



Evaluation of Mental Load of Drivers in Long Highway Tunnel Based on Electroencephalograph

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In recent years, the mileage of the tunnels has substantially increased with the rapid highway construction that led to increasing highway tunnels. Most studies on tunnel accidents have mainly focused on the external environments, such as tunnel structure, traffic volume, and lighting. In addition, although many studies on mental load of drivers have been conducted for public roads, such studies for highway tunnels have been limited. In this study, three scenarios with different front vehicle speeds (60, 45, and 30 km/h) in a two-lane long tunnel (one lane in each travel direction) were evaluated using a driving simulator. The experiment involved 24 participants (14 men and 10 women) with an average age of 25.8 years and an average experience of 3.2 years. The electroencephalogram (EEG) technology was used to collect the leading EEG indicators during the driving simulation of the scenarios: α , β , and θ waves and the wave ratio, ($\alpha + \theta$)/ β . According to the β -wave energy measurements, the alertness of drivers was the lowest at 45 km/h after adapting to the tunnel environment, indicating that the drivers were more comfortable at this speed. This preliminary finding should help in determining the speed limit in this type of tunnel.

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INTRODUCTION

The tunnel is an alternative solution for the roadway along rugged topography to overcome natural conditions. Thus, road tunnels usually represent bottlenecks in the road network (Bassan, 2016). The tunnels are at risk of hazard and intractable accidents. The severe accident rates and costs in tunnels were often higher than those on the corresponding roads (Caliendo and De Guglielmo, 2012). Therefore, safety studies on driving in tunnels are necessary.

For general highways, many studies on mental load of drivers have been conducted using electroencephalograph (EEG). These studies have made it possible to evaluate mental load and behavior of drivers in tunnels. The studies have used different indicators, such as heart rate variability, eye-tracking movements (Yang et al., 2019b, 2020d), and EEG. Using EEG to study the mental state of drivers in a driving simulator is a mature technique, which was first used in the 1980's (Lemke, 1982; Torsvall, 1987). The accuracy and efficiency of this technology have been demonstrated (Haak et al., 2008; Li et al., 2010; Borghini et al., 2012; Bashivan et al., 2016; Kim et al., 2018). Many researchers have studied essential driver characteristics, such as driver sleepiness (Resalat and Saba, 2015), drowsiness (Lin et al., 2005), fatigue (Jap et al., 2009; Arakawa et al., 2019), alertness level (Kiymik et al., 2004), and cognitive load (Barua et al., 2017). Other studies have used

EEG, as the effect of color scheme (Yang et al., 2020a), situation awareness (Yang et al., 2020b), and the effect of directional signs (Yang et al., 2020c). Other studies on brain activities, driver aggressiveness, music and emotion, and EEG classification have also been conducted (Fan et al., 2010; Liu et al., 2013; Lin et al., 2014; Yang et al., 2018, 2019a; Zeng et al., 2018).

For tunnels, numerous studies have been conducted on traffic safety. However, most studies have focused on tunnel geometric characteristics and traffic volumes, tunnel illumination and visibility (Miyake et al., 2019), accident zone locations (Amundsen and Ranes, 2000; Ma et al., 2009), and safety speed (Yan et al., 2019). The interesting study by Yan et al. (2019) addressed driving risk levels in continuous tunnels, 250-1,000 m long and two lanes in each direction, using various risk indicators. A naturalistic driving system equipped with a road environment and driving-behavior data acquisition system was used to collect the data in 130 tunnels on four highways. The American Association of State Highway and Transportation Officials (AASHTO) braking model and the convex hull algorithm were used to predict the critical safety speed and the critical time headway of each risk feature. In contrast, this study was designed to predict the speed of carfollowing that is most comfortable for the drivers using brain waves and eye movements. Specifically, this study evaluated the effect of a 1,800-m long tunnel on the EEG of drivers in a carfollowing situation. Thus, this study complements the study by Yan et al. (2019).

