









Article

# Graphene Oxide Carboxymethylcellulose Nanocomposite for Dressing Materials

Maria Luisa Saladino <sup>1,\*</sup>, Marta Markowska <sup>2,3</sup>, Clara Carmone <sup>1</sup>, Patrizia Cancemi <sup>1</sup>, Rosa Alduina <sup>1</sup>, Alessandro Presentato <sup>1</sup>, Roberto Scaffaro <sup>4</sup>, Dariusz Biały <sup>3,5,\*</sup>, Mariusz Hasiak <sup>6</sup>, Dariusz Hreniak <sup>2,3</sup> and Magdalena Wawrzyńska <sup>3,5,\*</sup>

<sup>1</sup> Department of Biological, Chemical and Pharmaceutical Sciences and Technologies (STEBICEF), University of Palermo, Viale Delle Scienze Bld. 16-17, I-90128 Palermo, Italy; claracarmone@gmail.com (C.C.); patrizia.cancemi@unipa.it (P.C.); valeria.aldaina@unipa.it (R.A.); alessandro.presentato@unipa.it (A.P.)

<sup>2</sup> Institute of Low Temperature and Structure Research, Polish Academy of Sciences, Okólna 2, PL-50-422 Wrocław, Poland; m.markowska@intibs.pl (M.M.); d.hreniak@intibs.pl (D.H.)

<sup>3</sup> Carbonmed Spółka z Ograniczoną Odpowiedzialnością, ul. Okólna 2, 50-422 Wrocław, Poland

<sup>4</sup> Department of Engineering, University of Palermo, Viale Delle Scienze Bld. 6, I-90128 Palermo, Italy; roberto.scaffaro@unipa.it

<sup>5</sup> Division of Preclinical Research, Faculty of Health Sciences, Wrocław Medical University, Ludwika Pasteura 1, PL-50-367 Wrocław, Poland

<sup>6</sup> Department of Mechanics and Material Science Engineering, Wrocław University of Science and Technology, Smoluchowskiego 25, PL-50-370 Wrocław, Poland; mariusz.hasiak@pwr.edu.pl

\* Correspondence: marialuisa.saladino@unipa.it (M.L.S.); dariusz.bialy@umed.wroc.pl (D.B.); magdalena.wawrzynska@umed.wroc.pl (M.W.)

Received: 18 March 2020; Accepted: 20 April 2020; Published: 23 April 2020



**Abstract:** Sore, infected wounds are a major clinical issue, and there is thus an urgent need for novel biomaterials as multifunctional constituents for dressings. A set of biocomposites was prepared by solvent casting using different concentrations of carboxymethylcellulose (CMC) and exfoliated graphene oxide (*Exf*-GO) as a filler. *Exf*-GO was first obtained by the strong oxidation and exfoliation of graphite. The structural, morphological and mechanical properties of the composites (CMC*x*/*Exf*-GO) were evaluated, and the obtained composites were homogenous, transparent and brownish in color. The results confirmed that *Exf*-GO may be homogeneously dispersed in CMC. It was found that the composite has an inhibitory activity against the Gram-positive *Staphylococcus aureus*, but not against Gram-negative *Pseudomonas aeruginosa*. At the same time, it does not exhibit any cytotoxic effect on normal fibroblasts.

**Keywords:** graphene oxide nanocomposite; carboxymethyl cellulose; biocompatibility; medical devices

## 1. Introduction

Nowadays, there is an urgent need for new innovative solutions in the field of biomedicine, since non-healing wounds remain a major clinical issue and are a significant burden to the medical system [1,2]. Chronic wounds are usually more prone to occur in those patients with a pre-existent physical condition (i.e., diabetes mellitus), and as such can negatively affect the overall clinical outcome. Besides, one of the most important factors that hinders the healing process is represented by bacterial infections. Moreover, the inadequate management of infected wounds is a major cause of amputation or life-threatening sepsis [3]. Thus, an ideal wound dressing should be highly biocompatible, with good mechanical properties and chemical structure, and also show a dynamic role in the wound healing process and be able to prevent bacterial infections [4]. Despite the recent progress in wound management, bacterial infections still lead to significant mortality and morbidity. Therefore, there is

a great need for designing advanced materials that could be used as wound dressings. One of the approaches consists of embedding antibiotics within the dressing material [2,5–8].

Recently, the study of graphene and its derivatives as a promising material for biomedical application—and particularly for wound dressing—has been considered [6–10]. Graphene is a single layer of  $sp^2$  hybridized carbon atoms creating a hexagonal lattice, and possessing unique properties, i.e., high specific surface area ( $\sim 2630 \text{ m}^2/\text{g}$ ), high electron mobility [11,12], thermal conductivity of between  $2\text{--}5 \text{ kW}\cdot(\text{m}\cdot\text{K})^{-1}$ , [13,14] and the highest known Young modulus ( $\sim 1 \text{ TPa}$ ) [15,16]. Moreover, several studies showed that graphene exhibits some antibacterial properties [17–20]. Its antibacterial mechanism is due to both physical (direct contact of the sharp edge of graphene with bacterial membranes) and chemical (induction of the oxidative stress generated by charge transfer) perturbation. One of the most studied graphene derivatives for bio-applications is graphene oxide (GO), mainly as it is naturally hydrophilic and stable in physiological solutions, and its preparation and functionalization is low-cost and easy to scale-up [21]. GO can be obtained by the oxidation and exfoliation of graphite. In the oxidation process, hydroxyl, carboxyl and epoxide groups are generated on the surface, increasing the GO hydrophilic character and further widening its possible functionalization, and therefore are also proposed for drug delivery and other biomedical applications [22–30]. Although GO exhibits antibacterial properties, aggregation phenomena limit its surface area and mode of action. Cellulose is a natural polysaccharide polymer composed of D-glucose units linked together, which can be found in the cell walls of plants and algae, exhibiting properties such as biodegradability, biocompatibility and low cytotoxicity [31]. Thus, cellulose represents a very attractive material for several biomedical applications, including membranes for dialysis, encapsulating agent for drug delivery [32], endotoxin encapsulation and removal, biodegradable implants, dressings for wound treatment, and in-bone regeneration and tissue engineering scaffolds [33].

Carboxymethylcellulose (CMC) is an anionic water-soluble biopolymer, which due to its characteristics such as hydrophilicity, bioadhesivity, pH-sensitivity, non-toxicity, high water solubility, non-allergenicity, low immunogenicity and gel-forming properties, is used in applications such as coating fluids, binders, textiles, paper, food, drug delivery systems and cosmetics [34]. CMC is a semi-synthetic derivative of cellulose produced by partial substitution of hydroxyl groups with carboxymethyl ones in positions 2, 3 and 6. Composite materials based on cellulose and GO—the latter as a filler—were proposed for some medical applications, as such a combination may overcome limitations of cellulose, improving its mechanical and biocompatibility properties [34]. Nor Hazwan et al. developed a reduced GO hydrogel which inhibited biofilm formation by *S. aureus* and *P. aeruginosa*-associated with infected wounds [7]. Rasoulzadeh et al. investigated a CMC/graphene oxide nanocomposite hydrogel beads as a drug delivery system, which is strongly dependent on the pH [35]. Justin et al. demonstrated that GO improves the mechanical properties of chitosan, enhancing its drug delivery profiles [36]. Shao et al. showed that the GO composites possess good cytocompatibility and excellent anti-bacterial rates to *Escherichia coli* and *S. aureus* [20].

In this work, we report the preparation and the characterization of CMC composites containing exfoliated GO (CMC $x$ /Exf-GO), also focusing on the evaluation of its biological activity, in terms of both cytotoxicity and antibacterial properties.

