

Communication



A Portable, Cost-Effective and User-Friendly Instrument for Colorimetric Enzyme-Linked Immunosorbent Assay and Rapid Detection of Aflatoxin B₁

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Abstract: Food analysis based on the enzyme-linked immunosorbent assay (ELISA) is simple, sensitive and rapid, but requires a costly colorimetric instrument. The aim of this work was to develop a portable, low-cost and user-friendly colorimetric instrument for colorimetric ELISA and aflatoxin B_1 (AFB₁) detection. The principle of the developed instrument was employing a light-emitting diode to generate the signal light and using a light-dependent resistor to measure the signal light absorbed by the oxidized 3,3',5,5'-tetramethyl benzidine. The absorption spectra revealed that the solution absorbed signal light more strongly after reaction with H_2SO_4 , and blue light would be favorably absorbed. Evaluations on the stability and accuracy of the instrument and interference from ambient light showed that the fabricated instrument was stable, accurate, capable of quantitative detection and insensitive to ambient light changes. In addition, this instrument is user-friendly since it could calculate and report the final amount of AFB₁ to the operator. Measurements of maize and peanuts showed that the instrument provided as accurate results as the professional equipment. With the low fabrication cost (about RMB 129 or USD 20), portability, and user-friendliness, this instrument presents attractive potential in the rapid detection of AFB₁.

Keywords: ELISA; colorimetric; food safety; mycotoxin; rapid detection

1. Introduction

Foods are always at high risk of contamination by pathogens and their toxic secondary metabolites [1–5], posing severe threats to public health [6,7]. Although bactericidal treatments could effectively eliminate pathogens, the toxic metabolites would still remain in foods. A most toxic, widely distributed and well-known example is aflatoxin B₁ (AFB₁), a Group I carcinogen with the maximum limits of 0.5 to 20 μ g kg⁻¹ in different foods [4,8–12]. AFB₁ is mainly produced by *Aspergillus* [11,13,14], and is thermally stable and would not be decomposed under normal cooking conditions [15]. Although many techniques, e.g., chromatography, mass spectrometry and electrochemical sensors, can accurately detect AFB₁, most of them require sophisticated operations in clinical labs, costly instruments or professional personnel [16–18], limiting their applications in rapid detection. Therefore, it is necessary to make the quantitative detection of AFB₁ more portable, low-cost and user-friendly [12,19].

The strategies based on specific recognition elements and subsequent conversion of recognition events into color changes present an attractive potential for rapid and low-cost detection of AFB₁. One strategy is to use an antibody-based lateral flow test or aptamer-based lateral flow test, enabling the AFB₁ detection by simply observing the test lines with naked eyes. However, the insufficient sensitivity and semi-quantitative results obtained by strip reader or image analysis software limit their application in AFB₁ quantification [12,20]. Another strategy is the colorimetric enzyme-linked immunosorbent assay (ELISA), an analytical biochemistry assay using an immunological reaction for target



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Copyright: © 2021 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (https:// creativecommons.org/licenses/by/ 4.0/). recognition and an enzymatic reaction for signal generation and amplification [9,21–24]. Conventionally, a microplate reader is used to measure the colored solution at a specific wavelength and get the quantitative result. Although ELISA is considered to be simple and low-cost [25], the high cost of the instrument limits the application of ELISA in well-equipped laboratories by trained technical professionals [12,19], failing to meet the demand in remote or low-income areas. To meet the standards of quantitative, simple and low-cost detection for modern analytical systems [18,26,27], invertase, glucose oxidase and Pt have been used as the markers to modify the signal generation and amplification strategy of ELISA, thereby generating detectable signals for personal glucose meter [28], smartphone-based image processing [5] and pressure meter [29], respectively. These approaches are quantitative and low-cost, but require sophisticated modification of ELISA.

Light-emitting diodes (LEDs) and a photodiode, which could convert the intensity of light into an electrical signal, have been used in a colorimetric assay to detect organophosphorus pesticides [30]. Moreover, the light-dependent resistor (LDR) and LED are used to develop low-cost instruments that could analyze the colored sample solutions to detect ions in water and *staphylococcus aureus* in milk samples [31,32], respectively. The establishments of these methods are based on measuring the intensity of signal lights. As they are low-cost and do not require the modification of colorimetric assays, it would be attractive to investigate whether the LDR and LED are also feasible for the colorimetric analysis of ELISA readout and user-friendly quantification of AFB₁ in food samples.