However, a few studies have been conducted on driver behavior in tunnels. The literature shows that the pathological discomfort of drivers strongly correlates with the accident rate when driving in tunnels (Calvi and D'amico, 2013). The behavioral training using virtual reality affects the self-evacuation during a drill (Kinateder et al., 2013). Thus, more studies on driver behavior in tunnels are needed. The novelty of this study lies in the evaluation of the mental state of drivers to determine the appropriate speed limit in a highway tunnel, which has not been addressed in the literature. In the experimental scenarios, the driver followed a car in front, which traveled at a specific speed to simulate different speed limits. The EEG of drivers was measured to determine the change in the mental state of drivers, mainly those undesirable emotions, such as tension, depression, and anger. The findings of this study might strengthen the inference and analysis of the motivation and mechanism of the lousy behavior of drivers and might provide a theoretical basis for the prevention of tunnel traffic accidents.

EXPERIMENTAL DESIGN

Experimental Subjects

Drivers of similar ages were selected to avoid the influence of age on driving. A total of 24 subjects were recruited for the experiments (14 men and 10 women). Each participant was in good physical condition, with no color weakness or color blindness. The driving experience of the subjects varied. The average age was 25.8 years, with an SD of 5.5 years. The average experience was 3.2 years, with an SD of 3.7 years. Notably, in previous driving simulation studies, this sample size was

considered enough to arrive at some preliminary conclusions, especially using the EEG index. The number of participants used in previous studies has ranged from 10 to 24 (Reed and Green, 1999; Risser et al., 2000; Godley et al., 2002; Philip et al., 2005; Ingre et al., 2006).

Driving Simulator and EEG System

The experiment was carried out indoor in a driving simulator cabin, eliminating the effects of weather, light, and noise on the experimental results. The indoor illumination was 300 lx. There is no noticeable light change in and out of the tunnel in the simulator test, which avoids physiological changes due to light changes, such as dim light that makes the pupils of drivers enlarged after entering the tunnel. The wireless EEG system and the driving simulator were used to collect the data in the experiments, as shown in Figure 1. The hardware parts of the driving simulator include the display, transmission, clutch, cockpit, sensors, steering, throttle, brake, and seat. The EEG acquisition part consists of the Enobio wireless EEG system, which transmits 24-bit EEG data and accurately restores the original EEG signal. Its bandwidth is 0-250 Hz, the sampling rate is 500 samples per second (sps), the resolution is 24 bits, i.e., 0.05 uv, and the noise is <1 uvrms (0–250 Hz).

The EEG test provides information concerning the dynamics and simulated electrical brain activity, where brain cells communicate through electrical impulses. An EEG can be used to help detect potential abnormalities in the brain waves. The small flat metal disks (i.e., electrodes) that are attached to the scalp with wires analyze the electrical impulses of the brain and send signals to a computer that records the results. The charges are amplified and appear as a graph on a computer screen. The details on the mathematical foundation of EEG can be found elsewhere (Doschoris and Kariotou, 2017).

Experimental Scenarios Experimental Road

The scene of this experiment was a long two-lane, second-class highway tunnel (i.e., one lane in each travel direction).



FIGURE 1 | Experimental equipment.

According to the highway technical standards by the Standardization Administration of the People's Republic of China (Standardization Administration of the People's Republic of China, 2014), the length of the long highway tunnel ranges from 1,000 to 3,000 m. The tunnel length was set as 1,800 m, which is classified as a long tunnel. Also, this length would help control the total time of the experiment to avoid driver fatigue. The length of the experimental section was 2.2 km. Figure 2 shows a schematic diagram of the experimental highway tunnel. The length of the section from the starting point to the tunnel entrance was 200 m, and the length from the tunnel exit to the end point was 200 m. The width of each lane was 3.75 m, and the total width of the cross-section was 7.5 m (i.e., there was no median). Figure 3 shows a schematic diagram of the internal environment of the tunnel. A truck escape ramp existed on the right-hand side of the traveled way, with a width of 1.8 m. The experiment was carried out in the driving simulator, where the illumination was controlled as the indoor lighting (300 lx). There was no specific noise interfering with the participants, apart from the driving simulator sound.

