#### Check for updates

#### OPEN ACCESS

EDITED BY Qichang Mei, Ningbo University, China

#### REVIEWED BY

Alessandra Bento Matias, Faculty of Medicine, University of São Paulo, Brazil Duo Wai-Chi Wong, Hong Kong Polytechnic University, Hong Kong SAR, China

\*CORRESPONDENCE Shen Zhang, zhangshen0708@163.com

#### SPECIALTY SECTION

This article was submitted to Biomechanics, a section of the journal Frontiers in Bioengineering and Biotechnology

RECEIVED 19 August 2022 ACCEPTED 20 September 2022 PUBLISHED 05 October 2022

#### CITATION

Shen B, Zhang S, Cui K, Zhang X and Fu W (2022), Effects of a 12-week gait retraining program combined with foot core exercise on morphology, muscle strength, and kinematics of the arch: A randomized controlled trial. *Front. Bioeng. Biotechnol.* 10:1022910. doi: 10.3389/fbioe.2022.1022910

#### COPYRIGHT

© 2022 Shen, Zhang, Cui, Zhang and Fu. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

# Effects of a 12-week gait retraining program combined with foot core exercise on morphology, muscle strength, and kinematics of the arch: A randomized controlled trial

Bin Shen<sup>1</sup>, Shen Zhang<sup>2,3,4</sup>\*, Kedong Cui<sup>1</sup>, Xini Zhang<sup>1</sup> and Weijie Fu<sup>1.3,4</sup>

<sup>1</sup>School of Exercise and Health, Shanghai University of Sport, Shanghai, China, <sup>2</sup>School of Athletic Performance, Shanghai University of Sport, Shanghai, China, <sup>3</sup>Key Laboratory of Exercise and Health Sciences of Ministry of Education, Shanghai University of Sport, Shanghai, China, <sup>4</sup>Shanghai Frontiers Science Research Base of Exercise and Metabolic Health, Shanghai University of Sport, Shanghai, China

**Objective:** This study aims to explore the effects of a 12-week gait retraining program combined with foot core exercise on arch morphology, arch muscles strength, and arch kinematics.

**Methods:** A total of 26 male recreational runners with normal arch structure who used rear-foot running strike (RFS) were divided into the intervention group (INT group) and control group (CON group) (n = 13 in each group). The INT group performed a 12-week forefoot strike (FFS) training combined with foot core exercises. The CON group did not change the original exercise habit. Before and after the intervention, the arch morphology, as well as the strength of hallux flexion, lesser toe flexion, and the metatarsophalangeal joint (MPJ) flexors were measured in a static position, and changes in the arch kinematics during RFS and FFS running were explored.

**Results:** After a 12-week intervention, 1) the normalized navicular height increased significantly in the INT group by 5.1% (p = 0.027, Cohen's d = 0.55); 2) the hallux absolute flexion and relative flexion of the INT group increased significantly by 20.5% and 21.7%, respectively (p = 0.001, Cohen's d = 0.59; p = 0.001, Cohen's d = 0.73), the absolute and relative strength of the MPJ flexors of the INT group were significantly improved by 30.7% and 32.5%, respectively (p = 0.006, Cohen's d = 0.94; p = 0.006, Cohen's d = 0.96); 3) and during RFS, the maximum arch angle of the INT group declined significantly by 5.1% (p < 0.001, Cohen's d = 1.49), the arch height at touchdown increased significantly in the INT group by 32.1% (p < 0.001, Cohen's d = 1.98).

**Conclusion:** The 12-week gait retraining program combined with foot core exercise improved the arch in both static and dynamic positions with a moderate to large effect size, demonstrating the superiority of this combined intervention over the standalone interventions. Thus, runners with

weak arch muscles are encouraged to use this combined intervention as an approach to enhance the arch.

KEYWORDS

gait retraining, foot core exercises, arch morphology, arch muscles strength, arch kinematics

# 1 Introduction

Running is one of the most popular fitness activities today as it offers easy accessibility and obvious health gains (De Wit et al., 2000). Many researchers have investigated extrinsic and intrinsic risk factors to reduce the risk of running-related injuries (Hespanhol Junior et al., 2016; Kelly et al., 2016; Krabak et al., 2017; Yang et al., 2020). However, in the past 50 years, the rate of various lower limb injuries caused by running has remained at a relatively high level (Kakouris et al., 2021), of which the incidence of foot injuries, such as plantar fascia injury, accounted for about 20% (Taunton et al., 2002). The fascia and ligaments of the plantar are important structures that maintain the dome structure of the foot. However, maintaining the stability of the medial longitudinal arch (MLA) during gait and controlling the movement of the foot rely on the intrinsic and extrinsic foot muscles (McKeon et al., 2015). Weak foot muscles cannot provide sufficient support to MLA during dynamic movement, resulting in repeated strains of the plantar fascia, which in turn, increase the risk of plantar injuries (Cheung et al., 2016).

The anatomical structure of the longitudinal arch gives it spring-like compression and rebound characteristics, which are affected by different running postures and modern running shoes (Lieberman, 2012; Perl et al., 2012). For rearfoot strike (RFS) running, MLA rarely compresses from the foot touch down to mid-stance. In addition, impact transients associated with RFS running are sudden forces with high rates and magnitudes of loading that travel rapidly up to the musculoskeletal system, thus resulting in a high incidence of running-related injuries, especially tibial stress fractures and plantar fasciitis (Kakouris et al., 2021; Milner et al., 2006; Lieberman et al., 2010). As a result, RFS runners prefer to wear cushioned running shoes with an elastic material in the heel to reduce the transient impact forces and disperse them over time (Lieberman et al., 2010; Zhang et al., 2019). Although modern cushioned running shoes have certain shock absorption advantages, some scholars believe that the thick cushioning medium between the foot and the ground surface may damage the feedback effect of plantar mechanoreceptors (Lieberman, 2012), thus limiting arch compression and rebound, resulting in the loss of elastic work and increased metabolic energy costs (Perl et al., 2012; Stearne et al., 2016). In contrast, the arch undergoes a three-point bending during the touchdown phase of the forefoot strike (FFS) running (Perl et al., 2012). To better control arch deformation, the foot muscles will have adaptive muscle strength enhancement (Jenkins and Cauthon,

2011; Perl et al., 2012; Kelly et al., 2018). Meanwhile, the longitudinal and transverse arches include many elastic tissues that recover an estimated 17% of the mechanical energy generated per step (Ker et al., 1987). Hence, FFS can be regarded as good training to enhance the performance of the arch (Kelly et al., 2018).