In this study, we developed a portable, low-cost and user-friendly instrument to analyze the colored solution of ELISA and detect AFB_1 . This instrument employed a blue LED and an LDR to measure the signal light absorbed by the yellow products generated in horseradish peroxidase (HRP)-catalyzed and H_2O_2 -mediated oxidation of 3,3',5,5'-tetramethyl benzidine (TMB), calculated and reported the AFB_1 concentration to the operator. To verify its reliability, the instrument was used for the detection of AFB_1 in peanuts and maize, and showed comparable performance as the commercial spectrophotometer.

2. Materials and Methods

2.1. Reagents and Equipment

HRP and TMB were purchased from Aladdin (Shanghai, China). The AFB₁ ELISA kit was provided by Shenzhen Finder Biotech Co., Ltd. (Shenzhen, China). The kit was composed of 8-well ELISA plate strips containing immobilized AFB₁, standard AFB₁ solutions (0 to 0.48 μ g L⁻¹), a bottle of AFB₁ antibody, a bottle of HRP-labeled secondary antibody, a bottle of washing buffer, a bottle of stop buffer and two bottles of substrates. Other reagents were of analytical grade and were used as received. The absorption spectra of colored solutions generated by HRP-catalyzed and H₂O₂-mediated oxidation of TMB were measured by a Shimadzu UV-2550 spectrophotometer. A Shimadzu UVmini-1240 spectrophotometer was used to measure the absorbance of sample solution at 450 nm.

2.2. Instrument Fabrication

As shown in Figure 1A, the portable instrument developed in this work was composed of two parts: an opto-collection unit to perform the optical measurement and generate electrical signals; a signal processing unit to process the generated signals, calculate AFB₁ concentration and display results. The main body of the opto-collection unit was an optical chamber designed with Autodesk123D Design and made with polylactic acid via 3D printing technique. The signal light from the LED was absorbed by the sample placed in the optical chamber and then received by the LDR.

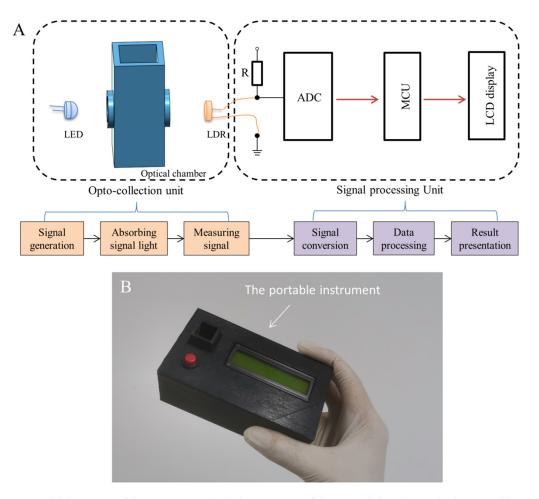


Figure 1. Design and fabrication of the instrument. (**A**) The structure of the optical chamber and schematic illustration of the portable instrument composed of the opto-collection unit (orange) and the signal processing unit (purple). (**B**) Photograph of the portable instrument.

The signal processing unit was fabricated by using an ADS1115 16-Bit analog-to-digital converter (ADC), a microcontroller unit (MCU) using an ATmega328P microcontroller and an LCD1602 display. The ADC converted the LDR response into readable outputs for the MCU [31], and then the MCU calculated the change of optical density (OD) according to the Lambert–Beer law shown in Equation (1) [32]:

$$OD = lg (I_0/I), \tag{1}$$

where I_0 was the value for the first blank sample, and I was the value during the measurement. The LCD display was used to present the result. Moreover, a chargeable battery together with a power switch was used as the power source. Additionally, a 3D printed box (12.4 × 6.8 × 4.7 cm) was used as the instrument shell. Figure 1B was a photograph of the developed instrument. All components used in the fabrication are commercially available and the cost was about RMB 129 or USD 20 in total.