Driving Speed and Traffic Flow

Both the mental state and the behavior of drivers were explored in a vehicle-following situation. The independent variable controlled in this study was a single factor, i.e., the speed of the leader vehicle. The speed limit of the second-class highway is normally set as 60 or 80 km/h, so this experiment took a design speed of 60 km/h as the maximum speed limit. The minimum speed limit zone was 30 km/h with increases of 15 km/h increments up to a maximum of 60 km/h. Thus, the three experimental scenarios in the following situations in the long tunnel were set with the driving speed of the front car set at 60 km/h (Scenario A), 45 km/h (Scenario B), and 30 km/h (Scenario C). Based on the United States Standards (Transportation Research Board, 2010), an average traffic flow in the steady-state of 700 passenger car units per hour (pcu/h) was selected as the experimental traffic flow for all scenarios.

Experimental Process

Each subject needed to be familiar with the operation of the driving simulator before starting the formal experiment. The drivers followed the vehicle in front of them and drove according to their everyday driving habits. When driving in a tunnel, overtaking was forbidden. The experimental scenarios were based on a fully balanced method that eliminated the mutual interference of the testing sequence caused by various experimental conditions. Experiments were carried out in the morning, afternoon, and evening. The experiment was carried out in a room with curtains closed and lights on to reduce the influence of light. All participants were asked to have a good sleep before the experiment to ensure that they were full of energy and good mental state.

An example of the subject sequence was as follows: Subject 1 completed driving in Scenario A; after that, the driver rested for a while and then drove the simulator in Scenarios B and C. Then, Subject 2 would drive in the sequence of Scenarios C, A, and B, while Subject 3 drives in the sequence of Scenarios A, C, and B. The rest of the 21 subjects followed the same sequence pattern of the three scenarios. The EEG data, such as α -, β -, and θ -wave energy, were collected during the experiment. Thus, all 24 subjects participated in the investigation.

DATA PREPROCESSING

Filtering and Re-referencing

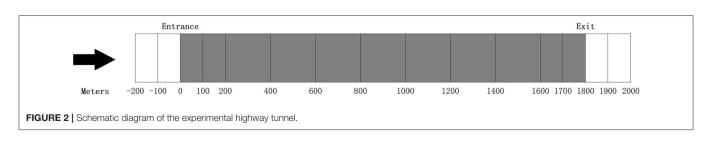
The filtering mainly filtered the useless part of the original EEG data from 32 electrode locations and included two steps. The first step was the low-pass filtering, which filtered the EEG waveform with a frequency below 0.5 Hz. The second step was the high-pass filtering, which screened the EEG waveform with a frequency above 40 Hz (i.e., this frequency is commonly used for EEG preanalysis). The re-referencing is to use the average value of EEG data on each electrode as a reference for calibration to prevent the artifacts from affecting the overall EEG data.

Independent Component Analysis Technology Denoising

The independent component analysis (ICA) is a data processing technology widely used in many fields. The ICA technology



FIGURE 3 | Schematic diagram of the internal environment of the tunnel.



is mainly used to find and remove specific EEG artifacts after filtering and re-referencing in EEGLAB.

EEG Energy Value Data Extraction

In this experiment, the data for the EEG energy value were extracted in the α , β , and θ waves, and the wave ratio $(\alpha + \theta)/\beta$.

TABLE 1 | Characteristics of three types of electroencephalogram (EEG) rhythms and a composite index.

EEG wave	Frequency (Hz)	Cognitive characteristics
α	8–13	A low-amplitude synchronous wave. The main waveform is recorded in the awake and quiet state. It is generally considered to be related to the preparation of the brain.
β	13–30	A high-frequency, low-amplitude asynchronous fast wave. It reflects the alertness state of the brain, which can be seen when nervous or excited, indicating that the cerebral cortex is in an excited state.
θ	4–8	It belongs to the low-to-medium amplitude slow wave, which appears when people calmly relax and turn to sleep. It manifests the central nervous system's inhibitory state and is related to working memory load.
Wave ratio	_a	An EEG composite index related to mental fatigue, suggesting the higher ratio, the higher the mental fatigue level.

