

Mindfulness-based Neurofeedback: A Systematic Review of EEG and fMRI studies

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1 **Abstract**

2 Neurofeedback concurrent with mindfulness meditation may reveal meditation effects on the brain and
3 facilitate improved mental health outcomes. Here, we systematically reviewed EEG and fMRI studies of
4 mindfulness meditation with neurofeedback (mbNF) and followed PRISMA guidelines. We identified 10 fMRI
5 reports, consisting of 177 unique participants, and 9 EEG reports, consisting of 242 participants. Studies of
6 fMRI focused primarily on downregulating the default-mode network (DMN). Although studies found decreases
7 in DMN activations during neurofeedback, there is a lack of evidence for transfer effects, and the majority of
8 studies did not employ adequate controls, e.g. sham neurofeedback. Accordingly, DMN decreases may have
9 been confounded by general task-related deactivation. EEG studies typically examined alpha, gamma, and
10 theta frequency bands, with the most robust evidence supporting the modulation of theta band activity. Both
11 EEG and fMRI mbNF have been implemented with high fidelity in clinical populations. However, the mental
12 health benefits of mbNF have not been established. In general, mbNF studies would benefit from sham-
13 controlled RCTs, as well as clear reporting (e.g. CRED-NF).

14 **Keywords:** Neurofeedback, mindfulness, EEG, fMRI, DMN, theta

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1 Introduction

Mindfulness meditation involves cultivating an accepting, open-minded attention to the present moment (Creswell, 2017). The word mindfulness originated from Eastern contemplative traditions, specifically, as a translation of the term *sati* from Pali or *smṛti* from Sanskrit, which mean remembering or being aware. Mindfulness was largely introduced to Western medicine with the advent of mindfulness-based stress reduction (MBSR) in the 1980s (Kabat-Zinn, 1982, 2003). MBSR and its adaptations have been used to treat chronic pain (Goyal et al., 2014; Kabat-Zinn, 1982), anxiety (Goldin et al., 2013; Hoge et al., 2022; Hölzel et al., 2013), addiction (Black, 2014; Garland et al., 2015; Vallejo & Amaro, 2009), and depression (Kuyken et al., 2016). Indeed, mindfulness has been documented to be equally effective as pharmacological treatment for anxiety disorders (Hoge et al., 2022) and potentially more effective than cognitive behavioral therapy (CBT) for treatment of mild-to-moderate depression (Strauss et al., 2023). Mindfulness is now a central component of leading psychotherapeutic approaches like dialectical behavioral therapy (DBT) (Linehan, 1993; McCauley et al., 2018) and acceptance and commitment therapy (ACT) (Hayes et al., 1999).

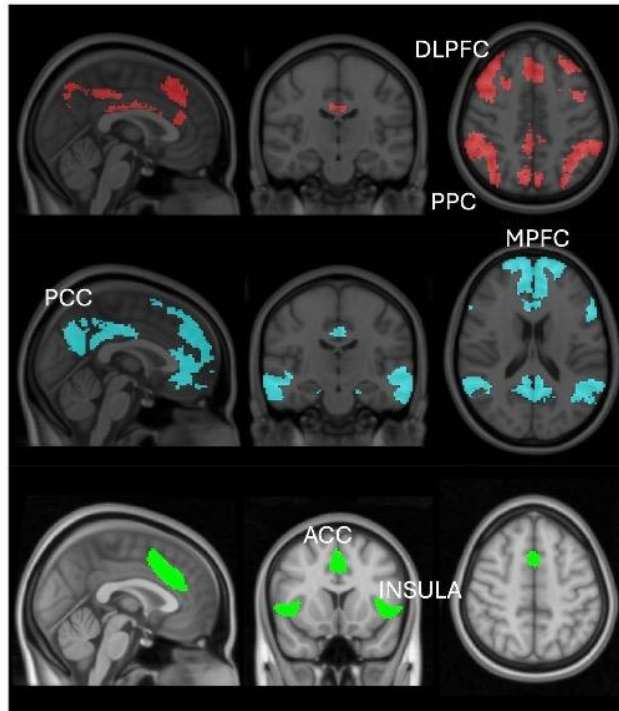
Mindfulness meditations include practices like *breath awareness*, which involves orienting attention to one's breath and practicing returning to the breath every time one's attention wanders away, and *body scans*, involving moving the spotlight of attention from body part to body part with a curious and non-judgmental attitude towards the sensations one encounters. Another practice is *open monitoring*, where one notices transient thoughts and sensations in an open state without attaching to them. Breath awareness and body scans are often called *focused attention* (FA) practices, aiming to cultivate a stable and precise attention, which contrasts with *open monitoring* (OM) practices, cultivating receptivity to experience (Lutz et al., 2008).

There are several theories regarding the neurobiological mechanisms behind mindfulness meditation. One influential account suggests that large-scale brain networks are involved (Hasenkamp et al., 2012; Mooneyham et al., 2016). Specifically, this account implicates the default-mode network (DMN), with core regions of the posterior cingulate cortex (PCC) and medial prefrontal cortex (mPFC) as well as the central executive network (CEN), with core regions of the dorsolateral prefrontal cortex (DLPFC) and parietal cortex, and the salience network (SN), with core regions of the anterior cingulate cortex (ACC) and insula (**Figure 1**). In this account, the DMN is involved in mind-wandering away from the object of meditation, the CEN is

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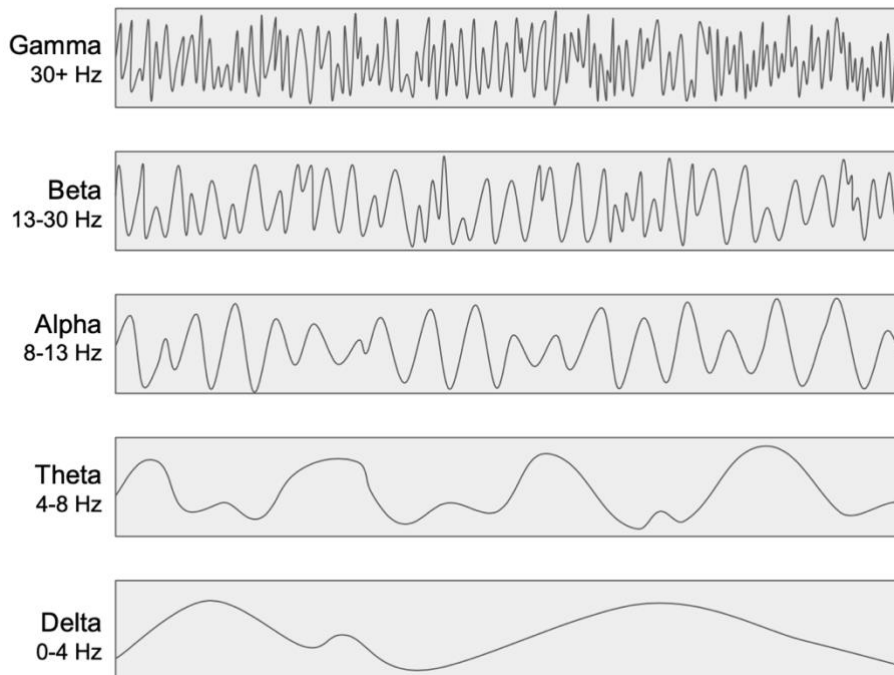
1 involved in goal-directed maintenance of the object, and the SN is involved in switching between the two
2 (Hasenkamp et al., 2012). This is based largely on functional magnetic resonance imaging (fMRI) during
3 focused attention meditation (Fox et al., 2016; Ganesan et al., 2022), changes observed in networks after
4 mindfulness training (Rahrig et al., 2022; Sezer et al., 2022), in addition to a robust cognitive neuroscience
5 literature on these networks (Menon, 2011). In tandem, researchers have examined changes in brain rhythms
6 or oscillations during meditation using electroencephalography (EEG) (**Figure 2**). Brain oscillations represent
7 information processing across wide-ranging brain regions, and change with attention (Herrmann et al., 2016).
8 There is evidence of power increases in alpha, theta and gamma waves during meditation (Chiesa & Serretti,
9 2010; Lee et al., 2018; Lomas et al., 2015; Stapleton et al., 2020). Alpha and theta power may correspond to
10 inwardly focused attention (Lomas et al., 2015), whereas gamma power may reflect broad awareness (Lomas
11 et al., 2015; Lutz et al., 2004; Stapleton et al., 2020). Despite this meaningful work, the field still lacks a
12 complete mechanistic account of mindfulness meditation. Take, for example, the assertion that mindfulness
13 decreases DMN activation (Brewer et al., 2011; Ganesan et al., 2022). This particular assertion is largely
14 founded on comparisons of meditation to control conditions, which do not directly imply mechanistic
15 involvement. For example, neural changes associated with mindfulness may be caused by decreases in stress
16 accompanying meditation, rather than the voluntary and directed actions of meditation. In addition, the choice
17 of control condition can lead to differing results. For example, Ganesan and colleagues (2022), found that the
18 DMN was less activated during meditation than control conditions in only 60% of the studies reviewed, with the
19 controls including rest, intentional instructions to mind wander, and other functional tasks. A final concern is
20 that reverse inferences from brain areas to psychological processes may be implausible (Poldrack, 2006). To
21 test theories about mindfulness meditation and uncover a more complete mechanistic account, researchers
22 need to manipulate brain function, and neurofeedback affords one opportunity to manipulate brain functions
23 directly implicated in mindfulness meditation.



1

2 **Figure 1: Brain networks involved in mindfulness meditation.** Central executive network, in red; Default-
3 mode network, in blue; Salience network, in green. DLPFC: dorsolateral prefrontal cortex; PPC: posterior
4 parietal cortex; PCC: posterior cingulate cortex; MPFC: medial prefrontal cortex; ACC: anterior cingulate
5 cortex; Insula: insular cortex. Adapted with permission from Treves et al., in press.

