

# Functionalized milk-protein-coated magnetic nanoparticles for MRI-monitored targeted therapy of pancreatic cancer

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**Abstract:** Engineered nanocarriers have emerged as a promising platform for cancer therapy. However, the therapeutic efficacy is limited by low drug loading efficiency, poor passive targeting to tumors, and severe systemic side effects. Herein, we report a new class of nano-constructs based on milk protein (casein)-coated magnetic iron oxide (CNIO) nanoparticles for targeted and image-guided pancreatic cancer treatment. The tumor-targeting amino-terminal fragment (ATF) of urokinase plasminogen activator and the antitumor drug cisplatin (CDDP) were engineered on this nanoplatform. High drug loading (~25 wt%) and sustained release at physiological conditions were achieved through the exchange and encapsulation strategy. These ATF-CNIO-CDDP nanoparticles demonstrated actively targeted delivery of CDDP to orthotopic pancreatic tumors in mice. The effective accumulation and distribution of ATF-CNIO-CDDP was evidenced by magnetic resonance imaging, based on the T<sub>2</sub>-weighted contrast resulting from the specific accumulation of ATF-CNIO-CDDP in the tumor. Actively targeted delivery of ATF-CNIO-CDDP led to improved therapeutic efficacy in comparison with free CDDP and nontargeted CNIO-CDDP treatment. Meanwhile, less systemic side effects were observed in the nanocarrier-treated groups than that in the group treated with free CDDP. Hematoxylin and Eosin and Sirius Red staining of tumor sections revealed the possible disruption of stroma during the treatment with ATF-CNIO-CDDP. Overall, our results suggest that ATF-CNIO-CDDP can be an effective theranostic platform for active targeting-enhanced and image-guided cancer treatment while simultaneously reducing the systemic toxicity.

**Keywords:** active targeting, drug delivery, cisplatin, magnetic nanoparticles, magnetic resonance imaging, pancreatic cancer

## Introduction

Pancreatic cancer is the fourth leading cause of cancer deaths in the United States.<sup>1,2</sup> Although significant discoveries and advances in cancer detection and therapeutic approaches have been made in the past decades, the prognosis of pancreatic cancer patients remains poor with a 5-year survival rate of only ~6%.<sup>2</sup> Currently, chemotherapy and radiotherapy are the major treatment options for pancreatic cancer patients, as 85% of patients are diagnosed at the advanced stage.<sup>2</sup> However, low specificity of chemotherapy drugs, poor efficiency in drug delivery, and drug resistance by cancer cells limit the treatment efficacy. Clinical trials of the combination chemotherapy with targeted therapy or radiation therapy are being conducted. Among them, several showed a statistically significant improvement in survival.<sup>3-5</sup> For example, the FOLFIRINOX regimen, composed of fluorouracil (5-FU), leucovorin, irinotecan, and oxaliplatin, has resulted in 4 months longer survival than the standard



treatment with gemcitabine alone.<sup>3</sup> However, severe side effects associated with the FOLFIRINOX regimen limit its application in pancreatic cancer patients. Cisplatin (also called *cis*-diamminedichloroplatinum (II) [CDDP]) is a potent anticancer chemotherapy drug that can intercalate into the double-stranded DNA in cancer cells. Despite its high potency, CDDP is only considered as an adjunct drug in pancreatic cancer treatment, usually combined with gemcitabine, because of the side effects and low efficiency caused by its fast clearance, leading to a lack of targeting and inactivation of drug during the process.<sup>6</sup>

Recent advances in nanomaterials and nanotechnology have presented a number of promising platforms to improve the specificity and efficiency of cancer drug delivery. Lipid- or polymer-based nanoparticle delivery methods/materials and cancer-cell-targeted delivery have been studied for improving treatment by reducing side effects and enhancing drug accumulation at the tumor site using pancreatic cancer cell lines and human pancreatic tumor xenograft models.<sup>5,7-12</sup> These studies demonstrated promising strategies to use nanotechnology for delivery of cancer therapeutics, but also suggested that new strategies are needed for developing stable nanocarriers with prolonged circulation time and target-specific delivery and for lowering the drug resistance of cancer cells.<sup>13-15</sup> In addition, noninvasive monitoring of drug delivery to the tumor site is desirable to optimize delivery in order to improve the treatment efficacy.<sup>16</sup>

Herein, we report a new targeted drug delivery nanosystem based on milk protein (casein [CN])-coated magnetic iron oxide (CNIO) nanoparticles, composed of a cancer cell targeting moiety that is the amino-terminal fragment (ATF) of urokinase plasminogen activator with an affinity to urokinase plasminogen activator receptor (uPAR), and the anticancer agent or CDDP for pancreatic cancer treatment. CNIO nanoparticles is not only an excellent magnetic resonance imaging (MRI) probe as previously reported,<sup>17,18</sup> but is also capable of loading a sufficient amount of CDDP in the CN layer through the ligand exchange of chloride groups in CDDP with the carboxyl groups in the CN protein.<sup>19</sup> The coating layer also renders sustained CDDP release, allowing sustained drug concentrations during circulation as well as targeted delivery and reduction of side effects due to the rapid release to the normal organs. Our result revealed that the developed ATF-CNIO-CDDP exhibited specific targeting to uPAR-overexpressing pancreatic cancer cells. Furthermore, ATF-CNIO-CDDP demonstrated targeted delivery of CDDP and improved therapeutic effect in an orthotopic pancreatic cancer model.

## Materials and methods

### Materials

All chemicals, including CDDP, were purchased from Sigma-Aldrich (St Louis, MO, USA) unless otherwise specified, and were used as received. 1-Ethyl-3-[3-dimethylaminopropyl]-carbodiimide hydrochloride (EDC) and *N*-hydroxy-sulfosuccinimide (Sulfo-NHS) were obtained from Thermo Scientific (Rockford, IL, USA). All cell culture materials (media and supplements) were purchased from Invitrogen (Burlington, ON, USA). Ultra-4 centrifuge tubes (100 kDa MWCO) were purchased from Millipore (Billerica, MA, USA).

### Preparation of ATF-CNIO-CDDP nanoparticles

First, CNIO nanoparticles were prepared as described previously.<sup>17</sup> Human ATF peptide of the receptor-binding domain of uPA was prepared according to the established protocol.<sup>20</sup> The ATF peptide was then conjugated to CNIO nanoparticles through EDC/NHS cross-link. Briefly, ATF (0.5 mg) was reacted with *N*-hydroxysuccinimide (NHS, 0.1 mg) and 1-ethyl-3-(3-dimethylaminopropyl)-carbodiimide (EDAC, 0.2 mg) in 2-(*N*-morpholino)ethanesulfonic acid (MES) buffer solution (1 M, pH 5.5) for 10 minutes, and then mixed with CNIO nanoparticles in borate buffer solution (0.5 M, pH 8.5). After reaction for 2 hours, the product was collected by ultracentrifugation (100 kDa MWCO) and washed with deionized water. For drug loading, CDDP was mixed with CNIO nanoparticles in 50 mM NaCl solution at 4°C overnight. Free CDDP was removed by ultracentrifugation (100 kDa MWCO) followed by washing three times with deionized water.