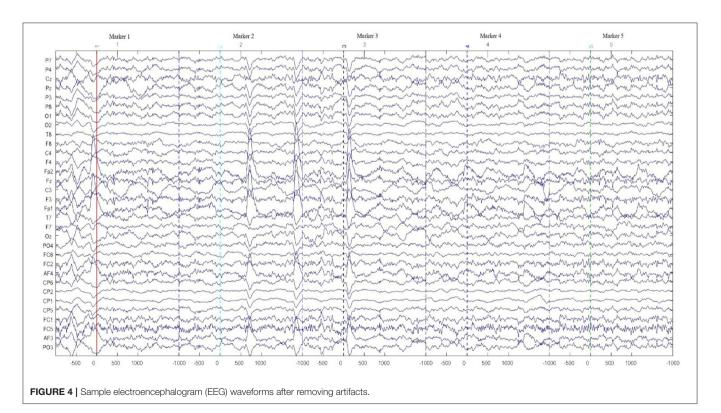
Their characteristics are presented in **Table 1**. The specific extraction process was as follows:

- (a) Export the original data from the Enobio system and import it into the EEGLAB toolbox. Perform filtering, sequencing, and ICA preprocessing to remove unwanted frequency waves and noise.
- (b) Use EEGLAB to remove the artifacts that still existed manually. The EEG signal after removing the artifacts is shown in Figure 4. Y-axis represents the 32 channels of EEG. The numbers -500, 0, 500, and 1,000 in the X-axis represent -500, 0, 500, and 1,000 ms at this marker time point. The changing lines in the figure represent the change of EEG collected from the participants. The marker 1-5 at the top of the figure refers to the time when the EEG data were collected from the participants. The markers are the specific points used to collect EEG signals in the experiment. The other six markers are not shown in the figure due to the size of the window. The markers are set every 300 m to collect the data of drivers for the first 500 ms and then 1,000 ms, adding up to 11 markers in this experiment. Then, MATLAB was used to extract the EEG energy data (μv^2), which correspond to various frequency waves, into Excel files for analysis.

RESULTS AND DISCUSSION

Analysis of Repeated Measurement of Variance

This analysis was based on the mean values of different speeds and involved Mauchly's sphericity test and the within-subject test.



^aNot applicable.

Mauchly's spherical hypothesis is used to test the autocorrelation degree of each level in a group. The repeated measures ANOVA is based on Mauchly's sphericity test of each data. If the spherical assumption is not satisfied, the Epsilon test should be used to correct the error. According to **Tables 2**, **3**, the significance of all variables was >0.05, which satisfied the spherical assumption, and thus, the Epsilon correction was not required.

The within-subject test aims to study the relationship between each dependent variable and the speed change. The withinsubject tests refer to the comparison of the mean-variance among the groups. There would be no significant difference in the mean among the groups if p > 0.05. If the statistical significance requirement is met, this proves that the speed change has a substantial effect on the dependent variable. All the indicators meet the spherical assumption. However, in terms of the speed of the assumed sphericity, only the β -wave and the wave ratio are rather significant but are still not <0.05. The indifference assumption is accepted. Although all variables in the withinsubject effects were not significant, in the tests of the withinsubject contrasts shown in **Table 4**, the significance of the β -wave

TABLE 2	Mauchly's test	t of sphericity.
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Variable (in frontal lobe)	Mauchly's W	Approx. Chi-Square	df	Sig.	Epsilon Greenhouse- Geisser
α-wave energy	0.785	2.423	2	0.298	0.823
β-wave energy	0.935	0.667	2	0.716	0.939
θ-wave energy	0.930	0.730	2	0.694	0.934
Wave ratio	0.659	4.170	2	0.124	0.746

TABLE 3 | Tests of within-subject effects.

energy and the wave ratio in the second measurement were 0.037 and 0.031, respectively, with a *p*-value <0.05. As noted, under the quadratic relationship, the β -wave energy and the wave ratio are related to the speed effect.

