

### **MODERATED POSTER PRESENTATION**

# *In Vivo* quantitative imaging of angiogenesistargeted PFOB nanoparticles in a hypercholesterol rabbit model using <sup>19</sup>F-MRI with ultra-short echo time balanced SSFP

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#### Summary

Herein, initial results are presented as obtained in a hypercholesterol rabbit model with the simultaneous  $^{19}\text{F}/^{1}\text{H}$  balanced UTE-SSFP technique and using  $\alpha_{\nu}\beta_{3}$ -targeted PFOB nanoparticles to establish the feasibility of high sensitivity MR molecular imaging of Gd-free, fluorine-based, clinically-relevant contrast agents.

#### Background

 $\alpha_{\nu}\beta_{3}$ -integrin targeted nanoparticle (NP) emulsions have been shown to detect and quantify angiogenesis and anti-angiogenic therapy in small animal models of atherosclerosis. While these NP were visualized in high resolution pre- and post-injection <sup>1</sup>H-MRI via a Gadolinium (Gd) chelate, we seek to image the perfluoro-octyl bromide (PFOB) core directly via <sup>19</sup>F MR. Early *in vivo* successes of <sup>19</sup>F MR molecular imaging exploited the single resonance peak of perfluoro-crown-ether. However, PFOB, which is the more clinically-relevant NP with a better-understood human safety profile, has a more complex spectrum with seven <sup>19</sup>F resonance peaks and multiple relaxation conditions, leading to chemical shift artifact and intra-voxel destructive interference. We hypothesize that a new technique-simultaneous dualfrequency <sup>19</sup>F/<sup>1</sup>H ultra-short echo time (UTE) balanced steady state free precession (b-SSFP) sequence with 3D radial readout-will allow efficient, sensitive imaging of the complex PFOB signal without the need for Gd and

#### Methods

The study was performed using a dual-tuned transmit/ receive surface coil (7×12cm) on a 3T clinical wholebody scanner (Achieva, Philips Healthcare) modified for truly-simultaneous <sup>19</sup>F/<sup>1</sup>H operation. Male New Zealand White rabbits were fed high cholesterol chow for 20 weeks. Imaging was performed 2h post-injection of 1.0ml/kg of the  $\alpha_{\nu}\beta_{3}$ -targeted PFOB-NP. A UTE b-SSFP sequence with simultaneous  ${}^{19}F/{}^{1}H$  excitation and 3D radial readout was acquired at six time points postinjection with the following parameters: FOV=140mm, matrix  $112^3$ , isotropic voxel  $\Delta x=1.25$  mm,  $\alpha=30^\circ$ , excitation bandwidth exBW=9kHz, pixel bandwidth pBW=900Hz, TR=2.0ms, TE=100µs (FID sampling), total scan time 28 min. The radial k-space data was reconstructed at full resolution for the <sup>1</sup>H component, and at lower resolutions with higher signal to noise for the <sup>19</sup>F component (Nyquist radius 7%). <sup>19</sup>F-data from subsequent time points were combined to provide an image of the spatial NP distribution. The <sup>19</sup>F-signal was calibrated for <sup>19</sup>F concentrations using an agar phantom containing PFOB-NP at 150mM<sub>19F</sub>.

#### Results

*In vivo* imaging of angiogenesis-targeted PFOB nanoparticles was successful using the  ${}^{19}F/{}^{1}H$  UTE b-SSFP sequence. Figure 1a shows an example of the proton image quality in a selected slice at the aorta, which is robust against motion due to the simultaneous 3D radial

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in sufficient resolution to discern the anatomy even in the presence of cardiac and respiratory motion.



acquisition. The isotropic voxel allows multi-planar reformatting for visualizing anatomy and prescribing ROIs for analyzing the directly-corresponding  $^{19}$ F NP signal. In this example,  $\alpha_{\nu}\beta_3$ -targeted PFOB-NP were detected in the aorta ROI (Fig.1b) in concentrations ranging from 10 to 16mM.

aortic region is in green, and extra-aortic <sup>19</sup>F signal is blue.

#### Conclusions

Dual frequency <sup>19</sup>F/<sup>1</sup>H radial 3D balanced ultra-short TE is a versatile pulse sequence that allows high-sensitivity, high-resolution *in vivo* detection of angiogenesistargeted PFOB-NP despite the possible complex resonant peak interaction.

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