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28 **Figure 2: EEG Frequency Bands.** This visualization demonstrates the differing frequencies of the various
29 EEG bands. Created in google slides.
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1 Neurofeedback originated in the 1960s for EEG (Kamiya, 2011), and early 2000s for fMRI (e.g.,
2 DeCharms et al., 2004; Yoo & Jolesz, 2002). Similar to biofeedback, it consists of relaying brain data (i.e., the
3 target measure) to a participant while they perform a task. The participant may be given instructions to
4 modulate the target by any number of strategies, or they may be given a specific strategy and told that correct
5 application will be indicated by changes in their brain data. This neurofeedback condition may be compared to
6 control conditions, wherein participants are presented with data from other brain regions not affected by the
7 strategy ('alternative ROI control'), or from other participants ('yoked' sham). Given well-designed controls
8 (Sorger et al., 2019), neurofeedback can provide more substantive evidence that a brain region or network is
9 involved in a process (for a complete account, neurostimulation methods may be most optimal). In addition to
10 providing mechanistic insights into mental processes (Kvamme et al., 2022), neurofeedback allows participants
11 to manipulate those processes. Neurofeedback has been used in many different applications, from the
12 regulation of chronic pain (deCharms et al., 2005), to attentional training (typically involving prefrontal regions)
13 (DeBettencourt et al., 2015; Wang & Hsieh, 2013), to stress reduction (typically involving the amygdala)
14 (Hellrung et al., 2018; Nicholson et al., 2017; Young et al., 2017). It is often considered to 'enhance' learning,
15 leading to improved outcomes (Haugg et al., 2021; Kadosh & Staunton, 2019). Researchers often conduct a
16 single session of neurofeedback and then evaluate behavioral outcomes days, weeks or months later
17 ((Pamplona et al., 2023; Ros et al., 2013); though, several studies have leveraged repeated sessions (Dekker
18 et al., 2014; Mehler et al., 2018). Overall, there is promising evidence for the clinical mental health benefits of
19 EEG and fMRI neurofeedback (Roy et al., 2020; Trambaiolli et al., 2021; Van Doren et al., 2019; c.f. Thibault et
20 al., 2018). Thus researchers have proposed that the clinical benefits of mindfulness (as well as cognitive
21 benefits) could be enhanced or facilitated by neurofeedback (Brandmeyer & Delorme, 2013; Brandmeyer &
22 Reggente, 2023).

23 Starting in the early 2010s, neurofeedback concurrent with mindfulness meditation has been gaining
24 popularity, and it is often referred to as mindfulness-based neurofeedback (mbNF). The purpose of this paper
25 is to systematically review the literature and thus answer two main questions. First, can participants learn to
26 modulate brain targets through mindfulness meditation practice, providing evidence of their involvement in
27 meditation? Second, what are the behavioral and brain outcomes of mbNF? By reviewing the literature, there

1 also are opportunities to discuss methodological limitations. The CRED-NF checklist (Ros et al., 2020), could
2 be a crucial initial step towards standardizing current methodological and outcome reporting practices. The
3 CRED-NF checklist includes preregistration, sample size justification, control group, double-blinding, whether
4 or not participants used a strategy, artifact removal, feedback specification, regulation success (target
5 engagement), brain and behavioral outcomes, and more. We evaluate the quality of studies herein based on
6 the CRED-NF checklist. The present review only examines controlled lab-based EEG and fMRI studies
7 (consumer-grade EEG studies are not reviewed, see Methods).

8 9 **2 Methods**

10 PRISMA guidelines were followed in this review (**Supplement 2**) (Page et al., 2021).

11 **2.1 Inclusion and Exclusion Criteria**

12 Studies that employed EEG or fMRI neurofeedback concurrently with mindfulness meditation were included.
13 Specifically, studies were selected that claimed to employ mindfulness meditation, and we then evaluated
14 whether the meditation met our definition of mindfulness. For the purposes of this review, mindfulness
15 meditation is defined as meditation practice with the aim of cultivating non-judgmental attention to the present
16 moment, including both focused attention (FA) and open monitoring (OM) practices (Lutz et al., 2008). FA and
17 OM are distinct practices, but both are taught in mindfulness interventions like MBSR (Santorelli, 2014) and
18 involve purposeful redirection of attention to the present moment (Britton et al., 2019; Dahl et al., 2015). Other
19 meditation (e.g. transcendental, compassion) was not included. Exclusion criteria included lack of EEG or fMRI
20 neurofeedback, lack of mindfulness meditation, lack of concurrent neurofeedback and mindfulness meditation,
21 and non-empirical status (e.g., reviews). Studies with consumer-grade EEG devices were considered beyond
22 the scope of this review, as there were substantial such studies (33), and consumer-grade devices don't allow
23 sufficient insight into brain mechanisms. No relevant conference papers or dissertations were identified.

24 25 **2.2 Systematic Search**

26 A search of PubMed, Web of Science, PsycInfo, and Scopus, was completed on November 11, 2023.

27 Databases were identified based on previous mindfulness systematic reviews and meta-analyses (Goldberg et

1 al., 2018; Treves et al., 2019). Search terms were “(mindfulness OR meditation) AND (neurofeedback OR
2 neural feedback OR neuro feedback)”. We additionally searched reference sections of included papers.

4 **2.3 Study Selection**

5 All studies were first screened for duplicate publications. Next, all abstracts were screened, including studies
6 based on two main criteria: full report of an empirical study (examples of excluded articles were review papers,
7 protocol papers, book chapters, and conference proceedings) and content relevance (based on above stated
8 inclusion/exclusion criteria). Then remaining studies were screened by reviewing the methods section and full
9 paper to further evaluate the presence of inclusion criteria. Determination of inclusion was established in cases
10 of disagreement by consulting with the first author.

12 **2.4 Coding**

13 Records were grouped according to neuroimaging technique (i.e., EEG or fMRI). Two reviewers (KDG & EW)
14 independently evaluated each EEG study and its characteristics, and two reviewers (INT & ZB) independently
15 evaluated each fMRI study and its characteristics. The studies were coded for sample, targets, neurofeedback
16 details, control conditions, target engagement, neural outcomes and behavioral outcomes (**Tables 1 and 2**).
17 Target engagement was defined as ‘whether or not the neurofeedback target was modulated’, whereas neural
18 outcomes are changes in other neural measures not targeted in the study neurofeedback protocol. Behavioral
19 outcomes may consist of outcomes like state mindfulness reported after the scan, or more distal but related
20 outcomes (e.g. cognitive performance on a separate task).

22 **2.5 Bias and quality coding**

23 No automation tools were used. Papers were coded independently to limit reviewer bias. Risk of bias in the
24 studies was not quantified given the limited number of RCTs. Instead, we coded studies based on the CRED-
25 NF checklist (Ros et al., 2020), reporting whether recommended items were present in the studies (**Table S1**).

26 **Box 1: Neurofeedback Terms**

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Bidirectional control: Testing whether participants may modulate a neurofeedback target in both directions. For example, decreasing the DMN by meditating, and increasing the DMN by ruminating.

Calibration: A preceding block of non-neurofeedback data used for the neurofeedback target estimates, typically eyes-open rest.

Control, Alternate ROI: Typically, feedback is given from a region or network that is not related to the task.

Control, Yoked Sham: Feedback is presented to a control participant from an experimental participant. This feedback is controlled for in terms of perceived reward but not contingent on a control participant's performance.

Functional/individual localization: Determining a brain area or network based on data from the participant. An example is conducting resting-state fMRI before the neurofeedback task, which can be used to extract intrinsic networks that are correlated at rest.

Intermittent vs continuous: Intermittent, or delayed, feedback is feedback presented after regular intervals, not concurrently with task. Continuous, or real-time, feedback is feedback presented throughout the task (e.g. every second). May involve different attentional demands (Hellrung et al., 2018).

Offline artifact correction: Estimates of motion or physiology are corrected for or tested for in post-processing.

Online artifact correction: Estimates of motion or physiology are included in real-time models (e.g. GLMs), so feedback is not presented based on those artifacts.

Target: The brain measure relayed to participants.

Target engagement: A test of whether participants successfully learned to modulate the target brain measure, may consist of examining overall levels of target, change in target, or target performance in transfer runs.

Transfer run: A neuroimaging run where participants perform the neurofeedback task without any feedback presented. Transfer tasks after feedback can be used to assess whether learning has occurred.

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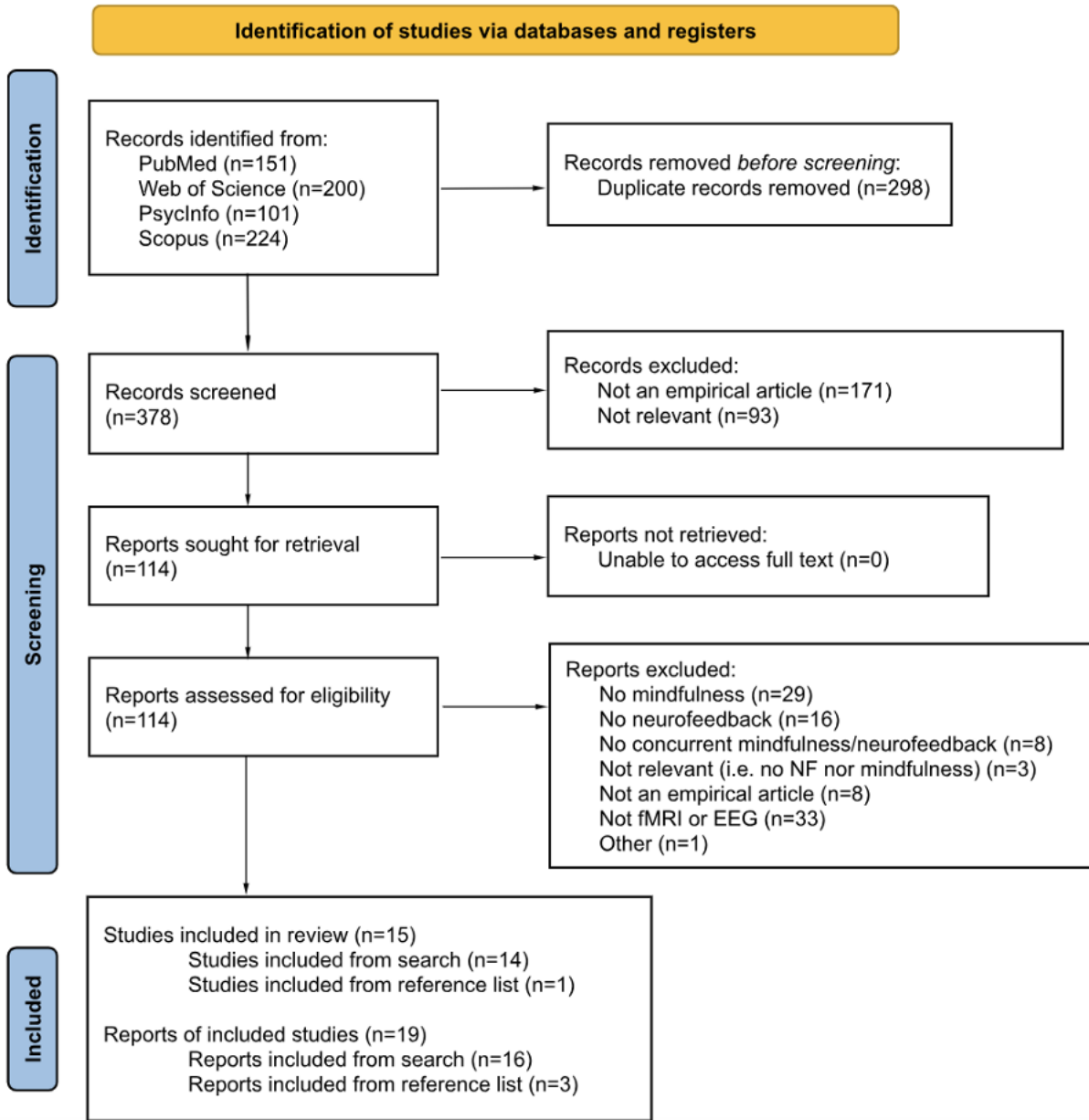
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3 Results