EEG Test Comparison During Driving

This test evaluates the significance of the changes in the EEG data during the follow-up process under a car-following situation. This test would help indicate whether the EEG data have changed significantly during the entire driving process. When the distance is 0, 100, 400, 600, 800, 1,200, 1,400, and 1,600 m, the number of contrasts is ≥ 2 , and the significance of each indicator is ≤ 0.05 , indicating that the energy value indicators are changed significantly at these positions. In general, as the driving distance changes, the changes in the EEG energy value are statistically significant. **Table 5** presents the results of the tests of contrasts of the three EEG indicators, which show the significance of the change in these indicators during the driving process.

EEG Topography in Three Following Scenarios in the Tunnel

Figure 5 shows the EEG topographic maps of the three waves for different speeds. The color in the topographic map (from yellow to dark blue) indicates the activation level of the brain wave. The bluer the color, the less active it is. Intuitively, under the scenarios of the α -wave and β -wave at 45 km/h, the blue area of the EEG topographic map is larger than that at 30 and 60 km/h, indicating that the mental state of drivers at 45 km/h is more stable than at other speeds. Notably, the depth of the color in the map represents the visualized EEG activity, which directly reflects the activity of drivers at each following speed. However, the map cannot be used for the quantitative analysis.

Variable (in frontal lobe)	Inspection type assumed	Type III sum of squares	Df	Mean	F	Sig.	Partial eta squared
Irontal lobej				squares			
α-wave energy	Sphericity	610055.9	2	305027.9	0.705	0.505	0.060
β-wave energy	Sphericity	1507640.6	2	753820.3	2.722	0.088	0.198
θ-wave energy	Sphericity	2307488.3	2	1153744.1	0.127	0.881	0.011
Wave ratio	Sphericity	0.898	2	0.449	1.865	0.179	0.145

TABLE 4 | Tests of within-subject contrasts.

Variable (in frontal lobe)	Speed	Type III sum of squares	Df	Mean square	F	Sig.	Partial eta squared
α-wave energy	Linear	252919.3	1	252919.3	0.457	0.513	0.040
	Quadratic	357136.6	1	357136.6	1.146	0.307	0.094
β-wave energy	Linear	213979.4	1	213979.4	0.663	0.433	0.057
	Quadratic	1293661.2	1	1293661.2	5.593	0.037	0.337
θ -wave energy	Linear	166878.0	1	166878.0	0.021	0.887	0.002
	Quadratic	2140610.2	1	2140610.2	0.210	0.656	0.019
Wave ratio	Linear	0.013	1	0.013	0.038	0.848	0.003
	Quadratic	0.885	1	0.885	6.102	0.031	0.357

TABLE 5	Tests of contrasts of different speeds for various driving distances.
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Variable	Speed	Comparison	Sig.	
(in frontal lobe)	(km/h)	First distance	Second distance	
α-wave	60	100	400	0.049
α-wave	60	400	600	0.048
α-wave	30	100	1,000	0.033
θ-wave	45	0	400	0.019
θ-wave	45	100	400	0.021
θ-wave	45	200	400	0.040
θ-wave	45	400	600	0.008
θ-wave	45	400	1,200	0.017
θ-wave	45	400	1,600	0.012
θ-wave	45	400	1,800	0.016
θ-wave	30	0	1,200	0.042
θ-wave	30	100	400	0.034
θ-wave	30	100	1,000	0.038
θ-wave	30	100	1,200	0.003
θ-wave	30	100	1,600	0.033
θ-wave	30	400	800	0.041
θ-wave	30	600	1,200	0.023
θ-wave	30	800	1,000	0.048
θ-wave	30	800	1,200	0.002
θ-wave	30	800	1,600	0.041
θ-wave	30	1,200	1,400	0.014
θ-wave	30	1,200	1,700	0.025
$(\alpha + \theta) / \beta$	30	0	1,200	0.034
$(\alpha + \theta) / \beta$	30	100	1,200	0.014
$(\alpha + \theta) / \beta$	30	800	1,200	0.037
$(\alpha + \theta) / \beta$	30	1,200	1,400	0.008
$(\alpha + \theta) / \beta$	30	1,200	1,600	0.036

Change in EEG Energy During Driving

The statistical analysis of the change in EEG shows the significance of the β -wave energy and the wave ratio. The second measurements are 0.037 and 0.031, respectively, with *p*-value <0.05. These results indicate that driving psychology varies for different vehicle-following conditions in the tunnel. The changes of the four EEG indicators during the driving process are described in the following. The unit of EEG wave energy is μv^2 , which represents the intensity of the three brain waves.