Foot core exercise includes foot doming, towel curls, toe spread, and more (Lynn et al., 2012; Goo et al., 2014; Kamonseki et al., 2016). In addition, the FFS has also been proven to effectively stimulate the foot muscles and strengthen the muscle function of the foot (Kelly et al., 2018). Numerous studies have investigated the separate effects of two interventions, namely, the effect of minimal shoes or FFS on foot muscles strength or size (Miller et al., 2014; Ridge et al., 2019), and the effects of foot core exercise on the balance and postural control (Rothermel et al., 2004; Lynn et al., 2012; Mulligan and Cook, 2013). However, foot core exercise alone may fail to meet the functional requirements of the arch under dynamic conditions (e.g., running, jumping.), while FFS training alone may increase the risk of running-related injury because the foot structure cannot support the rapid increase in load caused by the sudden change in strike pattern (Ridge et al., 2013). A more appropriate training program would be a combined intervention to enhance both the intrinsic and extrinsic foot muscles (i.e., active subsystem) of the foot core system, which can simultaneously improve foot function in static posture and dynamic activities (McKeon et al., 2015). Accordingly, previous gait retraining studies have begun to incorporate foot core exercise to reduce the risk of injury in participants when the strike pattern suddenly changes (Warne et al., 2014; Deng et al., 2020; Zhang et al., 2021). Nevertheless, few studies have investigated the effect of this combined intervention on the MLA at a static position and during running. Furthermore, as the conversion of RFS to FFS is a gradual process (McCarthy et al., 2014; Zhang et al., 2020), the effects of intervention training on arch kinematics reflected in both RFS and FFS remain unclear and require further exploration.

Therefore, this study aims to investigate the effects of a 12week gait retraining program combined with foot core exercise on arch morphology in static postures, arch muscles strength (i.e., separated toe flexion strength and the metatarsophalangeal joints (MPJ) flexor strength), and arch kinematics changes during RFS and FFS running among RFS runners. We hypothesized that the intervention would benefit arch shape maintenance, enhance arch muscle strength, and produce favorable changes in arch kinematics during running.

# 2 Methods

#### 2.1 Participants

Based on the previous data (a significant group\*time interaction effect on toe-flexor strength, effect size f = 0.6) published by Day and Hahn (2019), a priori power analysis (G\*Power, Version 3.1.9.6, Kiel University, Germany) was conducted for expected outcomes with a type I error probability of 0.05 and an effect size f of 0.6 (Cohen defines effect size f of 0.1, 0.25, and 0.4 as small, medium, and large effects, respectively). This analysis indicated that n = 26 would provide a statistical power of ~95% (Faul et al., 2007). Considering a drop-out rate of 15-20%, 32 male recreational runners were recruited through online social media, running clubs, and flyers (Wang J et al., 2020). They were all habitual runners who run at least 20 km/week in the RFS pattern while running on the ground with cushioned shoes were recruited (Lieberman et al., 2010). The inclusion criteria included the following: 1) normal arch height index (AHI, the height of the dorsum of the foot at 50% of the foot length divided by the truncated foot length) ranging from 0.31 to 0.37 (Butler et al., 2008), 2) no musculoskeletal injuries over the past 1 year and good exercise ability, 3) running distance that did not change in 3 months, and 4) never attempted foot core exercises, such as those included in this study or FFS pattern. All the participants signed an informed consent form provided by the Human Ethics Committee of Shanghai University of Sport prior to the study (IRB no. 2017007). After the baseline measurement, the participants were divided randomly into the intervention group (INT) or control group (CON). A research assistant generated the randomization schedule using a computer program and handed the results of allocation to the participants in a sealed envelope, ensuring that the researchers involved in outcome measurement and data analysis were unaware of the allocation.

#### 2.2 Intervention

The INT group performed FFS training combined with foot core exercise (Tam et al., 2015; Krabak et al., 2017) to enhance intrinsic and extrinsic foot muscle strength during static and dynamic tasks. To ensure that the INT group can master the intervention method, we gathered the INT group and our running coach explained and demonstrated the FFS and foot core exercises in the first week. For the subsequent 11 weeks, the INT group underwent centralized training on an indoor track on our campus once a week. The foot core exercise protocol was based on previous literature and previous results of our team, and it had shown to be effective in enhancing foot muscles and potentially reducing the risk of injury (Warne et al., 2014; Ridge et al., 2019; Wang B et al., 2020; Zhang et al., 2021). It included

heel raises, towel curls, foot doming, toe spread, balance board, and foot relaxation exercises by stepping on a tennis ball with progressive intensity (Table 1).

During the FFS training, each participant was required to run in an FFS pattern and was given an appropriately fitted pair of Vibram Five Fingers shoes, which aimed to protect the foot soles from the rough ground and simulate barefoot running to give the participant a habituation process for the strike pattern transition (Paquette et al., 2013; McCarthy et al., 2014). The duration of FFS running was increased every week based on protocols from previous literature (Tam et al., 2015; Zhang et al., 2021) (Table 2). The INT group was allowed to do rear-foot strike running with cushioning running shoes when out of training to maintain a running distance of a total of at least 20 km/week.

Participants in the CON group were required to continue their regular running routines in an RFS pattern using cushioned running shoes and running at their habitual pace in places where they were accustomed to running (e.g., parks, roads, tracks.) for 12 weeks. All participants in the INT and CON groups were required to provide us feedback after each training, including running location, duration, and mileage, as well as photos while doing foot core exercises. During the entire experiment and intervention, no participants suffered injuries.

The criteria for successful intervention were as follows: 1) completion of all the tests, 2) no more than three times of absences, and 3) completion of the last three-week training. During the intervention period, the participants were allowed to postpone or quit due to injuries or personal reasons (Zhang et al., 2020).

#### 2.3 Arch morphology

Initially, a participant was in a standing posture, and the most prominent aspect of the navicular tuberosity was palpated by a certified rehabilitation therapist who performed all of the palpation, manual measurements, and marker sticking throughout the whole experiment (Langley et al., 2016). If the navicular tuberosity was not sufficiently prominent, we instructed the subject to maintain the foot adducted and identified the navicular tuberosity by palpation along the clearly visible tendon of the posterior tibialis (Golano et al., 2004). The position of navicular tuberosity was marked with a washable pen for subsequent measurements. Then, a digital caliper was used to test the arch morphology in the standing and sitting positions in this study. In the standing position, participants were required to keep upright and maintain a bilateral standing posture with their bare feet pelvis-width apart as they tried to make their legs as parallel as possible to avoid foot inversion or eversion. When switching to a sitting position, the participants sat back in the seat without moving their feet and kept their hip, knee, and ankle joints in 90° flexion, as well as the hands hanging at

	1 ~ 2 weeks	3 ~ 4 weeks	5 ~ 6 weeks	7 ~ 8 weeks	9 ~ 10 weeks	11 ~ 12 weeks
Heel raises (double in a flat)	$1 \times 10$ times	$2 \times 10$ times	$2 \times 15$ times	_	_	_
Heel raises (double on a step)	_	_	_	$2 \times 20$ times	$2 \times 25$ times	$3 \times 30$ times
Heel raises (single on a step)	_	_	_	$1 \times 10$ times	$2 \times 10$ times	$3 \times 15$ times
Towel curls	$3 \times 10$ times	$3 \times 20$ times	$3 \times 10$ times (+0.25 kg)	$3 \times 15$ times (+0.25 kg)	$3 \times 10$ times (+0.5 kg)	$3 \times 15$ times (+0.5 kg)
Foot doming	$2 \times 10$ times	$2 \times 15$ times	$2 \times 20$ times	$3 \times 20$ times	$3 \times 25$ times	$4 \times 25$ times
Toe spread	$2 \times 10$ times	$2 \times 15$ times	$2 \times 20$ times	$3 \times 20$ times	$3 \times 25$ times	$4 \times 25$ times
Balance board	$2 \times 20 \text{ s}$	$2 \times 25 \text{ s}$	$2 \times 30 \text{ s}$	$3 \times 30 \text{ s}$	3 × 35 s	$3 \times 40 \text{ s}$
Foot relaxes	$1 \times 30 \text{ s}$	$1 \times 30 \text{ s}$	$1 \times 30 \text{ s}$	$1 \times 30 \text{ s}$	$1 \times 30 \text{ s}$	$1 \times 30 \text{ s}$

TABLE 1 Foot core exercise schedule.

