

## Skin Protectants Made of Curable Polymers: Effect of Application on Local Skin Temperature

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**Objective:** To measure the skin temperature after application of a new skin protectant intended for incontinence-associated dermatitis (IAD), compared with a commercial product with an analogous cyanoacrylate-based chemistry.

**Approach:** Twelve healthy human volunteers received an application of the new product on one thigh and of the comparator on the other thigh. An infrared camera using ThermoCAM™ software imaged the skin and measured the temperature at the skin surface over time to characterize the thermal cure profile induced by the products on the skin.

**Results:** The new product led to a drop in skin surface temperature (endothermic reaction), whereas the commercial product displayed an exotherm and a slight rise in skin surface temperature.

**Innovation:** Cyanoacrylate-based chemistries come in various formulations, differing in the side chains and additives used. They are liquid monomers that polymerize after application, and this polymerization is accompanied by an exothermic reaction that can be perceived as an unpleasant warming sensation, especially on compromised skin. A new formulation was designed to mitigate this rise in temperature.

**Conclusion:** The new skin protectant may potentially be more comfortable for IAD patients, since it causes a drop in skin surface temperature instead of a rise during the curing process that follows application.

**Keywords:** skin protectant, cyanoacrylate, skin temperature, incontinence-associated dermatitis

### INTRODUCTION

SUPERFICIAL SKIN DAMAGE OCCURS in various circumstances, such as skin tears and moisture-associated skin damage (MASD). MASD includes conditions such as incontinence-associated dermatitis (IAD), intertriginous dermatitis, periwound moisture-associated dermatitis, and peristomal moisture-associated dermatitis. This

topic has been reviewed by Gray *et al.*<sup>1</sup> In many circumstances, areas of breakdown are difficult to manage with dressings due to anatomic location and the presence of incontinence. Products that can be spread, sprayed, or painted on the skin have been developed to manage these conditions.

A new skin protectant with improved adhesion to denuded skin,



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improved barrier properties, and improved durability has been designed to protect skin with denudement, such as seen with IAD. The investigational formulation is based on customized acrylic polymers combined with 2-octyl cyanoacrylate to form a film structure curing after application. Curing reactions can be accompanied by changes in temperature, and the curing of cyanoacrylate-based chemistries occurs through an exothermic polymerization reaction.<sup>2</sup> Heat is, therefore, released in the process, possibly leading to a burning sensation. Patients with IAD frequently report high levels of pain, particularly during cleansing after an incontinence episode and during the application of the product intended to protect the skin. Temperature and pain are generally considered to be separate sensory systems that are served by different receptors and afferent fibers within the skin.<sup>3</sup> It is reasonable to expect that these sensations may be more intense in denuded skin. Cooling or heating the skin can cause stinging, pricking, or burning, and sensory thresholds are recognized as being highly individual and subjective. For skin temperature measurements, the proposed clinically significant mean skin temperature difference is  $\pm 0.5^{\circ}\text{C}$  and the limits of agreements between different measuring methods are  $\pm 1.0^{\circ}\text{C}$ .<sup>4</sup>

The objective of this study is to investigate the effect of the application of curing skin protectant formulations on the local skin temperature of healthy subjects in a laboratory setting.

### CLINICAL PROBLEM ADDRESSED

Cyanoacrylate-based products can be used in the management of superficial skin damage. A possible limitation of this chemistry is the burning sensation that can be experienced by patients due to the exothermic polymerization reaction.<sup>2</sup> This article describes a new skin protectant formulated to