$\alpha\text{-Wave Energy}$ in the Frontal Lobe

The change in the α -wave energy in the frontal lobe for different driving speeds is shown in **Figure 6**. The X-axis is the distance the driver reached in the tunnel, and the Y-axis is the magnitude of the α -wave energy. As noted, as the driver drives in the tunnel, the energy value of the α -wave of the EEG decreases when the driver enters the first 100 m. When the α -wave energy decreases, the drowsiness of the driver is reduced, and the cognitive resources increase (Schier, 2000). This corresponds to the concentration of attention when entering the tunnel (Klimesch et al., 1998; Wang et al., 2015). As the driving distance increases, the α -wave

energy increases two times and also decreases two times. The first increase occurs when the driver enters the middle of the tunnel, reaching the highest point at 400 m, and during 600-800 m, the α -wave energy fell rapidly. This trend indicates the distracted and concentrated process of drivers (from distraction to concentration). Then, during the driving process, the α -wave energy increases, but it does not recover to the level at 400 m. This trend might be due to that the driver is reaching the exit of the tunnel, where the driver is relieved when driving out of the tunnel without the tension of following other cars in the tunnel. However, the driver is still concentrating along with the highway driving conditions. After the driver enters the tunnel environment, the adaptation to the tunnel environment and the process of focusing attention have kept his level of drowsiness at a low level. As the driver enters the exit of the tunnel at 1,800 m, the driving task ends. The attention level of drivers drops rapidly.

$\beta\text{-Wave Energy}$ in the Frontal Lobe

The change in the β -wave energy in the frontal lobe for different driving speeds is shown in Figure 7. The X-axis is the distance the driver reached in the tunnel, and the Y-axis is the magnitude of the β -wave energy. As noted, the β -wave energy still shows the same effect as the participants drove in the first 0-400 m, i.e., the decline-increasing process when entering the tunnel. The increase in the β -wave represents an increase in the alertness level (Eoh et al., 2005). When the driver enters the tunnel, the alertness level first decreases and then increases. This reveals a distractive pattern of the drivers who enter the tunnel. In the first 100 m, drivers are distracted (due to the pressure of the tunnel, the environment, or the changing environment). However, in the next 100 m, the drivers regain their alertness when they adapt to the tunnel environment. After 400 m, the β -wave energy (i.e., the alertness level of drivers) is the lowest at 45 km/h. Then, from 800 to 1,600 m, the β -wave energy at 45 km/h is decreased steadily in contrast to the oscillation of the other two brain wave energies at the other speeds. This indicates that after adapting to the tunnel environment, the driver is more comfortable at 45 km/h.

θ -Wave Energy in the Frontal Lobe

Figure 8 shows the change in the θ -wave energy in the frontal lobe for different driving. The θ -wave energy does not show significance in the repeated measures ANOVA. The X-axis is the distance the driver reached in the tunnel. The Y-axis is the magnitude of θ -wave energy. Its unit is μv^2 . In the contrast tests, compared with the energy of the other two speeds, the θ -wave energy value at 30 km/h had changed significantly between most of the distances. At the three speeds, the θ -wave energy value of drivers still maintained a descent-rise at 400 m at the tunnel entrance, but at 45 km/h, the fall is not apparent. At 400 m, the θ -wave energy is higher than the other two speeds. Because the driver alertness level decreased when the θ -wave energy increased (Åkerstedt et al., 1991), the driver alertness decreased at the entrance. As noted, the θ -wave energy for 30 km/h is higher than that for the other two speeds during the distance from 800 to 1,400 m, but after that, the θ -wave energy is less than that for the other speeds. This trend is similar to the α -wave energy where the θ -wave energy at 45 km/h does not recover to the level of