TABLE 2 FFS training schedule.

Week	1	2	3	4	5	6	7	8	9	10	11	12
Duration (min)	5	10	15	20	25	30	35	40	42	44	46	48
Times per week	3	3	3	3	3	3	3	3	3	3	3	3



the sides of the body. Then, both forefeet were raised and lowered on the ground with subtalar joint in a natural position. The arch morphological variables (Williams and Mcclay, 2000; Fiolkowski et al., 2003) included the following: 1) standing/sitting arch height: distance from navicular center to the ground; 2) normalized arch height: navicular height divided by foot length; and 3) navicular drop: the difference between standing arch height and sitting arch height (Figure 1).

# 2.4 Arch muscles strength

#### 2.4.1 Separated toe flexion strength

A modified dynamometer (Ailitech ADF 500, China) attached to a wooden frame (Figure 2) was used to measure the hallux flexion initially, and then simultaneously with the lesser toe flexion (from 2nd to 5th toes). The board under the foot can provide support from the heel to the head of the first metatarsal, thereby allowing toe flexion. To avoid missing the force values, metal hooks and rings were used to connect the toes and the dynamometer. During the test, participants were required to maintain a sitting position with the hip, knee, and ankle joints flexed at 90°.

To test hallux flexion, the hallux was aligned with the dynamometer and then a metal ring was set to the hallux. When the hallux relaxed, the force value was 0 N. The participants were required to flex their big toe and pull the ring back as hard as possible. The tests were repeated if the participants' heel and/or ball of the foot left the board. The combined strength of the 2nd to 5th toes was assessed in a similar manner. This method has been associated with excellent repeatability and reliability for all tests between days, raters, and sessions (Ridge et al., 2017; Zhang et al., 2019).

#### 2.4.2 Metatarsophalangeal joint flexors strength

A customized strength tester (CN103278278B, China) was used to measure the MPJ flexors strength with the sampling rate of 120 Hz. The strength tester consisted of a chassis, a seat, force sensors, a computer, a foot platform, and a  $30^{\circ}$  raised toe platform,





and was similar to the device used in the study of Man et al. (2016). The participants were required to sit on a chair with their knees and feet fixed by a stopper plate to avoid the data being interfered with by other joints. During the tests, they were asked to keep the toes as close to the surface of the toe platform as possible and then try their best to flex all their MPJs together for 10 s to press the toe platform. If there was an elevation of the interphalangeal joints, the test was considered a failure and then repeated after a short rest. The tester used the pedal movement is transmitted the metatarsophalangeal by the tension sensor (Figure 3). The MPJ flexor strength data were measured and processed using a computer. The interclass correlation coefficients (ICC = 0.874) of this measurement were calculated in SPSS to test the reliability between sessions of the same rater on the same day (Ridge et al., 2017; Zhang et al., 2019).

## 2.5 Arch kinematics and arch stiffness

A 12-camera motion analysis system (100Hz, Vicon Motion Analysis Inc., Oxford, United Kingdom) was used to obtain the three-dimensional (3D) kinematic data of the foot. Given the methodological design described in the previous study, more accurate data on the arch kinematics of participants were obtained by placing infrared reflective markers onto the dominant leg at the following landmarks in the barefoot condition (Perl et al., 2012): 1) the first toe, 2) the medial side of the first metatarsal joint, 3) the lateral side of the 5th metatarsal head, 4) the navicular tuberosity, 5) the highest point on the dorsum, 6) the medial calcaneus process, 7) the lateral calcaneus process, and 8) the location of Achilles tendon insertion on the calcaneus (Figure 4). Two 90  $\times$  60  $\times$  10 cm force platforms



FIGURE 4 Marker position

(1000 Hz, 9287 B, Kistler Corporation, Winterthur, Switzerland) were used to collect ground reaction force (GRF) simultaneously with 3D kinematic data using the Vicon workstation during running.

The INT and CON groups were assessed using RFS and FFS barefoot running tests pre- and post-intervention. We introduced the RFS pattern to the participants, which was defined as initial heel contact, and the FFS pattern as initial forefoot contact much like "running on one's toes" (Williams et al., 2012; Rice and Patel, 2017). Before the running tests, the participants performed a warm-up protocol consisting of 5 min on the treadmill at a self-selected speed running followed by a set of static stretching exercises. At the start of the recording sessions, the participants were instructed to practice running barefoot across the running path until they could touchdown naturally. Three successful trials were recorded while their right foot comes into contact with the force plate at a speed of 3.33 m/s ( $\pm$ 5%) (McCarthy et al., 2014).

Kinematic data and GRF were analyzed *via* the Visual 3D (V5, C-Motion, Inc., Germantown, MD, United States). All marker trajectories were filtered using a fourth-order Butterworth low-pass filter with a cut-off frequency of 7 Hz. The GRF was filtered with a cut-off frequency of 50 Hz (Kelly et al., 2018). The ankle joint rotation was calculated *via* Cardan sequencing where motion about the X-axis was defined as plantarflexion/dorsiflexion (Williams et al., 2012).

Arch kinematic variables included the following (Holowka et al., 2018): 1)  $\Delta$ arch angle, which is the angle variation of the metatarsal bone relative to the calcaneus from touchdown to the maximum angle; 2) maximum arch angle, which is the arch angle compressed to maximum value during the stance phase; 3) arch height at touchdown, which is the perpendicular distance at touchdown between the navicular tuberosity and a line bisecting the medial side of the first metatarsal head and the medial calcaneus process; and 4)  $\Delta$ arch height, which is the difference between arch height at touchdown and arch height at 50% of stance phase 5) arch stiffness, the change in arch height



dividing the vertical GRF at mid-stance normalized by (body mass)<sup>0.67</sup> (Figure 5).

# 2.6 Statistics

The results are shown with mean and standard deviation for each variable. All variables were inspected for normality and for homogeneity of variance between the two groups. Arch stiffness was log-transformed to achieve normality (Holowka et al., 2018). A  $2 \times 2$  mixed factor ANOVA with baseline data as a covariate was used to examine the interaction effects of groups (INT vs. CON) and time (before vs. after intervention) on the arch morphology, arch muscle strength, and arch kinematics variables (Wang et al., 2021). When a significant interaction effect or main effect was detected, independent *t*-tests and paired *t*-tests were TABLE 3 The basic information of participants.