2.3. Characterization of the Instrument

The colored products generated by enzymatic oxidation of TMB were used to evaluate the performance of the instrument. To prepare the colored solution, 1 μ L HRP (10 U mL⁻¹, prepared in PBS) was added into 1 mL 0.1 mol L⁻¹ PBS (pH 5.5) containing 100 mg TMB and 0.0315% H₂O₂. The solution was incubated for 10 min, and then acidified by 0.5 mL 1 mol L⁻¹ H₂SO₄ to turn the blue solution into yellow. Cuvettes (10 mm, 50 μ L) containing a series of diluted yellow solutions were measured by the portable instrument.

2.4. Standard Curve for AFB₁ Detection

The standard curve for AFB₁ was obtained according to the instruction of the AFB₁ ELISA kit. Briefly, 50 µL of standard solution (0, 0.03, 0.06, 0.12, 0.24 and 0.48 µg L⁻¹ AFB₁), 50 µL of HRP-labeled secondary antibody solution and 50 µL of AFB₁ antibody solution were added into the microwells of the ELISA plate strip, which were washed by using the washing buffer after an incubation of 30 min. Next, 50 µL of stop buffer was added to initiate the catalytic reaction. After 15 min, 50 µL of stop buffer was added to terminate the enzymatic reaction. After that, the colored solution was transferred into a 50 µL cuvette with an optical path length of 1 cm to perform the measurement. The measured values were then normalized by Equation (2) provided in the instruction:

Normalized value =
$$(A/A_0) \times 100\%$$
, (2)

where A was the value of a measured sample, and A_0 was the value of the sample containing 0 µg L⁻¹ AFB₁. Then, the standard curve was obtained by using the normalized values.

2.5. Analysis of Food Samples

Six food samples (three Maize and three peanuts) were purchased from local markets (Yangling, China). According to the kit instruction, 2 g crushed sample was extracted with 5 mL of 70% methanol for 5 min, and centrifuged for 10 min at 4000 rpm (HC-3018 Centrifuge, ANHUI USTC Zonkia Scientific Instruments Co., Ltd., Hefei, China). After that, 0.5 mL extracted solution was diluted with 0.5 mL water. Then, the obtained sample solutions were analyzed by the ELISA kit. The resulted solutions were transferred into the cuvettes and measured by both the portable instrument and the UVmini-1240 spectrophotometer. The final amount of AFB_1 in the sample was calculated by Equation (3):

Final amount =
$$K \times C$$
, (3)

where K was the dilution factor and C was the value calculated using the measured absorbance and the standard curve. To facilitate the detection by the end-user, we further fitted the standard curve, Equations (2) and (3) into the equipment. In this way, the operator only needed to use a blank sample to subtract the background and a negative sample containing 0 μ g L⁻¹ AFB₁ to provide a normalized value of 100%. Then, the instrument would directly report the AFB₁ concentration in the sample when the sample was being measured. When a measured value was lower than the linear range of the standard curve, the readout of the instrument would be not detected.

3. Results and Discussion

3.1. Principle for the Detection of AFB₁

The detection was based on the colorimetric measurement of the colored readout of the AFB₁ ELISA kit. As shown in Figure 2, in the absence of AFB₁, the HRPs were bounded on the solid support as a result of the target recognition, thereby initiating catalyzed reaction of TMB to generate blue products. After adding H₂SO₄, the color of the products turned yellow. The yellow solution would absorb the signal light of the instrument. At the presence of AFB₁, the competition between free and immobilized AFB₁ resulted in less bounded HRPs, less yield of colored products and increased intensity of transmitted light. The instrument quantified the concentration of AFB₁ to the operator.

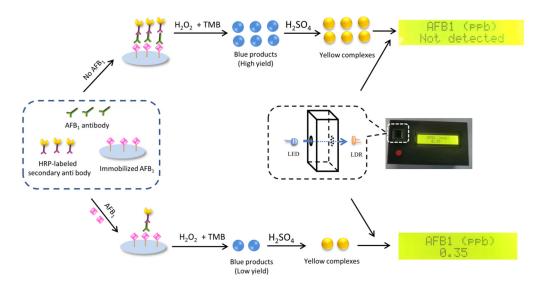


Figure 2. Schematic illustration of the principle for the AFB₁ detection.