### Characterization of ATF-CNIO-CDDP nanoparticles

The size and morphology of the prepared ATF-CNIO-CDDP nanoparticles were determined by transmission electron microscope (TEM, Hitachi H-7500 [Hitachi Ltd, Tokyo, Japan], with an accelerating voltage 75 kV). The average hydrodynamic sizes and zeta potentials of different nanoparticles were determined using dynamic light scattering (DLS; Malvern Zetasizer Nano S-90; Malvern Instruments, Malvern, UK) equipment. To quantify the amount of CDDP and iron, selected samples were dissolved in concentrated nitric acid, then carefully diluted, and finally pH adjusted. Pt concentration was measured by colorimetric method with *o*-phenylenediamine (OPDA),<sup>21</sup> while Fe concentration was determined by the phenanthroline colorimetric method.<sup>17</sup> The percentage of CDDP loaded on CNIO nanoparticles was

calculated as the ratio of the amount of CDDP loaded on the CNIO nanoparticles to Fe based on the weight, ie, CDDP loading % = (weight of CDDP in nanoparticles/weight of Fe in nanoparticles)  $\times$  100%.

## Measurement of CDDP release from ATF-CNIO-CDDP

To measure the amount of CDDP released from the nanoparticles, the ATF-CNIO-CDDP solution at a concentration equivalent to 60  $\mu$ g/mL free CDDP (or 200  $\mu$ M) was diluted and pH adjusted to pH 5.5 or 7.4, and then incubated at 37°C. At each predetermined time point and interval, a portion of the mixture was collected and centrifuged with an ultra-4 centrifuge tube (cut-off size 100 kDa). The supernatant was collected, and the same amount of fresh buffer solution was added. The CDDP content in the supernatant was then determined by a colorimetric method.<sup>21</sup> Briefly, 500  $\mu$ L of a CDDP sample solution was mixed with the same volume of OPDA solution in dimethylformamide (1.4 mg/mL). The mixture was heated to 100°C for 10 minutes, followed by cooling it in an ice bath at 0°C for 10 minutes. The absorbance of the solution was measured at 600, 720, and 800 nm with a microplate reader. The concentration of CDDP in the solution was obtained by calibrating against a standard curve.

## Determining specific binding of ATF-CNIO-CDDP to MIA PaCa-2 cells

Ethics approval for the use of cell lines was granted by Emory University. The uPAR targeting ability of ATF-CNIO-CDDP was assessed using the human pancreatic cancer MIA PaCa-2 cell line with uPAR overexpression. CNIO without a targeting moiety conjugated was used as the control. Cells were seeded in 8-well chamber slides at a density of  $5 \times 10^4$  cells/well. After recovering for 24 hours, the media was replaced with that containing ATF-CNIO-CDDP at a concentration of 0.1 mg Fe/mL. Cells were incubated with the ATF-CNIO-CDDP-containing media at 37°C for an additional 4 hours. The cell monolayer was then rinsed with phosphate-buffered saline (PBS) and fixed with 4% paraformaldehyde in the PBS solution. Prussian blue staining for iron was performed to investigate the specific binding of ATF-CNIO-CDDP or control samples to cells with different levels of uPAR expression. Briefly, freshly prepared 10% potassium ferrocyanide (II) trihydrate and 20% HCl solutions were mixed and then added to wells containing fixed cells. After incubating for 1 hour, the Prussian blue staining solution was removed and the cells were washed with PBS. Counterstaining for cells was performed by adding nuclear fast red solution and incubating for 8 minutes. Stained cells

were dehydrated with 70% and 100% ethanol, and then rinsed in xylene. The slides were mounted and examined under a light microscope.

## Assessment of anticancer efficacy in vitro

Human pancreatic cancer MIA PaCa-2 cells were seeded in a 96-well plate at a density of  $5 \times 10^3$  cells/well and allowed to adhere overnight. The culture medium was then replaced with medium containing free CDDP, CNIO-CDDP, or ATF-CNIO-CDDP at different CDDP concentrations. After cells were cultured for another 72 hours, the cytotoxicity was determined by CCK-8 assay following the vendor-provided protocol. Briefly, cells were carefully rinsed with PBS after the drug-containing medium was removed, and this was followed by adding the CCK-8 containing medium solution. The cells were then incubated with the CCK-8 medium for 4 hours. The plate was read at the absorbance wavelength of 450 nm using a microplate reader (Synergy2; BioTek, Winooski, VT, USA). Cell viability was determined by comparing the absorbance of cells incubated with drugs to that of the control cells incubated without the presence of the drug.

## Treatment evaluation using an orthotopic pancreatic tumor model

All animal experiments were conducted following a protocol approved by the Institutional Animal Care and Use Committee (IACUC) at Emory University. The orthotopic pancreatic cancer model was prepared by injecting MIA PaCa-2 cells into the pancreas of 8-week-old female nu/nu mice using an established surgical method.<sup>20</sup> Mice were anesthetized by intraperitoneal injection of a ketamine:xylazine mixture (95:5 mg/kg) during the surgery. Incision was made on the left flank of the abdominal region where the pancreas is typically located, behind the middle of the spleen. The pancreas was then gently pulled out using forceps and 50  $\mu$ L  $1 \times 10^6$  MIA PaCa-2 cells was carefully injected into the head of the pancreas. After injection, the pancreas was placed back in the abdominal cavity before the abdominal muscle and the skin were closed with 4-0 Polysorb sutures and surgical staples. Tumors typically reached 5 mm in diameter after 3 weeks and were ready for imaging and treatment experiments. Animals were randomly divided into four groups (n=6): treatment control, treated with free CDDP, treated with nontargeted CNIO-CDDP, and treated with ATF-CNIO-CDDP. The mice were treated through intravenous tail vein injection at a dose of 5 mg CDDP/kg mouse weight, while the control group received only saline injection. In total, there were four injections with 6- or 7-day intervals. The body weights were measured at each time point. At the last time point,

the tumors were collected and weighed to determine the antitumor activity.

## Monitoring of drug delivery in vivo by MRI

To investigate the delivery of ATF-CNIO-CDDP in vivo, tumor-bearing mice were scanned before and 1 week after first injection of ATF-CNIO-CDDP on a 3 T MRI scanner (Tim Trio; Siemens, Erlangen, Germany) using a  $T_2$ -weighted fast spin echo sequence followed by a multi-TE fast spin echo sequence for  $T_2$  relaxometry mapping of the tumor to further validate the accumulation of nanoparticles. The MRI acquisition parameters were repetition time (TR) = 3,600 ms, echo time (TE) = 12–180 ms, flip angle = 150, matrix = 154 × 320, field-of-view (FOV) = 70 × 120 mm<sup>2</sup>, slice thickness = 1 mm and number of averages = 3. Colorized  $T_2$  maps were then generated as described in a previous work.<sup>22</sup> Regions of interest were drawn surrounding the tumor to calculate the MRI signal changes or the  $T_2$  values.

