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Objective Activity Parameters Track Patient-specific Physical Recovery Trajectories After Surgery and Link With Individual Preoperative Immune States

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Objective: The longitudinal assessment of physical function with high temporal resolution at a scalable and objective level in patients recovering from surgery is highly desirable to understand the biological and clinical factors that drive the clinical outcome. However, physical recovery from surgery itself remains poorly defined and the utility of wearable technologies to study recovery after surgery has not been established.

Background: Prolonged postoperative recovery is often associated with long-lasting impairment of physical, mental, and social functions. Although phenotypical and clinical patient characteristics account for some variation of individual recovery trajectories, biological differences likely play a major role. Specifically, patient-specific immune states have been linked to prolonged physical impairment after surgery. However, current methods of quantifying physical recovery lack patient specificity and objectivity.

Methods: Here, a combined high-fidelity accelerometry and state-of-theart deep immune profiling approach was studied in patients undergoing major joint replacement surgery. The aim was to determine whether objective physical parameters derived from accelerometry data can accurately track patient-specific physical recovery profiles (suggestive of a 'clock of postoperative recovery'), compare the performance of derived parameters with benchmark metrics including step count, and link individual recovery profiles with patients' preoperative immune state.

Results: The results of our models indicate that patient-specific temporal patterns of physical function can be derived with a precision superior to benchmark metrics. Notably, 6 distinct domains of physical function and sleep are identified to represent the objective temporal patterns: "activity capacity" and "moderate and overall activity (declined immediately after surgery); "sleep disruption and sedentary activity (increased after surgery);

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"overall sleep", "sleep onset", and "light activity" (no clear changes were observed after surgery). These patterns can be linked to individual patients preopera-tive immune state using cross-validated canonical-correlation analysis. Importantly, the pSTAT3 signal activity in monocytic myeloidderived suppressor cells predicted a slower recovery.

Conclusions: Accelerometry-based recovery trajectories are scalable and objective outcomes to study patient-specific factors that drive physical recovery.

Keywords: machine learning, mass cytometry, surgery, surgical recovery, wearable activity recognition

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C urrently, more than 300 million surgeries are performed annually worldwide.¹ Recovery after surgery is highly variable, and protracted recovery affects up to 30% of patients, leading to personal suffering, impaired daily function, delayed return to work, and major socioeconomic costs.^{2–4} Although rapid advances in surgical and perioperative care have significantly shortened hospital length of stay, surgical recovery far exceeds the hospitalization period.^{5,6} From a patient's perspective, recovery includes the return to preoperative levels of independence and well-being.⁷ As such, studying the entire surgical recovery process, which can last weeks to months, is logistically challenging, resource-intense, and largely contingent on subjective data typically obtained with questionnaires.^{8–11} Additional concerns regarding subjective data

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include reporting biases and limited reliability.¹² For example, selfreported physical performance metrics are imprecise as they both, under and overestimate activity when compared to objective metrics.^{12,13} Finally, a large-scale study conducted in 6 countries comparing subjective and survey-based physical activity metrics to sensor-based metrics of physical activity that measured time spent in sedentary behavior and specific intensity levels of physical activity (light, moderate, and vigorous), indicated a large discordance between self-reported and sensor-based outcomes.¹³

One sentinel recovery outcome after surgery is physical function, which is likely to impact other domains of recovery. The scalable, low-cost, objective, remote, and continuous assessment of physical function over extended periods of time is highly desirable to understand mechanisms that improve, or conversely, impede physical function. As such, the application of sensing technologies included in wearable devices for monitoring of physical function is rapidly emerging in different clinical domains including inpatient rehabilitation, sleep, geriatric, and feto-maternal medicine.¹⁴⁻¹⁶ However, the utility of wearable technologies to study recovery after surgery has not been established.