3.1 Search Results

A Prisma flow diagram is shown in **Figure 3**. The search yielded 676 records across four databases. After removing duplicates and excluding based on title and abstract, full texts were reviewed for the remaining 114 studies. The final sample included 19 studies with 15 independent samples representing 419 participants.

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3 **Figure 3:** PRISMA flow diagram depicting number of identified and evaluated articles for concurrent
4 mindfulness and fMRI or EEG neurofeedback procedures.

5 *Note.* Studies refer to unique samples, while reports refer to publications on said samples. Our review
6 identified four samples which corresponded to more than one published report, as indicated in this flowchart
7 and in the study summary tables (Tables 1 and 2).

Author/ Date	Sample	Mindfulness Meditation	Control Condition	Neural Target	Feedback presentation	fMRI session details	Target Engagement	Neural Outcomes	Behavioral Outcomes
Garrison, Scheinost, et al., 2013	Exp1: 9 meditators (variety of traditions, M= 9.5 yrs, 8803 hrs), 11 non-meditators Exp2: 10 meditators (variety of traditions, M=18.4 yrs, 10567 hrs)	Focused attention/ breath practice	None ^a	PCC activation	Bar graph: blue upwards bar for activation increases, red downwards bar for activation decrease. Full graph with past feedback shown.	Exp1 : 3-min NF scan. Exp2: three 1-min NF scans.	Exp 1: More negative PCC activations during NF in meditators compared to controls. Exp 2: significant deactivation of PCC compared to self-reference.	Not reported	Effortless awareness was associated with decreased PCC activity.
Garrison, Santoyo, et al., 2013	Same sample as Exp2 from Garrison, Scheinost et al., 2013, 10 meditators	"	Within-subject no feedback	"	"	Six 1-min feedback scans	Not reported	"	Qualitative report: PCC deactivation was associated with experience of focused attention and effortless awareness, PCC activation was associated with opposite.
Kim et al., 2019	60 adults ^b	Focused attention/ breath practice	Yoked sham group	Individually localized DMN, CEN, and SN. Mediation slope excluding CEN from DMN and SN relationship.	Thermometer where higher bar reflects higher mediation slope. Calculated using windowed brain activity from 50 sec prior.	Two 5-min NF runs, one transfer fMRI run.	Mediation effect not significantly larger in experimental group. However, correlation between mediation effect and mindfulness/target performance feedback (TPF, self-report) only in experimental group.	Activations in DMN negatively correlated with mindfulness/TPF in experimental group.	No group X time effects on mood, state mindfulness, TPF, or stress. No reported changes in cognitive tasks.
Bauer et al., 2020	11 participants with schizophrenia or schizoaffective disorder	Open awareness (noting)	Alternative ROI control: from somatomotor cortex during finger tapping in same participants (7 completed)	Individually localized CEN and DMN networks. Increase CEN relative to DMN (PDA).	A moving ball. The ball moves relative to the difference between CEN and DMN. If CEN > DMN, ball moves up. If DMN > CEN, ball moves down. Activations from 30 sec prior.	Two no-feedback transfer runs (2.5- mins each), four feedback scans (2.5- mins each).	Participants showed significant CEN > DMN (more than chance) on average during NF. Unclear whether control condition also engaged target.	Decreased DMN connectivity (mPFC-PCC), decreased CEN- DMN connectivity (dIPFC- mPFC) from pre- to post- resting-state, not present in control condition.	AHs decreased 1-wk after, returning to baseline after >12- wks. AHs were not affected by control neurofeedback task.
Okano et al., 2020	Same sample as Bauer et al., 10 participants with schizophrenia or schizoaffective disorder	Open awareness (ignoring auditory stimuli)	"	Functionally localized STG activation	Thermometer, where height is activation in STG.	2 transfer runs and four NF runs (~ 1- min). Each run had 2 "listen" blocks and 2 "ignore" blocks (16- sec each).	Anatomically defined STG activation was less post- feedback transfer than pre- feedback. No differences after control condition.	Not reported	AHs decreased, not affected by control task. Correlation between right STG decrease and AH decrease. AHs returned to baseline after 12-wks.

Author/ Date	Sample	Mindfulness Meditation	Control Condition	Neural Target	Feedback presentation	fMRI session details	Target Engagement	Neural Outcomes	Behavioral Outcomes
Pamplona et al., 2020	30 adults	Focused attention ^c	No-feedback control group	SAN activation (composite of DAN and FPN) minus subject-specific DMN (core hubs and angular gyrus). Compared to baseline blocks.	Intermittent feedback with thermometer (red is high SAN-DMN, blue is low SAN-DMN) every 40 sec (with monetary rewards at end of run).	Two NF runs (6-mins each), two transfer runs.	Decreased DMN activations over training (specifically mPFC and PCC) and in post-transfer runs (compared to pre-transfer). Increased attentional network (specifically mid-cingulate and pre-SMA) activations during training and in transfer runs (specifically IPS).	Not reported	Control group improved more on multiple attention tests, but NF group improved in RTs for vigilance test, specifically during early trials. No changes in attentiveness and stress. No relationship between changes in self-report/behavior changes and target engagement.
Pamplona et al., 2023	Same sample as Pamplona et al. (2020), 15 adults	"	None	"	"	"	"	Transfer at 2 months: DMN deactivation present (PCC/mPFC), not present in SAN. DMN visual area correlations increased and maintained at follow-up, related to degree of psychomotor vigilance changes.	No behavioral effects persist at two months.
Kirlic et al., 2022	34 adolescents (ages 13-17)	Focused attention/breath practice	None	PCC activation	Bar graph: blue upwards bar for activation increases ("focused attention"), red downwards bar for activation decreases ("mind-wandering"). Tasked to match blue bar with green target bar.	Three 7-min NF runs, two transfer fMRI runs (OBS and TRS).	PCC deactivation during NF, consistent when compared to rest or self-referential processing. Not observed during post-transfer. Widespread deactivations in other regions. Limited evidence of correlations between PCC activation and self-reports (e.g. mindfulness) - doesn't survive MC.	Not reported	No changes in PSS or negative affect. State mindfulness increase maintained at 1-wk.
Yu et al., 2022	Same sample as Kirlic, 37 adolescents (ages 13-17)	"	"	"	"	"	"	Posterior insula activations decrease. Anterior insula activations increase. No transfer effects.	Self-report state mindfulness increased. No change for mind-wandering.
Zhang et al., 2023	9 adolescents (ages 17-19) with lifetime history of major depressive disorder/anxiety disorders	Open awareness (noting)	None	Individually localized CEN and DMN networks. Increase CEN relative to DMN (PDA).	A moving ball. The ball moves relative to the difference between CEN and DMN. If CEN > DMN, ball moves up. If DMN > CEN, ball moves down. Activations from 30 sec prior.	Five 2.5-min NF sessions. No transfer.	More overall time in CEN > DMN state. Marginally lower DMN activation.	sgACC-DMN (mPFC/PCC) connectivity decreased. Target performance (PDA) correlated with decrease (only in last NF block).	State mindfulness increased, correlated with target performance and connectivity decrease.

1 **Table 1.** Summary of studies of fMRI-based neurofeedback with concurrent mindfulness practice.
2

3 *Note.* AH = auditory hallucinations; CEN = Central executive network; DAN = Dorsal attention network; dlPFC = dorsolateral prefrontal cortex. DMN
4 = Default mode network; FPN = frontoparietal network; Hrs = hours. M = mean; MC = Multiple comparisons; Mdn = median; Min = minute; mPFC =
5 medial prefrontal cortex; OBS = Observe runs; PACE = prospective acquisition correction; PCC = posterior cingulate cortex; PDA = Positive
6 diametric activity; PSS = Perceived Stress Scale; RT = Reaction time; SAN = Sustained attention network; SD = standard deviation; Sec = second;
7 SN = Salience network; STG = superior temporal gyrus; TPF = task-performance feedback; TRS = Transfer runs; Wk = week; Yr = year.
8

9 ^a Feedback from parietal cortex only used during monitoring phase.

10 ^b All male participants.

11 ^c Participants allowed to use any strategy that works for them.

3.2 fMRI Studies

3.2.1 Summary

We identified 10 reports of fMRI neurofeedback including 7 unique samples (**Table 1**). There were two studies that used different neurofeedback protocols with the same sample, patients with schizoaffective disorders (Bauer et al., 2020; Okano et al., 2020). In total, there were 177 unique participants, and most samples were at or below 30 participants (**Figure S1 & S2**). Studies employed focused attention and open monitoring meditations. The first study published was Garrison et al. (2013a), a breath-focused attention study, which was also the only study to involve experienced meditators. Garrison et al. (2013b) examined qualitative reports from meditators who were asked to explore correspondence between brain signals and meditation experiences. A typical open monitoring protocol asked participants to label thoughts and feelings as they came up (Bauer et al., 2020). Only one study reported participants' actual mental strategies during neurofeedback regulation (Pamplona et al., 2020), and found a variety of strategies employed, some of which weren't typical mindfulness. Control conditions encapsulated yoked sham, alternate ROI, and mindfulness meditation without feedback, but many studies did not include controls (**Figure S3 & S4**). Only two studies examined between-subjects controls (**Figure S5**) (Kim et al., 2019; Pamplona et al., 2020), and transfer runs (**Box 1**) were inconsistently used across studies. Zhang et al. (2023) was the only study to examine adolescents. Qualitative assessments of the mbNF experience are found in **Table S3**.

