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Potency and Stability of Intradermal Capsaicin: Implications for Use as a Human Model of Pain in Multicenter Clinical Trials

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Abstract

Intradermally injected capsaicin has been used extensively both as a human pain model and to assess analgesic efficacy. Factors such as dose, formulation, route, and site are known to affect its sensitivity. We determined whether potency and stability of capsaicin solutions were further sources of variability when following strict manufacturing guidelines. Capsaicin solution (1.0 mg/mL) was prepared according to Current Good Manufacturing Practice (cGMP) guidelines and aseptically filled into sterile amber borosilicate vials and stored at 5°C, 25°C, and 30°C. All samples were analyzed at one, three, six, and twelve months. Chemical stability was determined using HPLC and physical stability was evaluated by visual inspection of color changes, clarity, particulate matter, and product/ container closure abnormalities during each sampling time. Capsaicin intradermal injection was found to be sterile and retained 95% of the initial concentration for at least one year, regardless of studied storage temperatures ($P < 0.0001$). Visual inspection indicated no changes in color, clarity, particulate matter, and product/ container closure abnormalities in all samples. These data show that capsaicin solutions (1.0 mg/mL) maintain their potency and stability over one year when manufactured according to cGMP guidelines. These

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results suggest that in clinical trials manufacturing of capsaicin solutions is recommended over extemporaneous compounding.

Keywords

Capsaicin; Human pain model; Intradermal; Variability; Manufacture

Introduction

Inflammatory substances, such as capsaicin, have been used experimentally to measure clinical pain dimensions of hyperalgesia and allodynia, characteristics of central sensitization [1-5]. Following intradermal and topical application, capsaicin binds to the vanilloid receptor VR-1 and initiates nociceptive C-fiber activity [6,7]. Within a period of seconds to minutes enhanced cutaneous sensitivity (punctuate hyperalgesia and dynamic allodynia) develop beyond the region of initial pain and characterize alterations in central nervous system activity called central sensitization.

Capsaicin-induced cutaneous sensitivity has been observed in a number of painful conditions, including post herpetic neuralgia [8], complex regional pain syndrome [9], fibromyalgia [10,11], rheumatoid arthritis [12], vulvodynia [13], unilateral sciatica [14], and multiple chemical sensitivity [15]. These disorders may represent a common dysfunction in central processing of pain stimuli [16]. Thus, capsaicin may represent an important aid in the study of pain mechanisms and to demonstrate the analgesic potential of new compounds.

However, the sensitivity of capsaicin models has been limited by significant variability in measuring allodynia and hyperalgesia. Capsaicin sensitivity has been shown to be influenced by skin temperature [2,17], arm dominance [18,19], limb position [18] and site of injection [17,18]. More recent studies show that administration route [17-19], dose [1,4,19-21], and formulation [18] also produce variability. Methods that insure uniformity are crucial to the understanding of pain mechanisms and for evaluating analgesic efficacy.

The intradermal route of administration is most commonly used in pain studies and has more consistent effects on allodynia and hyperalgesia than topical application [17]. The enhanced reliability of intradermal administration is most likely due to the dose dependent effects of capsaicin, where the magnitude and duration of pain have been shown to have a linear relationship from 1 to 100 μg [4]. At present, only two studies have evaluated the potency and stability of stored capsaicin solutions, even though these factors may directly affect capsaicin concentrations. In these studies by the same research laboratory, very low concentrations of capsaicin were prepared to study cough reactivity and antitussive efficacy with aerosol administration [22,23]. They found concentrations were less than predicted, were enhanced by addition of an emulsifier, and varied according to temperature, light exposure, and concentration over a 12-month period. These results have not been replicated at the higher concentrations used for intradermal administration in chronic pain models.

Most chronic pain studies have relied on extemporaneous compounding of capsaicin. A standardized intradermal formulation for centralized distribution would be advantageous in

multicenter clinical trials, where the accuracy of pain measurement is crucial, and where compounding facilities and techniques may vary among clinical sites. Our goal was to determine the potency of a capsaicin solution for intradermal administration and its stability over time at various temperatures.