The role of the immune system in determining recovery in patients suffering from trauma including major surgery is prominent.^{17–19} Mass cytometry,²⁰ a recent breakthrough technology for highly parameterized single-cell immune profiling has rapidly been adopted in different clinical settings including vaccine development,²¹ feto-maternal health,^{22,23} oncology and immunotherapy.²⁴ More recently, mass cytometry has been used in perioperative medicine, by our group, to study how a patient's preoperative immune state and immune responses to surgery determine clinical recovery trajectories (derived from self-reported measurements).^{19,25} Evidence from these important and resource-intense but limited-sized studies suggests that patient-specific differences in immune cell signaling responses are strongly associated with the rate at which patients regain physical function after surgery.

Here, a novel patient-centric computational approach is presented that leverages wearable acceleration data and highparameter functional immune profiling to (1) objectively quantify the temporal pattern of physical recovery in individual patients (suggestive of a 'clock of postoperative recovery' indicating time to return to their preoperative state), and (2) link such recovery patterns to individual patients' preoperative immune states. Integration of accelerometry and biological data is a novel and personalized framework to identify biological factors that drive physical recovery. The outlined approach, once validated, can be scaled to larger and more diverse surgical cohorts with the final goal to advance physical recovery in a personalized and preemptive fashion.

METHODS

Clinical Study Design

Patients undergoing primary hip arthroplasty were recruited at the Arthritis and Joint Replacement Clinic of the Department of Orthopedic Surgery at Stanford University School of Medicine (see "CONSORT Chart" and "Study Materials" in Supplemental Digital Content, http://links.lww.com/SLA/D476). The study was approved by the Institutional Review Board of Stanford University. Seventy-five patients were enrolled after providing written informed consent. Fifty-three patients completed the study and 49 patients provided accel-erometry data suitable for analysis (Table 1). Refer to "Study Materials" in Supplemental Digital Content for the exclusion criteria.

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Demographics and presurgical clinical characteristics	
Sex (male/female)	23/26
Age (yrs; median & IQR)	63 (57-68)
Body mass index (kg/m ² ; median & IQR)	26.7 (24.2–30.5)
Race/ethnicity	· · · · ·
African American	1
Asian	2
White	42
Unknown	4
Cumulative Illness Rating Scale (0–56; median &	10 (7-12)
IQR)	
Beck Depression Inventory (0–63; median & IQR)	7 (5–14)
Profile of Moods Anxiety Scale (0-36; median & IQR	7 (3–11)
10-time Stress Scale (0–40; median & IQR)	12 (6–18)
36-item Short Form Health Survey (median & IQR)	
Physical component summary score (15.0-61.7)	33.9 (30.0–38.0)
Mental component summary score (7.4-65.6)	42.7 (35.9–52.8)
Surgical Recovery Scale (17–100; median & IQR)	63.7 (54.1–72.6)
Western Ontario and McMaster Universities	
Osteoarthritis Index (median & IQR)	
Hip pain (0–40)	21.5 (15.5–28.5)
Hip function (0–60)	32.5 (23.0-42.0)
Hip Disability and Osteoarthritis Outcomes Score (0-	-100; median &
IQR)	
Pain	45.0 (32.5–52.5)
Symptom	35.0 (20.0-50.0)
Activity of daily living	50.0 (32.0-60.0)
Sport	18.8 (6.3–31.3)
Quality of life	19.0 (6.0–31.0)
Anesthesia and surgery	
ASA class (1–5; median & IQR)	2 (2–3)
Anesthetic technique	
General & neuraxial	30
General	10
Neuraxial	9
Times (min; median & IQR)	102 (01 112)
Surgery	102 (81–113)
Anesthesia	183 (158–198)
Postanestnesia care unit	103(82-148)
Blood loss (mL; median & IQR)	300(200-300)
Intraoperative fluids (mL; median & IQR)	1500 (1000-2000)
IOR)*	1.3 (3.4–12.0)
Time to discharge (days; median & IQR)	2.1 (2.0-2.9)
*Intravenous hydromorphone equivalent. ASA indicates American Society of Anesthesiology; IQR	k, i nterquartile range