3.2.2 fMRI Targets

The majority of studies employed activation-based, default-mode network targets (**Figure 4**). There was some variety in the specification of the DMN. Two studies targeted PCC activity (Garrison et al., 2013; Kirlic et al., 2022, Yu et al., 2022). Multiple studies used individualized networks generated from independent component analysis of resting-state scans (Bauer et al., 2020; Kim et al., 2019; Pamplona et al., 2020, 2023). These studies combined network activations from not only the DMN but also attentional networks like the dorsal attention network (Pamplona et al., 2020, 2023), the salience network (Kim et al., 2019), and the CEN (Bauer et al., 2020). One study used a task to functionally localize the superior temporal gyrus (STG) in order to modulate auditory processing (Okano et al., 2021). Kim et al. (2019) was the only study which used a

1 connectivity-like target, and they examined the direct effect from DMN-SN, excluding the influence of the CEN
2 (as the CEN was proposed to be involved with the visual feedback monitoring and not the meditation). Target
3 measures did not appear to depend on whether participants performed focused attention vs open monitoring.
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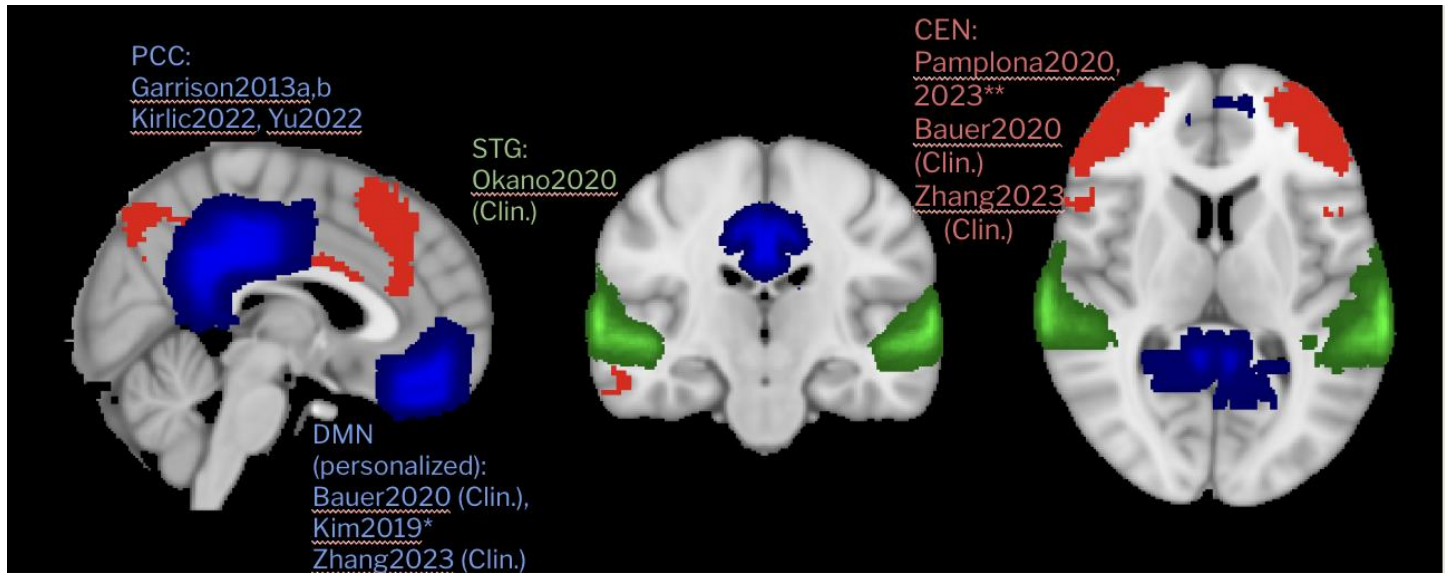


Figure 4: fMRI targets for neurofeedback. In blue, default-mode network (DMN) regions. In green, the superior temporal gyrus (STG). In red, the central executive network (CEN). Networks are taken from the Yeo atlas (Yeo et al., 2011), and STG was extracted from the Harvard-Oxford cortical atlas. *Kim used DMN-SN slope **Pamplona used sustained attention network.

1 There were different approaches to computing the target measure. Multiple studies used baseline periods in
2 the same fMRI scan to scale and baseline the neurofeedback target measure (e.g., 30 seconds of rest ;Bauer
3 et al., 2020; Okano et al., 2020; Zhang et al., 2023). Garrison et al., 2013a, 2013b used a self-reference task.
4 Some studies used online motion artifact correction, and two studies additionally conducted online correction
5 for physiological signals like breathing and heart rate (Kirlic et al., 2022; Yu et al., 2022). No differences were
6 observed between neurofeedback and rest in terms of motion or physiological signals.

7
8 Feedback was displayed visually to participants during fMRI in all cases. Some studies used delayed
9 feedback, e.g. continuous feedback but with a time lag (Bauer et al., 2020; Kim et al., 2019), and one used
10 intermittent feedback (Pamplona et al., 2020). One study displayed a continuously updating graph containing
11 past values of the measure (Garrison et al., 2013). Negative and positive feedback was shown. One study
12 incorporated rewards for target engagement (Pamplona et al., 2020).

14 **3.2.3 fMRI Target Engagement**

15 All studies evaluated target engagement. Garrison et al. (2013) found that meditators showed more negative
16 PCC (the target) activation than controls. Two studies examined the amount of time spent in a 'correct' brain
17 state (CEN > DMN), and found above chance engagement for the group (Bauer et al., 2020; Zhang et al.,
18 2023). Another study examined change over neurofeedback blocks in activation, and found significant
19 decreases in the DMN (Pamplona et al., 2020), but no increases in their individually defined attentional
20 networks. Transfer runs can also be used to assess whether target engagement or learning has taken place.
21 Kirlic et al. (2022) observed decreased PCC activation during neurofeedback compared to control tasks, but
22 not in the post-transfer run. Although there seems to be consistent evidence of DMN deactivation during
23 neurofeedback, the only study to use a sham control and a large (n~60) sample did not find evidence for target
24 engagement (mediation slope between the DMN-SN) (Kim et al., 2019). This and the transfer results from Kirlic
25 and colleagues make it unclear whether participants have learned to modulate their brain networks.

27 **3.2.4 Neural Outcomes**

1 Many studies examined the possibility of neural changes due to neurofeedback. Some reports focused on
2 DMN-based connectivity assessed during resting-state fMRI before and after neurofeedback. There are
3 indications of reduced within-DMN connectivity (e.g. between the MPFC and PCC), as well as more negative
4 correlations between DMN and CEN (Bauer et al., 2020). Other studies found reduced DMN connectivity with
5 the sgACC (sometimes considered part of the DMN; Zhang et al., 2023), reduced DMN connectivity with the
6 STG (Okano et al., 2020), and increased DMN-visual area connectivity (Pamplona et al., 2023) even at a 2-
7 month follow-up assessment. Of the findings, only the DMN-STG finding was established as specific to the
8 mindfulness-based neurofeedback, as Okano and colleagues did not find DMN-STG changes in an alternative
9 ROI control session (finger tapping). However, Zhang et al. (2023) found associations between DMN-sgACC
10 connectivity decreases and target engagement and state mindfulness in their small sample.

11
12 Researchers also examined activations in non-target and target brain regions. Yu et al. (2022) found that
13 neurofeedback increased anterior insula activations, and decreased posterior insula activations, without any
14 transfer effects. This could reflect changes in interoceptive processing during mbNF. Kim et al. (2019) found
15 that activations in the DMN negatively correlated with state mindfulness, but only in the experimental group
16 and not the sham feedback group.

18 **3.2.5 State Mindfulness**

19 To assess whether participants are learning from neurofeedback, studies also tested whether they experienced
20 increases in state (or momentary) mindfulness, as reported after the scans. State mindfulness assessments
21 typically involved questions about present-focused awareness of the mind and body (Tanay & Bernstein,
22 2013). Kim et al. (2019) found no mbNF vs control group effects on state mindfulness or self-report target
23 efficacy. However, two uncontrolled studies found increases in state mindfulness after neurofeedback (Kirlic et
24 al., 2022; Zhang et al., 2023).

26 **3.2.6 Behavioral Outcomes**

1 A central motivation for many of the studies was the possibility of beneficial behavioral or self-reported
2 outcomes. Pamplona et al., (2020) observed improvements in reaction time on a vigilance test, but this was not
3 maintained at the 2-month follow-up (Pamplona et al., 2023). They also did not observe a correlation between
4 target engagement and vigilance reaction time. Kirlic et al. (2022) did not observe any changes in perceived
5 stress or negative affect after neurofeedback. Bauer et al. and Okano et al. observed decreases in auditory
6 hallucinations that were not present after a control neurofeedback task, however, the protocols were conducted
7 on the same sample and the same baseline was used for both. Overall, there is limited evidence for
8 mindfulness-based fMRI neurofeedback benefits as yet.

10 **3.2.7 Clinical Applications**

11 Three studies conducted neurofeedback with small clinical samples (Bauer et al., 2020; Okano et al., 2020;
12 Zhang et al., 2023). Bauer and Okano et al. examined neurofeedback in the same 10 individuals with
13 schizophrenia, and found decreases in auditory hallucinations - although these changes were not sustained at
14 12 weeks. Zhang et al. examined neurofeedback in 9 adolescents with affective disorder history, and found
15 decreases in sgACC-DMN connectivity which is heavily implicated in adolescent depression (Chai et al., 2016);
16 though symptom changes were not assessed. These studies can be considered pilots—focused mostly on
17 establishing feasibility of the neurofeedback protocols in clinical samples.