Group	Age (yrs)	Height (cm)	Weight (kg)	AHI	Running distance (km/w)	Training frequency (d/w)
INT $(n = 13)$	25.2 ± 4.8	175.5 ± 8.2	72.8 ± 14.9	0.34 ± 0.02	29.4 ± 4.3	2.8 ± 0.4
CON (n = 13)	23.8 ± 1.7	176.6 ± 4.9	72.0 ± 7.1	$0.35\pm0.01$	28.8 ± 3.0	2.8 ± 0.4



used as a post-hoc test to compare differences between-groups and within-subjects, respectively. When a significant main effect of time was detected, independent *t*-tests were used to compare the differences in percentage changes between the two groups. Effect sizes were calculated for ANOVA and *t*-test comparisons using  $\eta_p^2$  and Cohen's *d* respectively.  $\eta_p^2$  of 0.01, 0.09, and 0.25 were respectively interpreted as small, medium and large effects, while Cohen's *d* of 0.2–0.5, 0.5–0.8 and >0.8 were respectively interpreted as small, moderate and large effects (Miller et al., 2014; Wang et al., 2021). The level of significance was set at  $\alpha = 0.05$ . If no significant changes were found, the Cohen's *d* was calculated and reported. All statistical analyses were performed in SPSS (19.0, SPSS Inc., Chicago, IL, U.S.A.).

## **3** Results

#### 3.1 Dropout rate

Six participants dropped out. Among them, three FFS participants were excluded from the test before training due to their inability to meet the inclusion criteria, one participant did not train for more than 4 weeks due to a



business trip, and two participants lost contact with us. Given that the per-protocol approach has been widely used in previous studies on gait retraining or foot muscle training (Miller et al., 2014; Ridge et al., 2019), which could be because including participants who did not complete the intervention program in the final analysis would underestimate the potential benefits of the intervention (Moher et al., 2010). Based on the above consideration, we also used a per-protocol approach to analyse all outcomes. Thus, 26 participants who completed the intervention and met the inclusion criteria (13 in the INT, 13 in the CON) were included in the final analysis and statistics (Table 3; Figure 6).

#### 3.2 Arch morphology

A significant main effect of time on the normalized standing arch height was observed ( $F_{1,23} = 6.430$ , p = 0.018,  $\eta_p^2 = 0.218$ ). Paired *t*-tests indicated that after the intervention, the normalized standing arch height increased significantly in the INT group by 5.1% (p = 0.027, Cohen's d = 0.55) while decreased in the CON group by 1.6% (p = 0.427, Cohen's d = 0.55)

0.18), and independent *t*-tests showed a significant difference in percentage changes between the INT group and the CON group (p = 0.025, Cohen's d = 0.94). There was no significant interaction effect or main effect on standing/sitting arch height and navicular drop (Figure 7).

#### 3.3 Arch muscles strength

#### 3.3.1 Separated toe flexion strength

Significant interaction effects between time and group on the hallux absolute flexion ( $F_{1,23} = 5.840$ , p = 0.024,  $\eta_p^2 =$ 0.202) and the hallux relative flexion ( $F_{1,23} = 4.974$ , p = 0.036,  $\eta_p^2 = 0.178$ ) were observed. Paired *t*-tests revealed that after the intervention, the hallux absolute flexion and relative flexion of the INT group increased significantly by 20.5% and 21.7%, respectively (p = 0.001, Cohen's d = 0.59; p =0.001, Cohen's d = 0.73), while the CON group showed no significant changes (p = 0.842, Cohen's d = 0.04; p = 0.762, Cohen's d = 0.06). There was no significant interaction effect or main effect on lesser toe absolute flexion and lesser toe relative flexion.

Variables	INT		CON		
	Pre	Post	Pre	Post	
Hallux absolute flexion (N)	103.31 ± 34.38	124.55 ± 37.25*	$118.65 \pm 25.97$	119.86 ± 31.00	
Hallux relative flexion (N/kg)	$1.43 \pm 0.39$	$1.74 \pm 0.44^{*}$	$1.67 \pm 0.44$	$1.70 \pm 0.50$	
Lesser toe absolute flexion (N)	$67.52 \pm 17.58$	90.79 ± 27.39	69.24 ± 22.95	$73.77 \pm 30.04$	
Lesser toe relative flexion (N/kg)	$0.94 \pm 0.21$	$1.29 \pm 0.43$	$0.98 \pm 0.34$	$1.05 \pm 0.46$	
Metatarsophalangeal joint flexors absolute strength (N)	83.47 ± 24.54	109.08 ± 29.71*	112.44 ± 41.57	108.36 ± 41.89	
Metatarsophalangeal joint flexors relative strength (N/kg)	$1.17\pm0.39$	$1.55 \pm 0.40^*$	$1.58 \pm 0.60$	$1.54\pm0.60$	

TABLE 4 Effects of a 12-week gait retraining program combined with foot core exercise on the arch muscles strength.

\* significant difference from pre- to post-tests.



#### 3.3.2 Metatarsophalangeal joint flexors strength

There were significant main effects of time on the absolute  $(F_{1,23} = 9.399, p = 0.005, \eta_p^2 = 0.290)$  and relative strength  $(F_{1,23} = 11.785, p = 0.002, \eta_p^2 = 0.339)$  of the MPJ flexors. Paired *t*-tests revealed that after the intervention, the absolute and relative strength of the MPJ flexors increased significantly in the INT group by 30.7% and 32.5%, respectively (p = 0.006, Cohen's d = 0.94; p = 0.006, Cohen's d = 0.96), while no significant changes in the CON group (p = 0.749, Cohen's d = 0.10; p = 0.813, Cohen's d = 0.07). (Table 4; Figure 8).

#### 3.4 Arch kinematics and arch stiffness

All participants exhibited consistent ankle dorsiflexion at touchdown in RFS (INT vs. CON in the pre-test:  $6.74 \pm 4.29$  vs.  $5.05 \pm 4.38$ ; INT vs. CON in the post-test:  $7.46 \pm 4.10$  vs.  $6.52 \pm 4.59$ ), and ankle plantarflexion at touchdown in FFS (INT vs. CON in the pre-test:  $-14.65 \pm 5.81$  vs.  $-15.48 \pm 4.31$ ; INT vs. CON in the post-test:  $-12.70 \pm 6.54$  vs.  $-14.59 \pm 3.83$ ).

During RFS, there was a significant interaction effect between time and group on the maximum arch angle

 $(F_{1,23} = 5.296, p = 0.031, \eta_p^2 = 0.187)$ , paired *t*-tests revealed that after the intervention, the maximum arch angle of the INT group declined significantly by 5.1% (p < 0.001, Cohen's d =1.49), while the CON group showed no significant change (p =0.733, Cohen's d = 0.08). The significant main effects of time were observed on  $\Delta$  arch angle ( $F_{1,23} = 6.885$ , p = 0.015,  $\eta_p^2 =$ 0.230), the arch height at touchdown ( $F_{1,23} = 41.658, p < 0.001$ ,  $\eta_p^2 = 0.644$ ),  $\Delta$ arch height ( $F_{1,23} = 13.949$ , p = 0.001,  $\eta_p^2 = 0.378$ ), and arch stiffness ( $F_{1,23} = 31.030, p < 0.001, \eta_p^2 = 0.574$ ). Paired t-tests indicated that after the intervention, the arch height at touchdown and the ∆arch height increased significantly in the INT group by 32.1% and 29.5%, respectively (p < 0.001, Cohen's d = 1.98; p = 0.023, Cohen's d = 0.71), and the arch stiffness decreased significantly in the INT group by 33.3% (p = 0.021, Cohen's d = 0.80, while no significant changes in the CON group (*p* = 0.811, Cohen's *d* = 0.08; *p* = 0.620, Cohen's *d* = 0.09; p = 0.210, Cohen's d = 0.42). Independent *t*-tests showed a significant difference in percentage changes between the INT group and the CON group on the arch height at touchdown (p <0.001, Cohen's d = 1.80).