## 2. Materials and Methods

### 2.1. Materials

Graphite powder, 11 microns of 99% purity, was purchased from AlfaAesar (Haverhill, MA, USA). Sodium carboxymethyl cellulose (CMC) was purchased from Sigma-Aldrich (Saint Louis, MO, USA), average Mw  $\sim 250,000$ , degree of substitution 0.7.  $\text{H}_2\text{SO}_4$  (98%, p.a.),  $\text{H}_2\text{O}_2$  (30%, p.a.),  $\text{KMnO}_4$  (p.a.),  $\text{P}_2\text{O}_5$  (p.a.) and  $\text{K}_2\text{S}_2\text{O}_8$  (p.a.) were purchased from Chempur, (Piekary Śląskie, Poland), while HCl (35–38%, p.a. basic) was purchased from POCH (Avantor Performance Materials Poland S.A. (formerly POCH), Gliwice, Poland)

## 2.2. Preparation of Exfoliated Graphite Oxide (Exf-GO)

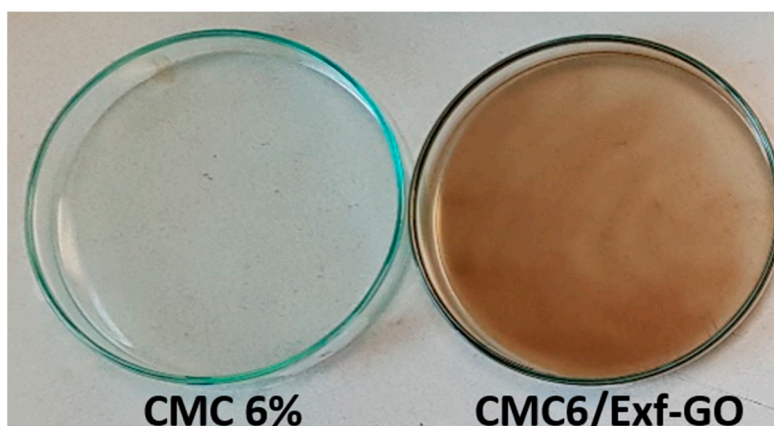
Exf-GO was prepared through oxidation of graphite powder in a two-step synthesis (pre-oxidation and actual oxidation), according to the modified Hummers' method [31,36]. In the first step, a concentrated solution containing  $\text{H}_2\text{SO}_4$  (1.5 mL),  $\text{K}_2\text{S}_2\text{O}_8$  (0.5 g) and  $\text{P}_2\text{O}_5$  (0.5 g) was mixed at 80 °C for 30 min. Then, 1 g of graphite was added. When the color of the mixture became dark blue, it was thermally isolated by coating with aluminum foil and being left to cool at room temperature (6 h). The mixture was then carefully diluted with distilled water, and then filtered and washed with water until the pH became neutral. The solution was air-dried at room temperature for 16 h on top of a Petri Dish, in order to obtain pre-treated graphite.

In the second step, the pre-treated graphite was oxidized. For this purpose, 1 g of the pre-treated graphite powder was added to  $\text{H}_2\text{SO}_4$  (23 mL) cooled in an ice-water bath.  $\text{KMnO}_4$  (3 g) was then gradually added to the mixture, which was maintained at a temperature below 20 °C. After this, the reaction mixture was heated up to 35–40 °C and stirred for 2 h. The mixture was then diluted by adding 46 mL of distilled water. The rapid reaction was stopped after 15 min by adding 140 mL of water and 2.5 mL of 30%  $\text{H}_2\text{O}_2$  solution. The product was then filtered and washed with 1:10 water:HCl solution (250 mL), in order to remove metal ions. The mixture was suspended in distilled water to give a viscous brown 2 wt% dispersion.

Exf-GO was obtained by liquid-phase exfoliation assisted by ultrasonication. Fully oxidized graphene oxide (GO) (0.1 g) was dispersed in distilled water (20 mL). The suspension was sonicated (Ultrasonic dispergator UZDN-A Ukrospribor, Sumy, Ukraine) and purified by centrifugation at 3000 rpm for 30 min (Hermle Universal Centrifuge Z 306, Wehingen, Germany).

## 2.3. Nanocomposites Preparation (CMCx/Exf-GO)

CMC-based nanocomposites have been obtained by solvent casting. Four aqueous dispersions of CMC at 1, 2, 4 and 6 wt% were added to 2.5 mL of Exf-GO aqueous dispersion, which were maintained in agitation at room temperature for 3 h and then sonicated for 1 h. The total volume was 30 mL. The pH of each dispersion was 7. The dispersions were then transferred into Petri dishes and kept in an oven at 50 °C to facilitate the evaporation of the solvent, which occurred within 24 h. All the obtained nanocomposites were homogeneous and brown. The colorless and transparent sample of Exf-GO free polymer has been also prepared as a reference (Figure 1).



**Figure 1.** Photo of the CMC 6% film and CMC6/Exf-GO nanocomposite in Petri dishes.

## 2.4. Characterization Techniques

**Raman Spectroscopy.** Raman spectra were recorded in the 1000–1800  $\text{cm}^{-1}$  range using a Renishaw InVia Raman spectrometer equipped with a confocal DM 2500 Leica optical microscope (Wotton-under-Edge, Great Britain, UK), a thermoelectrically cooled CCD as a detector, and an argon laser operating at 514 nm, power 5% (~0.5 mW), acquisition time 10 s and 10 accumulations.

Fourier Transform Infrared Spectroscopy (FT-IR, Billerica, MA, USA). The Attenuated Total Reflectance (ATR) spectra (FT-IR, Billerica, MA, USA) were recorded in the 40–4000  $\text{cm}^{-1}$  range, with a step of 2  $\text{cm}^{-1}$ , by using a FT-IR Bruker Vertex 70 Advanced Research Fourier Transform Infrared Spectrometer (FT-IR, Billerica, MA, USA) equipped with Platinum ATR (diamond crystal).

Atomic Force Microscopy (AFM). Topography of the produced materials (measured as deflection of the cantilever in the vertical direction) was investigated in contact mode by using an Atomic Force Microscope (XE-100, Park Systems, Suwon, Korea). The deflection of the cantilever in the horizontal direction was also measured with the help of a Lateral Force Microscope (NX-100, Park Systems, Suwon, Korea). All measurements were performed for the following scanning area 45  $\mu\text{m} \times 45 \mu\text{m}$ , 20  $\mu\text{m} \times 20 \mu\text{m}$ , 10  $\mu\text{m} \times 10 \mu\text{m}$ , 5  $\mu\text{m} \times 5 \mu\text{m}$ , 2.5  $\mu\text{m} \times 2.5 \mu\text{m}$  and 1  $\mu\text{m} \times 1 \mu\text{m}$ . The data were analyzed using XEI Software (Version 4.3.4) provided by the microscope's manufacturer.

X-ray Diffraction (XRD). XRD patterns were acquired by a PANalytical X'Pert pro X-ray powder diffractometer (Panalytical, Eindhoven, the Netherlands) using nickel-filtered Cu  $\text{K}\alpha 1$  radiation operating at 40 keV and 30 mA.

Mechanical properties. Tensile mechanical measurements were carried out using a dynamometer (model 3365; Instron, Norwood, MA, USA) on rectangular-shaped specimens (10  $\times$  90 mm) that were cut off from films. The grip distance was in all cases 30 mm, and the crosshead speed 5 mm/min. Five samples were tested for each material.

## 2.5. Biological Activity

Antibacterial tests. *Pseudomonas aeruginosa* ATCC<sup>®</sup> 10145<sup>™</sup> and *Staphylococcus aureus* ATCC<sup>®</sup> 25923<sup>™</sup> were used as tester strains of Gram-negative and Gram-positive bacteria, respectively. Bacterial cells were pre-cultured for 16 h in sterile glassware tubes containing 3 mL of Luria Bertani (LB) broth (Condalab, Lennox) at 37 °C with shaking (160 rpm). The day after, bacterial cells were inoculated (1% *v/v*) in 3 mL of LB broth amended with 2  $\times$  2 cm of different films (composite and polymer film alone reference sample), as well as 10% GO powder in an aqueous solution. Bacterial cells were challenged for 24 h at 37 °C with shaking (160 rpm). The effect of films and *Exf*-GO on bacterial growth was evaluated through the spot plate count method [37], incubating an aliquot of challenged bacterial suspensions on LB agar recovery plates at 37 °C for 24 h, and comparing the number of colony forming units (CFU) to those obtained in the case of an unchallenged culture. The data are expressed as the average of the logarithm of the CFU per milliliter of culture ( $\text{Log}_{10}$  CFU  $\text{mL}^{-1}$ ) for each biological trial ( $n = 3$ ) with standard deviation.

