inflammation score among the three stent groups (neointima area normalized to injury score; 1.58 ± 0.43 mm² in the abciximab-coated stent group vs. 1.69 ± 0.57 mm² in the SES group vs. 1.92 ± 0.86 mm² in the PES group, and neointima area normalized to inflammation score; 1.57 ± 0.39 mm² in the abciximab-coated stent group vs. 1.72 ± 0.49 mm² in the SES group vs. 1.79 ± 0.87 mm² in the PES group, respectively) (Fig. 2).

Neointimal response to inflammation

Although there was a trend that the inflammation score for each cross-section was higher in the PES group, this was

Table 1. Stented porcine coronary arteries



Fig. 2. The neointima area normalized to injury score (A) and inflammation score (B) in the three types of stents.

not statistically significant (Table 2). All the sections examined revealed various amounts of inflammatory infiltrate surrounding at least one or more of the struts. In neointima, most inflammatory cells were lymphohistiocytes. The inflammatory reaction consisted of groups of pale histiocytic cells adjacent to the struts with occasional multinucleated giant cells. A rim of small, dark lymphocytes was also noted at the periphery, along with fibroblasts and capillaries. In contrast, eosinophils and plasma cells were not prominent (Fig. 1). A significant positive correlations were found between lymphohistiocyte count and the neointimal area (r=0.551, p=0.001), and between lymphohistic count and percent area stenosis (r=0.620, p=0.001) (Fig. 3). This correlation between lymphohistiocyte count and neointimal formation was similarly observed among three stent groups. Significant correlations were found between the injury score and neointimal area (r=0.645, p < 0.001), between the injury score and the inflammation score (r=0.837, p<0.001), and between the inflammation score and neointimal area (r= 0.536, *p*=0.001) (Fig. 4).

Inflammatory reaction according to the stent type, injury score, and inflammation score

Because there was a strong trend that injury score and in-

Table 2. Coronary artery morphometric measurements in thirty stented vessels

	Abciximab- coated stent (n=50)	Sirolimus- eluting stent (n=50)	Paclitaxel- eluting stent (n=50)	p value
IEL area (mm²) Lumen area (mm²) Neointima area (mm²) % area stenosis Injury score Inflammation score	$19.8 \pm 4.4 \\ 17.9 \pm 4.1 \\ 1.9 \pm 0.8 \\ 9.6 \pm 5.0 \\ 1.20 \pm 0.40 \\ 1.21 \pm 0.35$	$19.7 \pm 5.8 \\ 17.5 \pm 5.1 \\ 2.2 \pm 1.1 \\ 11.2 \pm 6.0 \\ 1.30 \pm 0.54 \\ 1.28 \pm 0.47 \\ \end{array}$	21.7±8.5 18.9±7.5 2.8±1.6 12.9±8.6 1.46±0.85 1.56±0.85	NS NS NS NS NS NS

IEL, internal elastic lamina; NS, not significant.





Fig. 3. Correlations between the lymphohistiocyte count and (A) neointimal area and (B) percent area stenosis



Fig. 4. Correlations between the injury score and neointimal area (A), between the injury score and the inflammation score (B), and between the inflammation score and neointimal area (C).



Fig. 5. The neointimal inflammatory cell count normalized to injury score in the three types of stents.

flammation score were higher in the PES group and there was a correlation between the injury score and the inflammation score, we evaluated inflammatory cell infiltration normalized to the injury score. Although there was a strong trend that inflammatory cell counts normalized to the injury score was lower in the abciximab-coated stent group compared to the PES group, this was not statistically significant $(75.5 \pm 23.1/\mu L$ the in abciximab-coated stent group vs. $78.8 \pm 33.2/\mu L$ in the SES group vs. $130.3 \pm 46.9/\mu L$ in the PES group) (Fig. 5).

DISCUSSION

This study demonstrated that abciximab-coated stent showed comparable anti-inflammatory effect and comparable inhibition of neointimal hyperplasia with other drug-eluting stents in a porcine coronary restenosis model. ISR due to neointimal hyperplasia remains the major limitation of coronary stents (4-8). There is increasing evidence that inflammation plays an important role in the initiation and development of neointimal hyperplasia and subsequent restenosis (9, 10).

Because of the role of inflammatory cells in restenosis, these cells seemed to be an optimal target in the fight against restenosis. The pathological process of ISR is characterized by an inflammatory healing response after stretch and damage of the vessel wall. Initially, platelets are activated and attach around the stent struts followed by adhesion of inflammatory cells. Cytokines and growth factors are released, leading to smooth muscle cell migration and proliferation (10-12). Therefore, modulation of the inflammatory response is expected to decrease ISR. Several immunosuppressive and antiproliferative therapies have been investigated to inhibit these processes (31-35). Recent successes in early clinical trials with drug-eluting stents using the anti-proliferative agents Sirolimus (rapamycin) and Paclitaxel (Taxol) have been quite promising (36-38).