3.2. Instrument Evaluation

Because of the complicated instrumental design in generating a signal light with a specific wavelength, we firstly tested the feasibility to simplify the opto-collection unit by using an LED to provide the detection signal. To choose an optimal signal light, the absorption spectrum of the blue solution obtained by using HRP, H_2O_2 and TMB were measured. The blue solution showed a maximum absorption peak at \sim 650 nm (Figure 3A). After adding H_2SO_4 , the color of the solution turned yellow, and the peak shifted to \sim 450 nm with an increased absorbance value. As this spectrum overlap with the wavelengths of blue lights, a blue LED was used as the light source of the instrument, obtaining a portable instrument measuring the OD of blue signal light (Figure 3B). A cuvette containing different solutions was used to evaluate the stability and accuracy of this portable instrument. As shown in Figure 3C and Video S1, the readout of the instrument was 0.00 and remained stable when the optical chamber was empty. Upon putting the cuvette containing sample solution into the optical chamber, the readout immediately reached 0.38 and remained at this value. When the cuvette was taken out of the chamber, the readout returned to 0.00 again, demonstrating a stable response of the portable instrument. Next, the accuracy of the instrument was investigated by measuring water, yellow sample solution and their mixtures containing 20%, 40%, 60% and 80% yellow solution, respectively. According to Figure 3D, the measured ODs were linearly proportional to the concentrations of the diluted solutions with a correlation coefficient of $R^2 = 0.9994$, and all standard deviations (SDs) were less than 0.012 (n = 3). These results demonstrated that the absorption of unfiltered light from the blue LED also complied with the Lambert–Beer law, and the instrument was capable to provide a reliable and quantitative result for the colorimetric ELISA kit.

3.3. Effect of Ambient Light

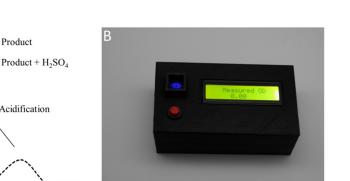
The ambient light conditions may be changed during the measurement. As the opto-collection unit of this instrument was not placed in an enclosed environment, we investigated the effect of ambient light by measuring a blank solution and a colored solution, respectively. As shown in Figure 4, the light was turned on at 5 s and turned off at 10 s, but the responses of the instrument remained unchanged in both measurements, suggesting that the instrument was insensitive to the interference from ambient light changes. It indicated that there was no need to block ambient light for the opto-collection unit, simplifying the instrument design/fabrication and facilitating the operation, i.e., sample in/out processes.

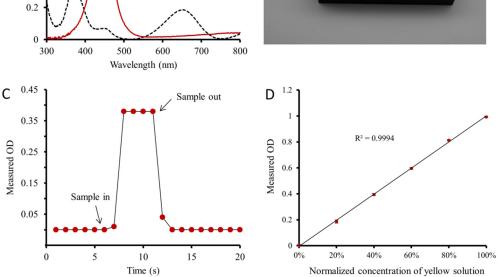
A

Absorbance 0.6

0.8

0.4





- Product

Acidification

Figure 3. Evaluation of the portable instrument. (A) Absorption spectra of the colored compound before (dash line) and after (solid line) acidification. (B) A photo that a portable instrument using blue LED was measuring OD. (C) Response of the instrument during sample in/out. The sampling interval of the instrument was 1 s. (D) Measurement of a series of diluted sample solutions by the portable instrument (n = 3).

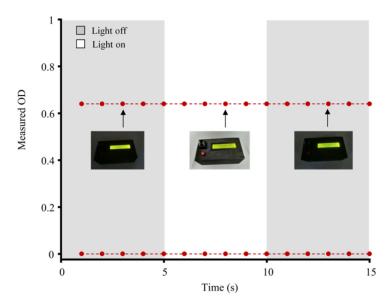


Figure 4. Effect of ambient light on the instrument. Insets were the photographs taken during the measurement.