### 2.5.1. Fluorescence Microscopy to Assess Loss of Bacterial Membrane Integrity

*P. aeruginosa* and *S. aureus* cells were grown for 24 h in the presence of CMC, CMC6/*Exf*-GO and *Exf*-GO, prior to their imaging by means of a fluorescence microscope (Carl Zeiss, Oberkochen, Germany), as described by [38]. Briefly, bacterial cells were diluted 10 times in phosphate buffer saline (PBS) and stained with a 1:1 (*v/v*) mixture of acridine orange (100  $\mu\text{g}/\text{mL}$ ) and ethidium bromide (100  $\mu\text{g}/\text{mL}$ ), and were then immediately imaged at 1000 $\times$  magnification by using excitation and emission wavelength of 488 nm and 550 nm, respectively.

### 2.5.2. Cell Cultures

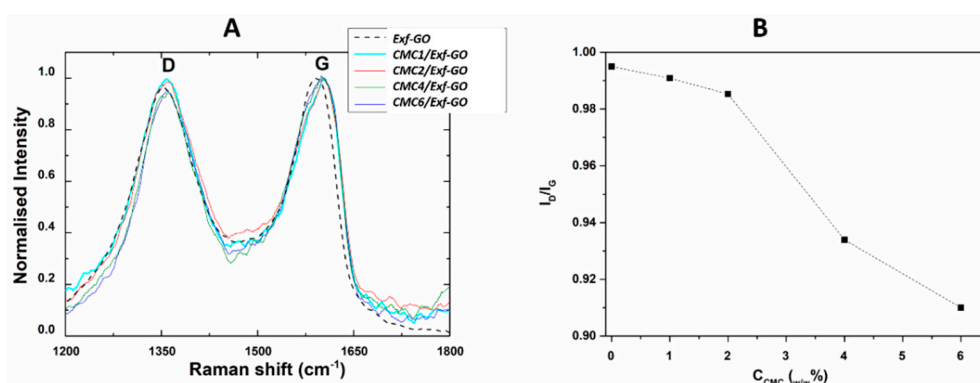
IMR-90 (ATCC<sup>®</sup> CCL-186<sup>™</sup>) cell line, derived from the normal lungs of a 16-week female fetus and used as a prototype of normal fibroblasts cells, was cultured in Eagle's Minimum Essential Medium (EMEM), supplemented with 10% fetal bovine serum, 100  $\text{U mL}^{-1}$  penicillin and 100  $\text{mg mL}^{-1}$  streptomycin. Cells were maintained at 37 °C in a humidified atmosphere of 5%  $\text{CO}_2$ , as previously described [39–44]. For the treatment, 50,000 cells per well in six-well plates were plated and incubated for 48 h at 37 °C in a  $\text{CO}_2$  incubator. 300  $\mu\text{l}$  of *Exf*-GO, diluted in culture medium, and 4  $\times$  4 cm of each composite were added to the wells for 48 h. At the end of treatment, the cells were observed

under inverted microscopy, and then detached from the plates and counted after staining with trypan blue dye.

### 3. Results and Discussion

#### 3.1. Structural, Morphological and Mechanical Characterization

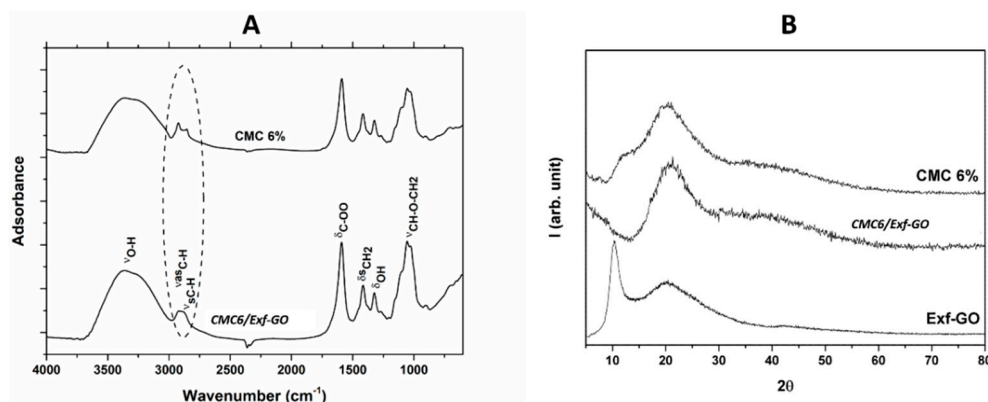
The obtained nanocomposites were analyzed to investigate their structure, antibacterial properties and biocompatibility. Raman spectra of exfoliated graphene oxide (*Exf*-GO) and carboxymethylcellulose (CMC) composites containing exfoliated graphene oxide (GO) ( $\text{CMC}_x/\text{Exf}$ -GO) nanocomposites are reported in Figure 2A, showing two broad overlapping bands in the range of 1200–1800  $\text{cm}^{-1}$ .



**Figure 2.** (A) Raman spectra of  $\text{CMC}_x/\text{Exf}$ -GO nanocomposites; (B)  $I_D/I_G$  ratio for CMC-based nanocomposites as a function of CMC%.

The G band, centered at 1580  $\text{cm}^{-1}$ , originates from the plane vibrations of carbon rings, while the D band at 1350  $\text{cm}^{-1}$  is defect-related, which can be ascribed to carbon-oxygen bonds created during graphite oxidation, grain boundaries and point defects, to name a few, which can cause deviation from the ideal planar structure [42]. The D peak is present in defective carbon materials. The G band is due to the  $\text{sp}^2$  C-C bond stretching in graphitic materials, while the D band is caused by disorder in the graphene structure [45]. The broadened G and D bands observed in all samples indicated the severe disruption of  $\text{sp}^2$  carbon lattice. The position of the two bands was red-shifted respective to the ones of the *Exf*-GO in the Raman spectra of the nanocomposites. This aspect could be due to the structural change in the *Exf*-GO caused by physical or chemical interaction with the CMC. The  $I_D/I_G$  ratio, reported in Figure 2B, relates to the  $\text{sp}^3/\text{sp}^2$  carbon ratio that is used to estimate the degree of defects. The observed trend indicates that all composites have a lower  $I_D/I_G$  ratio than that of *Exf*-GO, suggesting that the *Exf*-GO structure in the composites is less organized and the defects decreased with increasing concentrations of CMC. On the contrary, Yadav et al. observed an increase of the  $I_D/I_G$  ratios when GO in embedded in the CMC nanocomposites, which suggested that the structure of  $\text{CMC}_n/\text{Exf}$ -GO nanocomposite was of the ordered carbon nanosheet type [44].

Infrared (IR) spectra and X-ray diffraction (XRD) patterns were recorded to investigate possible interactions between *Exf*-GO and CMC. All IR spectra and XRD patterns of nanocomposites are reported in the Figures S1–S4 of Supporting Information. Here, representative IR spectra and XRD patterns of  $\text{CMC}_6/\text{Exf}$ -GO and CMC 6% film are reported (Figure 3A,B).