## Immunohistochemistry analysis

The organs (liver, spleen, and kidney) and tumors were collected after final treatment. Prussian blue staining for the presence of iron was performed on tissues collected from the major organs and tumors following our established protocol.<sup>17,22</sup> Immunofluorescence labeling for uPAR was performed using a rabbit anti-uPAR monoclonal antibody, followed by Alexa Fluor 555 goat anti-rabbit IgG secondary antibody. Sirius red staining for collagen in stromal structures was performed following an established protocol.<sup>23</sup> The stained slices were examined with a light or fluorescent microscope. For the comparison of relative collagen content, the red channel of the micrographs of Sirius-red-stained tumor sections were extracted using METLAB. Since the iron concentration is directly correlated to the  $T_2$  relaxation time measured by MRI at the given transverse relaxivity of the material,<sup>24</sup> we used MRI relaxivity measurement to determine the relative amount of iron oxide nanoparticles accumulated in tumors collected after the imaging experiments. Briefly, tumors were homogenized in an equal weight of lysis buffer. The homogenized tissue samples were placed in the vials and then scanned on a 3 T MRI scanner using  $T_2$ -weighted and multi-TE fast spin echo sequences.

## Statistical analysis

Results were expressed as means ± standard deviation when a measurement was made. When comparing two different conditions or different samples, Student *t*-tests were used to determine statistical significance. A *P*-value < 0.05 was considered statistically significant.

## Results and discussion

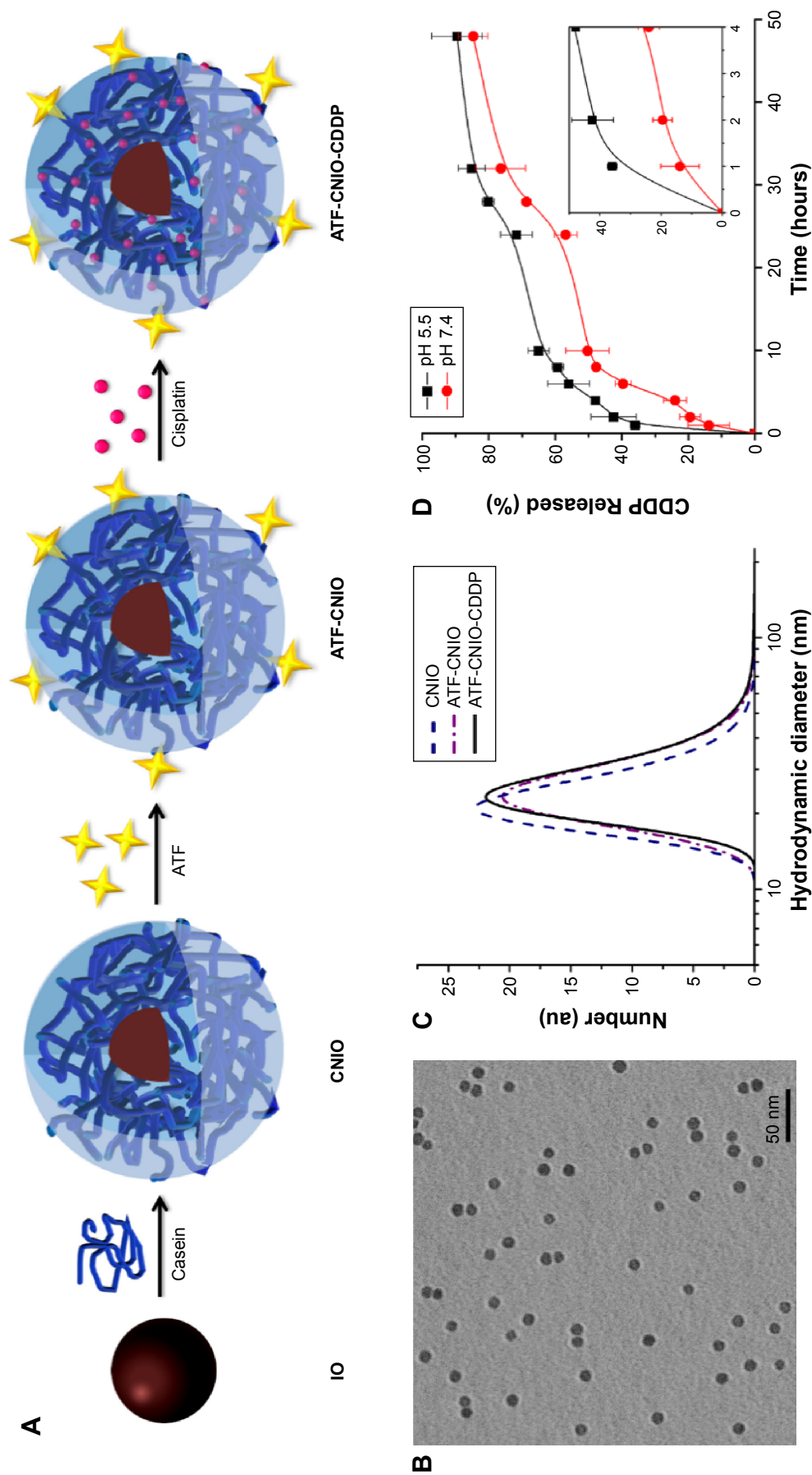
### Synthesis and characterization of ATF-CNIO-CDDP

The schematic structure of ATF-CNIO-CDDP is illustrated in Figure 1A. Bovine milk casein protein was selected as the coating material. In addition to stabilizing IO nanoparticles, casein coating provides abundant functional groups for incorporating targeting ligands on the surface.<sup>17</sup> ATF, which has been previously demonstrated as an efficient targeting ligand to pancreatic tumors,<sup>20,25,26</sup> was conjugated onto the surface using EDC/NHS via a covalent link between the carboxyl groups in ATF and the amine groups of casein coating, thus giving uPAR targeted ATF-CNIO nanoparticles. CDDP was subsequently loaded onto the particle through ligand exchange of chloride in CDDP with the carboxyl groups in CN protein.<sup>27,28</sup>

TEM images revealed that the magnetic iron oxide nanoparticle core with a diameter of 10.3 ± 0.5 nm remained intact after surface functionalization with ATF and CDDP (Figure 1B). On the other hand, DLS measurement showed a slightly larger hydrodynamic diameter of ATF-CNIO (26.0 nm) compared with CNIO (24.6 nm), indicating the successful conjugations of targeting ligands. The amount of ATF ligands conjugated was estimated at 17 ATF molecules per particle, as determined by the Bradford assay. After loading CDDP, little change in hydrodynamic diameter was observed for ATF-CNIO-CDDP (Figure 1C). However, the surface charge shifted from −35.2 to −31.9 mV as the result of loading CDDP further neutralized the COOH groups. Using the OPDA colorimetric method,<sup>21</sup> the amount of CDDP loaded on ATF-CNIO was determined to be 25:100 (wt) for CDDP:Fe. Compared with other early reported IO or protein-based nanoparticle carriers developed for CDDP delivery,<sup>28–30</sup> the significantly higher CDDP loading on ATF-CNIO-CDDP can be attributed to the unique structure of casein proteins, ie, the abundant carboxyl groups together with the phosphate groups.<sup>31</sup>