During FFS, the significant main effects of time were observed on  $\Delta$  arch angle ( $F_{1,23} = 15.411$ , p = 0.001,  $\eta_p^2 =$ 

Variables	INT		CON		
	Pre	Post	Pre	Post	
RFS					
$\Delta$ Arch angle (°)	$11.29 \pm 1.47$	$11.22 \pm 2.26$	$9.69 \pm 3.74$	9.60 ± 2.79	
Maximum arch angle (°)	$170.07 \pm 6.51$	$161.45 \pm 5.00^*$	$160.58 \pm 5.47$	$160.20 \pm 4.63$	
Arch height at touchdown (cm)(cm)	$1.84 \pm 0.30^{*}$ #	$2.43 \pm 0.30^{*}$	$2.44 \pm 0.44$	$2.41 \pm 0.24$	
ΔArch height (cm)	$0.44 \pm 0.19$	$0.57 \pm 0.17^*$	$0.52 \pm 0.21$	$0.54 \pm 0.18$	
Arch stiffness (N/cm·kg <sup>2/3</sup> )	266.47 ± 142.63	$177.68 \pm 64.47^*$	269.20 ± 210.21	203.77 ± 71.77	
FFS					
$\Delta$ Arch angle (°)	$15.47 \pm 2.22$	$15.59 \pm 2.05$	$12.14 \pm 3.04$	13.59 ± 2.73	
Maximum arch angle (°)	$169.48 \pm 18.27$	$161.02 \pm 4.72$	$158.40 \pm 7.41$	$159.92 \pm 4.00$	
Arch height at touchdown (cm)(cm)	$2.47 \pm 0.33$	$2.72 \pm 0.30^{*}$	$2.71 \pm 0.56$	$2.68 \pm 0.20$	
$\Delta$ Arch height (cm)	$0.81 \pm 0.19$	$0.87 \pm 0.19$	$0.76 \pm 0.21$	$0.84 \pm 0.19$	
Arch stiffness (N/cm·kg <sup>2/3</sup> )	127.51 ± 30.25	119.15 ± 30.10	161.74 ± 76.30	132.75 ± 30.47	

TABLE 5 Effects of a 12-week gait retraining program combined with foot core exercise on the arch kinematics.

\* significant difference from pre- to post-tests.



0.401), the maximum arch angle ( $F_{1,23} = 221.248, p < 0.001, \eta_p^2 = 0.906$ ), the arch height at touchdown ( $F_{1,23} = 77.381, p < 0.001, \eta_p^2 = 0.771$ ),  $\Delta$ arch height ( $F_{1,23} = 13.565, p = 0.001, \eta_p^2 = 0.371$ ), and arch stiffness ( $F_{1,23} = 20.507, p < 0.001, \eta_p^2 = 0.471$ ). Paired

*t*-tests indicated that after the intervention, the arch height at touchdown increased significantly in the INT group (p = 0.040, Cohen's d = 0.81), while no significant changes in the CON group (p = 0.845, Cohen's d = 0.08) (Table 5; Figure 9).

# 4 Discussion

The purpose of this study was to investigate the effect of a 12week gait retraining program combined with foot core exercise on arch morphology and arch muscle strength, and to further explore changes in arch kinematics in the RFS and FFS patterns. Overall, 12-week gait retraining combined with foot core exercise improved the arch height when standing, strengthen the toe flexors, decrease the maximum arch angle, and increase the arch height at touchdown during RFS running. Furthermore, the proposed intervention caused adaptive changes in the arch and surrounding muscles, which were also reflected in the arch kinematic of the running gait.

#### 4.1 Arch morphology

The 12-week gait retraining combined with foot core exercise significantly increased the normalized standing arch height in the INT group, thus corroborating the finding of McKeon et al. (McKeon et al., 2015). Moreover, the improvement reached a moderate effect size (Cohen's d = 0.55), which was superior to previous studies with no significant changes in arch height after standalone interventions (Lynn et al., 2012; Miller et al., 2014). Some researchers pointed out that the function of the foot intrinsic muscles is directly related to the structure of the longitudinal arch (Fiolkowski et al., 2003; Soysa et al., 2012; Kelly et al., 2014; Xiao et al., 2020). For example, to prevent the occurrence of excessive arch deformation, the recruitment of foot muscles increases with external increasing load when a decrease in electromyographic activity of these muscles leads to an increase in the navicular drop, thus revealing the relationship between the lower extremity loading and the foot muscles activation levels (Fiolkowski et al., 2003; Kelly et al., 2014). Accordingly, the shape of the arch could be stabilized by strengthening the foot muscles using the rowel curls, foot doming, and toe spread, which were proven to be effective interventions to strengthen the arch muscles (Jung et al., 2011; Yoo, 2014; McKeon et al., 2015). In addition, forefoot strike running with minimal shoes can stimulate the arch muscle function development in the activity due to the lack of plantar support, which will increase the work requirements of the foot and ankle muscles (Altman and Davis, 2012). For example, an intervention comprising 12-week forefoot running in minimal shoes increased the anatomical cross-sectional area and muscle volume of flexor digitorum brevis and abductor digiti minimi (Miller et al., 2014). Studies have also shown that the crosssectional area is proportional to the maximum strength of the muscle (An et al., 1991). Given a number of studies that the foot intrinsic and extrinsic muscles are effective in maintaining the arch shape, the 12-week intervention method in this research can strengthen the function of the foot muscles and improve the arch shape under the condition of weight-bearing.

## 4.2 Arch muscles strength

After the 12-week gait retraining combined with foot core exercise, the strength of hallux flexion and the MPJ flexors improved effectively. It is worth noting that the improvements in arch muscles strength all had a moderate to large effect size, with the percentage change in relative strength of the MPJ flexors reaching 32.5%, which was higher than that achieved by Day and Hahn (2019) who used foot muscle training alone (27%). The plantar intrinsic muscles include abductor hallucis, flexor digitorum brevis and quadratus plantae as accessory toe flexors (Kelly et al., 2014), which produce force at the MPJ (Koyama et al., 2019). In the single-support phase and early stage of double support phase in the gait, the metatarsophalangeal moment plays a role in controlling the angular momentum of the whole body, with the maximum metatarsophalangeal moment being as large as one-fifth to one-third of the maximum ankle joint plantarflexion moment (Miyazaki and Yamamoto, 1993). Accordingly, the toe flexion and extension activities are particularly important in running and jumping, which need the action to push off. Therefore, many coaches of sprint and jumping events believe that increasing the output power of the MPJ can improve athletes' sports performance (Goldmann et al., 2013).