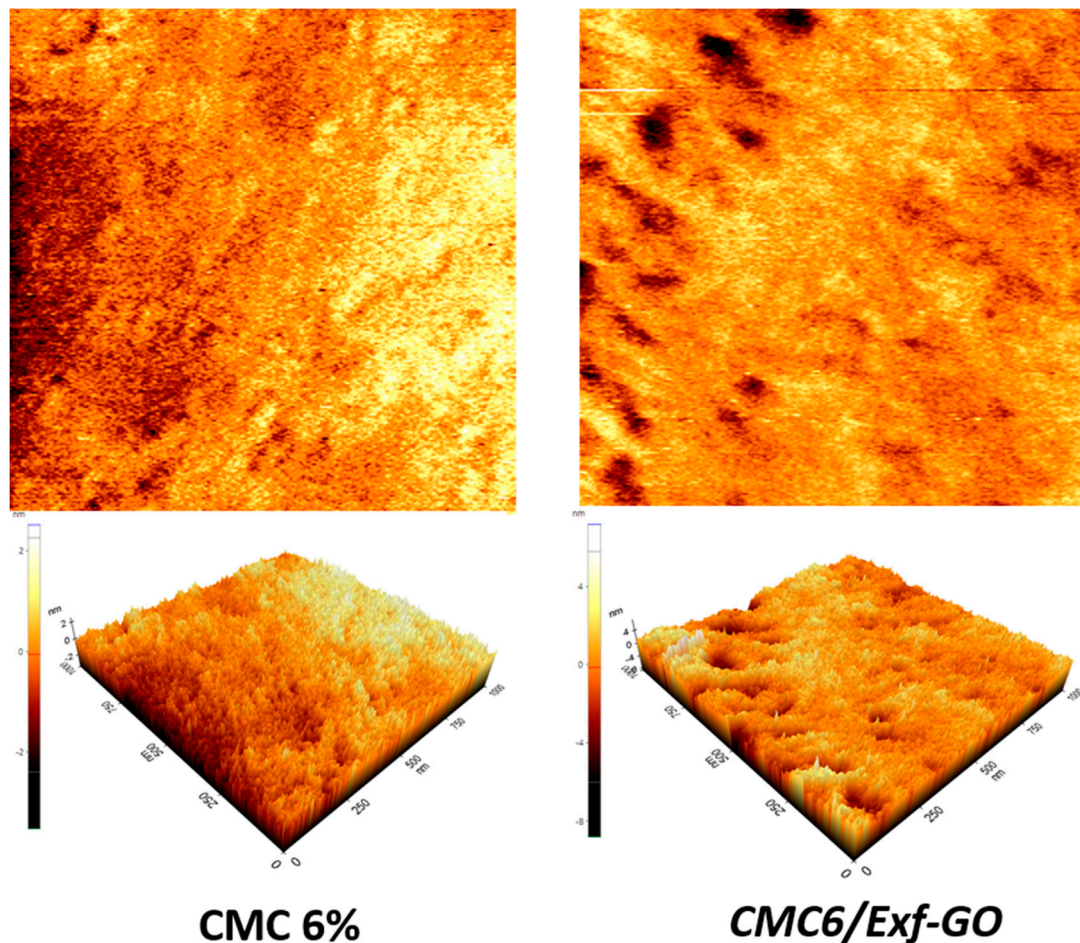


**Figure 3.** (A) IR spectra of CMC6/Exf-GO nanocomposites and CMC 6% film; (B) XRD patterns of Exf-GO, CMC6/Exf-GO and CMC 6% film.

The typical IR spectrum of CMC shows a broad absorption band at  $3440\text{ cm}^{-1}$ , due to the  $\text{-OH}$  group stretching. The bands at  $2924$  and  $2856\text{ cm}^{-1}$  are due to C-H asymmetric and symmetric stretching of the  $\text{CH}_2$  vibration. The bands at  $1590$ ,  $1415$ ,  $1324$  and  $1053\text{ cm}^{-1}$  are due to bending modes of the  $\text{-COO}$  group, the scissoring of  $\text{-CH}_2$ , the bending vibration of  $\text{-OH}$  and the stretching of the  $\text{CH-O-CH}_2$  group, respectively. No significant differences, in terms of IR bands (both shape and position), are observed in the IR spectra of the nanocomposites, suggesting that Exf-GO does not interact with CMC through intermolecular hydrogen bonds. By adding Exf-GO, however, the C-H stretching modes of  $\text{CH}_2$  vibration became sharper as two partially overlapped bands, indicating that there should be good compatibility between CMC and GO, as evident by the transparency of the material.

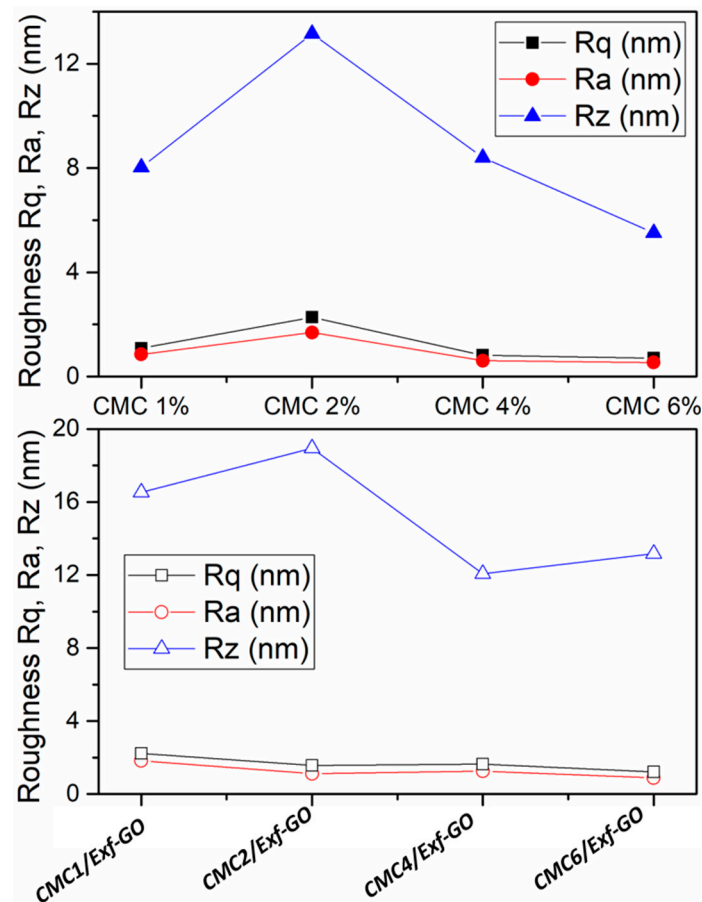
The XRD pattern of Exf-GO shows a strong peak at  $2\theta = 10.35^\circ$  and a large band at  $2\theta = 20.18^\circ$ , corresponding to d-spacing of  $8.54$  and  $4.40\text{ \AA}$  respectively, which are related to the inter-layer distance between the GO layers and to a short-range order in stacked graphene layers. The XRD patterns of CMC films show two large bands ( $101$  and  $110$  planes of cellulose—direction  $c$  of the unit cell is along the chain axis of the polymer), indicating a relative ordered structure characterized for the crystalline form of cellulose II [45–48]. The position of the peaks does not significantly change with CMC concentration. They fall at  $2\theta = 11.96^\circ$  and  $20.18^\circ$ , corresponding to d-spacing of  $7.39$  and  $4.40\text{ \AA}$ , respectively. Regardless of the CMC amount (i.e., 1, 2, or 3%), the presence of Exf-GO does not cause any change in the nanocomposite. Alternately, when combined with CMC 6%, the disappearing of the band can be observed at  $2\theta = 11.96^\circ$ , while the second band at  $20.18^\circ$  remains almost unvaried (see Figure 3B). The band of Exf-GO is also not present. These results indicated a crystal transition of cellulose during the composite formation in the presence of Exf-GO, indicating that Exf-GO was well exfoliated in the CMC matrix, being finely dispersed in the latter, in agreement with Raman data. The glycosidic linkages between the sugar units were partially destroyed during the dissolving and embedding of Exf-GO, which resulted in a probable reduction of the crystallinity [7].

Atomic force microscopy (AFM) can provide spatial information both parallel and perpendicular to the surface, thus allowing a 3D reconstruction of the sample surface. In doing so, we investigated both the topographical properties and the quality of the materials. 2D/3D AFM topography images of all CMC films and nanocomposites are reported in the Figures S5–S7 of the Support Information. For a general comment, here we report those of CMC6/Exf-GO and CMC 6% film (Figure 4).



**Figure 4.** 2D/3D AFM topography images for the CMC films (left side) and CMC6/Exf-GO nanocomposite (right side) obtained in contact mode for a scanning area of  $1\ \mu\text{m} \times 1\ \mu\text{m}$ .