3.4. Standard Curve for AFB₁ Detection

To assess the applicability of the portable instrument for AFB₁ detection, standard buffers containing 0, 0.03 0.06, 0.12, 0.24 and $0.48 \ \mu g \ L^{-1} \ AFB_1$ were analyzed by the AFB₁ ELISA kit and measured by both the portable instrument and the UVmini-1240 spectrophotometer. As shown in Figure 5, the normalized values of the portable instrument decreased with the AFB₁ concentration, and almost overlapped with the values calculated according to the absorbance from the UVmini-1240 spectrophotometer. Thus, the portable instrument was as accurate as the professional instrument.

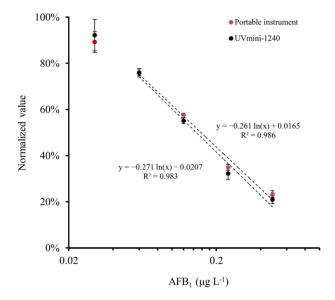


Figure 5. Calibration curve for AFB_1 obtained by both the portable instrument and the professional spectrophotometer (n = 4).

Generally, this type of ELISA assay would give a sigmoid standard curve with a linear range between 20% and 80%. The values for the sample containing 0.03 µg L⁻¹ AFB₁ were out of this range and fluctuated significantly, which might not be reliable for quantitative detection. Hence, an empirical formula of $y = -0.261 \ln(x) + 0.0165$ with the determine coefficient (R²) of 0.986 was established between 0.06 and 0.48 µg L⁻¹ AFB₁. The limit of detection (LOD) was determined to be 0.06 µg L⁻¹, since its value was significantly different from that of 0.03 µg L⁻¹ AFB₁ (p < 0.05 by *t*-test). This LOD is capable to meet the requirement in monitoring AFB₁ with the maximum limits in the range from 0.5 to 20 µg kg⁻¹ [4,8–12].

3.5. Detection of AFB₁ in Food Samples

Given the complicated process to calculate the AFB₁ concentration using the raw readout, we investigated the feasibility to automatically subtract the background, measure the ODs, normalize the measured values, calculate and output the amounts of AFB₁ in the samples by fitting the standard curve, Equations (2) and (3) into the equipment, obtaining a protocol for the portable instrument (Figure 6A): (1) Subtracting the background (BC). An operator turns on the instrument, and puts a blank solution into the chamber during a 9 s countdown. (2) Measuring the negative control (NC) containing 0 μ g kg⁻¹ AFB₁. The operator takes out the blank sample and then puts in the NC, which is requested to be accomplished in a 9 s countdown as well. (3) Measuring the sample. The operator takes out the NC from the optical chamber, puts the sample into the chamber, and then reads the AFB₁ concentration from the LCD display. For the detection of more samples, the operator only needs to place them into the chamber one by one. Because of this proposed protocol, the instrument could be easily calibrated by using a blank solution and a negative sample containing 0 μ g L⁻¹ AFB₁, and could report the AFB₁ concentration without additional data management by operators.

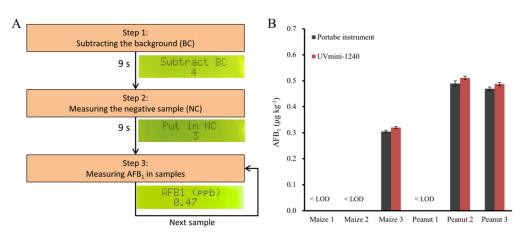


Figure 6. Rapid quantification of AFB₁ in food samples. (A) Schematic illustration of the rapid quantification by using the portable instrument. Insets were the screenshots taken during steps 1, 2 and 3, respectively. (**B**) Detection of AFB₁ in real samples (n = 3).

Peanuts and maize were used to evaluate the feasibility of this user-friendly strategy. The instrument readouts were compared with the results calculated by using the absorbance values from the spectrophotometer. As shown in Figure 6B, the readouts of the portable instrument were similar to the results obtained by the spectrophotometer, demonstrating the capability of the developed instrument for rapid quantification of AFB₁ in food samples. Compared with the costly instrument operated by the trained personnel in an advanced laboratory, this portable instrument provides a low-cost and user-friendly alternative to facilitate the quantitative detection of AFB₁. On the other hand, ELISA tests are generally performed in a high-throughput manner by using the microplate reader, but this developed instrument has to measure the samples one by one. In this case, further improvement can be focused on the realization of rapid and multi-channel measurements to enhance detection efficiency.