Our previous study showed that abciximab-coated stent reduced neointimal hyperplasia by inhibition of neointimal cell proliferation and extracellular matrix synthesis compared to bare-metal stent in a porcine coronary restenosis model (27-29). In our previous study (29), the area of neointima of abciximab-coated stent was reduced to 45.7% and 45.5% of the control bare-metal stent at 28 days and 56 days after stenting, respectively, the content ratio of proteoglycan within the neointima of abciximab-coated stent was reduced to 23% of the control bare-metal stent at 14 days after stenting, the content ratio of collagen within the neointima of abciximab-coated stent was reduced to 19.7% and 25% of the control bare-metal stent at 28 days and 56 days after stenting, respectively, proliferating cell nuclear antigen index of neointima of abciximab-coated stent was reduced to 22.2% of the control bare-metal stent at 14 days after stenting, and the apoptosis of abciximab-coated stent by TUNEL analysis during a 56-day follow-up after stent implantation was not different compared to control bare-metal stent. We previously reported that abciximab-coated stent was feasible and produced a significant inhibition of neointimal hyperplasia, showing a potential therapeutic benefit in the prevention of stent restenosis in human trials (39, 40). In this study, we suggested that the possible mechanisms responsible for inhibition of neointimal hyperplasia by abciximab might be antiplatelet, anti-inflammatory, and anti-proliferative actions.

Platelet activation and aggregation induces arterial thrombosis and plays a pivotal role in the pathophysiology of acute coronary syndromes (41, 42). Platelets have been incriminated in contributing to neointimal hyperplasia via the release of platelet-derived growth factor that induces smooth muscle cell proliferation and migration. By virtue of the ability of platelets to facilitate the generation of thrombin, they may also act as a smooth muscle cell mitogen. Additionally, platelets express multiple counterreceptors for leukocytes, thereby providing a nidus for vessel wall inflammation.

A glycoprotein II/IIIa receptor blocker, abciximab, is a potent inhibitor that block the final pathway of platelet aggregation and decreases short- and long-term event rates after percutaneous coronary intervention (19-21). Besides the blocking effect for platelet aggregation, the blockade of the glycoprotein IIb/IIIa receptor by abciximab may inhibit the interaction between platelets and leukocytes, and hence limit the inflammatory response to coronary intervention. Abciximab cross-reacts and inhibits $\alpha V\beta \beta$. The $\alpha V\beta \beta$ receptor has also been implicated in neointimal hyperplasia since smooth muscle cells express $\alpha V\beta \beta$ receptors that are upregulated further after vascular injury (22). Moreover, in a number of different animal models, the inhibition of $\alpha V\beta \beta$ receptors has resulted in decreased neointimal thickening. Abciximab has cross-reactivity with other integrin receptors, including Mac-1, which is a major fibrinogen receptor on the polymorphonuclear neutrophil surface, and inhibits inflammatory reaction (23-26).

In the present study, significant positive correlations were found between the extent of inflammatory reaction and the neointimal area and between the extent of inflammatory reaction and percent area stenosis, respectively. Although the degrees of arterial injury correlated with inflammation score and neointimal area and there was a trend that injury score and inflammation score were higher in the PES group, inflammatory cell infiltration normalized to injury score was not different significantly among three stent groups. Thus, abciximab-coated stent might prevent ISR via a comparable antiinflammatory effect with other drug-eluting stents.

There are several limitations to be mentioned. Firstly, it remains to be established whether our findings in normal nonatherosclerotic porcine coronary arteries stimulated with oversized stents for neointimal proliferation could be extrapolated to human clinical scenarios with preexisting atherosclerosis and stent sizes matched to the reference vessel. Secondly, our study did not examine the early inflammatory response, as there is little neointimal formation at that time. Thirdly, although there was a trend toward larger neointima area in the PES group, injury score also had a trend for increase in this group, and injury score correlated with inflammation score and neointimal formation. This may suggest the extent of injury against intima by overstreching of oversized stent is related with inflammatory reaction and reactive hyperplasia. Fourthly, although the functional impact of abciximab might involve the reduced formation of leukocyte-platelet coaggregates, we did not demonstrate whether abciximabcoated stent inhibits formation of leukocyte-platelet aggregates. Thus, further studies are needed to demonstrate whether abciximab-coated stent may inhibit the interaction between platelets and leukocytes. Fifthly, we did not have a true control group. We compared different stent designs, lengths, and polymer drug combinations. Given these model that induces fairly minimal stenosis, it might not be clear that we had sufficient numbers to show that there would be a difference between a true control group and drug-eluting stents. Sixthly, we examined the histology of inflammation on H&E stain. It would be more appropriate and accurate to utilize immunohistochemistry, which is the standard for these types of studies and with appropriate techniques employed on resin-embedded sections.

In conclusion, abciximab-coated stent showed a comparable inhibitory effect for inflammatory cell infiltration and neointimal hyperplasia with other drug-eluting stents in a porcine coronary restenosis model.

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