AFM images showed that all films displayed a typical regular morphology. Analysis of the topography images obtained for the investigated materials shows that no visible grains were observed on the surface of the tested CMC and CMCx/Exf-GO samples. The same conclusion was obtained from simultaneous analysis of the topographies during left-to-right and right-to-left scanning, with the help of later force microscopy (LFM). Roughness  $R_q$ ,  $R_a$  and  $R_z$  for the AFM measured topographies of CMC and CMCx/Exf-GO composites (Figure 5), calculated with the help of XEI software (Park Systems), suggest that the surface's irregularities for all investigated materials result only from the preparation process of both CMC and CMCx/Exf-GO materials. This is particularly visible for the CMC 2% sample, for which the roughness parameter  $R_z$  is higher than for other materials. On the other hand, the roughness values presented in Figure 5 clearly suggest excellent quality of both CMC and CMCx/Exf-GO materials. The preparation of Exfoliated Graphite Oxide samples perfectly reflects the surface of CMC films, and the roughness of the CMCx/Exf-GO composite is not significantly different with respect to CMC films.

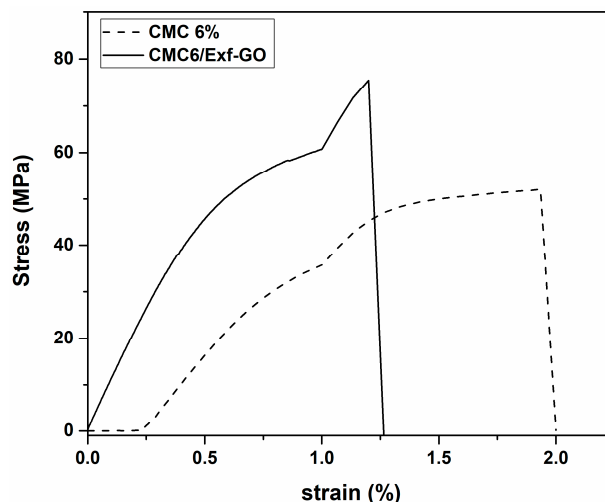


**Figure 5.** Roughness Rq, Ra and Rz for the CMC samples (upper figure, close symbols) and CMC6/Exf-GO samples (lower figure, open symbols), where: Rq is the root-mean-squared roughness; Ra is the roughness average; and Rz is the ten-point average roughness.

In order to study the effect of Exf-GO on the tensile properties of the CMC, the tensile test was carried out. Representative stress-strain curves of CMC6/Exf-GO nanocomposites and CMC 6% film are reported in Figure 6. Adding Exf-GO to CMC causes an increase of the elastic modulus, causing it to rise from 65 MPa to about 80 MPa, i.e., +23%. The increase in tensile stress is even more impressive, as it rises from about 45 MPa to about 80 MPa, i.e., +78%. This could be due to the different organization of the CMC chains in the composite [49,50]. The elongation at break, however, seems almost unaffected by the presence of the filler. It is worth noting that this set of mechanical properties is compatible with the applications foreseen for these materials.

The antibacterial and the cytotoxic activities were evaluated on CMC 6%-based composites, the composite constituted by CMC 6%, and on 2.5 mL Exf-GO (so called CMC6/Exf-GO), since this formulation, among those investigated, showed the lower value  $I_D/I_G$ , and is also the lesser organized.

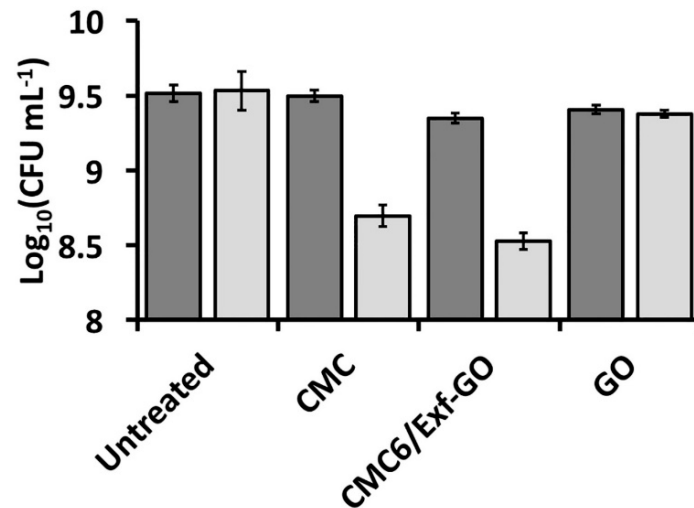




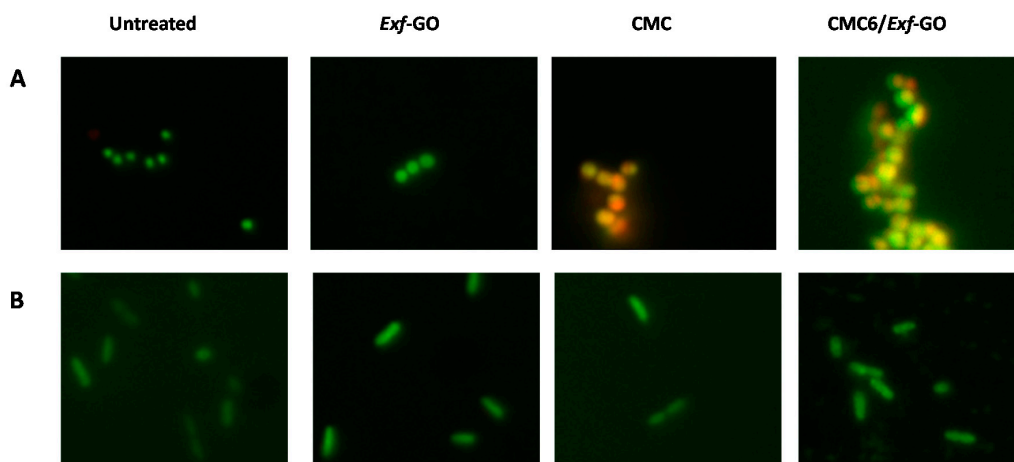
**Figure 6.** Stress-Strain curves of CMC6/Exf-GO nanocomposites and CMC 6% film.

### 3.2. Antibacterial and Cytotoxic Activity

*S. aureus* cell growth was inhibited by the presence of either CMC or CMC6/Exf-GO in the culture broth, which determined a decrease in the number of viable cells, corresponding to 0.8 and 1 log units (Figure 7), respectively. On the other hand, none of the analyzed samples affected the growth of *P. aeruginosa*, reaching  $3.7 \pm 1.6 \times 10^9$  CFU mL<sup>-1</sup> under each experimental condition (Figure 7). These results are in line with other studies aimed to unveil the antibacterial potential of CMC-based formulations, such as those containing reduced graphene oxide (rGO) [7] sodium alginate and chitosan [51], a zinc-based metal-organic framework and graphene oxide [52], or sodium alginate and pyrogallol acid [53], all of which in the form of either composite or bio-nanocomposite films. Here, a reasonable explanation for the lack of the antimicrobial activity of the composite films against the *P. aeruginosa* strain may rely on the higher resistance of Gram-negative bacteria as compared to Gram-positive ones, due to differences in the structure of the cell envelope. Indeed, Gram-positive strains are protected by a cell wall mostly composed of mucopeptide, while Gram-negative microorganisms possess a thin layer of the latter and an additional layer of lipoproteins and lipopolysaccharides (LPS) [54,55], which might contribute to a high degree of resistance towards the composites tested in this study. Antibacterial activity against Gram-positive bacteria is much more frequent than that one against Gram-negative bacteria ones [42,56–60]. The effect exerted by either CMC or CMC6/Exf-GO upon *S. aureus* and *P. aeruginosa* cells was corroborated by fluorescence microscopy imaging, after dual staining with acridine orange and ethidium bromide (Figure 8). *S. aureus* cells treated with CMC and CMC6/Exf-GO appeared swollen and emitted red fluorescence deriving from ethidium bromide dye, likely due to a loss of cell membrane integrity, in contrast to untreated and GO exposed cells, which appeared to be vital. Alternately, *P. aeruginosa* cells were vital, as they mostly emitted green fluorescence due to the acridine orange dye in all the tested conditions. All the above test results clearly indicate that the obtained composite can be considered for use as a bioactive advanced material for wound dressings against infections due to Gram-positive bacteria.