4. Conclusions

In this study, a portable, cost-effective and user-friendly instrument was fabricated for rapid quantification of AFB₁. The opto-collection unit made by using an LDR and blue LED obeyed the Lambert–Beer law, and the signal processing unit was able to accurately convert the response of the LDR sensor into quantitative readouts in a user-friendly way. Integration of the two units simplified the instrumental design, reduced the manufacturing cost and provided a portable and easy-to-use colorimetric instrument. With the low manufacturing cost (about RMB 129 or USD 20) and the user-friendly protocol of the instrument, users could rapidly and easily quantify the AFB₁ in food samples. Additionally, the application of this instrument would be extended to various targets by using different ELISA kits, presenting considerable promise towards quantitative and cost-effective detection of contaminants in foods.

Supplementary Materials: The following are available online at https://www.mdpi.com/article/10 .3390/foods10102483/s1, Video S1: Response of the portable instrument during the measurement.

Author Contributions: Conceptualization, W.T.; methodology, W.T. and Y.Q.; software, W.T.; validation, W.T.; formal analysis, W.T.; investigation, W.T. and Y.Q.; resources, W.T. and Z.L.; data curation, W.T. and Y.Q.; writing—original draft preparation, W.T.; writing—review and editing, W.T. and Z.L.; visualization, W.T. and Y.Q.; supervision, Z.L.; project administration, Z.L.; funding acquisition, W.T. All authors have read and agreed to the published version of the manuscript.

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Conflicts of Interest: The authors declare no conflict of interest.