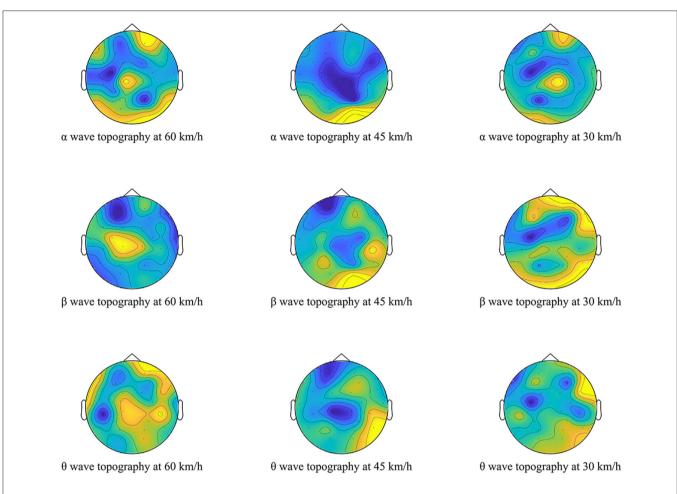
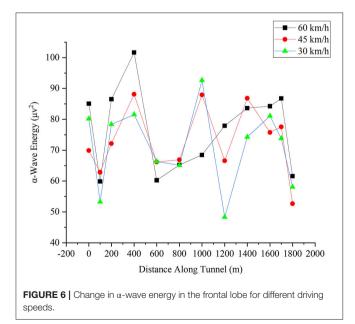
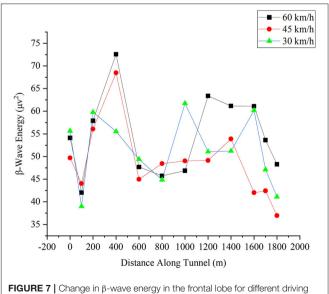


FIGURE 5 | EEG topographic maps of the three waves of drivers for different speeds.



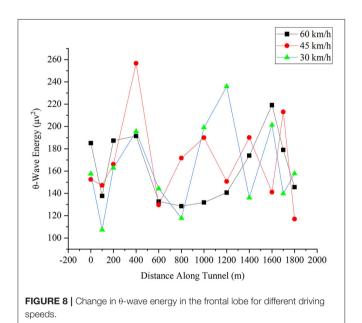


speeds.

400 m. This might also be due to the relief of drivers, as noted in the analysis of the α -wave energy. At 60 km/h, the θ -wave energy also has a descent-rise, presumably indicating that the driver is attentive to the tunnel entrance.

Wave Ratio in the Frontal Lobe

The wave ratio has been demonstrated in the repeated measures ANOVA to illustrate the significance of change with speed. **Figure 9** shows the change in the wave ratio in the frontal lobe for different driving speeds. The X-axis is the distance the driver reached in the tunnel, and the Y-axis is the magnitude of the wave