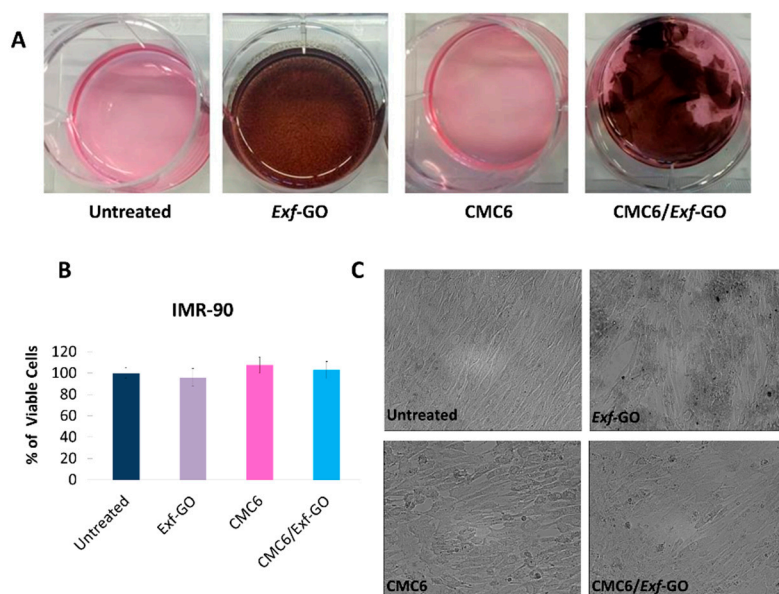


**Figure 7.** Bar graph reporting the biomass yield of both *P. aeruginosa* ATCC® 10145™ (dark grey bar) and *S. aureus* ATCC® 25923™ (light grey bar).



**Figure 8.** Fluorescence microscopy images of *S. aureus* ATCC® 25923™ (A) and *P. aeruginosa* ATCC® 10145™ (B), either not exposed (untreated) or exposed to *Exf*-GO, CMC and CMC6/*Exf*-GO.

GO, CMC and CMC6/*Exf*-GO nanocomposite were also evaluated for their biocompatibility, performing cytotoxicity tests on normal fibroblasts cell line (IMR-90). As a result, no cytotoxic effect was observed on normal fibroblasts after 48 h of treatment. CMC6/*Exf*-GO was more resistant to solubilization than CMC, although its structural change in terms of softening and delamination was observed (Figure 9A). Moreover, none of the tested samples inhibited cell growth (Figure 9B), and no morphological changes were observed under optical microscopy (Figure 9C). These results support the conclusion that the synthesized composites are biocompatible, and suitable for biomedical applications.



**Figure 9.** The effect of CMC6/Exf-GO treatment on normal fibroblasts IMR-90 cell line; (A) details of the culture plates in which the fibroblasts not exposed (untreated) or exposed to Exf-GO, CMC and CMC6/Exf-GO were grown; (B) graph showing the % of viable cells with respect to untreated ones, counted by trypan blue exclusion method; and (C) optical microscopy images of normal fibroblasts either not exposed (untreated) or exposed to GO, CMC and CMC6/Exf-GO for 48 h, where no morphological changes were observed. Magnification 200 $\times$ .

#### 4. Conclusions

Nanocomposites consisting of carboxymethylcellulose (CMC) and exfoliated graphene oxide (Exf-GO) were prepared and characterized by using microstructural techniques and biological tests. Raman, infrared (IR) spectra and X-ray diffraction (XRD) patterns showed that there is an increasing of disorder in the Exf-GO into polymer structure, as well as in the CMC chain structure. Atomic force microscopy (AFM) images evidenced no changes in the morphology of the CMC in presence of Exf-GO. The AFM and later force microscopy (LFM) investigations of the topography show a good quality of both CMC and Exf-GO samples. Moreover, the fabrication process of CMCx/Exf-GO materials does not change topography-obtained materials. On the other hand, the increase in tensile stress was observed in the composite compared to CMC.

It was demonstrated that the composite constituted by CMC 6% and on 2.5 mL Exf-GO exhibits antimicrobial activity against Gram-positive *S. aureus*. At the same time, the same composite does not exhibit any cytotoxic effect on normal fibroblasts and haemolytic activity, which makes it a promising candidate for use in medical materials such as wound dressing.

**Supplementary Materials:** The following are available online at <http://www.mdpi.com/1996-1944/13/8/1980/s1>, Figure S1: XRD patterns of cellulose films, Figure S2: XRD patterns of CMCx/Exf-GO nanocomposites, Figure S3: IR spectra of cellulose films, Figure S4: IR spectra of CMCx/Exf-GO nanocomposites, Figure S5: 2D (a, b) and 3D (c, d) AFM topography images for the CMC 1% film (a, c) and CMC1/Exf-GO nanocomposite (b, d) recorded in contact mode for scanning area of 1  $\mu\text{m} \times 1 \mu\text{m}$ , Figure S6: 2D (a, b) and 3D (c, d) AFM topography images for the CMC 2% films (a, c) and CMC2/Exf-GO nanocomposites (b, d) recorded in contact mode for scanning area of 1  $\mu\text{m} \times 1 \mu\text{m}$ , Figure S7: 2D (a, b) and 3D (c, d) AFM topography images for the CMC 4% films (a, c) and CMC4/Exf-GO nanocomposites (b, d) recorded in contact mode for scanning area of 1  $\mu\text{m} \times 1 \mu\text{m}$ .

**Author Contributions:** Conceptualization D.H. and M.L.S.; methodology: M.L.S.; preparation of samples: C.C. and M.M.; antibacterial test: R.A. and A.P.; cytotoxicity studies: P.C.; AFM: M.H.; mechanical test: R.S.; XRD, Raman and FT-IR data: C.C. and M.L.S.; writing—original draft preparation: M.M., A.P. and P.C.; writing—review and editing: M.L.S., R.A. and M.W.; supervision: D.B., D.H. and M.W.; funding acquisition: D.B., D.H. and M.W. All authors have read and agreed to the published version of the manuscript.

**Funding:** This work was partially supported by Grants from University of Palermo (FFR-D15-16024, FFR-D15-180463) to P.C. and M.L.S and partially funded from Statutory Funds of the Wrocław Medical University.

D.B. and M.L.S. thank the University of Palermo for the CORI2018–Action C2 Project (CORI-2018-C-D15-180463) for the possibility of visits between the two institutions. C.C. thanks the University of Palermo for supporting this research through the Erasmus+ Student Mobility for Traineeships A.A. 2018–2019.