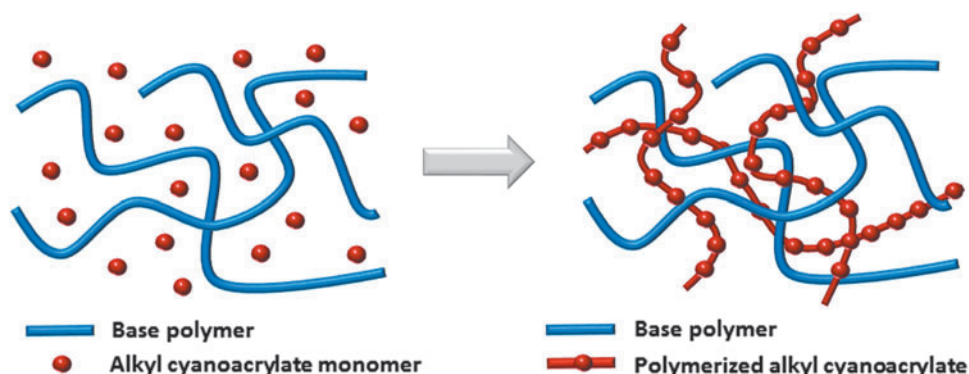
mitigate this effect and to eliminate the rise in skin temperature after application.

### SUBJECTS AND METHODS

Twelve healthy volunteers were recruited to participate in a study protocol approved by our Institutional Review Board (IRB). The goal was to measure the skin temperature after applying a new skin protectant compared with a commercial product with an analogous cyanoacrylate-based curing chemistry.

The investigational formulation tested is a solution based on a patented acrylate chemistry, which forms a durable, transparent elastomeric barrier on application to skin. This film is breathable and capable of preventing irritants from reaching the skin surface (data on file). A customized acrylic polymer, combined with 2-octyl cyanoacrylate, creates the film structure, as illustrated in Fig. 1. The film formers are delivered from a well-tolerated solvent. Testing done before applying the product to humans included cytotoxicity, irritation, sensitization, genotoxicity, and systemic toxicity based on the criteria of expected use (>30 days in contact with a breached skin barrier) and guidance covering the biological evaluation of medical devices outlined in EN ISO 10993-1:2009. The results supported the conclusion that the product is safe for its intended use. Animal models were also used to test this product.<sup>5</sup>

Volunteers were asked to not use skin creams or lotions on the test sites for 24 h before the study and to not exercise before testing on the day of the study. A skin marking pen was used to mark a 3 × 3 inch area on the mid-anterior part of both thighs for each subject. The hair was clipped if necessary. Areas were marked on each corner with an aluminum dot (for camera positioning). Subjects took a seated position and were allowed to acclimate to the room temperature for 30 min, and a baseline



**Figure 1.** Cartoon representation of the interpenetrating molecular network of the new skin protectant both before and after curing.

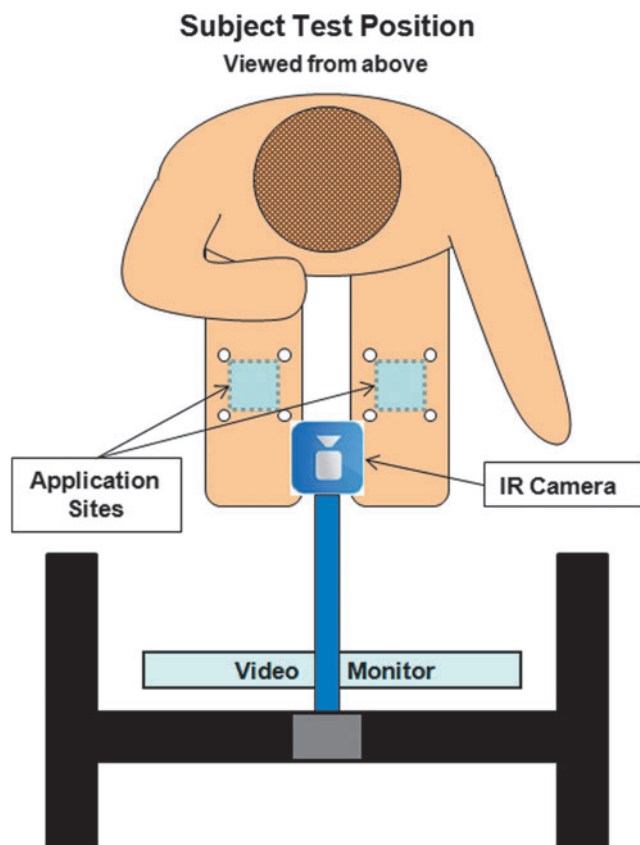


Figure 2. Subject test position.

skin temperature measurement was obtained by using a thermographic camera system (FLIR SC660 infrared camera with ThermaCAM<sup>TM</sup> Researcher Pro software v2.9, United Kingdom). The set-up is illustrated in Fig. 2. The products (new investigative skin protectant and Marathon<sup>®</sup> Liquid Skin Protectant; Medline Industries, Mundelein, IL) were applied simultaneously by two investigators, one on each thigh of each subject according to a randomization schedule. Postapplication, the skin temperature was measured every 15 s for 6 min, for a total of 25 pictures per subject.