References

- 1. Law, J.W.F.; Ab Mutalib, N.S.; Chan, K.G.; Lee, L.H. Rapid methods for the detection of foodborne bacterial pathogens: Principles, applications, advantages and limitations. *Front. Microbiol.* **2015**, *5*, 770. [CrossRef] [PubMed]
- 2. Luo, J.; Vogel, R.F.; Niessen, L. Rapid detection of aflatoxin producing fungi in food by real-time quantitative loop-mediated isothermal amplification. *Food Microbiol.* **2014**, *44*, 142–148. [CrossRef] [PubMed]
- Qian, W.J.; Lu, Y.; Meng, Y.Q.; Ye, Z.Z.; Wang, L.; Wang, R.; Zheng, Q.Q.; Wu, H.; Wu, J. Field detection of citrus huanglongbing associated with 'candidatus liberibacter asiaticus' by recombinese polymerase amplification within 15 min. *J. Agric. Food Chem.* 2018, 66, 5473–5480. [CrossRef] [PubMed]
- 4. Xu, X.; Liu, X.J.; Li, Y.B.; Ying, Y.B. A simple and rapid optical biosensor for detection of aflatoxin B1 based on competitive dispersion of gold nanorods. *Biosens. Bioelectron.* **2013**, *47*, 361–367. [CrossRef] [PubMed]
- Guo, R.Y.; Wang, S.Y.; Huang, F.C.; Chen, Q.; Li, Y.B.; Liao, M.; Lin, J.H. Rapid detection of salmonella typhimurium using magnetic nanoparticle immunoseparation, nanocluster signal amplification and smartphone image analysis. *Sens. Actuators B Chem.* 2019, 284, 134–139. [CrossRef]
- 6. Martinovic, T.; Andjelkovic, U.; Gajdosik, M.S.; Resetar, D.; Josic, D. Foodborne pathogens and their toxins. *J. Proteom.* **2016**, 147, 226–235. [CrossRef] [PubMed]
- 7. Qiao, Z.H.; Cai, Q.Q.; Fu, Y.C.; Lei, C.Y.; Yang, W.G. Visual and quantitative detection of E. coli O157:H7 by coupling immunomagnetic separation and quantum dot-based paper strip. *Anal. Bioanal. Chem.* **2021**, *413*, 4417–4426. [CrossRef] [PubMed]
- Di Nardo, F.; Alladio, E.; Baggiani, C.; Cavalera, S.; Giovannoli, C.; Spano, G.; Anfossi, L. Colour-encoded lateral flow immunoassay for the simultaneous detection of aflatoxin B1 and type-B fumonisins in a single Test line. *Talanta* 2019, *192*, 288–294. [CrossRef] [PubMed]
- 9. Azri, F.A.; Selamat, J.; Sukor, R. Electrochemical Immunosensor for the detection of aflatoxin B-1 in palm kernel cake and feed samples. *Sensors* **2017**, *17*, 2776. [CrossRef]
- 10. Duan, H.; Huang, X.L.; Shao, Y.N.; Zheng, L.Y.; Guo, L.; Xiong, Y.H. Size-dependent immunochromatographic assay with quantum dot nanobeads for sensitive and quantitative detection of ochratoxin A in corn. *Anal. Chem.* **2017**, *89*, 7062–7068. [CrossRef]
- 11. Neme, K.; Mohammed, A. Mycotoxin occurrence in grains and the role of postharvest management as a mitigation strategies. A review. *Food Control.* **2017**, *78*, 412–425. [CrossRef]
- 12. Zhang, L.L.; Wang, H.R.; Zhang, X.L.; Li, X.C.; Yu, H.Z. Indirect Competitive Immunoassay on a Blu-ray Disc for Digitized Quantitation of Food Toxins. *ACS Sens.* **2020**, *5*, 1239–1245. [CrossRef]
- McCullum, C.; Tchounwou, P.; Ding, L.S.; Liao, X.; Liu, Y.M. Extraction of aflatoxins from liquid foodstuff samples with polydopamine-coated superparamagnetic nanoparticles for HPLC-MS/MS analysis. J. Agric. Food Chem. 2014, 62, 4261–4267. [CrossRef]
- 14. Aldars-Garcia, L.; Sanchis, V.; Ramos, A.J.; Marin, S. Time-course of germination, initiation of mycelium proliferation and probability of visible growth and detectable AFB1 production of an isolate of Aspergillus flavus on pistachio extract agar. *Food Microbiol.* **2017**, *64*, 104–111. [CrossRef] [PubMed]
- 15. Yamada, M.; Hatsuta, K.; Niikawa, M.; Imaishi, H. Detoxification of aflatoxin B1 contaminated maize using human CYP3A4. *J. Microbiol. Biotechnol.* **2020**, *30*, 1207–1213. [CrossRef] [PubMed]
- 16. Xu, C.N.; Ying, Y.B.; Ping, J.F. Colorimetric aggregation assay for kanamycin using gold nanoparticles modified with hairpin DNA probes and hybridization chain reaction-assisted amplification. *Microchim. Acta* **2019**, *186*, 448. [CrossRef] [PubMed]
- 17. Duan, N.; Gong, W.H.; Wu, S.J.; Wang, Z.P. Selection and application of ssDNA Aptamers against clenbuterol hydrochloride based on ssdna library immobilized SELEX. *J. Agric. Food Chem.* **2017**, *65*, 1771–1777. [CrossRef] [PubMed]
- 18. Yan, L.; Zhu, Z.; Zou, Y.; Huang, Y.S.; Liu, D.W.; Jia, S.S.; Xu, D.M.; Wu, M.; Zhou, Y.; Zhou, S.; et al. Target-responsive "sweet" hydrogel with glucometer readout for portable and quantitative detection of non-glucose targets. *J. Am. Chem. Soc.* **2013**, *135*, 3748–3751. [CrossRef]
- Tao, F.F.; Yao, H.B.; Zhu, F.L.; Hruska, Z.; Liu, Y.L.; Rajasekaran, K.; Bhatnagar, D. A rapid and nondestructive method for simultaneous determination of aflatoxigenic fungus and aflatoxin contamination on corn kernels. *J. Agric. Food Chem.* 2019, 67, 5230–5239. [CrossRef] [PubMed]
- 20. Wang, L.; He, K.Y.; Wang, X.Q.; Wang, Q.; Quan, H.R.; Wang, P.L.; Xu, X.H. Recent progress in visual methods for aflatoxin detection. *Crit. Rev. Food Sci. Nutr.* **2021**, *133*, 115966.
- 21. Asensio, L.; Gonzalez, I.; Garcia, T.; Martin, R. Determination of food authenticity by enzyme-linked immunosorbent assay (ELISA). *Food Control.* **2008**, *19*, 1–8. [CrossRef]
- 22. He, F.; Liu, H.; Guo, X.G.; Yin, B.C.; Ye, B.C. Direct exosome quantification via bivalent-cholesterol-labeled dna anchor for signal amplification. *Anal. Chem.* 2017, *89*, 12968–12975. [CrossRef] [PubMed]
- Masud, M.K.; Yadav, S.; Isam, M.N.; Nguyen, N.T.; Salomon, C.; Kline, R.; Alamri, H.R.; Alothman, Z.A.; Yamauchi, Y.; Hossain, M.S.A.; et al. Gold-loaded nanoporous ferric oxide nanocubes with peroxidase-mimicking activity for electrocatalytic and colorimetric detection of autoantibody. *Anal. Chem.* 2017, *89*, 11005–11013. [CrossRef] [PubMed]