**Acknowledgments:** Authors thank A. Di Leonardo for providing the IMR-90 cell line.

**Conflicts of Interest:** The authors declare no conflict of interest.

## References

1. Han, G.; Ceilley, R. Chronic Wound Healing: A Review of Current Management and Treatments. *Adv. Ther.* **2017**, *34*, 599–610. [[CrossRef](#)] [[PubMed](#)]
2. Negut, I.; Grumezescu, V.; Grumezescu, A.M. Treatment strategies for infected wounds. *Molecules* **2018**, *23*, 2392. [[CrossRef](#)] [[PubMed](#)]
3. Gottrup, F.; Apelqvist, J.; Bjarnsholt, T. EWMA document: Antimicrobials and non-healing wounds: Evidence, controversies and suggestions. *J. Wound Care* **2013**, *22*, S1–S89. [[CrossRef](#)]
4. Qian, W.; Hu, W.; He, W.; Zhan, R.; Liu, M.; Zhou, D.; Huang, Y.; Hu, X.; Wang, Z.; Fei, G.; et al. Plydimethylsiloxane incorporated with reduced graphene oxide(rGO) sheets for wound dressing application: Preparation and characterization. *Colloids Surf. B Biointerfaces* **2018**, *166*, 61–71. [[CrossRef](#)]
5. World Health Organization. Who Publishes List of Bacteria for Which New Antibiotics Are Urgently Needed. Available online: <https://tinyurl.com/kmva5da> (accessed on 21 April 2020).
6. Ramasubbu, D.A.; Smith, V.; Hayden, F.; Cronin, P. Systemic antibiotics for treating malignant wounds. *Cochrane Database Syst. Rev.* **2017**, *8*, 1–28. [[CrossRef](#)]
7. Hazwan Ali, N.; Cairul Iqbal, M.; Amin, M.; Shiow-Fern, N. Sodium carboxymethyl cellulose hydrogelscontaining reduced graphene oxide (rGO) as afunctional antibiofilm wound dressing. *J. Biomater. Sci. Polym. Ed.* **2019**, *30*, 629–645.
8. Hany Hussein, K.; Abdelhamid, H.N.; Zou, X.; Heung-Myong, W. Ultrasonicated graphene oxide enhances bone and skin wound regeneration. *Mater. Sci. Eng.* **2019**, *94*, 484–492.
9. Ghafari, R.; Scaffaro, R.; Maio, A.; Gulino, E.F.; Lo Re, G.; Jonoobi, M. Processing-structure-property relationships of electrospun PLA-PEO membranes reinforced with enzymatic cellulose nanofibers. *Polym. Test.* **2020**, *81*, 106182. [[CrossRef](#)]
10. Scaffaro, R.; Maio, A.; Lo Presti, F.; Botta, L. Nanocarbons in Electrospun Polymeric Nanomats for Tissue Engineering: A Review. *Polymers* **2017**, *9*, 76. [[CrossRef](#)]
11. Jauregui, L.A.; Cao, H.; Wu, W.; Yu, Q.; Chen, Y.P. Electronic properties of grains and grain boundaries in graphene grown by chemical vapor deposition. *Solid State Commun.* **2011**, *151*, 1100–1104. [[CrossRef](#)]
12. Bolotin, K.I.; Sikes, K.J.; Jiang, Z.; Klima, M.; Fudenberg, G.; Hone, J.; Kim, P. Ultrahigh electron mobility in suspended graphene. *Solid State Commun.* **2008**, *146*, 351–355. [[CrossRef](#)]
13. Balandin, A.A.; Ghosh, S.; Bao, W.; Calizo, I.; Miao, F.; Lau, C.N. Superior Thermal Conductivity of Single-Layer Graphene. *Nano Lett.* **2008**, *8*, 902–907. [[CrossRef](#)] [[PubMed](#)]
14. Pop, E.; Varshney, V.; Roy, A.K. Thermal properties of graphene: Fundamentals and applications. *MRS Bull.* **2012**, *37*, 1273–1281. [[CrossRef](#)]
15. Tonelli, F.M.; Goulart, V.A.; Gomes, K.N.; Ladeira, M.S.; Santos, A.K.; Lorençon, E.; Ladeira, L.O.; Resende, R.R. Graphene-based nanomaterials: Biological and medical applications and toxicity. *Nanomedicine* **2015**, *10*, 2423–2450. [[CrossRef](#)] [[PubMed](#)]
16. Lee, C.; Wei, X.; Kysar, J.W.; Hone, J. Measurement of the Elastic Properties and Intrinsic Strength of Monolayer Graphene. *Science* **2008**, *321*, 385–388. [[CrossRef](#)] [[PubMed](#)]
17. Wawrzyńska, M.; Bil-Lula, I.; Krzywonos-Zawadzka, A.; Arkowski, J.; Łukaszewicz, M.; Hreniak, D.; Stręk, W.; Sawicki, G.; Woźniak, M.; Drab, M.; et al. Biocompatible carbon-based coating as potential endovascular material for stent surface. *Biol. Med. Res. Int.* **2018**, *2758347*, 1–10. [[CrossRef](#)]
18. Kumar, P.; Huo, P.; Zhang, R.; Liu, B. Antibacterial Properties of Graphene-Based Nanomaterials. *Nanomaterials* **2019**, *9*, 737. [[CrossRef](#)]
19. Son, Y.R.; Park, S.J. Green preparation and characterization of graphene oxide/carbon nanotubes-loaded carboxymethyl cellulose nanocomposites. *Sci. Rep.* **2018**, *8*, 2–11. [[CrossRef](#)]
20. Shao, W.; Liu, H.; Liu, X.; Wang, S.; Zhang, R. Anti-bacterial performances and biocompatibility of bacterial cellulose/graphene oxide composites. *RSC Adv.* **2015**, *5*, 4795–4803. [[CrossRef](#)]

21. Singh, V.; Joung, D.; Zhai, L.; Das, S.; Khondaker, S.I.; Seal, S. Graphene based materials: Past, present and future. *Prog. Mater. Sci.* **2011**, *56*, 1178–1271. [[CrossRef](#)]
22. Maio, A.; Giallombardo, D.; Scaffaro, R.; Palumbo Piccionello, A.; Pibiri, I. Synthesis of a fluorinated graphene oxide–silica nanohybrid: Improving oxygen affinity. *RSC Adv.* **2016**, *6*, 46037–46047. [[CrossRef](#)]
23. Maio, A.; Scaffaro, R.; Lentini, L.; Palumbo Piccionello, A.; Pibiri, I. Perfluorocarbons–graphene oxide nanoplateforms as biocompatible oxygen reservoirs. *Anal. Chim. Acta* **2018**, *1037*, 1–380. [[CrossRef](#)]
24. Scaffaro, R.; Lopresti, F.; Maio, A.; Botta, L.; Rigogliuso, S.; Gherzi, G. Electrospun PCL/GO-g-PEG structures: Processing–morphology–properties relationships. *Compos. Part S Appl. Sci. Manuf.* **2017**, *92*, 97–107. [[CrossRef](#)]
25. Scaffaro, R.; Maio, A.; Lo Presti, F.; Giallombardo, D.; Botta, L.; Bondi, M.L.; Agnello, S. Synthesis and self-assembly of a PEGylated-graphene aerogel. *Compos. Sci. Technol.* **2016**, *128*, 193–200. [[CrossRef](#)]
26. Wang, Y.; Li, Z.; Wang, J.; Li, J.; Lin, Y. Graphene and graphene oxide: Biofunctionalization and applications in biotechnology. *Trends Biotechnol.* **2011**, *29*, 205–212. [[CrossRef](#)] [[PubMed](#)]
27. Zhang, H.; Zhai, D.; He, Y. Graphene oxide/polyacrylamide/carboxymethyl cellulose sodium nanocomposite hydrogel with enhanced mechanical strength: Preparation, characterization and the swelling behavior. *RSC Adv.* **2014**, *4*, 44600–44609. [[CrossRef](#)]
28. Li, X.; Li, F.; Gao, Z.; Fang, L. Toxicology of graphene oxide nanosheets against *paecilomyces catenulatus*. *Bull. Environ. Contam. Toxicol.* **2015**, *95*, 25–30. [[CrossRef](#)]
29. Liu, S.; Zeng, T.H.; Hofmann, M.; Burcombe, E.; Wei, J.; Jiang, R.; Kong, J.; Chen, Y. Antibacterial activity of graphite, graphite oxide, graphene oxide, and reduced graphene oxide: Membrane and oxidative stress. *ACS Nano* **2011**, *5*, 6971–6980. [[CrossRef](#)]
30. Song, Z.; Xu, Y.; Yang, W.; Cui, L.; Zhang, J.; Liu, J. Graphene/tri-block copolymer composites prepared via RAFT polymerizations for dual controlled drug delivery via pH stimulation and biodegradation. *Eur. Polym. J.* **2015**, *69*, 559–572. [[CrossRef](#)]
31. Klemm, D.; Heublein, B.; Fink, H.P.; Bohn, A. Cellulose: Fascinating biopolymer and sustainable raw material. *Angew. Chem. Int. Ed.* **2005**, *44*, 3358–3393. [[CrossRef](#)]
32. Mishra, P.-K.; Ekielski, A.; Mukherjee, S.; Sahu, S.; Chowdhury, S.; Mishra, M.; Talegaonkar, S.; Siddiqui, L.; Mishra, H. Wood-Based Cellulose Nanofibrils: Haemocompatibility and Impact on the Development and Behaviour of *Drosophila melanogaster*. *Biomolecules* **2019**, *9*, 363. [[CrossRef](#)] [[PubMed](#)]
33. Ummartyotin, S.; Manuspiya, H. A critical review on cellulose: From fundamental to an approach on sensor technology. *Renew. Sustain. Energy Rev.* **2015**, *2015*, 402–412. [[CrossRef](#)]
34. Javanbakht, S.; Shaabani, A. Carboxymethyl cellulose-based oral delivery systems. *Int. J. Biol. Macromol.* **2019**, *13*, 21–29. [[CrossRef](#)] [[PubMed](#)]
35. Rasoulzadeh, M.; Namazi, H. Carboxymethyl cellulose/graphene oxide bio-nanocomposite hydrogel beads as anticancer drug carrier agent. *Carbohydr. Polym.* **2017**, *168*, 320–326. [[CrossRef](#)] [[PubMed](#)]
36. Justin, R.; Chen, B. Characterisation and drug release performance of biodegradable chitosan-graphene oxide nanocomposites. *Carbohydr. Polym.* **2014**, *103*, 70–80. [[CrossRef](#)]
37. Piacenza, E.; Presentato, A.; Ambrosi, E.; Speghini, A.; Turner, R.J.; Vallini, G.; Lampis, S. Physical-chemical properties of biogenic selenium nanostructures produced by *Stenotrophomonas maltophilia* SeITE02 and *Ochrobactrum* sp. MPV1. *Front. Microbiol.* **2018**, *9*, 3178. [[CrossRef](#)]
38. Ciabocco, M.; Cancemi, P.; Saladino, M.L.; Caponetti, E.; Alduina, R.; Berrettoni, M. Synthesis and antibacterial activity of iron-hexacyanocobaltate nanoparticles. *J. Biol. Inorg. Chem.* **2018**, *23*, 385–398. [[CrossRef](#)]
39. Di Cara, G.; Marengo, G.; Albanese, N.N.; Marabeti, M.R.; Musso, R.; Cancemi, P.; Pucci-Minafra, I. Proteomic profiling of Trastuzumab (Herceptin(R))-sensitive and -resistant SKBR-3 breast cancer cells. *Anticancer Res.* **2013**, *33*, 489–503.
40. Cancemi, P.; Albanese, N.N.; Di Cara, G.; Marabeti, M.R.; Costantini, F.; Minafra, S.; Pucci-Minafra, I. Multiple changes induced by fibroblasts on breast cancer cells. *Connect. Tissue Res.* **2010**, *51*, 88–104. [[CrossRef](#)]
41. Pucci-Minafra, I.; Cancemi, P.; Di Cara, G.; Minafra, L.; Feo, S.; Forlino, A.; Tira, M.E.; Tenni, R.; Martini, D.; Ruggeri, A.; et al. Decorin transfection induces proteomic and phenotypic modulation in breast cancer cells 8701-BC. *Connect. Tissue Res.* **2008**, *49*, 30–41. [[CrossRef](#)]