19 **3.2.8 Quality (CRED-NF)**

20 In general, the control conditions in fMRI studies (within and across-subjects) were lacking, with only one study
21 involving adequate controls and reporting. Reporting of feedback specifications, target engagement (in the
22 feedback condition), data processing methods, etc. was present across the vast majority of studies. Few
23 studies conducted preregistration, power analyses, or made their data/code open access. A full table may be
24 found in **Table S2**.

Author/Date	Sample	Mindfulness Meditation	Control Condition	Neural Target	Feedback presentation	EEG session details	Target Engagement	Neural Outcomes	Behavioral Outcomes
Hinterberger & F�rnrohr, 2016	26 meditators (M 8.2 yrs practicing), 10 non-meditators	Focused attention and body scan ^a	Within-person control. Focused attention meditation only, body scan meditation only, and yoked sham.	EEG frequency bands (USP, SCP, delta1, delta2, theta, alpha, beta, gamma, wide) amplitude and time from peak-to-peak of a wave cycle.	Sensorium (multimodal NF environment using sound and light changes)	Two 20-min sessions on two separate days.	Compared to the aggregate of non-Sensorium conditions, the aggregate of all Sensorium conditions showed a stronger increase in power in the theta2, alpha1, and alpha2 bands. ^b	Not reported	Subjective feedback ratings show Sensorium was not inferior to meditation alone, and was rated as a more extraordinary experience. The Pseudo-Sensorium was found to be inferior to Sensorium3.
Kosunen et al., 2016	43 adults	Focused attention and body scan	Within-person controls. Followed both meditation exercises (1) using a computer screen with no VR headset or NF and (2) using the VR headset with no NF.	Increase in power of alpha band and theta band	VR headset. Users begin on a platform. Increases in theta band power correspond to platform levitating, while increases in alpha band power correspond to increases in opacity of energy bubble surrounding user.	Two 10-min NF sessions in one day.	Not reported	Not reported	On a meditation depth questionnaire, the VR+NF condition performed significantly better than the Screen only condition, but not the VR+no NF condition.
Salminen et al., 2023	Same sample as Kosunen et al. 2016, 43 adults	"	"	"	"	"	No significant effect for alpha. Significantly greater frontal theta activation during NF sessions versus no-NF conditions.	Significantly more gamma power during VR vs. computer screen. Significantly more gamma power during NF vs. no-NF. Significantly more gamma power during body scans than focused attention.	Higher self-reported sense of presence during NF vs. no-NF. Higher self-reported sense of presence was reported in VR vs. computer screen conditions.
van Lutterveld et al., 2017	16 novice meditators, 16 experienced meditators (Mdn 6164 hrs, minimum 5 yrs experience)	Noting practice (for novices), and effortless awareness (for experienced meditators)	Within-person control. Bidirectional control	Decreased gamma band PCC activity	Bar graph: upward bar for increases in PCC power and downward bar for decreases in PCC power. Full graph with past feedback shown.	Three 1.5-min runs of concurrent meditation and NF.	Novice meditators were able to decrease PCC power in noting practice runs only. Experienced meditators were able to for all runs. Neither group was able to upregulate PCC (bidirectional control)	Not reported	Both groups associated effortless awareness with decreased PCC activity.
Dunham et al., 2018	10 adults	Open awareness	None	BIS value (higher value correlates with higher power in high-frequency bands)	Continuous display of raw EEG and a BIS value (0–100). Participants were told a BIS value more than 94 indicates fast brainwave activity, which might denote stress.	Up to 4 days over a 21 day period. Each day has two 12-min blocks.	BIS value significantly decreased compared to baseline. For the one participant who completed 4 days, mean BIS score significantly decreased from day 1 to day 4.	Not reported	For the one participant who completed 4 days, wellbeing score increased from day 1 to day 4.

Author/ Date	Sample	Mindfulness Meditation	Control Condition	Neural Target	Feedback presentation	EEG session details	Target Engagement	Neural Outcomes	Behavioral Outcomes
Dunham et al., 2019	57 adults	Open awareness	None	“	“	4 days over a 21 day period. Each day has two 12-min blocks.	Mean BIS and minimum BIS lower than baseline BIS for each of 4 training days, but no significant change in values across days.	Not reported	Wellbeing scores significantly increased from day 1 to day 4, and were significantly higher than the single time point comparison sample.
Prestel et al., 2019	6 meditators (Mdn 70 hrs experience)	Focused attention and open monitoring ^c	Within-person control. Final session was meditation only with no NF.	Increase frontal midline theta (FMT)	Grayscale sphere, increases in FMT power correspond to sphere becoming larger, decreases in FMT power correspond to sphere becoming smaller.	Eight sessions over 2 weeks. Each session has five 5-min training blocks.	Number of sessions was significantly positively associated with greater FMT power. However, this was mostly due to 2 subjects who had a strong significant positive correlation, while the other 4 subjects had nonsignificant effects. Mixed results for control condition.	Not reported	In post-session interviews, some participants reported negative experiences with NF (e.g. distraction, pressure to perform). Subjective appraisal of performance did not always align with one's FMT power values.
Brandmeyer & Delorme, 2020	24 adults	Focused attention/breath practice	Between-person control. Yoked sham NF (from gender-matched pair in the experimental group)	Increase frontal midline theta (FMT)	Colored square, color was updated 4X per sec, with a gradient from black (low FMT amplitude) to light blue (high FMT amplitude).	Eight sessions over 2 weeks. Each session has six 5-min training blocks.	NF group had significant increase in FMT activity across sessions. No significant differences in FMT across sessions among sham control group.	Significant increase in gamma power in frontal midline and left temporal parietal areas during N-2 back task pre to post NF for NF group only. No significant differences in EEG activity for SART or local-global task (attention).	Faster reaction times post-NF on correct trials during the N-2 back working memory task for NF group only. No significant results for SART or local-global task (attention).
Chen et al., 2021	34 meditation-naive participants (17 with anxiety disorder; 17 healthy)	Mindfulness recording therapy ^d	None	Alpha band power of right and left frontal lobes	Bar graph with two bars representing alpha power on the left (colored red) and right (colored green) sides of the frontal lobe.	One 8-min session	Not reported	Significant increase in alpha, gamma, and theta power pre-post mindfulness NF for both groups. An ANOVA revealed a significant main effect of condition (anxiety vs healthy), condition x brain region, condition x hemisphere, and condition x region x hemisphere.	Not reported

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Table 2. Summary of studies of EEG-based neurofeedback with concurrent mindfulness practice.

Note. BIS = Bispectral IndexTM; EEG = Electroencephalography; FMT = frontal midline theta; Hrs = hours; M = Mean; Mdn = Median; Min = minutes; NF = neurofeedback; PCC = Posterior Cingulate Cortex; SART = Sustained attention to response task; SCP = Slow Cortical Potentials; Sec = seconds; USP = Ultra-Slow Potentials; VR = Virtual Reality; Wide = 1–40 Hz. Yrs = years.

- 1 ^a Mindfulness instructions for control conditions were different than instructions for Sensorium conditions, which were more general
- 2 ^b Two of the three Sensorium conditions utilized neurofeedback (Sensorium 1 condition did not)
- 3 ^c Participants allowed to use any strategy that works for them
- 4 ^d Details of mindfulness task were not further specified

1
2 **3.3 EEG studies**

3 **3.3.1 Summary**

4 Nine reports of EEG neurofeedback during mindfulness meditation were identified, corresponding to eight
5 unique samples (**Figure S1 & S2**). In total, there were 242 unique participants, and all samples were adults.
6 Multiple samples looked at meditators, or compared meditators to non-meditators (Hinterberger & Fürnrrohr,
7 2016; Prestel et al., 2019; van Lutterveld et al., 2017). Only one sample included a clinical population (anxiety
8 disorders; Chen et al., 2021) and only two samples did not include a control condition (Chen et al., 2021;
9 Dunham et al., 2018; Dunham et al., 2019). All control conditions were within-subject with the exception of
10 Brandmeyer and Delorme (2020) (**Figure S5**). However, the control conditions varied; most were compared to
11 some form of meditation without neurofeedback and others included yoked shams (**Figure S3 & S4**)
12 (Hinterberger & Fürnrrohr, 2016; Brandmeyer & Delorme, 2020). The most common types of meditation were
13 focused attention, body scan, and open monitoring. The terminology for the type of meditation was not always
14 consistent, and we used specific reporting from studies to classify meditation types. That said, reporting on
15 specific mindfulness instructions was not always clear (Chen et al., 2021) and participants were sometimes
16 allowed to use various strategies (Prestel et al., 2019). It is also important to note that even within a single
17 study, the instructions of the control condition mindfulness did not always match the instructions of the active
18 NF session (Hinterberger & Fürnrrohr, 2016). Qualitative assessments of the mbNF experience are found in
19 **Supplement Table 2.**

20
21 **3.3.2 EEG Targets**

22 Almost all studies used changes in frequency band power as their neural target (**Figure 5**); the most common
23 was alpha and theta, though some studies used gamma (van Lutterveld et al., 2017) or Bispectral Index™
24 (BIS) value, which is an EEG technique most commonly used to measure depth of consciousness for patients
25 under general anesthesia (Dunham et al., 2018; Dunham et al., 2019). Multiple studies focused on more than
26 one frequency band (Hinterberger & Fürnrrohr, 2016; Kosunen et al., 2016; Salminen et al., 2023). Some
27 studies focused on whole brain frequency band power, while others looked at frontal midline sites (Brandmeyer
28 & Delorme, 2020; Prestel et al., 2019) or source localized areas like the PCC (van Lutterveld et al., 2017). The

1 density of EEG ranged from high density 128-channel (van Lutterveld et al., 2017) to extremely low density
 2 Bispectral Index, which generally has 2-4 channels though the exact number of channels was not reported in
 3 this case (Dunham et al., 2018; Dunham et al., 2019). Notably, the way the target was calculated varied, even
 4 within a sample. For example, Salminen et al. (2023) calculated theta power from an average of two electrodes
 5 (F3 and F4) and alpha power from an average of all electrodes (F3, F4, C3, C4, P3, and P4). Other studies
 6 used an independent component analysis (ICA) to calculate the target (Chen et al., 2021; Prestel et al., 2019).
 7 Interestingly, the only two samples that had the same neural target (frontal midline theta) calculated the
 8 feedback differently, with Brandmeyer & Delorme (2020) using the signal from a single frontal electrode (Fz)
 9 while Prestel et al. (2019) used an ICA to determine frontal midline theta. Almost all feedback was displayed
 10 visually, most commonly on some sort of screen, though virtual reality was also used (Kosunen et al., 2016;
 11 Salminen et al., 2023). One study used both sounds and light changes as their feedback presentation
 12 (Hinterberger & FÜRnrrohr, 2016). Positive and negative feedback was shown for all studies.