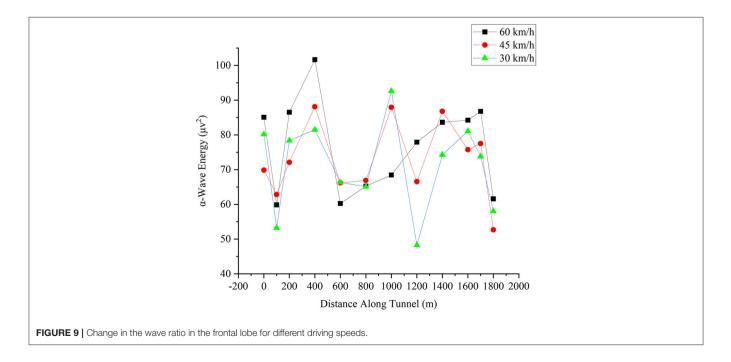


ratio. As noted, the drop-rise effect occurred during 0–200 m. From 0 to 600 m, the ratio of the three following car speeds is almost the same, but at 600 m, the ratio at 45 km/h started to rise, drops at a distance between 1,200 and 1,600 m, and then sharply rises at 1,700 m. After the jump, the ratio decreases again. After 1,200 m, the ratio for 45 km/h is in the neutral position relative to the other two speeds (although a sudden jump occurs at 1,700 m) and then returns to around 5 at the exit. The increase in the wave ratio as driver fatigue increases (Cao et al., 2014) indicates that the fatigue value for 45 km/h is generally in the neutral position during tunnel driving. The ratio is not much different from that of the other two speeds.

CONCLUSION

This study has evaluated three simulated driving scenarios in a long highway tunnel with different speeds of the front vehicle. The EEG technology was used to provide information about the dynamics and simulated electrical brain activity of subjects. Based on this study, the following comments are offered:

1. The analysis of the EEG energy data showed that the driver had the lowest alertness level and the best driving experience at 45 km/h. The wave ratio showed that the fatigue value for 45 km/h was generally in the middle and was not much different from the other two speeds. The study experiments involved a specific two-lane tunnel (i.e., one lane in each direction), which is 1,800 m long, and participants with an age range of 20–30 years. Since the tunnel length and the age of participants would affect the optimum speed of the tunnel, the preliminary finding that the 45 km/h is an appropriate speed applies only to the two-lane highway tunnels with lighting/sound and participants similar to those used in this study. Also, this finding is likely to apply to the tunnels



in China, which exhibit similar conditions and may not be transferrable to other countries.

- 2. The results showed that the EEG energy of drivers had a falling-rising effect during tunnel driving. Since the environmental illuminance of the experiment was controlled, there was no interference in the dark adaptation process in vision. The analysis of the α , β , and θ waves revealed a similar effect in the EEG index when driving in the middle and the rear end of the tunnel. Researchers have recently studied the sustained attention and the attention behavior in distracted driving (Wang et al., 2013; Pallavi and Harish, 2016; Ding et al., 2019; Karran et al., 2019), especially the reduction and oscillations of the α -wave energy and the increase in the θ wave energy (Klimesch et al., 1998; Wang et al., 2015). It could be speculated that the trends of these wave energies were related to the attention-concentration behavior of drivers during tunnel driving.
- 3. The results of the study showed different psychological reactions of drivers at different speeds. For the three speeds of 60, 45, and 30 km/h, the drivers had a better driving experience at a moderate speed (i.e., 45 km/h) when following the front car. A falling-rising effect on the three brain waves was also found. This finding might contribute to the analysis of driving behavior in the tunnel using physiological indicators. Furthermore, the conclusion of this study may help set the index weight when modeling the car-following behavior from the psychological state of drivers. Also, the finding might strengthen the inference and analysis of the motivation and mechanism of lousy behavior of drivers and might provide a theoretical basis for the prevention of tunnel traffic accidents.
- 4. This study has some limitations. The error of the EEG data process was relatively large, and the test scene was too restrictive. In addition, it was necessary to study the speed variable only due to the experimental conditions. Future studies might consider more complex driving scenarios involving a broader selection of speeds and various physiological indicators, such as ECG and skin electricity, which can be combined to study driver behavior more comprehensively. In addition, the effect of different tunnel lighting and noise levels can be explored.

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DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/supplementary material, further inquiries can be directed to the corresponding author/s.

ETHICS STATEMENT

The studies involving human participants were reviewed and approved by Committee of Department of Civil Engineering, Fuzhou University. The patients/participants provided their written informed consent to participate in this study. Written informed consent was obtained from the individual(s) for the publication of any potentially identifiable images or data included in this article.

AUTHOR CONTRIBUTIONS

YY and YF contributed to the study conception and design. YF performed the data collection. YY, YF, XZ, and SE contributed to the analysis and interpretation of results. YF, XZ, and SE prepared and drafted the manuscript. All authors reviewed the results and approved the final version of the manuscript.

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