These muscles that affect the strength of the MPJ are also necessary structures to support the longitudinal arch. A previous study has provided evidence that strengthening these muscles can attenuate the mechanical load directly related to runningrelated injuries, with the result that participants in the foot core training group had a 2.42-fold lower rate of running-related injuries compared with the control group (Taddei et al., 2020). In our research, an intervention method combining FFS training and foot core exercise was used to try to strengthen the arch muscles' ability to exert force in a relatively static and running gait. Some of our findings confirm the hypothesis of this research, therefore, our methods can be referenced by athletes in running and jumping events to obtain stronger foot muscle function.

### 4.3 Arch kinematics and arch stiffness

During RFS, the 12-week gait retraining combined with foot core exercise reduced the maximal arch angle by 5.1% while increasing the arch height at touchdown by 32.1%. However, Day and Hahn (2019) showed that foot muscle training alone had no effect on the mechanics of the MPJ and ankle during running, suggesting that kinematic changes in this study may benefit from additional effects of the combined intervention. When a certain type of exercise forms a repetitive load on the body, special neuromuscular adaptability will appear, such as the sport-specific adaptability of foot muscle function and foot structure (Häkkinen and Keskinen, 1989; Koyama et al., 2019). In the late swing of FFS, the abductor hallucis activation is increased,

10.3389/fbioe.2022.1022910

resulting in a higher arch at touchdown to allow the midfoot to compress a larger range of motion during the stance phase without altering arch peak deformation (McDonald et al., 2016; Kelly et al., 2018). Considering the abovementioned results of arch muscle strength, the foot training methods in this research effectively enhanced the arch muscles, and the arch kinematic performance in running was improved to a certain extent. Furthermore, when considering how to increase the footspring function during the gait, Perl et al. (Perl et al., 2012) found that at the same running speed, the FFS pattern has higher arch compliance compared to RFS, which means a greater range of midfoot motion. As the foot intrinsic muscles and tendons have relatively long tendons, they can be stretched and shortened during the running stance phase, thus allowing the storage of energy in the tendons. The resulting higher compliance may be very conducive to elastic energy storage and release, thus reducing the elastic potential energy loss in this process (Kelly et al., 2018). This research found that after intervention training, RFS showed similarities in arch movement characteristics with the FFS, namely, the arch height increased at touchdown, and the motion of the midfoot increased. However, whether the increase in the motion of the midfoot during the RFS stance phase is conducive to the advancement of the body may require further analysis.

The arch stiffness decreased in the post condition during RFS, it may be that the participants gradually mastered a more comfortable running gait during multiple familiarization sessions prior to the test to reduce the peak impact in the RFS (Altman and Davis, 2012; Thompson et al., 2015). Furthermore, the greater decrease in stiffness in the INT group (33.3%) than in the CON group (24.3%) may benefit from the increased compliance of the arch due to the 12-week gait retraining program combined with foot core exercise (Kelly et al., 2018).

In summary, the 12-week gait retraining combined with foot core exercise in this study had certain effects on the arch morphology, arch muscle strength, and arch kinematics characteristics of RFS. As an important part of the lower limb system, whether the changes in the arch kinematics during the RFS are beneficial to the health of the foot may need further exploration.

There are several limitations to this study: 1) we did not continue to observe the adaptive changes of arch function in different running postures to judge the durability of the intervention; 2) arch dynamics were not analyzed in this study, which may further explore the arch work in different running strike patterns; and 3) only male habitual runners were recruited in this study.

# 5 Conclusion

The 12-week gait retraining program combined with foot core exercise significantly increased the normalized navicular height

during standing and the strength of arch muscles. During RFS running, such intervention decreased the maximum arch angle and increase arch height at touchdown, which indicated that the arch was improved in both static and dynamic positions. Furthermore, all of these significant changes had a moderate to large effect size, demonstrating the superiority of the combined intervention over the standalone interventions. Therefore, it is recommended that runners with weak arch muscles use this combined intervention as an approach to strengthen the arch muscles.

# Data availability statement

The original contributions presented in the study are included in the article/supplementary material, further inquiries can be directed to the corresponding author.

## Ethics statement

The studies involving human participants were reviewed and approved by the Human Ethics Committee of Shanghai University of Sport. The patients/participants provided their written informed consent to participate in this study.

# Author contributions

BS and SZ contributed to study design, data collection, drafting and revising the manuscript; KC and WF, contributed to supervising study design, completing data analysis and interpretation, and revising the manuscript; XZ revised the manuscript. All authors have read and approved the final version of the manuscript and agree with the order of the presentation of the authors.

# Funding

This research was funded by the National Key Technology Research and Development Program of the Ministry of Science and Technology of China (2021YFC2009201), the National Natural Science Foundation of China (12272238, 11772201), the "Outstanding Young Scholar" Program of Shanghai Municipal and the "Dawn" Program of Shanghai Education Commission, China (19SG47).

# Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

# Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated

## References

Altman, A. R., and Davis, I. S. (2012). Barefoot running: biomechanics and implications for running injuries. *Curr. Sports Med. Rep.* 11 (5), 244–250. doi:10. 1249/JSR.0b013e31826c9bb9

An, K. N., Linscheid, R. L., and Brand, P. W. (1991). Correlation of physiological cross-sectional areas of muscle and tendon. *J. hand Surg. Edinb. Scotl.* 16 (1), 66–67. doi:10.1016/0266-7681(91)90130-g

Butler, R. J., Hillstrom, H., Song, J., Richards, C. J., and Davis, I. S. (2008). Arch height index measurement system: establishment of reliability and normative values. J. Am. Podiatr. Med. Assoc. 98 (2), 102–106. doi:10.7547/0980102

Cheung, R. T. H., Sze, L. K. Y., Mok, N. W., and Ng, G. Y. F. (2016). Intrinsic foot muscle volume in experienced runners with and without chronic plantar fasciitis. *J. Sci. Med. Sport* 19 (9), 713–715. doi:10.1016/j.jsams.2015.11.004

Day, E. M., and Hahn, M. E. (2019). Increased toe-flexor muscle strength does not alter metatarsophalangeal and ankle joint mechanics or running economy. *J. Sports Sci.* 37 (23), 2702–2710. doi:10.1080/02640414.2019.1661562

De Wit, B., De Clercq, D., and Aerts, P. (2000). Biomechanical analysis of the stance phase during barefoot and shod running. *J. Biomechanics* 33 (3), 269–278. doi:10.1016/s0021-9290(99)00192-x

Deng, L., Zhang, X., Xiao, S., Yang, Y., Li, L., and Fu, W. (2020). Changes in the plantar flexion torque of the ankle and in the morphological characteristics and mechanical properties of the Achilles tendon after 12-week gait retraining. *Life* (*Basel*) 10 (9), 159. doi:10.3390/life10090159

Faul, F., Erdfelder, E., Lang, A. G., and Buchner, A. (2007). G\*Power 3: a flexible statistical power analysis program for the social, behavioral, and biomedical sciences. *Behav. Res. Methods* 39 (2), 175–191. doi:10.3758/bf03193146