Materials and Methods

Materials

Capsaicin USP analytical standard sample was obtained from USP (Rockville, MD, USA) and High Performance Liquid Chromatography (HPLC) grade methanol and water were obtained from Fisher (Pittsburg, PA, USA). Capsaicin solution was manufactured using capsaicin (95% purity) obtained from Sigma-Aldrich (St. Louis, MO, USA) dissolved in polysorbate 80 NF (Fluka, St. Louis, MO, USA), and 0.9% sodium chloride solution (Hospira Inc., Lake Forest, IL, USA).

Preparation of 0.1% capsaicin solution

The capsaicin solution was prepared according to the method used by Simone et al. [4], where a dose-response relationship was observed in early pain studies and according to previous methods [13]. Capsaicin solution (0.1% capsaicin, 7.5% polysorbate 80, and 0.9% sodium chloride solution q.s.t 100%) was prepared by dissolving an accurately weighed amount of capsaicin at the required concentration in polysorbate 80. Capsaicin was solubilized with the aid of heat between 50 to 70°C. Upon dissolution, 0.9% sodium chloride solution was added to the polysorbate solution to bring up the volume to the required batch size. The product was then sterilized by filtering through a 0.1 µm Durapore PVDF membrane Millipak® 40 (Millipore, Billerica, MA, USA) and aseptically filled into sterile amber borosilicate single-dose glass vials with a fill volume of 1.1 g. Each vial was overlaid with sterile filtered nitrogen, sealed with a sterile rubber closure, and crimped. Specific gravity of the product was determined to be 1.0 g/mL.

Sterility and Bacterial Endotoxin Testing

Samples for sterility and Bacterial Endotoxin Testing (BET) were selected from the beginning, middle and the end of the fill process. Method suitability testing was conducted as part of sterility testing. Samples were provided to a referral analytical laboratory for this testing in accordance to USP Chapters <71> and <85> [24,25].

Stability testing

Stability testing of the product was conducted on the manufactured lot. Samples were randomly selected from the lot and placed in temperature controlled environments under refrigerated (5°C) and ambient conditions (25°C, 30°C). Each vial was collected from each temperature controlled environment at time points of one, three, six, and twelve months and subjected to physical and chemical stability testing. Additionally, a short term stability test at freezing conditions was performed for the product stored at freezer temperature (-18°C) overnight (at least 12 h). Product in the vials were thawed at ambient temperature and immediately evaluated for presence of precipitate or any abnormal occurrences using a

validated HPLC method. Potency testing after 24 h was conducted on thawed vials stored at freezer (-18°C) and at refrigerated (5°C) conditions.

The physical characteristics of the solutions were evaluated qualitatively at each sampling point. Each sample was visually inspected without magnification for changes in color, clarity, particulate matter, and product/container closure abnormalities.

Determination of potency

The concentration of capsaicin solutions were measured by a modified Capsaicin USP HPLC method [26], by using a Waters HPLC Alliance system on an e2695 separations module with a Waters 2998 Photo-Diode Array (PDA) detector (Waters Inc., Milford, MA, USA). Samples ($20\ \mu\text{L}$) were injected using a Waters auto injector and the instrument was controlled by use of Empower2® software (Waters Inc., Milford, MA, USA). Components were separated on a Nova-Pak® C18 reversed-phase column (Waters Inc., Milford, MA, USA) with $150\ \text{mm} \times 3.9\ \text{mm}$ dimensions and $5\ \mu\text{m}$ particle size. The column was kept thermostatic at 30°C in a Waters column oven (Waters Inc., Milford, MA, USA).