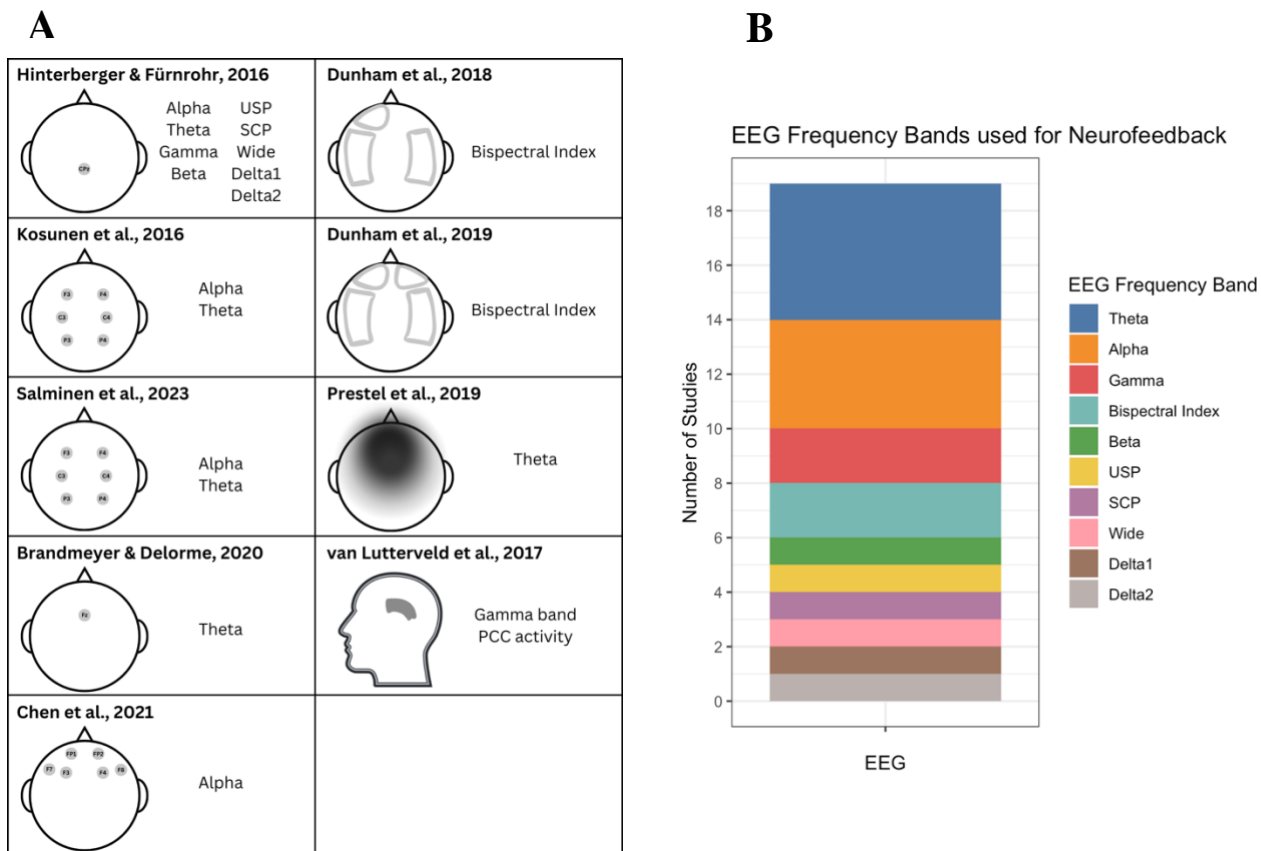


Figure 5. This figure displays the variety in methods of calculating EEG-neurofeedback. In **A**), the spatial layouts of the neurofeedback targets are displayed. Hinterberger & FÜRnrrohr, 2016 calculated alpha, theta, beta, gamma, USP, SCP, wide, delta1, and delta2 from CPz. Kosunen et al., 2016 calculated theta and alpha

1 using an average from F3, F4, C3, C4, P3, and P4. Salminen et al., 2023 calculated theta power using an
2 average F3 and F4, while alpha power was calculated as an average of F3, F4, C3, C4, P3, and P4.
3 Brandmeyer & Delorme, 2020 used Fz to calculate frontal midline theta. Chen et al., 2021 used FP1, F3, F7
4 and FP2, F4, F8 to calculate alpha of the left and right frontal lobes, respectively. Dunham et al., 2018 placed
5 the BIS sensor on the left forehead and the temporal fossa. Dunham et al., 2019 placed the BIS sensor on the
6 left or right forehead and the temporal fossa. Prestel et al., 2019 used independent component analysis (ICA)
7 with a 32-channel setup to calculate frontal midline theta. van Lutterveld et al., 2017 used source estimation
8 with a 128-channel setup to determine Gamma band PCC activity. In **B**), the frequency bands used by each
9 study are displayed. Theta was used the most by five studies, closely followed by alpha, which was used in
10 four studies.

13 **3.3.3 EEG Target Engagement**

14 Not all papers reported on target engagement (Kosunen et al., 2016; Chen et al., 2021). For those that did, the
15 way the target engagement was reported differed. For example, some studies looked at activation compared to
16 baseline (Dunham et al., 2018; Dunham et al., 2019; van Lutterveld et al., 2017), compared to no NF
17 conditions (Salminen et al., 2023), or across sessions using different linear models (Prestel et al., 2019;
18 Brandmeyer & Delorme, 2020). The difference in reporting and measures used makes synthesizing results
19 difficult, as well as the fact that support for target engagement was mixed. The strongest support was for an
20 impact on theta (Brandmeyer & Delorme, 2020; Hinterberger & FÜRNRÖHR, 2016; Salminen et al., 2023; Prestel
21 et al., 2019), while alpha had both significant and null results (Hinterberger & FÜRNRÖHR, 2016; Salminen et al.,
22 2023). However, it is important to note Hinterberger and FÜRNRÖHR's (2016) significant results were collapsed
23 across multiple experimental conditions, one of which did not include NF. Others found significant changes in
24 BIS values compared to baseline (Dunham et al., 2018; Dunham et al., 2019), but the significant decrease
25 from day one to day four (Dunham et al., 2018) did not hold up in a larger sample (Dunham et al., 2019). For
26 those who did find significant results across days, the significant effect was in one case driven by two
27 participants (Prestel et al., 2019), and was stronger when certain "non-responders" were excluded
28 (Brandmeyer & Delorme, 2020). It is also important to note the spatial limitations of neural targets using EEG,
29 given that spatial resolution of EEG is limited even when using source localization. For example, the one study
30 that used source localization of the PCC found that over 80% of runs examined had significant correlations
31 between the right lateral occipital cortex and the PCC, though less than 36% of runs showed significant
32 correlation between the left supplementary motor area and the PCC (van Lutterveld et al., 2017). Correlations
33 between 40-57Hz PCC time series and delta, theta, alpha, and beta were calculated, but never surpassed

1 more than 40% of runs showing significant correlations. The frequency specific to the PCC may be more
2 accurate than the source localization, which may be capturing signals from occipital regions of the brain more
3 broadly.

4 **3.3.4 Neural Outcomes**

5 Only four studies out of nine reported on other neural outcomes. All four studies examined EEG bands beyond
6 the bands of the neural target, focusing on: (a) other frequency bands during NF and/or control (Salminen et
7 al., 2023; van Lutterveld et al., 2017), (b) frequency bands at rest before and after NF (Chen et al., 2021), and
8 (c) frequency bands in tasks before and after NF (Brandmeyer & Delorme, 2020). The following results discuss
9 frequency bands that were not the target of NF. There is support that alpha, theta, and gamma power
10 significantly increase from pre to post mindfulness NF (Chen et al. 2021), as well as support for gamma
11 increases during NF compared to no-NF (Salminen et al., 2023). The delivery of NF (Virtual Reality (VR) >
12 computer screen) and the type of meditation (body scan > focused attention) can also have an impact on the
13 level of gamma (Salminen et al., 2023). There is mixed support for NF's effect on cognitive tasks, with no
14 significant changes found for attentional tasks, but a significant increase in gamma power during a working
15 memory task done before and after NF for those that received NF (Brandmeyer & Delorme, 2020).

17 **3.3.5 Behavioral Outcomes**

18 All but one study reported on some sort of behavioral outcome. Most focused on how individuals felt doing the
19 mbNF (Hinterberger & FÜRnrohr, 2016; Kosunen et al., 2016; Prestel et al., 2019; Salminen et al., 2023), while
20 others looked at changes in well-being (Dunham et al., 2018; Dunham et al., 2019) or even performance on
21 cognitive and attentional tasks (Brandmeyer & Delorme, 2020). When looking at immersive ways to deliver
22 neurofeedback, such as the Sensorium or VR, findings suggest participants find these types of modalities more
23 extraordinary, more engaging, have more positive experiences and less negative experiences compared to
24 audio/visual guided meditations without VR or Sensorium enhancements (Hinterberger & FÜRnrohr, 2016;
25 Kosunen et al., 2016; Salminen et al., 2023). However, this difference is not always due to the addition of
26 neurofeedback, as control conditions with these enhancements with yoked sham or no NF did not always show
27

1 significant differences (Hinterberger & Fürnrohr, 2016; Kosunen et al., 2016). Accordingly, some participants
2 report that too much focus on the NF can be distracting and lead to poorer performance; however, it is
3 interesting to note that subjective experience of performance did not always align with objective performance,
4 as measured by frontal midline theta (Prestel et al., 2019). Beyond experiences during mbNF, studies have
5 found that wellbeing scores increase from baseline to completion of all sessions, and are significantly higher at
6 completion than a control group who received no mbNF (Dunham et al., 2018; Dunham et al., 2019). There is
7 also some evidence to suggest NF may help improve performance on memory tasks (NF group compared to
8 sham control had faster reaction times post-NF for correct trials during the N-2 back working memory task)
9 (Brandmeyer & Delorme, 2020). However no significant effects were found for attention tasks.