To evaluate the release profile in vitro, the ATF-CNIO-CDDP solutions were incubated in PBS (pH 5.5 and 7.4) at 37°C. At both pH conditions, ATF-CNIO-CDDP showed sustained CDDP release (Figure 1D), with a half-life time around 10 and 4.5 hours at pH 5.5 and 7.4, respectively. The accelerated release of CDDP at pH 5.5 may indicate the pH-triggered release of CDDP at low pH in a tumor tissue or cellular lysosome. The sustained release manner implies that most CDDP bound to casein coating through the exchange process, which could be re-exchanged by chloride or hydroxide ions after the protonation of carboxyl groups.<sup>31</sup>





**Figure 1** Synthesis and characterizations of CNIO, ATF-CNIO and ATF-CNIO-CDDP nanoparticles. **Notes:** (A) Schematic illustration of preparation of ATF-CNIO-CDDP nanoconstructs. (B) Typical TEM images of ATF-CNIO-CDDP nanoparticles. (C) Corresponding hydrodynamic sizes of nanoparticles before and after surface modification. (D) CDDP release profile of ATF-CNIO-CDDP in PBS at pH 5.5 and 7.4. The inset figure indicates the initial release of CDDP from ATF-CNIO-CDDP within the first 4 hours. **Abbreviations:** ATF, amino-terminal fragment; au, absorbance units; CDDP, cisplatin; CNIO nanoparticles, milk protein (casein)-coated magnetic iron oxide; PBS, phosphate-buffered saline; TEM, transmission electron microscopy.

## Cell targeting and cytotoxicity of ATF-CNIO-CDDP

To investigate the efficiency of uPAR-specific targeting of ATF-CNIO to uPAR-overexpressing pancreatic cancer cells, human pancreatic cancer MIA PaCa-2 cells were incubated with ATF-CNIO and non-targeted CNIO nanoparticles (as a control) at 37°C for 4 hours. Subsequent Prussian blue staining for iron revealed the specific binding of ATF-CNIO to MIA PaCa-2 cells, as evidenced by strong positive blue stains (Figure 2A). No such blue stains were observed in the cells treated with nontargeted IO.

In vitro cytotoxicity of ATF-CNIO-CDDP was tested in MIA PaCa-2 cells by MTT assay. Free CDDP and nontargeted CNIO-CDDP were used as controls. Cell viability of all three groups showed dose-dependent decrease after 72 hours of treatment (Figure 2B). Both ATF-CNIO-CDDP and CNIO-CDDP showed more potent cytotoxicity than free CDDP. Half-maximal inhibitory concentrations were determined to be 1.1, 1.6, and 16.1  $\mu\text{M}$  for ATF-CNIO-CDDP, CNIO-CDDP and free CDDP, respectively. Targeted ATF-CNIO-CDDP increased the in vitro treatment efficacy by 15-fold, while the efficacy of nontargeted CNIO-CDDP increased about 10-fold over that of free CDDP. This is consistent with some previous studies that reported higher toxicity of some lipid- and polymer-formulated CDDP than free CDDP.<sup>12,32,33</sup> The limited amount of CDDP loaded in delivery systems (eg, less than 10 wt%), together with the inevitable deactivation of CDDP during their long-time preparation procedures (ie, long period of hydration),<sup>6</sup> is usually considered as one of the

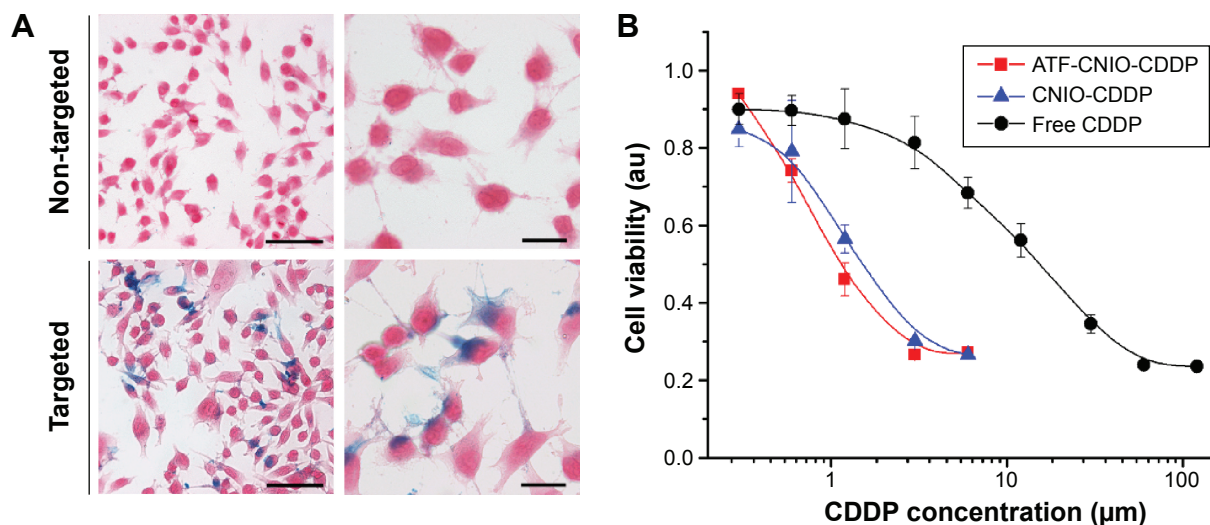
major reasons for reduced therapeutic efficiency. In our case, as much as 25 wt% CDDP was loaded on the CNIO-CDDP delivery system, which is significantly higher than that used in other protein drug carrier formulations.<sup>20,28</sup> In addition, drug activity is preserved by shortened preparation time and enhanced coating stability in chloride buffers.