Fiolkowski, P., Brunt, D., Bishop, M., Woo, R., and Horodyski, M. (2003). Intrinsic pedal musculature support of the medial longitudinal arch: an electromyography study. *J. Foot Ankle Surg.* 42 (6), 327–333. doi:10.1053/j.jfas.2003.10.003

Golano, P., Fariñas, O., and Sáenz, I. (2004). The anatomy of the navicular and periarticular structures. *Foot ankle Clin.* 9 (1), 1–23. doi:10.1016/S1083-7515(03) 00155-4

Goldmann, J. P., Sanno, M., Willwacher, S., Kai, H., and Brüggemann, G. P. (2013). The potential of toe flexor muscles to enhance performance. *J. Sports Sci.* 31 (4), 424–433. doi:10.1080/02640414.2012.736627

Goo, Y. M., Heo, H. J., and An, D. H. (2014). EMG activity of the abductor hallucis muscle during foot arch exercises using different weight bearing postures. *J. Phys. Ther. Sci.* 26 (10), 1635–1636. doi:10.1589/jpts.26.1635

Häkkinen, K., and Keskinen, K. L. (1989). Muscle cross-sectional area and voluntary force production characteristics in elite strength- and endurancetrained athletes and sprinters. *Eur. J. Appl. Physiol. Occup. Physiol.* 59 (3), 215–220. doi:10.1007/bf02386190

Hespanhol Junior, L. C., de Carvalho, A. C., Costa, L. O., and Lopes, A. D. (2016). Lower limb alignment characteristics are not associated with running injuries in runners: Prospective cohort study. *Eur. J. Sport Sci.* 16 (8), 1137–1144. doi:10.1080/ 17461391.2016.1195878

Holowka, N. B., Wallace, I. J., and Lieberman, D. E. (2018). Foot strength and stiffness are related to footwear use in a comparison of minimally- vs. conventionally-shod populations. *Sci. Rep.* 8 (1), 3679. doi:10.1038/s41598-018-21916-7

Jenkins, D. W., and Cauthon, D. J. (2011). Barefoot running claims and controversies: a review of the literature. *J. Am. Podiatr. Med. Assoc.* 101 (3), 231–246. doi:10.7547/1010231

Jung, D. Y., Kim, M. H., Koh, E. K., Kwon, O. Y., Cynn, H. S., and Lee, W. H. (2011). A comparison in the muscle activity of the abductor hallucis and the medial longitudinal arch angle during toe curl and short foot exercises. *Phys. Ther. Sport* 12 (1), 30–35. doi:10.1016/j.ptsp.2010.08.001

Kakouris, N., Yener, N., and Fong, D. T. P. (2021). A systematic review of running-related musculoskeletal injuries in runners. *J. Sport Health Sci.* 10 (5), 513–522. doi:10.1016/j.jshs.2021.04.001

Kamonseki, D. H., Goncalves, G. A., Yi, L. C., and Junior, I. L. (2016). Effect of stretching with and without muscle strengthening exercises for the foot and hip in

organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

patients with plantar fasciitis: A randomized controlled single-blind clinical trial. *Man. Ther.* 23, 76–82. doi:10.1016/j.math.2015.10.006

Kelly, L. A., Cresswell, A. G., Racinais, S., Whiteley, R., and Lichtwark, G. (2014). Intrinsic foot muscles have the capacity to control deformation of the longitudinal arch. J. R. Soc. Interface 11 (93), 20131188. doi:10.1098/rsif.2013.1188

Kelly, L. A., Farris, D. J., Lichtwark, G. A., and Cresswell, A. G. (2018). The influence of foot-strike technique on the neuromechanical function of the foot. *Med. Sci. Sports Exerc.* 50 (1), 98–108. doi:10.1249/mss.000000000001420

Kelly, L. A., Lichtwark, G. A., Farris, D. J., and Cresswell, A. (2016). Shoes alter the spring-like function of the human foot during running. *J. R. Soc. Interface* 13 (119), 20160174. doi:10.1098/rsif.2016.0174

Ker, R. F., Bennett, M. B., Bibby, S. R., Kester, R. C., and Alexander, R. M. (1987). The spring in the arch of the human foot. *Nature* 325 (7000), 147–149. doi:10.1038/325147a0

Koyama, K., Hirokawa, M., Yoshitaka, Y., and Yamauchi, J. (2019). Toe flexor muscle strength and morphological characteristics of the foot in judo athletes. *Int. J. Sports Med.* 40 (4), 263–268. doi:10.1055/a-0796-6679

Krabak, B., Lipman, G., and Waite, B. (2017). The long distance runner's guide to injury prevention and treatment: How to avoid common problems and deal with them when they happen. New York: Simon & Schuster.

Langley, B., Cramp, M., and Morrison, S. C. (2016). Clinical measures of static foot posture do not agree. *J. Foot Ankle Res.* 9, 45–46. doi:10.1186/s13047-016-0180-3

Lieberman, D. E., Venkadesan, M., Werbel, W. A., Daoud, A. I., D'Andrea, S., Davis, I. S., et al. (2010). Foot strike patterns and collision forces in habitually barefoot versus shod runners. *Nature* 463 (7280), 531–535. doi:10.1038/nature08723

Lieberman, D. E. (2012). What we can learn about running from barefoot running: an evolutionary medical perspective. *Exerc. Sport Sci. Rev.* 40 (2), 63–72. doi:10.1097/JES.0b013e31824ab210

Lynn, S. K., Padilla, R. A., and Tsang, K. K. (2012). Differences in static- and dynamic-balance task performance after 4 weeks of intrinsic-foot-muscle training: the short-foot exercise versus the towel-curl exercise. *J. Sport Rehabilitation* 21 (4), 327–333. doi:10.1123/jsr.21.4.327

Man, H. S., Leung, A. K., Cheung, J. T., and Sterzing, T. (2016). Reliability of metatarsophalangeal and ankle joint torque measurements by an innovative device. *Gait Posture* 48, 189–193. doi:10.1016/j.gaitpost.2016.05.016

McCarthy, C., Fleming, N., Donne, B., and Blanksby, B. (2014). 12 weeks of simulated barefoot running changes foot-strike patterns in female runners. *Int. J. Sports Med.* 35 (5), 443–450. doi:10.1055/s-0033-1353215

McDonald, K. A., Stearne, S. M., Alderson, J. A., North, I., Pires, N. J., and Rubenson, J. (2016). The role of arch compression and metatarsophalangeal joint dynamics in modulating plantar fascia strain in running. *PLoS One* 11 (4), e0152602. doi:10.1371/journal.pone.0152602

McKeon, P. O., Hertel, J., Bramble, D., and Davis, I. (2015). The foot core system: a new paradigm for understanding intrinsic foot muscle function. *Br. J. Sports Med.* 49 (5), 290. doi:10.1136/bjsports-2013-092690

Miller, E. E., Whitcome, K. K., Lieberman, D. E., Norton, H. L., and Dyer, R. E. (2014). The effect of minimal shoes on arch structure and intrinsic foot muscle strength. *J. Sport Health Sci.* 3 (2), 74–85. doi:10.1016/j.jshs.2014.03.011