Accelerometry for Measurement of Physical Activity and Sleep Patterns

Physical activity and sleep patterns of each participant were collected via an ActiGraph smartwatch (ActiGraph, LLC, FL) continuously worn on the wrist of the dominant arm starting 5 days before surgery and ending 40 days after surgery (Fig. 1A). Two patients wore the watch on the nondominant wrist. The 3-dimen-sional acceleration data were sampled at 30 Hz, which produced about 350 million acceleration measurements per patient. A broad array of algorithms extracted time-series attributes (or features) representing various aspects of daily physical activity (eg, step counts, energy expenditure, and time spent at various physical activity levels) and sleep features. For example, the Cole-Kripke algorithm²⁶ and the Freedson algorithm²⁷ were used for deriving sleep and energy expenditure features, respectively. A complete list of features is provided in Supplemental Digital Content Table 1, http://links.lww.com/



FIGURE 1. Study overview and analytical approach. Forty-nine patients undergoing hip replacement surgery were included in the analysis. (A) Patients were instructed to wear a clinical grade motion sensing smart-watch continuously on their wrist for 5 days before and for 40 days after surgery to monitor physical activity and sleep patterns. (B) Whole blood samples were obtained from each patient 1 hour before surgery for analysis with mass cytometry to determine immune cell-type specific signaling activities at baseline and in response to ex vivo stimulation with the receptor-specific ligands granulocyte-macrophage colony-stimulating factor (GMCSF), interferon alpha (IFN- α), interleukins 2, 4, and 6 (IL), lipopolysaccharide (LPS), and a mixture of phorbol 12-myristate 13-acetate and ionomycin (PI). (C) An antibody-based proteomic platform was used for measuring 1012 proteins in plasma of the same samples. (D) Patient-specific daily activity and sleep patterns adjusted to preoperative metrics were used for inferring model parameters reflecting the rate of recovery, ie, the time to return to preoperative states. Correlation networks were built for (E) mass cytometry and (F) proteomic data sets. (G) The feature sets presented in the correlation networks trained multivariate models predicting the rate of recovery based on patients' preoperative immune and proteomic states.

SLA/D476. ActiGraph's actigraphy data analysis software platform ActiLife v6.13.3 was used for the purpose of feature extraction. Missing values were imputed using a 2-Nearest Neighbors imputation approach. The resulting multifaceted array of daily physical health attributes was used to derive patient-specific recovery trajectories and infer rates of recovery surrogates (Fig. 1D).

Single-cell Immune Profiling

To comprehensively characterize a patient's preoperative immune state, plasma and whole blood samples were collected 1 hour before surgery for analyses with a highly multiplexed proteomic platform and single-cell mass cytometry (Fig. 1B and C). Proteomics and immunome data from 35 patients passed quality control standards. These 2 platforms were used in combination with objective physical recovery surrogates to elucidate baseline proteomic and immunological features associated with the rate of physical recovery (Fig. 1E-G).

Blood for proteomic analysis was collected in ethylenediamine tetraacetic acid tubes, placed on ice, double-spun within 60 minutes and stored at -80° C until further analysis. The proteomic analysis was performed by Olink Proteomics Inc. (Watertown, MA) with a highly multiplex platform using proximity extension technol-ogy.²⁸ For this study, 11 panels were used, each measuring 92 different proteins simultaneously in 1 µL of plasma. Each protein was detected by a matched pair of antibodies that were coupled to unique and partially complementary oligonucleotides. When in close proximity, a new and protein-specific DNA reporter sequence was formed by hybridization and extension, which was then amplified and quantified by real-time polymerase chain reaction.²⁹ Quality metrics were as follows: 538 of 539 plasma samples passed, 865 of 1012 proteins were detected, and the median intraassay coefficient of variation was 8%.³⁰