## MRI monitoring of ATF-CNIO-CDDP in tumor-bearing mice

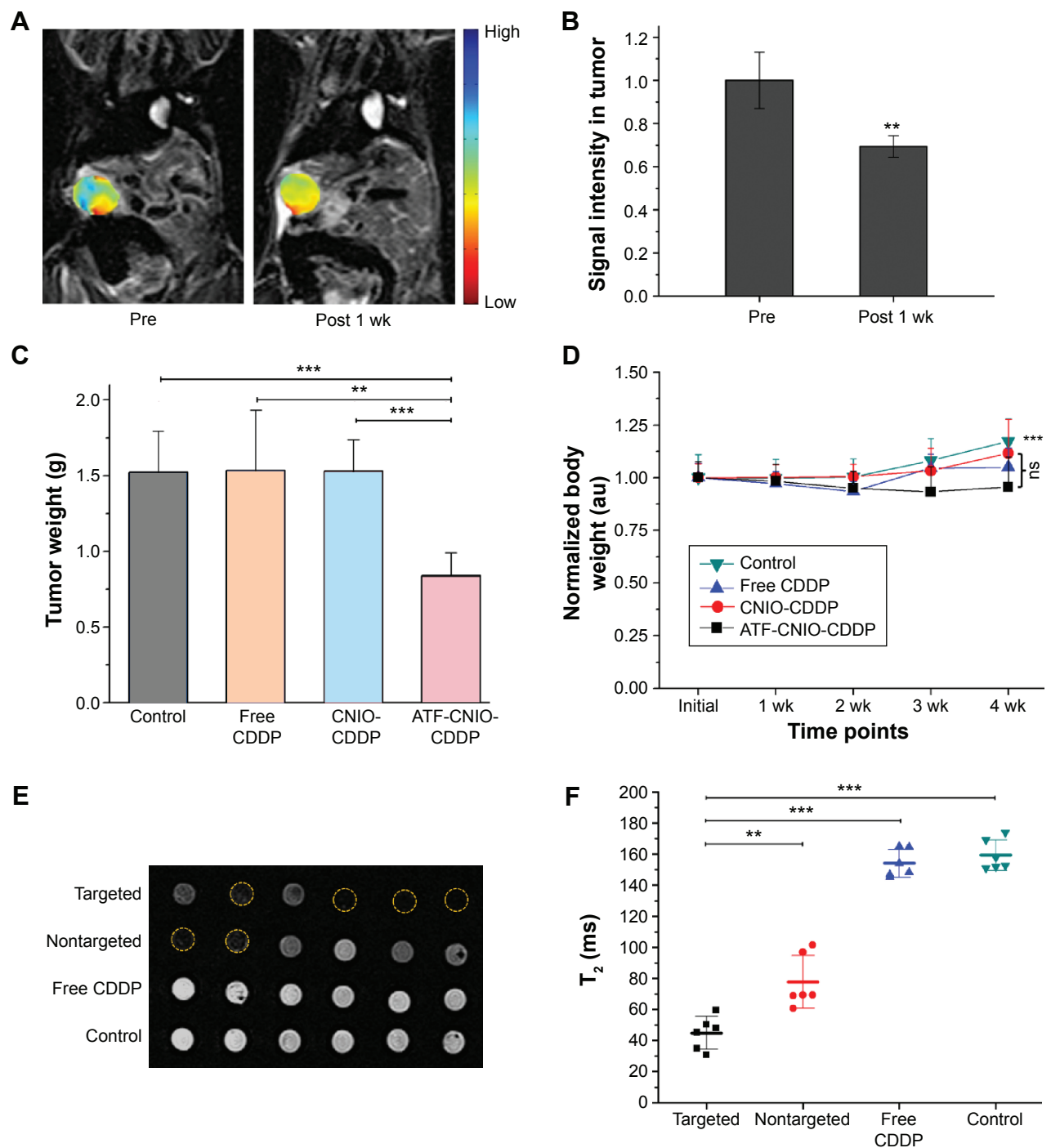
The accumulation and distribution of drug-loaded nanoparticles at the tumor site was monitored by in vivo MRI before and 1 week after administering ATF-CNIO-CDDP. Regions of interest were drawn at the level of the maximum diameter of the tumor using the corresponding T<sub>2</sub>-weighted scans, excluding regions of pancreatic ducts, cystic lesions, and fat. Significant MRI signal intensity (SI) drops were observed in tumor areas after the administration of ATF-CNIO-CDDP, as shown in Figure 3A, resulting from the accumulation of these magnetic nanoparticles at the tumor site. The heterogeneous distribution of ATF-CNIO-CDDP reflected the tumor heterogeneity, with SI drop observed in both peripheral and central areas, indicating the efficient delivery and perfusion into tumor. The average decrease of SI in the tumor was estimated to be ~31% after administration of ATF-CNIO-CDDP (Figure 3B).

## In vivo test of the anticancer efficacy of ATF-CNIO-CDDP

Therapeutic efficacy of ATF-CNIO-CDDP was evaluated using orthotopic MIA PaCa-2 pancreatic tumor-bearing



**Figure 2** In vitro assay for targeting specific binding test of CNIO and ATF-CNIO nanoparticles and cellular cytotoxicity of ATF-CNIO-CDDP, CNIO-CDDP and free CDDP. **Notes:** (A) Representative Prussian blue staining micrographs (left) and magnifications (right) show the target specific binding of uPAR targeted ATF-CNIO comparing to non-targeted CNIO nanoparticles to human pancreatic cancer MIA PaCa-2 cells, which overexpress uPAR. Scale bars correspond to 40 and 20  $\mu\text{m}$  in full and magnified panels respectively. (B) In vitro cytotoxicity of ATF-CNIO-CDDP, CNIO-CDDP and free CDDP at various concentrations against MIA PaCa-2 cells measured by MTT cell proliferation assay. **Abbreviations:** ATF, amino-terminal fragment; au, absorbance units; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide; uPAR, urokinase plasminogen activator receptor.



**Figure 3** Treatment efficacy of ATF-CNIO-CDDP in the orthotopic pancreatic tumor model evaluated by MRI.

**Notes:** (A) In vivo  $T_2$ -weighted MRI of a mouse bearing orthotopic pancreatic tumor, overlapped with  $T_2$  mapping MRI of tumor, before and 1 week after the treatment. (B) Corresponding quantitative MR signal changes. Data are presented as mean  $\pm$  SD ( $n=3$ ). (C) Comparison of the averaged tumor weights from different treatment groups ( $n=6$ ) showed the significant inhibition of the tumor growth by ATF-CNIO-CDDP ( $P<0.01$ ) after once-weekly IV administration for 4 weeks, and (D) the changes of relative body weight over the treatment course. (E) Ex vivo  $T_2$ -weighted MR images of tumors collected from mice after the 4-week treatment, and (F) the corresponding  $T_2$  relaxation time measured by MRI. \*\* $P<0.01$ , \*\*\* $P<0.001$ .

**Abbreviations:** ATF, amino-terminal fragment; au, absorbance unit; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide; IV, intravenous; MRI, magnetic resonance imaging; ns, nonsignificant; SD, standard deviation; wk, week.

mice ( $n=6$ ) in comparison with PBS, nontargeted CNIO-CDDP, and free CDDP. As shown in Figure 3C, ATF-CNIO-CDDP exhibited superior antitumor activity compared to the other groups. The average tumor weight from the

ATF-CNIO-CDDP-treated group was  $0.8\pm 0.1$  g, compared with around 1.5 g for the other groups ( $P<0.01$ ). No significant tumor suppression evaluated by the tumor weight was observed for the groups treated with free CDDP and

nontargeted CNIO-CDDP; however, histological studies revealed the inhibition of tumor metastasis in neighboring organs after the animals received either CDDP or CNIO-CDDP or ATF-CNIO-CDDP, respectively (Figure S1). In addition, less body weight change was observed in mice treated with CDDP, CNIO-CDDP, or ATF-CNIO-CDDP than the control group treated with PBS (Figure 3D), which gained 17% of initial body weight due to the malignant ascites caused by the metastasis. Reduced anaphylaxis, such as skin irritation and ulceration, was observed in the mice that received CNIO-CDDP or ATF-CNIO-CDDP, compared with those that received free CDDP, suggesting the protection and slow release of CDDP with CNIO and ATF-CNIO nanocarriers. Necropsy analysis of organ tissues collected from the animals treated with ATF-CNIO-CDDP showed no detectable toxicity in liver and spleen tissues, while hepatocellular damage was observed in the mouse livers treated with free CDDP (Figure S2), indicating that the delivery of CDDP with CNIO nanocarriers potentially reduced the CDDP systemic toxicity at the same dosage used in conventional delivery methods.