The first image in each sequence was the “baseline” image taken after subject acclimatization for 30 min and before product application. The second image in each sequence was taken 15 s after application of both products was complete. The last image was taken 6 min (360 s) after application of both products was complete. The reference image for subtraction was the baseline image for each subject. This baseline was subtracted from each subsequent image.

#### Statistical Methods

Thermal data were analyzed by subtraction of the baseline skin temperature from the post-test

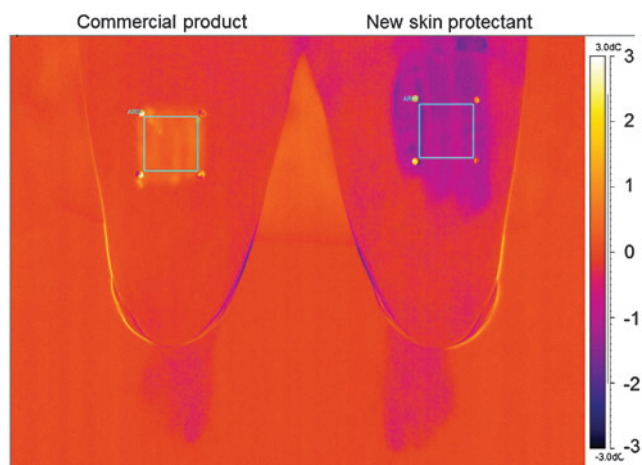


Figure 3. Representative image from the thermal camera with temperature scale on the right hand side. The temperature scale expresses the difference from baseline (set at 0°C). This image shows the 15 s time point (15 s after product application). The *left* side of the image (right thigh on this subject) received the commercial product, and the area of application displays a rise in temperature (toward the *yellow* end of the temperature scale); the *right* side of the image (left thigh on this subject) received the new skin protectant, and the area of application displays a decrease in temperature (toward the *purple* end of the temperature scale).

condition temperatures (every 15 s for 6 min) on stored digital images. The data were compared at each time point by using a mixed-model analysis of variance with subject as a random factor and protectant as a fixed factor. A *p*-value of less than 0.05 was considered significant. This same model was used to test whether the change at each time for each protectant was statistically significant from zero.

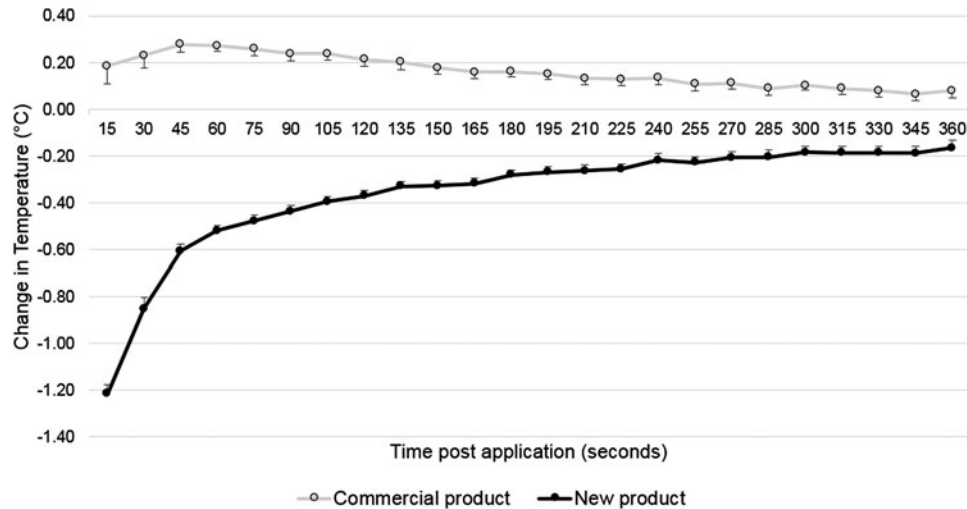
The peak change was calculated for each subject and protectant. If the largest change was in the negative direction, that was used. If the largest change was in the positive direction, that was used. The peak change was tested with the same statistical model.