Blood collected for mass cytometry analysis was processed within 30 minutes after blood draw. Individual aliquots were stimulated with 5 receptor-specific ligands [ie, granulocyte-macrophage colony-stimulating factor, interferon (IFN)-α, lipopolysaccharide, a mixture of interleukins (IL)-2, IL-4, and IL-6, and phorbol 12-myristate 13-acetate and ionomycin]. A 46-parameter mass cytometry assay (Supplemental Digital Content Table 2, http://links.lww.com/SLA/D476) was used to analyze the distribution and intracellular signaling activities of 28 major innate and adaptive immune cell subsets (Fig. 1B and E, Supplemental Digital Content Figure 2, http:// links.lww.com/SLA/D476). Intracellular mass cytometry parameters were chosen to capture important cell signaling pathways known to be activated in innate or adaptive immune cells after surgery (including JAK/STAT, P38MAPK, and NFkB signaling pathways).^{18,31} Refer to "Study Materials" in Supplemental Digital Content for more details on mass cytometry analysis.



FIGURE 2. Accelerometer signal processing and feature extraction. (A) Depicted is the average normalized (I2 norm) vector magnitude of high-fidelity 3-dimensional acceleration measurements recorded over distinct 24-hour periods. Color-coded lines track the signal magnitude at different postoperative days. (B) The correlation network of relevant activity and sleep parameters (nodes) reveals distinct components derived by applying an unsupervised clustering algorithm (kMeans). Major components of the network included moderate and overall activity (orange), activity capacity (blue), light activity (yellow), overall sleep attributes (ocean green), sleep onset (lawn green), and sleep disruption overlapping with sedentary activity (pink). Node sizes indicate the strength of the correlation between a parameter and the number of days after surgery. The edges indicate statistical significance (P < 0.01, Spearman correlation). (C) Shown is the average magnitude for each component over the course of the observation period starting 5 days before and ending 40 days after surgery. The color code is identical with (B), shaded areas mark the 90% confidence intervals, the horizontal grey line indicates the average before surgery, and the vertical grey line indicates the day of surgery.

RESULTS

An Accelerometry-based Clock of Postoperative Recovery

Tridimensional acceleration data were collected continuously in 49 patients wearing a clinical-grade ActiGraph smartwatch (Acti-Graph GT9X Link, LLC, FL) starting 5 days before and ending 40 days after surgery. The average 12 normalized vector magnitude of the 3-dimensional data is depicted over time in Figure 1A. Each spike represents a 24-hour cycle with peak and trough activities. Magnifications of a 24-hour cycle at different postoperative days is shown in Figure 2A. Physical activity generally began increasing at 6 AM and started decreasing at 6 PM reaching trough levels close to midnight. Peak and plateau activity levels continuously increased over the course of the 40-day postoperative observation period. Although there were considerable interpersonal variations in the human physical patterns after surgery, an evident steep decline followed by a gradual return in overall activity is the dominant pattern (Fig. 2A and C). Exceptions included light and sedentary activity, which were increased, and substantial disruption is the onset of sleep.

Several functional aspects were captured by the wearable sensors including a range of physical activity parameters (eg, intensity, periods of activity, daily activity capacity, estimates of step count, estimates of caloric intake) and sleep patterns (eg, sleep fragmentation index, sleep onset, number of awakenings). Developing time-series signal processing algorithms that extract acceleration-based functional parameters is a high-yield current research emphasis. Various algorithms were applied to extract 62 temporal physical and sleep features from the current dataset. Using a static sliding window of 24 hours, daily feature vectors were derived for each patient. The sliding window approach is a common high level feature extraction method in time series physical activity monitoring.^{32,33} To facilitate the optimization algorithm and reduce the adverse effects of outliers, a 0 mean unit variance standard scaler was built on each of the preoperative data feature vectors. The scalers were then applied to the entire corresponding feature vector, independent of the other feature vectors. A correlation graph displays the complex interconnectivity of the 62 features (Fig. 2B). Each node represents 1 feature and edges indicate a significant pairwise statistical correlation (P < 0.01) between nodes.