The HPLC system was calibrated for at least 30 min before determining the concentration of each stored capsaicin solution with the calibration curve developed with fresh capsaicin solutions of different concentrations. The percentage of Relative Standard Deviation (RSD) of the assay was determined to be $\pm 4\%$, so we assumed any change in concentration greater than 4% was greater than the expected deviation due to the sensitivity of the HPLC system and assay itself. The concentration of each solution was analyzed in triplicate and the mean concentrations were recorded for each solution at the different time intervals. The Limit of Detection (LOD) and Limit of Quantification (LOQ) were determined by applying the following formula [27,28]; $LOD=3.3\sigma/m$ $LOQ=10\sigma/m$ where σ is the standard deviation of the intercept of regression line, and m is the slope of the calibration curve. The LOD and LOQ were found to be 0.2 and 0.6 $\mu\text{g/ml}$ respectively with a RSD of less than 3%.

Statistical analysis

A two-way ANOVA with interaction was used to analyze the percent change of capsaicin concentrations stored at 5°C , 25°C and 30°C at one, three, six, and twelve months. Subgroup analyses were carried out at each temperature (respectively at each time point) and each time point (respectively at each temperature) to determine interaction effects. The Mann-Whitney test was used in case of unrecognized non-normality due to small sample size. The statistical analysis was performed using SAS 9.3 (SAS Inc., Cary, NC).

Results

Potency and stability

Figure 1 depicts the percent change in concentration over time of capsaicin stored at the three environmental temperatures. The concentration of capsaicin in freshly manufactured solutions was found to be 104% of predicted. Product samples were found to be stable, between 90 to 110% of the labeled potency.

Percent change in concentration of capsaicin was found over time at 5°C ($p<0.0001$), 25°C ($p=0.0012$), and 30°C ($p<0.0001$). Percent change in concentration was observed at 1 month ($p<0.004$), 3 months ($p<0.004$) and 12 months ($p<0.004$), but it was not significantly changed at 6 months ($p=0.896$) (Table 1).

Samples that underwent freeze thaw cycles showed no deviation from labeled potency. The change in concentration from pre-freeze to following freeze-thaw was 97.72 ± 1.32 ($p=0.0002$) and the change in concentration after 24 h on thawed vials stored at freezer (-18°C) was 90.47 ± 0.10 ($p=0.0002$) and stored at refrigerated (5°C) conditions was 103.48 ± 0.70 ($p=0.0002$).

Sterility and BET

The product met the requirement of both sterility and BET tests in accordance to USP Chapters <71> and <85> [24,25]. Samples were sterile and free from bacterial endotoxins. Visual examination of samples at each time point showed no evidence of any change in color or clarity or the presence of particulate matter.

Discussion

Attempts have been made to improve the sensitivity of the capsaicin model of allodynia and hyperalgesia by reducing sources of variability. Although a clear relationship has been established between dose and pain response [4,18,20], the potency and stability of prepared capsaicin solutions has not been examined in human pain models. Ensuring the accuracy of capsaicin concentrations is as crucial as controlling for other sources of variability, including dose [1,4,18,20,21], formulation [18], administrative route [17-19], and injection site [17,18] if it is to serve as an effective biomarker for underlying pain mechanisms and treatment response.

Capsaicin contained 104% of the labeled potency in freshly manufactured solutions. The difference between the predicted concentrations and the actual concentrations are comparable to Kopec's first study (88% of predicted) [22] and higher than the second (69-83% of predicted) [23]. Our increased accuracy may be due to the use of polysorbate 80 (Tween 80) to improve capsaicin solubility, as Kopec found actual concentrations were higher in solutions containing this emulsifier compared to those without this ingredient [23]. Differences may also be due to minor differences in assay methods or preparation procedures between laboratories.

Although our drug stability data showed statistically significant differences over time, the 90 to 110% range in concentrations observed were within the Food and Drug Administration's allowable guidelines of $100 \pm 10\%$ [29] at all time points (1 month: 95-101%, 3 months: 101-107%, 6 months: 98-99%, and 12 months: 106-110%) in samples protected from light. These results are similar to those reported by Kopec for refrigerated samples protected from light (2 months: 104%, 4 months: 108%, 6 months: 109%, 8 months: 110%, 10 months: 106%, and 12 months: 90%).