## RESULTS

In our study, the new product led to a drop in skin surface temperature (endothermic reaction) per camera imaging, whereas the commercial product displayed an exotherm and a slight rise in skin temperature. Figure 3 provides a representative example of an image from the thermal camera.

Figure 4 displays the mean temperature measured every 15 s for 6 min for the 2 products tested ( $n = 12$  for each product).

The statistical analysis showed a significant ( $p < 0.001$ ) difference between the treatment groups at each time point (Fig. 4). For the commercial skin protectant, the temperature change



**Figure 4.** Mean change in temperature ( $^{\circ}\text{C}$ ) for 12 subjects (*bars* represent the standard error of the mean). The difference between protectants was significant ( $p < 0.001$ ) at all time points.

was significant (different from  $0^{\circ}\text{C}$ , with a rise in temperature) at all time points from 30 to 270 s, and for the new skin protectant, the temperature change was significant (different from  $0^{\circ}\text{C}$ , with a decrease in temperature) at all time points, that is, 15–360 s.

In each treatment group, the biggest change in temperature (peak) was identified for each subject and the mean of these values was calculated. For the commercial skin protectant, the mean peak increase was  $+0.3^{\circ}\text{C}$ , and for the new skin protectant, the mean peak decrease was  $-1.2^{\circ}\text{C}$ . The difference in the peak changes was statistically significant ( $p < 0.001$ ) between the two protectants. The estimate of the mean difference was  $1.5^{\circ}\text{C}$ , with a standard error of 0.054.

## DISCUSSION

This study looked at the thermal curing profile of a new skin protectant and a commercial product comparator after application to the skin of 12 healthy volunteers (one product on each thigh). There was a statistically significant difference in temperature at the skin surface between the two protectants. The difference was consistent across all 12 subjects, with results showing a decrease in temperature for the new product and an increase in temperature for the comparator. These temperature changes were statistically different from baseline for both products.

Cyanoacrylates include methyl-2-cyanoacrylate, ethyl-2-cyanoacrylate (found in commercial glues and branded as “Super Glue” and “Krazy Glue”), n-butyl-cyanoacrylate, and 2-octyl-cyanoacrylate.

They are unique in their ability to instantly polymerize at room temperature when applied to a surface: The polymerization is triggered by the presence of trace amounts of weakly basic or nucleophilic species on the surface, including moisture. Cyanoacrylate adhesives cure rapidly on skin surfaces (within 5–60 s).<sup>6</sup> The first generation of cyanoacrylate adhesives were based on lower alkyl (methyl) ester monomers and caused tissue toxicity. Research showed that the longer the hydrocarbon group at the  $-R$  position, the slower the rate of polymerization, the less heat released during polymerization, and the lower the histotoxicity.<sup>7</sup> In addition, longer chain esters degrade much slower, allowing more efficient metabolism of the degradation products and reducing the inflammatory response.<sup>8</sup> 2-octyl-cyanoacrylate was developed to address toxicity concern and to reduce skin irritation and allergic response, improving properties for medical applications.