An unsupervised k-means clustering algorithm was used to objectively identify distinct components of highly correlated features. Six distinct components or domains were identified and labeled based on the included features: overall sleep, sleep onset, sleep disruption and sedentary activity, light activity, moderate and overall activity, and activity capacity (Fig. 2B). The time course of the average magnitude of the 6 domains is shown in Figure 2C. Each domain followed a unique temporal pattern. Importantly, the domains "moderate and overall activity" and "activity capacity" sharply declined immediately after surgery and then gradually returned to preoperative levels over the course of weeks. In contrast, the domains "sleep disruption and sedentary activity" increased moderately after surgery and gradually returned to preoperative levels. This is consistent with observed decrease in "moderate and overall activity" and "activity capacity". Although the domains "light activity" and "sleep onset" decreased after surgery, no clear temporal patterns were observed. Finally, the domain "overall sleep" did not noticeably change after surgery.

Inferring Patient-specific Trajectories of Recovery

To quantify physical recovery patterns after surgery, the temporal postoperative accelerometry data were used to build a patient-specific model, predicting the number of 'days since surgery'. A supervised model was trained on the feature matrix of each individual patient, independently. The feature matrix consisted of 62 feature vectors of medium to high-level patient physical attributes characterizing each postoperative day as the target variable. The Random Forest (RF) regression algorithm³⁴ was used because of the continuity of the output variable and the highly interrelated nature of the feature vectors. RF is a robust ensemble method that allows for relatively easy interpretation of the results, leverages the specificity and nonlinearity of the tree-

based approaches, and takes advantage of the generalization and robustness of ensemble methods. For each patient, a RF model was trained to infer time since surgery using the patient-specific feature matrix (as previously visualized in Fig. 2B). The repeated k-fold cross-validation showed high performance of the patient-specific RF model predicting 'days since surgery' (P < 0.05) with median prediction P values of 5.9×10^{-7} (Fig. 3A, Supplemental Digital Content Figure 3, http://links.lww.com/SLA/D476). Refer to the section "Modeling and Analysis" in Supplemental Digital Content for details regarding model training and evaluation.

The performance of RF models varied between patients with a median Root Mean Square Error of ~8days when estimating the 'day since surgery' (Fig. 3B). Importantly, the multivariate model (shown in pink) was compared against univariate models using a single accelerometry feature as provided by the manufacturer for training the RF predictor. Six univariate models are shown in Figure 3B for manufacturer provided features (1) total steps taken in a day (24-hour period), (2) estimated daily metabolic equivalent of task, (3) number of awakening episodes detected during a patient's sleep in 1 day, (4) duration of time spent performing light activities, (5) onset of bedtime for a given day, and (6) total of activity counts (measured by Freedson algorithm) detected during sleep intervals for 1 day. The performance comparisons of all univariate models are shown in Supplemental Digital Content Figure 4, http://links. lww.com/SLA/D476. Importantly, the multivariate RF models were clearly superior to the univariate models using a single accelerometry feature. As an additional control, the preoperative baseline data (before the grey dashed line) were fed into the models to predict a postoperative day. Data were normalized to baseline to ascertain within-subject control given uncertainties regarding the accuracy of absolute accelerometry metrics. This analysis demonstrated that the model's inference on the baseline (preoperative) data points ranges more than 21 days after surgery. Interestingly, this observation independently confirms the sanity of the RF models.

Figure 3C highlights the relative contribution of the 62 accelerometry features used to derive the RF model predicting 'days since surgery'. The color intensity is indicative of relative importance of each node computed using Gini importance.³⁵ Features in the domains 'Activity Capacity' and 'Sleep Disruption and Sedentary Activity' ranked highest followed by the features in the domains 'Moderate and Overall Activity', 'Overall Sleep', and 'Light Activity'.