11 **3.3.6 Clinical Applications**

12 Only one study examined EEG neurofeedback in a clinical sample of 17 individuals with anxiety disorders
13 (Chen et al., 2021). Compared to healthy controls, anxious subjects exhibited initial lower power in alpha,
14 theta, and gamma. After NF, anxious subjects significantly increased power across all bands in all brain areas.
15 Chen et al. (2021) suggest that the increase in gamma power indicated a reduction in anxiety symptoms,
16 though they did not report on changes in subjective measures of anxiety. ANOVAs revealed interactions of
17 condition vs brain region/hemisphere, but the direction of differences were not reported. Although the
18 remaining studies reported on non-clinical samples, Dunham et al., 2018 and Dunham et al., 2019 examined
19 well-being as a target for mindfulness neurofeedback among physicians/nurses, a group within which stress
20 and emotional exhaustion are common (Dunham et al., 2018). Participants' subjective well-being was found to
21 improve following the mbNF, suggesting that even in non-clinical samples, NF may be a promising avenue to
22 increase well-being.

24 **3.2.8 Quality (CRED-NF)**

25 There were control conditions in the majority of the EEG studies, but they typically lacked blinding (sham).
26 Reporting of feedback specifications and target engagement was common. Few studies reported artifact

- 1 correction. Few studies conducted preregistration, justified their sample sizes or made their data/code open
- 2 access. A full table may be found in **Table S3**.

4. Discussion

Mindfulness meditation consists of purposefully bringing one's attention back to the present moment, and cultivating an open-minded and non-judgmental attitude (Creswell et al., 2017). Though mindfulness meditation is increasingly used for promoting mental health, there are many open questions about its neural bases. In this review, we investigate a promising tool for understanding the neural mechanisms of mindfulness, neurofeedback. Neurofeedback consists of relaying neural signals (the target) to the participant and examining if they can learn to modulate the signals (target engagement). Successful modulation provides evidence that a target brain region is involved in meditation. In addition, given the right targets, neurofeedback may help participants practice correctly and lead to better attention, deeper mindfulness, and positive behavioral outcomes. In this systematic review, we assess whether participants can modulate brain targets (insight into neural mechanisms) and whether participants benefit from the practice (behavioral outcomes). We included studies utilizing mindfulness meditation with concurrent EEG or fMRI feedback (i.e., mindfulness-based neurofeedback [mbNF]).

The search yielded 19 reports, with 15 independent samples. The earliest study was published in 2013, underscoring the nascency of the mbNF field (systematic inquiry of neurofeedback more generally extends back to the early 2000s for fMRIs and the 1960s for EEG). Studies used a wide range of targets across brain areas and frequency bands, and often reported different metrics of target engagement. Neurofeedback duration and number of runs varied (from single 15-min sessions to multiple weeks of training). Sample sizes were generally small, given the resource-intensive nature of neurofeedback. Few studies were RCTs, which are critical for establishing mbNF efficacy and testing mechanisms.

4.1 Brain Targets

One of the prominent neuroscientific theories of mindfulness posits that successful practice leads to downregulation of the DMN, perhaps most robustly the core hubs of the PCC and mPFC (Ganesan et al., 2022). The DMN has a well-established role in internally-generated, self-referential thought (Andrews-Hanna, 2012; Buckner et al., 2008). Mindfulness meditation involves recognizing self-referential thoughts, disengaging from them, and engaging in attention on an object like the breath. Thus, mindfulness may involve downregulating DMN activity. Accordingly, many fMRI studies of mbNF chose to target the DMN. Some studies

1 calculated and displayed anatomically defined PCC activations compared to a control self-reference condition
2 (Garrison, Santoyo, et al., 2013; Garrison, Scheinost, et al., 2013), whereas others used subject-specific,
3 functionally derived maps of the DMN (Bauer et al., 2020; Kim et al., 2019; Okano et al., 2020; Pamplona et
4 al., 2020; Zhang et al., 2023). Consistent downregulation of the DMN was found. Neurofeedback studies often
5 included other networks like the central executive network (CEN) and salience network (SN). There is
6 extensive reason to believe that DMN and other network interactions may be involved in mindfulness
7 meditation, specifically in the switching between external and internal modes of attention (Hasenkamp et al.,
8 2012; Mooneyham et al., 2016; Rahrig et al., 2022). Accordingly, studies relayed the participants' difference
9 between CEN and DMN (Bauer et al., 2020; Zhang et al., 2023), sustained attention networks and DMN
10 (Pamplona et al., 2020, 2023), and the slope of the DMN-SN connectivity excluding the CEN (Kim et al., 2019).
11 It is unclear when participants are given these multivariate measures which variable is being trained –one
12 study found that the DMN was modulated and not the sustained attention network (Pamplona et al., 2020).

13 Researchers also examined neuroplastic changes dependent on their DMN-based neurofeedback,
14 finding changes in DMN region connectivity with other brain areas like the anterior cingulate cortex (Zhang et
15 al., 2023). These changes suggest that neurofeedback may modulate intrinsic features of the DMN, offering a
16 key inroad to mitigate ruminative and depressogenic perseveration tendencies (Zhang et al., 2021).

17 Mindfulness meditation has been associated with power increases in alpha, theta and gamma waves
18 during meditation (Chiesa & Serretti, 2010; Lee et al., 2018; Lomas et al., 2015; Stapleton et al., 2020). Alpha
19 and theta power may correspond to shifting attention to internal sensations and thoughts (Lomas et al., 2015),
20 whereas gamma power may reflect wider awareness (Lomas et al., 2015; Lutz et al., 2004; Stapleton et al.,
21 2020). There is considerable evidence that gamma EEG activity can be contaminated by muscle activity
22 (Muthukumaraswamy, 2013; Whitham et al., 2007). However, it is not necessary to disregard gamma power
23 altogether, as long as multiple precautions are taken to remove muscle artifacts and confirm they are not
24 correlated with data (e.g., van Lutterveld et al., 2017). Accordingly, the 9 EEG studies of mbNF selected
25 alpha, theta and gamma targets. The most consistent evidence was for theta increases, specifically frontal
26 midline theta, which is often an indicator of cognitive control (Cavanagh & Frank, 2014). Results were mixed
27 when probing alpha and gamma power.

1 The study of EEG and fMRI have often been conducted in isolation, and each has advantages and
2 disadvantages. EEG-neurofeedback is useful for precise temporal modulation as well as cost-effective
3 application but lacks spatial specificity and may be susceptible to motor artifacts (Muthukumaraswamy, 2013;
4 Whitham et al., 2007). fMRI-neurofeedback is useful for targeting specific brain regions with specificity,
5 however, it is expensive and the underlying signals are slow to change. There have been meaningful efforts to
6 develop EEG measures with spatial specificity. Frontal midline theta may be negatively correlated with DMN
7 activation (Scheeringa et al., 2008; Prestel et al., 2018), while gamma may be positively correlated with DMN
8 activation (Berkovich-Ohana et al., 2012). One neurofeedback study included, Van Lutterveld et al. (2017),
9 specifically targeted activity in the PCC by using source localization. Yet, they did find that occipital cortex
10 activity correlated heavily with localized PCC activity. It may be necessary to conduct EEG-fMRI fusion
11 experiments to develop better measures. In a seminal paper, Keynan et al. (2019) created an EEG target
12 measure of amygdala activity derived from machine learning based on simultaneous EEG-fMRI and showed
13 that participants could modulate the target. The amygdala-EEG neurofeedback led to increases in emotional
14 awareness and regulation and decreases in amygdala activation as measured by fMRI.

15 **4.3 Brain Target Summary and Limitations**

17 Extant research has, at times, corroborated neuroscientific theories of mindfulness; however, the
18 majority of research did not include robust control conditions, which results in a lack of specificity. For example,
19 decreases in DMN activation during neurofeedback does not indicate that participants are learning or that DMN
20 deactivation is linked to mindful states. One possibility is that focusing on the display of the feedback itself may
21 lead to DMN decreases. There is substantial evidence that engaging in external tasks leads to decreases in
22 DMN activations (Raichle, 2015; Whitfield-Gabrieli & Ford, 2012), and likely changes in power as well
23 (Fitzgibbon et al., 2004; Khader & Rösler, 2011). Another possibility is that mindfulness meditation leads to
24 decreases in DMN activation, but that this process is implicit and beyond conscious control (thus,
25 neurofeedback would not make a difference). To obviate these concerns, researchers need to employ blinded
26 control conditions or/and transfer tasks. Gold-standard control conditions involve delivering participants
27 feedback that should be unaffected by meditation (e.g. activations from another brain area, from another
28 subject, or reversed activation) (Sorger et al., 2019; Thibault et al., 2016). A weaker control condition is

1 mindfulness-as-usual, which is effective for examining general neurofeedback mechanisms, and
2 neurofeedback benefits, but not target-specific mechanisms (Ros et al., 2020). Transfer tasks involve asking
3 participants to meditate but removing the influence of neurofeedback- and one can examine differences in
4 transfer tasks assessed before and after neurofeedback. Notably, the fMRI studies that employed sham
5 controls or transfer tasks did not find significant differential evidence for target engagement (Kim et al., 2019;
6 Kirlic et al., 2022). EEG studies did not employ transfer tasks, and only one study employed sham
7 (Brandmeyer & Delorme 2020). Brandmeyer and Delorme (2020) found evidence of increased target
8 engagement of frontal midline theta in mbNF, while the sham group showed no significant changes.
9 Comparisons of EEG-neurofeedback to mindfulness-as-usual also resulted in improved target engagement
10 (Hinterberger & FÜRnrrohr, 2016; Salminen et al., 2023). In summary, there is not currently evidence from the
11 strongest designs supporting mbNF-specific mechanisms of DMN activation control, while there are some
12 indications of control over frontal midline theta.