Prolonged circulation time and improved drug accumulation in the tumor have been obtained by using polymer- and lipid-based nanocarriers, compared with free small-molecule drugs.<sup>33,34</sup> Given the hydrodynamic size of ~30 nm, ATF-CNIO-CDDP can take advantage of the prolonged blood circulation half life time ( $t_{1/2}$ ~4.2 hours), allowing sufficient time to reach the targeted tumor, thus enhancing tumor accumulation via the enhanced permeability and retention (EPR) effect. The lower antitumor effect of free CDDP in the orthotopic pancreatic cancer model here can be explained by the fact that free CDDP has a much shorter blood circulation time and faster clearance, thus it fails to maintain a sufficient plasma level and gradient that can drive the drug to the tumor. Furthermore, the developed ATF-CNIO-CDDP demonstrated sustained release of CDDP, which potentially ensures the effective release inside a tumor after accumulation. All those favorable conditions may contribute to the observed better delivery of CDDP by the CNIO nanoparticle drug delivery system.

Pancreatic tumors are noted for the abundant stromal structures and poorly developed vasculature, impairing the therapeutic efficiency.<sup>35-38</sup> Among the cancer biomarkers, uPAR is known to be overexpressed in both tumor cells and stromal structures. ATF has been demonstrated to be able to target uPAR-expressing cancer cells when being used as the targeting ligand conjugated on nanoparticle drug carriers.<sup>25,26</sup> Therefore, this targeting approach is

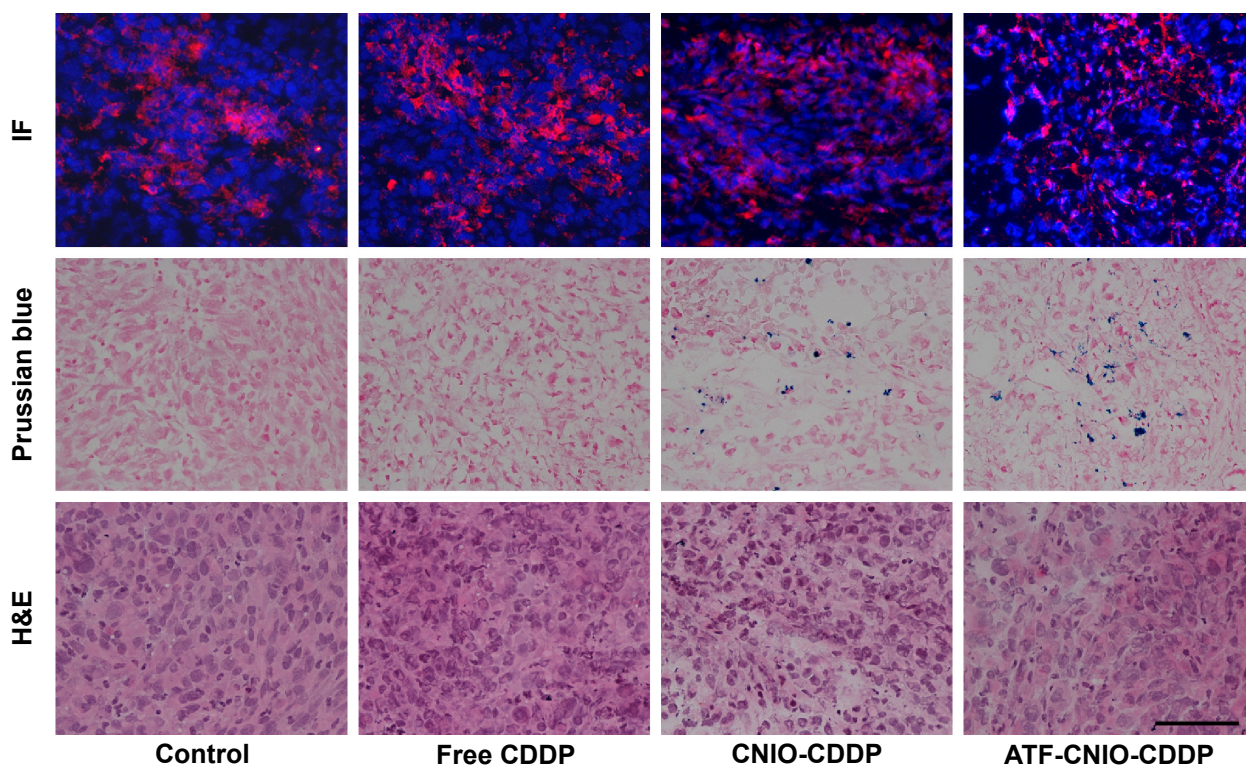
expected to promote the delivery of ATF-CNIO-CDDP into pancreatic tumors, resulting in higher accumulation of ATF-CNIO-CDDP, which benefits from the greater cellular uptake via receptor-mediated endocytosis.<sup>39,40</sup> Earlier studies have proved that receptor-mediated targeting can enhance tumor accumulation rather than the EPR-effect-mediated delivery.<sup>41,42</sup> Here in this study, nontargeted CNIO-CDDP failed at improving the treatment efficacy *in vivo* due to the insufficient drug concentration inside the tumor, although these nontargeted CNIO-CDDP showed efficient tumor cell killing activity *in vitro*. In contrast, ATF-CNIO-CDDP showed potential against drug resistance for pancreatic cancer treatment by improving tumor targeting and tumor retention, as well as sustained- and pH-facilitated-release at the tumor site. Consequently, the results from the current study further demonstrate that active targeting can enhance therapeutic efficacy over passive targeting.

## Ex vivo and histological validations of targeted delivery of ATF-CNIO-CDDP in tumors

The improved delivery of ATF-CNIO-CDDP in tumors was further confirmed by *ex vivo* MRI measurement of the  $T_2$  relaxation time of tumor tissues. As shown in Figure 3E, ATF-CNIO-CDDP-treated tumors exhibited much darker  $T_2$  signals (ie, shorter  $T_2$  relaxation times) than those that received nontargeted CNIO-CDDP, indicating much higher accumulation of ATF-CNIO-CDDP in tumors. The average transverse  $T_2$  relaxation time, which is known to be dependent on the iron concentration,<sup>24</sup> was determined to be 44.8 ms for the ATF-CNIO-CDDP-treated tumors, which is about half of the  $T_2$  for the tumors treated with CNIO-CDDP (77.8 ms), and one-third of that for the tumors treated with free CDDP and PBS (154.0, 159.3 ms, respectively) (Figure 3F).