An array of recovery surrogates for each patient was devised such that it quantifies the patient's recovery trajectory with respect to each accelerometry feature. The accelerometry data collected for 5 days preceding surgery (ie, the baseline accelerometry feature vectors) were inputted into the personalized RF models to estimate days after surgery. Note that the baseline inferences are made by models trained solely on postoperative data. The models use the temporal patterns learned from postoperative data to infer the time point along the postoperative timeline that most closely matches baseline patterns. The RF inference on preoperative data will reveal the day after surgery that is closest to a patient's preoperative state. Based on this, an array of 62 recovery surrogates (corresponding to 62 accelerometry features) is constructed. Each element of this array (ie, 1 recovery surrogate) indicates the earliest time that the postoperative feature value returns to the patient's baseline levels. The smaller the surrogate, the faster a patient is returning to his/her preoperative physical status (as inferred from the corresponding accelerometry feature). The detailed formulation of



FIGURE 3. An accelerometry clock of recovery from surgery. (A) The patient-specific correlated accelerometry network of temporal physical activity and sleep quality features was used to predict 'days since surgery' (Spearman $\rho = 0.7$, $P = 5.9 \times 10^{-7}$, cross validation). The model predictions versus ground truth 'Day since surgery' is plotted. Personalized model predictions are shown in grey (n = 49). The mean predictions and 90% confidence intervals are shown in red. The vertical dashed line indicates the day of surgery. (B) The multivariate clock of recovery in (A) is compared against univariate models using metrics provided by the manufacturer. The y axis depicts the median Root Mean Square Error and the black line atop each bar depicts the 90% Cl. (C) The correlated accelerometry network shows the major domains of accelerometry-derived attributes (daily sleep and activity). The color of the nodes corresponds to the relative contribution of each component to the cross-validated model predicting 'days since surgery' (ie, gini importance). The darker shades indicate higher importance.

recovery surrogates is presented in "Modeling and Analysis" section in Supplemental Digital Content, http://links.lww.com/SLA/D476.

Association of Accelerometry-based Recovery Surrogates With Self-reported Outcomes

Self-reported outcomes were captured before surgery, on postoperative days 1 to 3, bi-weekly after discharge for postoperative weeks 1 to 4, and weekly for postoperative weeks 5 to 6. The surgical recovery scale (SRS) and an adapted version of the Western Ontario and McMaster Universities Osteoarthritis Index, 2 extensively validated questionnaires, were used to assess general fatigue and resulting functional impairment, and pain and function of the operated lower extremity.^{19,36,37} The patientspecific area under the curve was derived for each longitudinal self-reported outcome. Refer to "Study Materials" in Supplemental Digital Content for a detailed description of self-reported outcome tools. As shown in Figure 4, the univariate analysis revealed a significant correlation between the SRS and recovery surrogates derived from the proposed clock of postoperative recovery (P < 0.003).

Preoperative Immune States are Associated With Physical Recovery Trajectories

A total of 1848 mass cytometry immune features were extracted from blood samples collected before surgery. These included endogenous intracellular activities of 28 innate and adaptive immune cell subsets and their capacity to respond to the 5 external ligands. The immunological dataset formed a complex network of cell type-specific frequencies and signaling activities, which highlight the interconnectivity of the immune system (Fig. 5A). In parallel, the concentrations of 1008 plasma proteins were measured. The assay quantifies proteins over a wide dynamic range as normalized protein expression values, which is unit less number derived on a \log_2 scale that is proportional to relative plasma concentrations. Similar to the immunological parameters, proteins built a complex correlational network (Fig. 5B), which is annotated by gene ontology terms as provided by Olink Proteomics Inc. (Water-town, MA). The resulting immunome datasets are original and have not been reported previously.

To determine whether patients' preoperative immune and proteomic states could predict their physical recovery surrogates, canonical-correlation analysis (CCA) models were trained to reveal linear associations between the physical recovery

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Correlation with clinical outcomes

FIGURE 4. Correlation with self-reported clinical outcomes. The univariate correlation (Spearman) between patients' objective physical recovery trajectory, and questionnaire-based subjective outcomes including fatigue (SRS), pain and function of the operated limb (WOMAC), and comorbidity burden (index) are shown. Fatigue and physical recovery trajectories correlated significantly (P < 0.003).

surrogates and the correlated immune or proteomic network parameters. To improve robustness, a leave-one-out cross validation algorithm was used, so that the results are predictions derived in patients not included when training the model. Refer to "Modeling and Analysis" in Supplemental Digital Content, http://links.lww.com/SLA/D476 for detailed discussion of CCA training and evaluation. Immune network parameters predicted physical recovery surrogates of individual patients (P < 0.01), whereas proteomic network parameters were not predictive (P = 0.69) as shown in Figure 5C and D.