Cyanoacrylates were first introduced for medical use as skin tissue adhesives to approximate the edges of incisional wounds and to achieve closure by primary intention.<sup>9</sup> In some circumstances, they can provide an alternative to sutures and staples for surgical wounds<sup>10</sup> and for simple traumatic lacerations.<sup>11</sup> Another use for cyanoacrylates has been as a preoperative skin care strategy, applying them on top of the surgical skin prep to reduce surgical site infections (SSIs) by immobilizing any bacteria left on the skin after prepping and to prevent growth. A Cochrane review published on this topic concludes that the results show a significant difference, but it cautiously states that more research is needed.<sup>12</sup> Dohmen has also reviewed

the literature on this and concluded that this approach is an attractive option to reduce SSIs.<sup>13</sup> In a similar thought process, Grimaldi *et al.* shared their experience of using octyl-2-cyanoacrylate to cover the suture after surgical incision closure and reported a decrease in the incidence of wound infection and wound dehiscence in a group of 900 patients over 8 years.<sup>14</sup> The literature has described concerns in using such adhesives in the actual incision, reporting that they can delay healing by acting as a barrier between the growing edges of the incision.<sup>2,15,16</sup> However, this may depend on the formulation, because others have reported an enhancement of the healing process in a partial-thickness wound animal model.<sup>17</sup> The current study highlights a different application for this chemistry, consisting of a skin protectant to manage superficial skin lesions or to protect skin exposed to irritants.<sup>18</sup>

The new skin protectant presented here is delivered in a nonstinging solvent and as this solvent evaporates, the heat of volatilization causes a cooling effect, compensating for the heat released during polymerization. This composition also contains a smaller percentage of reactive chemistry than the comparator product. Comparatively, the commercial product has no solvent and contains 100% reactive monomer, leading to a greater exothermic reaction on curing. The new skin protectant may potentially be more comfortable for patients, since it does not add any heat to the skin during the curing process that follows application. An additional benefit provided by the nonstinging solvent is that it prevents the cyanoacrylate from bonding tissues together, which is a critical concern when dealing with skin folds such as the gluteal cleft where such a product is used to manage IAD.

This study has some limitations. The measurements were taken on a small number of healthy volunteers, and the skin was not damaged. However, the conditions were well controlled and the results were remarkably consistent and reproducible. This formulation has been recently tested in a clinical setting (manuscript accepted for publication) on 16 patients suffering from IAD and showed promise for this indication. A larger scale study is underway.

## INNOVATION

Film-forming tissue adhesives based on cyanoacrylate chemistries have been available since the

## KEY FINDINGS

- A commercially available cyanoacrylate skin protectant causes an exothermic reaction lasting 4.5 min with a peak of +0.3°C on application to healthy human skin.
- A new skin protectant formulation designed to mitigate the rise in temperature causes an endothermic reaction lasting at least 6 min with a peak of -1.2°C on application to healthy human skin.
- The new skin protectant formulation causes a drop in skin surface temperature instead of a rise during the curing process that follows application.

1950s. The first FDA-approved product for human use was Dermabond® (1998), cleared to approximate surgical wound edges. Variations in chemistries have led to different formulations and additional uses. The commonality between these cyanoacrylate-based products is their exothermic polymerization. The heat released may cause the patient to experience a burning sensation.<sup>2</sup> This could be exacerbated in denuded skin such as is often seen with severe IAD. We present here a new formulation designed to mitigate this rise in temperature; the new skin protectant may potentially be more comfortable for patients by causing a drop in skin surface temperature instead of a rise during the curing process after application.

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## AUTHOR DISCLOSURE AND GHOSTWRITING

M.W., N.A., S.F.B., B.P.E., and R.A. are employees of 3M. All authors contributed to writing this article, and no ghostwriters were used to write this article.

## ABOUT THE AUTHORS

**Michael J. Walt** received a **BS** in Mechanical Engineering (Biomedical) from the University of Minnesota. At 3M since 1979, he spent 18 years in mechanical testing and development of orthopedic implants. He served on the ASTM Committee F4, Medical and Surgical Devices and Materials, helping develop test standards. In 1997, he transitioned to clinical research. He has used infrared thermography to determine human skin temperature changes when exposed to electrosurgical radiofrequency (RF) current. **Nancy Atwood** received her **BA** from the University of Minnesota, and she currently works at 3M in clinical research. **Stéphanie F. Bernatchez** received her **PhD** in

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### Abbreviations and Acronyms

- IAD = incontinence-associated dermatitis  
 IRB = Institutional review board  
 MASD = moisture-associated skin damage  
 SSI = surgical site infection