13 **4.4 State Mindfulness**

14
15 It is critical to identify whether neural feedback can engage the proposed target mechanism, but this is
16 insufficient if it does not yield greater mindfulness and associated mental health benefits. Ideally, target
17 engagement also leads to increases in state mindfulness, or deeper mindfulness during practice. There is only
18 limited evidence in our included studies for increased state mindfulness (Hinterberger & FÜRnrrohr, 2016; Kim et
19 al., 2019; Kirlic et al., 2022; Zhang et al., 2023 c.f., Kim et al., 2019, Prestel et al., 2019). One concern is that
20 monitoring of the feedback may cause distraction during meditation. For this reason, some studies provided
21 feedback intermittently after blocks of meditation (Pamplona et al., 2020, 2023), or allowed practitioners to
22 close their eyes during meditation (van Lutterveld et al, 2017). The studies mostly used visual feedback, which
23 may be distracting. Future research could examine the impact of design choices on state mindfulness during
24 mbNF, including visual/auditory modality, continuous vs intermittent feedback, etc. It may also be useful to
25 collect data throughout the course of mbNF to assess inattention.

26 27 **4.5 Behavioral Outcomes**

1 Of note, mbNF has often been proposed to enhance mindfulness acquisition (Brandmeyer & Delorme,
2 2013). A prime motivation for many of the studies reviewed was the possibility of beneficial outcomes in
3 cognition and affect. An fMRI study observed some improvements in reaction times on a cognitive task beyond
4 a control condition (Pamplona et al., 2020), but it wasn't maintained at follow-up. An EEG study identified
5 memory improvements but not RT improvements (Brandmeyer & Delorme, 2020). Another fMRI study tested
6 perceived stress and negative affect, and didn't observe any improvements (Kirlic et al., 2022), whereas an
7 EEG study identified improvements beyond a waitlist control (Dunham et al., 2018). Two fMRI studies
8 observed decreases in auditory hallucinations (Bauer et al., 2020; Okano et al., 2020), a striking finding with
9 implications for deleterious psychosis symptoms, however the findings were extracted from two protocols on
10 the same sample. Of course, studies may have measured cognitive and affective outcomes but not reported
11 them (many EEG studies did not report behavioral outcomes). Preregistration of measures and analyses was
12 scarce. Overall, there is limited existing evidence for mindfulness-based neurofeedback benefits in terms of
13 behavioral or clinical outcomes.

14 **4.6 Clinical Relevance**

15 Clinical populations may benefit from adaptations of mindfulness instruction. Individuals with histories of
16 trauma may experience traumatic re-experiencing and distress due to meditation (Treleaven, 2018; Zhu et al.,
17 2019). Ruminative individuals with a tendency to engage in repetitive negative thoughts may particularly have
18 trouble learning meditation (Alleva et al., 2014; Crane & Williams, 2010; Hilton et al., 2017). It may be
19 especially helpful for these clinical populations to have scaffolds while they meditate. Mindfulness-based NF
20 may be such a scaffold, providing an engaging external locus of attention plus the same essential components
21 of mindfulness - redirection of attention and non-judgement. Studies on mbNF included here involved clinical
22 participants (Bauer et al., 2020, Okano et al., 2020, Zhang et al., 2023) but none involved healthy control
23 groups. Future studies should assess directly whether the benefits of mbNF are more pronounced in clinical
24 groups. Of course, mbNF should not be considered a replacement for more traditional mindfulness training
25 (e.g., with in-person teaching). There is a rich psychotherapeutic literature on developing mindfulness
26 adaptations for clinical groups (e.g. mindfulness-based cognitive therapy; Segal et al., 2004) and acceptance

1 and commitment therapy; (Hayes et al., 1999), and mbNF requires more validation before joining these
2 frontline treatments.

4 **4.7 Summary**

5 This systematic review of mindfulness meditation concurrent with EEG or fMRI neurofeedback
6 suggests that participants can learn to downregulate the DMN and increase power in the theta band. However,
7 the lack of adequate control conditions limits mechanistic assertions. In addition, the downstream benefits of
8 mindfulness-based neurofeedback require systematic examination. There is evidence for the feasibility of
9 neurofeedback with clinical populations, and future work should directly compare the effects of mbNF between
10 clinical and non-clinical populations.

12 **4.7 Limitations**

13 Our conclusions should be tempered in light of the heterogeneity of the studies. Targets, outcomes,
14 and sample characteristics varied widely across the studies. These differences are well-known to affect neural
15 outcomes (e.g. neuromaturation in adolescents, Fan et al., 2021; Norbom et al., 2021). Mindfulness training
16 may be more effective for reducing psychological distress than for improving cognitive function ((Gill et al.,
17 2020; Whitfield et al., 2022), and it is unclear whether this applies to mbNF. Reporting was also variable, which
18 we assessed using the CRED-NF checklist (Ros et al., 2020). The vast majority of studies lacked blinded
19 control conditions, reported brain target engagement as a single outcome instead of comprehensively, and did
20 not engage in open science practices. In the future, full reporting of targets and outcomes could help identify
21 why some studies may see effects and others do not, and it could lead to possible quantitative synthesis of
22 effects.

23 Another limitation is the scope of the review. We chose not to review all meditation based
24 neurofeedback, restricting our selection to studies that employed mindfulness practices. There are multiple
25 families of meditations, including attentional, constructive and deconstructive practices (Dahl et al., 2015). The
26 studies included here involved attentional practices. Future work should examine the effects of neurofeedback
27 on other practices, perhaps targeting different brain processes.

4.8 Future Directions

To study the mechanisms of mbNF and associated effects, the field would benefit from adopting best practices. Chief among these may be a confirmatory-exploratory distinction. Exploratory studies may examine multiple targets, multiple modalities of feedback, qualitative as well as quantitative feedback – all with the aim of establishing preliminary hypotheses about neural targets. These studies are necessary and important given the nascency of the field. Three studies reviewed provide a sound roadmap for this type of work (Garrison et al., 2013ab, Van Lutterveld et al., 2017). One innovation in particular is working with experienced meditators, who have detailed awareness of mental phenomena during meditation. Another innovation is developing individualized targets - one method could be monitoring neural data during meditation for a given participant, with self-report probes (experience samples), and then in a subsequent task delivering feedback that was trained on that initial period. This personalization may be more effective than using ‘one-size-fits-all’ brain signals (Brandmeyer & Reggente, 2023).

It is critically important, however, to build on this work using RCTs with carefully designed sham control conditions. Such confirmatory work, through tests of clear and a priori hypotheses, can help the field evaluate whether participants learn to modulate a neural signal, and whether it leads to higher state mindfulness and positive mental health or cognitive outcomes. Sham or alternative ROI controls are preferred, given their ability to control for effects of placebo as well as feedback monitoring, but mindfulness-as-usual controls are useful and easier to implement. Researchers may even choose to examine different dosages of mbNF (Bloom et al., 2023). Clinical trial registration and/or preregistration is useful, and when deviations emerge as they always do during empirical research, they should be reported. As mentioned previously, the CRED-NF checklist should be used for standardized reporting.

A final aim is real-world translation. In contrast to fMRI, which is costly and largely only accessible via academic medical centers, there is burgeoning interest in consumer-grade EEG tools like MUSE (Hashemi et al., 2016; Sawangjai et al., 2019), which are relatively cheap (~\$250) and easy to use. We believe that this interest should be tempered given the limited knowledge base in lab settings. EEG tools like MUSE may rely on the potent influence of *neurosuggestion* (Schönenberg et al., 2017), which is a cultural emphasis and trust

1 in Western society for neuroscientific technology. Speculatively, *neurosuggestion* effects may not be
2 sustainable in supporting a habit of meditation, and may obscure the self-insight that comes with meditation
3 (Vago & David, 2012).

4
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18
19
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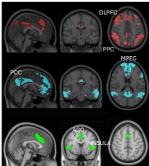
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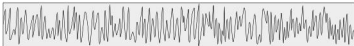
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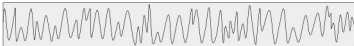
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Gamma
30+ Hz



Beta
13-30 Hz



Alpha
8-13 Hz



Theta
4-8 Hz



Delta
0-4 Hz



Identification of studies via databases and registers

Identification

Records identified from:
 PubMed (n=131)
 Web of Science (n=200)
 PsycInfo (n=101)
 Scopus (n=224)

Records removed before screening:
 Duplicate records removed (n=298)

Screening

Records screened
 (n=375)

Records excluded:
 Not an empirical article (n=171)
 Not relevant (n=93)

Reports sought for retrieval
 (n=114)

Reports not retrieved:
 Unable to access full text (n=0)

Reports assessed for eligibility
 (n=114)

Reports excluded:
 No mindfulness (n=29)
 No neurofeedback (n=16)
 No concurrent mindfulness/neurofeedback (n=8)
 Not relevant (i.e. no NF nor mindfulness) (n=3)
 Not an empirical article (n=8)
 Not fMRI or EEG (n=33)
 Other (n=1)

Included

Studies included in review (n=15)
 Studies included from search (n=14)
 Studies included from reference list (n=1)

Reports of included studies (n=13)
 Reports included from search (n=10)
 Reports included from reference list (n=3)

POC:

[Garrison2013](#) (sub)

[Kirk2022](#), [Yu2022](#)

STG:

[Okano2020](#)

(Clin.)

CEN:

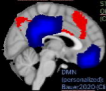
[Pamplona2020](#),
2023*

[Bauer2020](#)

(Clin.)

[Zhang2023](#)

(Clin.)



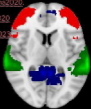
DMN

(personalized)










[Bauer2020](#) (Clin.)

[Kim2019*](#)

[Zhang2023](#) (Clin.)



A

<p>Hinterberger & Fürnrohr, 2016</p>  <p>Alpha USP Theta SCP Gamma Wide Beta Delta1 Delta2</p>	<p>Dunham et al., 2018</p>  <p>Bispectral Index</p>
<p>Kosunen et al., 2016</p>  <p>Alpha Theta</p>	<p>Dunham et al., 2019</p>  <p>Bispectral Index</p>
<p>Salminen et al., 2023</p>  <p>Alpha Theta</p>	<p>Prestel et al., 2019</p>  <p>Theta</p>
<p>Brandmeyer & Delorme, 2020</p>  <p>Theta</p>	<p>van Lutterveld et al., 2017</p>  <p>Gamma band PCC activity</p>
<p>Chen et al., 2021</p>  <p>Alpha</p>	

B

EEG Frequency Bands used for Neurofeedback