Examination of the most informative immune model features (top 10% of ranked model features considering absolute coefficient) revealed intracellular signaling responses that were reminiscent of prior studies linking patients' immune response to surgery to their recovery.¹⁹ Notably, the phosphor-(p)-STAT3 signal in monocytic myeloid-derived suppressor cells (M-MDSCs) in response to IL-2/4/6 stimulation with IL-2/4/6 positively correlated with slower physical recovery. Notably, among the 184 most informative model features, 89.6% (165 features) were negatively correlated with the physical recovery surrogate (Supplemental Digital Content Table 3, http://links.lww.com/ SLA/D476). Importantly, the pSTAT1 and pSTAT3 responses to IFN-a stimulation in CD4T, NK, and memory B cells were negatively correlated, ie, associated with slower physical recovery.

To gain a better understanding of the correlations between specific accelerometry and immune features, additional statistical analyses considered each accelerometry feature independently (Supplemental Digital Content Figure 5, http://links.lww.com/ SLA/D476). Inspection of the bipartite correlation between immunological and accelerometry networks (Supplemental Digital Content Figure 5A, http://links.lww.com/SLA/D476) revealed additional interconnected immunological and physical recovery parameters that change concordantly. Significant correlations were highlighted between the accelerometry and immune features using graph edges. As shown in Supplemental Digital Content Figure 5B, http://links.lww.com/SLA/D476, this analysis confirmed several significant correlations between pSTAT1 response to IFN-a stimulation in NK cells and CD4T cells and the "moderate and overall activity", and "activity capacity" domains.

DISCUSSION

Our results indicate that wearable technologies enable the objective, scalable, and longitudinal tracking of individual patient's physical recovery after surgery. Notably, the machinelearning centered approach anchored in multivariate vector analysis offered significantly improved accuracy compared to benchmark metrics provided by manufacturers such as step count. Importantly, individual physical recovery trajectories were linked to patient-specific immune states before surgery. These findings suggest that accelerometry can be adopted as an affordable and scalable technology to track individual patient's physical recovery over time and link it to presurgical biological and other attributes that drive such recovery. Such insight is valuable for risk stratification and interventional strategies facilitating patients' physical recovery.

Six distinct groups of physical activity and sleep monitoring represented domains of surgical recovery. Each domain followed a unique temporal pattern. Each domain pattern indicated a noticeable disruption at the time of surgery with the exception of "Overall Sleep" domain. Features in the domains 'Activity Capacity' and 'Sleep Disruption and Sedentary Activity' were found the most informative in prediction of time after surgery and demonstrated larger univariate correlation with recovery surrogates followed by features in the domains 'Moderate and Overall Activity'. Importantly, the highly informative "Activity Capacity" domain is supported by previous studies of using submaximal capacity parameters such as "5-Chair Stand and Timed Up and Go" in assessment of physical performance and surgical recovery.³⁸ This result warrants studying similar physical performance attributes in a continuous and pervasive fashion.