To validate the targeted delivery of ATF-CNIO-CDDP, Prussian blue staining for Fe and immunofluorescence labeling of uPAR were performed on the collected tumor sections. ATF-CNIO-CDDP was found to be colocalized well with areas that express high levels of uPAR (Figure 4). In addition, more intense Prussian blue stains were observed in the tumor sections from the ATF-CNIO-CDDP-treated group compared to other groups, further confirming the higher accumulation of ATF-CNIO-CDDP in tumors. To investigate the effect of the tumor microenvironment on delivery, we particularly examined collagen fibers, which are the main component of tumor stroma, with haematoxylin and eosin (H&E) and Sirius red staining. The results from Sirius red staining in which collagen was stained in red showed that there was a





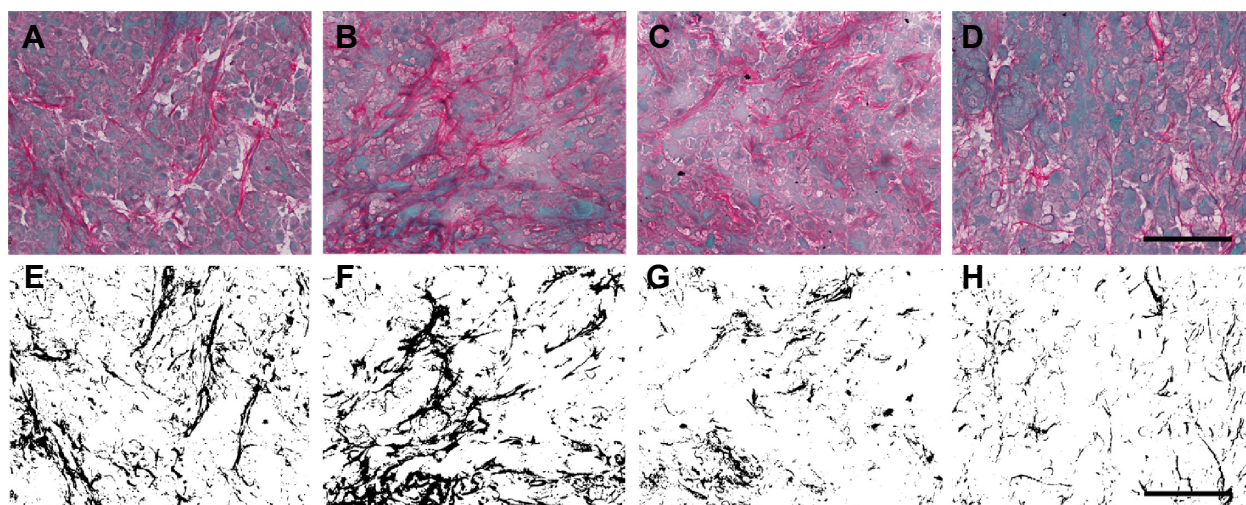
**Figure 4** Histological validation of nanoparticle accumulation in orthotopic MIA PaCa-2 tumors with IF labeling of uPAR, Prussian blue for iron, and H&E staining. **Notes:** Heterogeneous expression of uPAR (in red) was detected in MIA PaCa-2 tumors, where nuclei were stained with DAPI (in blue). Prussian blue staining revealed the area accumulated with targeted ATF-CNIO-CDDP overlapped with the area showing uPAR overexpression. The scale bar is 50  $\mu$ m. **Abbreviations:** ATF, amino-terminal fragment; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide; H&E, hematoxylin and eosin; IF, immunofluorescence; uPAR, urokinase plasminogen activator receptor; DAPI, 4',6-diamidino-2-phenylindole.

decrease in the amount of collagen bundles in tumors after the treatment with ATF-CNIO-CDDP when compared to the tumors that received other treatments (Figure 5). Although the mechanism and effect of the ATF-CNIO-CDDP treatment on the tumor microenvironment remain to be fully investigated, the decrease of collagen bundles may indicate the disruption

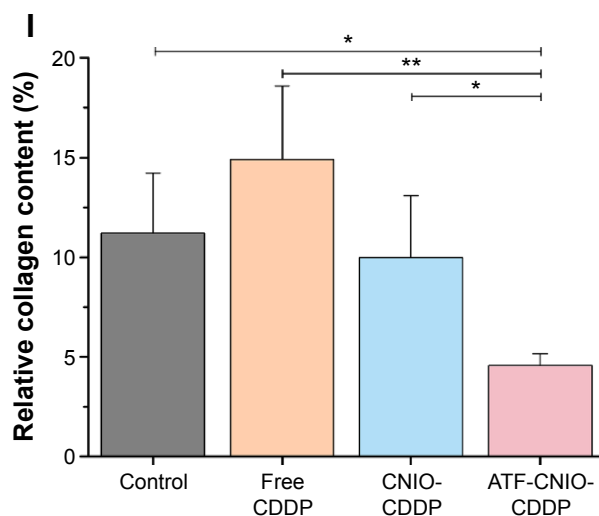
of the tumor stroma, thus leading to more efficient delivery of the ATF-CNIO-CDDP and improved treatment.<sup>43</sup>

## Conclusion

A new class of multifunctional nanotheranostics that combines imaging capability (ie, MRI), tumor targeting,



**Figure 5** (Continued)



**Figure 5** Sirius red staining and quantitative analysis of collagen fiber bundle of orthotopic MIA PaCa-2 tumors after treatment.

**Notes:** (A–D) Representative Sirius red staining of tumor sections from treated and untreated groups and (E–H) the extracted collagen bundles from corresponding images, which revealed fewer collagen bundles in ATF-CNIO-CDDP treated tumors. The scale bar is 50  $\mu\text{m}$ . (I) Relative collagen contents of tumors treated with different CDDP formulations which were estimated based on analysis of semiautomatic segmentation of the collagen bundles stained from corresponding images of Sirius red stained tumor sections. \* $P < 0.05$ , \*\* $P < 0.01$ .

**Abbreviations:** ATF, amino-terminal fragment; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide.

and drug delivery has been developed with milk protein (casein)-coated iron oxide nanoparticles. With the ATF ligand, ATF-CNIO-CDDP nanoparticles actively targeted uPAR-overexpressed pancreatic tumor and tumor stroma in vivo, promoting sufficient tumor-targeted delivery of CDDP. The sustained- and low-pH-facilitated release of CDDP following the improved accumulation in tumor facilitated the antitumor activity. Subsequently, ATF-CNIO-CDDP demonstrated improved tumor inhibition and reduced side effects in orthotopic pancreatic tumor mouse models, exhibiting high relevance to clinical research. Furthermore, the delivery of active drugs by these nanovehicles could be monitored by MRI in vivo. As such, milk-protein-coated magnetic nanoparticles may offer a promising platform for image-guided and targeted delivery in cancer treatment.

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## Disclosure

The authors report no conflicts of interest in this work.