Although Kopec found solutions to meet 90% of labeled potency with refrigeration (90-110%) and at higher concentrations (95-110%), solutions stored at room temperature whether or not exposed to light (20-100%) and solutions at lower concentrations (60-100%) were not stable [22,23]. Similar to Kopec, we observed significantly different changes in concentration at varying temperatures, but unlike Kopec, they remained within the FDA guidelines at all temperatures (5°C: 99-108%, 25°C: 99-106%, and 30°C: 95-110%) and differences were not uniformly found at higher temperatures. We also found that samples undergoing short freeze thaw cycles showed no significant deviation from labeled potency, while Kopec found that frozen solutions degraded after 1 year [22,23]. It is possible that long term freezing of solutions disrupts the structure of capsaicin during the freezing process or during re-warming. Further short-term and long-term studies are warranted.

The temperature-dependent effects in Kopec's study may be due to the lower concentrations used (up to 0.004% solution), as capsaicin was being tested for aerosol administration rather than for intradermal administration. The higher concentrations used in our study (0.1% capsaicin solution) are those commonly used in intradermal pain studies, and may be more stable over time, since the chemical may aggregate to form more stable complexes and is thus less likely to precipitate out [22]. It is unlikely that our use of polysorbate 80 was contributory since even though Kopec found that the emulsifier improved the accuracy of initial concentrations, it did not prevent product degradation [23].

Our formulation provides a useful intradermal capsaicin model because it maintains its potency and stability for twelve months when stored at 5°C, 25°C and 30°C in an environment protected from light. The stability of capsaicin solution during freeze thaw cycles indicates it could be safely transported in a frozen state. Centralized manufacturing capsaicin solution, for each study site provides important product uniformity and quality control across a multicenter effort. These findings suggest that centralized manufacturing may be an effective and convenient way to provide capsaicin intradermal injection to assess pain and analgesic efficacy in multicenter trials. Stability studies are continuing in order to replicate our current findings over longer testing periods.

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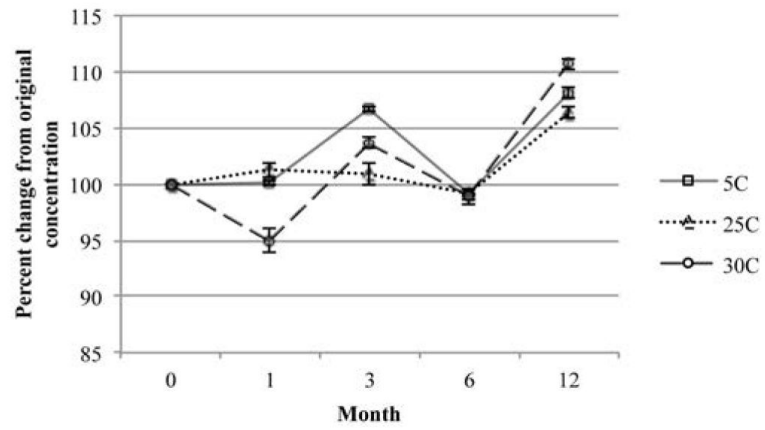


Figure 1. Percent change in concentration over time (in months) of capsaicin solutions stored at 5°C (squares), 25°C (triangles), and 30°C (circles). Data are presented as mean \pm SD.

Table 1

Percent change in capsaicin concentration (mean \pm SD) according to time and temperature.

Time **	Temperature *		
	5°C	25°C	30°C
1 month	100.09 \pm 0.15	101.22 \pm 0.61	94.96 \pm 1.05
3 months	106.64 \pm 0.17	100.90 \pm 0.96	103.64 \pm 0.48
6 months	99.10 \pm 0.48	99.07 \pm 0.18	98.89 \pm 0.71
12 months	108.10 \pm 0.50	106.35 \pm 0.50	110.72 \pm 0.50

* Percent change in concentration was observed at 5°C, 25°C, and 30°C over the 12 month period ($p < 0.001$).

** Percent change in concentration was observed at 1 month, 3 months, and 12 months ($p < 0.004$).