- 24. Chen, S.M.; Wan, Q.Q.; Badu-Tawiah, A.K. Mass spectrometry for paper-based immunoassays: Toward on-demand diagnosis. J. Am. Chem. Soc. 2016, 138, 6356–6359. [CrossRef] [PubMed]
- 25. Azri, F.A.; Sukor, R.; Selamat, J.; Abu Bakar, F.; Yusof, N.A.; Hajian, R. Electrochemical immunosensor for detection of aflatoxin B₁ based on indirect competitive ELISA. *Toxins* **2018**, *10*, 196. [CrossRef]
- Wu, H.; Zhang, X.J.; Wu, B.Q.; Qian, C.; Zhang, F.; Wang, L.; Ye, Z.Z.; Wu, J. Rapid on-site detection of genetically modified soybean products by real-time loop-mediated isothermal amplification coupled with a designed portable amplifier. *Food Chem.* 2020, 323, 126819. [CrossRef]
- 27. Xu, L.Z.; Li, D.Y.; Ramadan, S.; Li, Y.B.; Klein, N. Facile biosensors for rapid detection of COVID-19. *Biosens. Bioelectron.* **2020**, 170, 112673. [CrossRef]
- Huang, F.C.; Zhang, H.L.; Wang, L.; Lai, W.H.; Lin, J.H. A sensitive biosensor using double-layer capillary based immunomagnetic separation and invertase-nanocluster based signal amplification for rapid detection of foodborne pathogen. *Biosens. Bioelectron.* 2018, 100, 583–590. [CrossRef]
- 29. Zhu, Z.; Guan, Z.C.; Liu, D.; Jia, S.S.; Li, J.X.; Lei, Z.C.; Lin, S.C.; Ji, T.H.; Tian, Z.Q.; Yang, C.Y.J. Translating molecular recognition into a pressure signal to enable rapid, sensitive, and portable biomedical analysis. *Angew. Chem.* **2015**, *54*, 10448–10453. [CrossRef]
- Lan, W.S.; Chen, G.P.; Cui, F.; Tan, F.; Liu, R.; Yushupujiang, M. Development of a novel optical biosensor for detection of organophoshorus pesticides based on methyl parathion hydrolase immobilized by metal-chelate affinity. *Sensors* 2012, 12, 8477–8490. [CrossRef]
- 31. Santra, D.; Mandal, S.; Santra, A.; Ghorai, U.K. Cost-effective, wireless, portable device for estimation of hexavalent chromium, fluoride, and iron in drinking water. *Anal. Chem.* **2018**, *90*, 12815–12823. [CrossRef] [PubMed]
- 32. Tang, W.Z.; Zhang, M.; Yue, T.L.; Wang, X.; Li, Z.H. Low-cost colorimetric reader and label-free strategy for user-friendly detection of nucleic acid amplification products. *Sens. Actuators B Chem.* **2021**, *346*, 130523. [CrossRef]