42. Mao, A.; Zhang, D.; Jin, X.; Gu, X.; Wei, X.; Yang, G.; Liu, X. Synthesis of graphene oxide sheets decorated by silver nanoparticles in organic phase and their catalytic activity. *J. Phy. Chem. Solids* **2012**, *73*, 982–986. [[CrossRef](#)]
43. Yadav, M.; Rhee, K.Y.; Jung, I.H.; Park, S.J. Eco-friendly synthesis, characterization and properties of a sodium carboxymethyl cellulose/graphene oxide nanocomposite film. *Cellulose* **2013**, *20*, 687–698. [[CrossRef](#)]
44. Hult, L.E.; Iversen, T.; Sugiyama, J. Characterisation of the supramolecular structure of cellulose in wood pulp fibers. *Cellulose* **2003**, *10*, 103. [[CrossRef](#)]
45. Ferrari, A.C. Raman spectroscopy of graphene and graphite: Disorder, electron-phonon coupling, doping and nonadiabatic effects. *Solid State Commun.* **2007**, *143*, 47–57. [[CrossRef](#)]
46. Garvey, C.J.; Parker, I.H.; Simon, G.P. On the interpretation of X-ray diffraction powder patterns in terms of the nanostructure of cellulose I fibres. *Macromol. Chem. Phys.* **2005**, *206*, 1568. [[CrossRef](#)]
47. He, J.; Cui, S.; Wang, S.-Y. Preparation and crystalline analysis of high-grade bamboo dissolving pulp for cellulose acetate. *J. Appl. Polym. Sci.* **2008**, *107*, 1029. [[CrossRef](#)]
48. Langan, P.; Nishiyama, Y.; Chanzy, H. A revised structure and hydrogen-bonding system in cellulose II from a neutron fiber diffraction analysis. *J. Am. Chem. Soc.* **1999**, *121*, 9940–9946. [[CrossRef](#)]
49. Motaung, T.E.; Saladino, M.L.; Chillura Martino, D.; Luyt, A.S. Influence of the modification, induced by zirconia nanoparticles, on the structure and properties of polycarbonate. *Eur. Polym. J.* **2013**, *49*, 2022–2030. [[CrossRef](#)]
50. Motaung, T.E.; Luyt, A.S.; Saladino, M.L.; Caponetti, E. Study of morphology, mechanical properties and thermal degradation of titania-polycarbonate nanocomposites as function of crystalline phase and amount. *Polym. Compos.* **2013**, *34*, 164–172. [[CrossRef](#)]
51. Lan, W.; He, L.; Liu, Y. Preparation and properties of sodium carboxymethyl cellulose/sodium alginate/chitosan composite film. *Coatings* **2018**, *8*, 291. [[CrossRef](#)]
52. Karimzadeh, Z.; Javanbakht, S.; Namazi, H. Carboxymethylcellulose/MOF-5/Graphene oxide bio-nanocomposite as antibacterial drug nanocarrier agent. *BioImpacts* **2018**, *9*, 5–13. [[CrossRef](#)]
53. Han, Y.; Wang, L. Sodium alginate/carboxymethyl cellulose films containing pyrogallol: Physical and antibacterial properties. *J. Sci. Food Agric.* **2017**, *97*, 1295–1301. [[CrossRef](#)] [[PubMed](#)]
54. Tassou, C.C.; Nychas, G.J.E. Antimicrobial activity of the essential oil of mastic gum (*Pistacia lentiscus* var. *chia*) on Gram positive and Gram negative bacteria in broth and in Model Food System. *Int. Biodeterior. Biodegrad.* **1995**, *36*, 411–420. [[CrossRef](#)]
55. Bachir, R.G.; Benali, M. Antibacterial activity of the essential oils from the leaves of *Eucalyptus globulus* against *Escherichia coli* and *Staphylococcus aureus*. *Asian Pac. J. Trop Biomed.* **2012**, *2*, 739–742. [[CrossRef](#)]
56. Dresler, C.; Saladino, M.L.; Demirbag, C.; Caponetti, E.; Chillura Martino, D.; Alduina, R. Development of controlled release systems of biocides for the conservation of cultural heritage. *Int. Biodeterior. Biodegrad.* **2017**, *125*, 150–156. [[CrossRef](#)]
57. Rubino, S.; Saladino, M.L.; Attanzio, A.; Busà, R.; Girasolo, M.A.; Caponetti, E.; Chillura Martino, D.; Tesoriere, L. Loading and release of the complex Pt(II) with the 2,2'-dithiobis(benzothiazole) ligand [Pt(DTBTA)(DMSO)Cl]<sub>2</sub>·CHCl<sub>3</sub> into mesoporous silica and studies of antiproliferative activity. *Polyhedron* **2018**, *153*, 234–239. [[CrossRef](#)]
58. Buttacavoli, M.; Albanese, N.N.; Di Cara, G.; Alduina, R.; Faleri, C.; Gallo, M.; Pizzolanti, G.; Gallo, G.; Feo, S.; Baldi, F.; et al. Anticancer activity of biogenerated silver nanoparticles: An integrated proteomic investigation. *Oncotarget* **2017**, *9*, 9685–9705. [[CrossRef](#)] [[PubMed](#)]
59. Saladino, M.L.; Rubino, S.; Colomba, P.; Girasolo, M.A.; Chillura Martino, D.; Demirbag, C.; Caponetti, E. Pt(II) complex @mesoporous silica: Preparation, characterization and study of release. *Biointerface Res. Appl. Chem.* **2016**, *6*, 1621–1626.
60. Poma, P.; Labbozzetta, M.; Zito, P.; Alduina, R.; Ramarosandratana, A.V.; Bruno, M.; Rosselli, S.; Sajeva, M.; Notarbartolo, M. Essential Oil Composition of *Alluaudia procera* and in Vitro Biological Activity on Two Drug-Resistant Models. *Molecules* **2019**, *24*, 2871. [[CrossRef](#)]