The proposed recovery surrogates derived from the wearable data demonstrated a significant correlation with the self-reported SRS. The SRS is specifically designed to capture surgical recovery as it measures attributes of fatigue and



FIGURE 5. Preoperative immune parameters predict patient-specific physical recovery trajectories. (A) The immune correlation network within and across various features is color-coded to reflect cellular phenotypical and functional basal conditions and cellular responses to ex-vivo stimulation with different ligands including granulocyte-macrophage colony-stimulating factor (GMCSF), interferon alpha (IFN- α), interleukins (IL)-2, -4, and -6, lipopolysaccharide (LPS), and a mixture of phorbol 12-myristate 13-acetate (PMA), ionomycin (PI). (B) The proteomic correlation network is colored by gene ontology terms. (C) Preoperative immune network parameters predict physical recovery trajectories (R = 0.46, $P = 5.2 \times 10^{-3}$). The shaded area denotes the 90% confidence interval of the regression line (solid black). (D) Preoperative proteomic network parameters were not predictive.

resulting functional consequences on daily activities in surgical patients.^{36,39} The SRS is sensitive to change and correlates with course and severity of postoperative complications.^{19,40} Importantly, this result provides validation that the accelerometry derived surrogates resonate with a relevant patient reported outcome.

The CCA revealed immune correlates of clinical recovery that echoed findings of previous studies.^{18,31} Importantly, the pSTAT3 signal activity in M-MDSCs predicted a slower recovery. M-MDSCs are a monocyte subset with suppressive capacity that expand in the context of certain malignancies, sepsis, and traumatic injury.^{41,43} Prior in vitro and in vivo studies suggest that STAT3 is an essential transcription factor for M-MDSCs to suppress the proliferation and function of CD4T cells and other immune cells, including NK cells.⁴⁴ In the context of surgery, our group previously showed that the pSTAT3 signal in M-MDSCs strongly correlated with prolonged postoperative functional recovery.¹⁹ As such, the derived recovery surrogates can reveal biological determinants of surgical recovery.

Additional analysis in Supplemental Digital Content Figure 5, http://links.lww.com/SLA/D476 revealed negative correlations between preoperative adaptive immune responses and the rate of postoperative recovery. They included the STAT1 and STAT6 signaling responses to IFN-a in B and CD4T cell subsets (particularly related to "moderate and overall activity" and "activity capacity" domains). Type I IFN-a stimulation lowers the threshold for adaptive cell activation, especially by inducing up-regulation of CD69, CD86, and CD25 receptors.⁴⁵ Interestingly, adaptive cells such as B and T cells are well described as being key elements in bone^{46,47} and wound healing.⁴⁸ They also included the STAT1 response to IFN-a stimulation in NK cells. Taken together, the results suggest that preopera-tive immune states characterized by increased JAK/ STAT signaling in B cell, CD4+T cell, and NK cell and decreased JAK/STAT signaling in M-MDSC JAK/STAT benefit patients' physical recovery trajectory. An important next step is to examine whether selective modulation of the JAK/STAT signaling pathways before surgery can accelerate physical recovery.

This study has several limitations. Although the models were cross-validated and tested on previously unseen patients, the relatively small sample size limits the generalizability of our results. As such, larger studies are required to independently validate our results and test the boundaries of their generalizability. The study was conducted in patients undergoing major joint replacement surgery. As such, larger studies are likely needed to develop models general-izable across, or specific to, various surgery types. Finally, the preoperative period was limited to only 1 week. We note that data during this week before surgery are likely impacted by pain and impairment and do not represent baseline activity levels of cohort not suffering from osteoarthritis. However, a post-hoc analysis demonstrated that our results were not confounded by preoperative activity levels (Supplemental Digital Content Figure 6, http://links.lww.com/ SLA/D476).

Taken together, to the best of our knowledge this is the first study to combine wearable technologies, machine learning approaches, and state-of-the-art immune monitoring to describe patient-specific physical recovery trajectories that outperform benchmark metrics and provide insight into biology that may drive important aspects of postoperative recovery. The outlined strategy is scalable and therefore amenable for implementation in larger scale studies providing more detailed and generalizable insight into peri-operative patient factors that drive clinical recovery.

Reproducibility and Data Availability

Data and source codes for reproduction of the results are publicly available at https://github.com/raminfl/hipval. Acti-Graph's actigraphy data analysis software platform ActiLife v6.13.3 can be downloaded from https://actigraphcorp.com/ actilife/.

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