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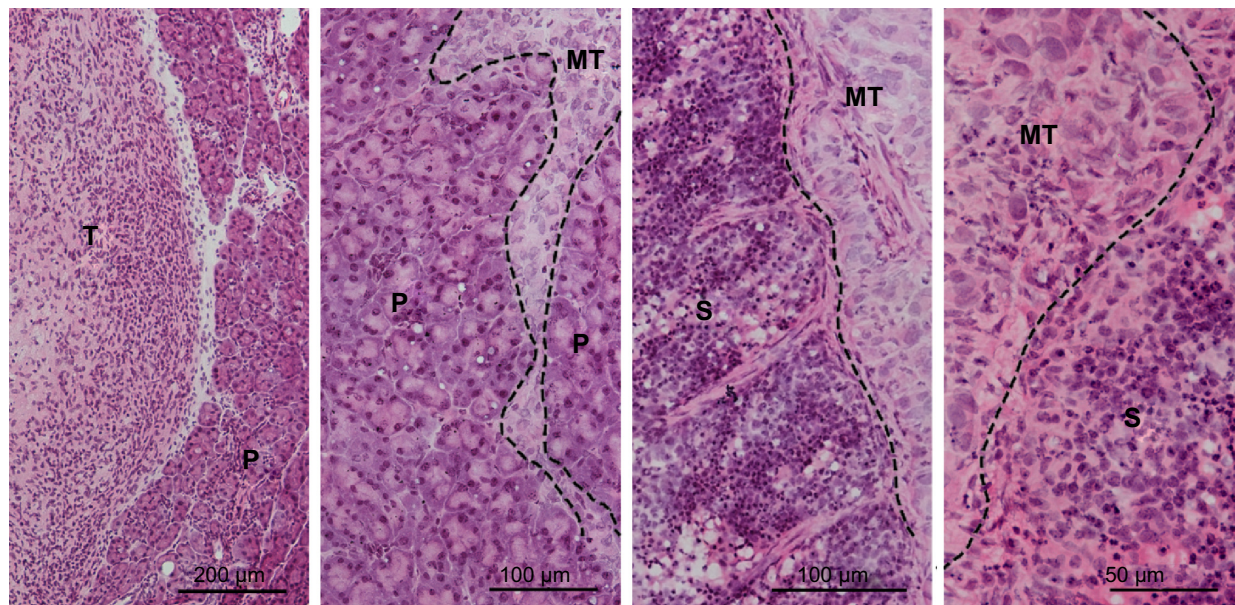
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## Supplementary materials

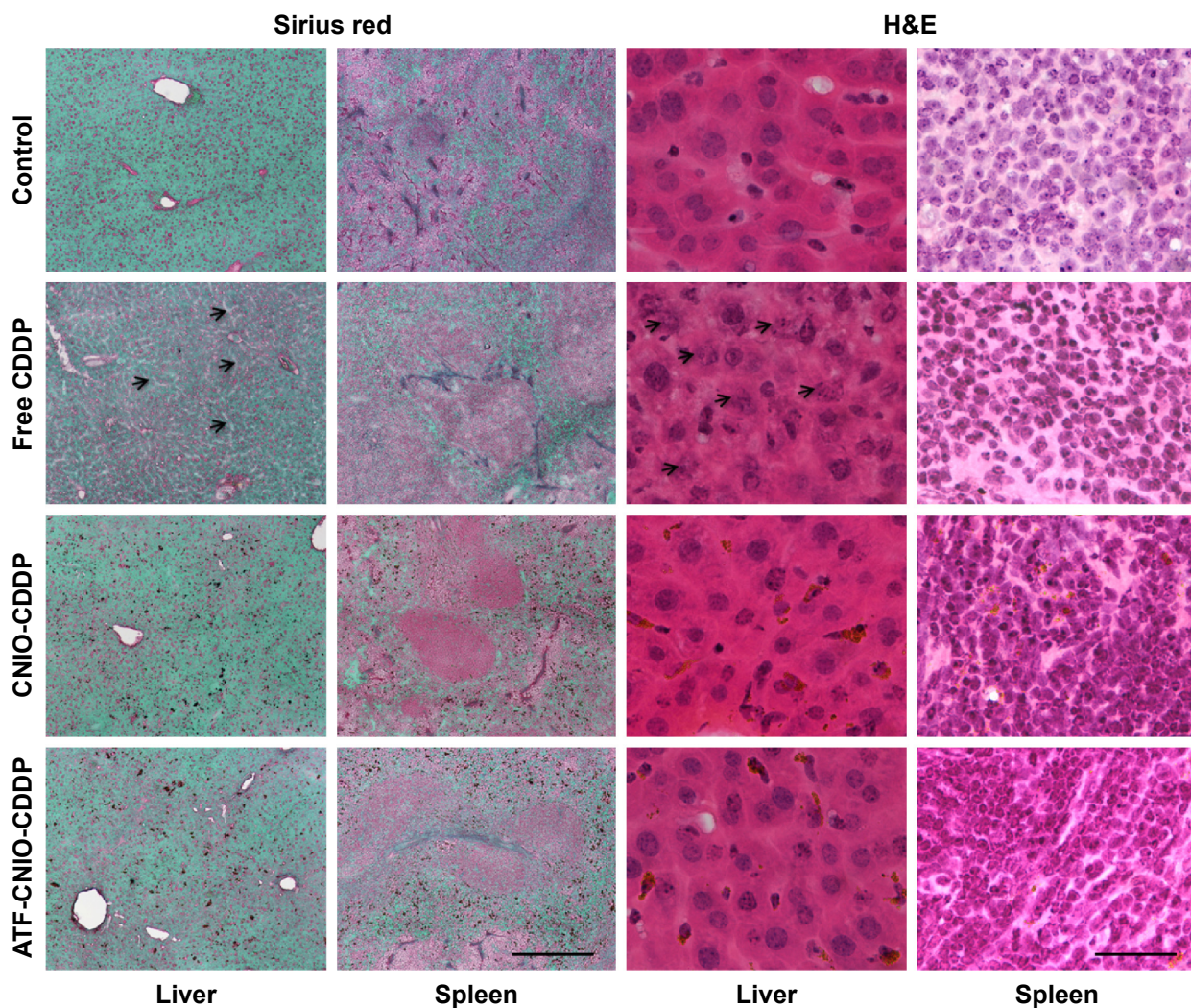


**Figure S1** Representative H&E staining of initial and metastatic tumors from the group treated with PBS only.

**Notes:** Most of the tumors (T) have obvious boundary along with pancreas (P) (left first panel), while metastatic tumors (MT) were observed invading into deeper pancreas (P) or spleen (S). No such metastasis was observed in the groups treated with free CDDP, CNIO-CDDP, or ATF-CNIO-CDDP.

**Abbreviations:** ATF, amino-terminal fragment; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide; H&E, hematoxylin and eosin; PBS, phosphate-buffered saline.





**Figure S2** Representative Sirius red and H&E staining of liver and spleen sections.

**Notes:** As indicated by black arrows, hepatic degeneration and vacuolization with necrotic cells were observed in the group that received free CDDP, while little damage was observed in the groups that received CNIO-CDDP and ATF-CNIO-CDDP, demonstrating reduced systemic toxicity to normal tissues by nanocarriers. The scale bar is 100 and 50  $\mu\text{m}$ , respectively.

**Abbreviations:** ATF, amino-terminal fragment; CDDP, cisplatin; CNIO, milk protein (casein)-coated magnetic iron oxide; H&E, hematoxylin and eosin.

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