Milner, C. E., Ferber, R., Pollard, C. D., Hamill, J., and Davis, I. S. (2006). Biomechanical factors associated with tibial stress fracture in female runners. *Med. Sci. Sports Exerc.* 38 (2), 323–328. doi:10.1249/01.mss.0000183477.75808.92

Miyazaki, S., and Yamamoto, S. (1993). Moment acting at the metatarsophalangeal joints during normal barefoot level walking. *Gait Posture* 1 (3), 133–140. doi:10.1016/0966-6362(93)90054-5

Moher, D., Hopewell, S., Schulz, K. F., Montori, V., Gøtzsche, P. C., Devereaux, P. J., et al. (2010). CONSORT 2010 explanation and elaboration: updated guidelines for reporting parallel group randomised trials. *BMJ* 340, c869. doi:10.1136/bmj.c869

Mulligan, E. P., and Cook, P. G. (2013). Effect of plantar intrinsic muscle training on medial longitudinal arch morphology and dynamic function. *Man. Ther.* 18 (5), 425–430. doi:10.1016/j.math.2013.02.007

Paquette, M. R., Zhang, S., and Baumgartner, L. D. (2013). Acute effects of barefoot, minimal shoes and running shoes on lower limb mechanics in rear and forefoot strike runners. *Footwear Sci.* 7 (3), 9–18. doi:10.1080/19424280.2012. 692724

Perl, D. P., Daoud, A. I., and Lieberman, D. E. (2012). Effects of footwear and strike type on running economy. *Med. Sci. Sports Exerc.* 44 (7), 1335–1343. doi:10. 1249/MSS.0b013e318247989e

Rice, H., and Patel, M. (2017). Manipulation of foot strike and footwear increases Achilles tendon loading during running. *Am. J. Sports Med.* 45 (10), 2411–2417. doi:10.1177/0363546517704429

Ridge, S. T., Johnson, A. W., Mitchell, U. H., Hunter, I., Robinson, E., Rich, B. S., et al. (2013). Foot bone marrow edema after a 10-wk transition to minimalist running shoes. *Med. Sci. Sports Exerc.* 45 (7), 1363–1368. doi:10.1249/MSS. 0b013e3182874769

Ridge, S. T., Myrer, J. W., Olsen, M. T., Jurgensmeier, K., and Johnson, A. W. (2017). Reliability of doming and toe flexion testing to quantify foot muscle strength. *J. Foot Ankle Res.* 10, 55. doi:10.1186/s13047-017-0237-y

Ridge, S. T., Olsen, M. T., Bruening, D. A., Jurgensmeier, K., Griffin, D., Davis, I. S., et al. (2019). Walking in minimalist shoes is effective for strengthening foot muscles. *Med. Sci. Sports Exerc.* 51 (1), 104–113. doi:10.1249/mss. 000000000001751

Rothermel, S. A., Hale, S. A., Hertel, J., and Denegar, C. R. (2004). Effect of active foot positioning on the outcome of a balance training program. *Phys. Ther. Sport* 5 (2), 98–103. doi:10.1016/s1466-853x(04)00027-6

Soysa, A., Hiller, C., Refshauge, K., and Burns, J. (2012). Importance and challenges of measuring intrinsic foot muscle strength. *J. Foot Ankle Res.* 5 (1), 29. doi:10.1186/1757-1146-5-29

Stearne, S. M., McDonald, K. A., Alderson, J. A., North, I., Oxnard, C. E., and Rubenson, J. (2016). The foot's arch and the energetics of human locomotion. *Sci. Rep.* 6, 19403. doi:10.1038/srep19403

Taddei, U. T., Matias, A. B., Duarte, M., and Sacco, I. C. N. (2020). Foot core training to prevent running-related injuries: A survival analysis of a single-blind, randomized controlled trial. *Am. J. Sports Med.* 48 (14), 3610–3619. doi:10.1177/0363546520969205

Tam, N., Tucker, R., Astephen Wilson, J. L., and Santos-Concejero, J. (2015). Effect on oxygen cost of transport from 8-weeks of progressive training with barefoot running. *Int. J. Sports Med.* 36 (13), 1100–1105. doi:10.1055/s-0035-1548888

Taunton, J. E., Ryan, M. B., Clement, D. B., Mckenzie, D. C., and Lloyd-Smith, D. R. (2002). Plantar fasciitis: a retrospective analysis of 267 cases. *Phys. Ther. Sport* 3 (2), 57–65. doi:10.1054/ptsp.2001.0082

Thompson, M. A., Lee, S. S., Seegmiller, J., and McGowan, C. P. (2015). Kinematic and kinetic comparison of barefoot and shod running in mid/forefoot and rearfoot strike runners. *Gait Posture* 41 (4), 957–959. doi:10.1016/j.gaitpost.2015.03.002

van Gent, R. N., Siem, D., van Middelkoop, M., van Os, A. G., Bierma-Zeinstra, S. M., Koes, B. W., et al. (2007). Incidence and determinants of lower extremity running injuries in long distance runners: a systematic review \* COMMENTARY. *Br. J. Sports Med.* 41 (8), 469–480. doi:10.1136/bjsm.2006.033548

Wang, B., Yang, Y., Zhang, X., Wang, J., Deng, L., and Fu, W. (2020). Twelveweek gait retraining reduced patellofemoral joint stress during running in male recreational runners. *BioMed Res. Int.* 2020, 1–9. doi:10.1155/2020/9723563

Wang, J., Luo, Z., Dai, B., and Fu, W. (2020). Effects of 12-week cadence retraining on impact peak, load rates and lower extremity biomechanics in running. *PeerJ* 8, e9813. doi:10.7717/peerj.9813

Wang, S., Chan, P. P. K., Lam, B. M. F., Chan, Z. Y. S., Zhang, J. H. W., Wang, C., et al. (2021). Sensor-based gait retraining lowers knee adduction moment and improves symptoms in patients with knee osteoarthritis: A randomized controlled trial. *Sensors (Basel)* 21 (16), 5596. doi:10.3390/s21165596

Warne, J. P., Kilduff, S. M., Gregan, B. C., Nevill, A. M., Moran, K. A., and Warrington, G. D. (2014). A 4-week instructed minimalist running transition and gait-retraining changes plantar pressure and force. *Scand. J. Med. Sci. Sports* 24 (6), 964–973. doi:10.1111/sms.12121

Williams, D. S., 3rd, Green, D. H., and Wurzinger, B. (2012). Changes in lower extremity movement and power absorption during forefoot striking and barefoot running. *Int. J. Sports Phys. Ther.* 7 (5), 525–532.

Williams, D. S., and Mcclay, I. S. (2000). Measurements used to characterize the foot and the medial longitudinal arch: reliability and validity. *Phys. Ther.* 80 (9), 864–871. doi:10.1093/ptj/80.9.864

Xiao, S., Zhang, X., Deng, L., Zhang, S., Cui, K., and Fu, W. (2020). Relationships between foot morphology and foot muscle strength in healthy adults. *Int. J. Environ. Res. Public Health* 17 (4), 1274. doi:10.3390/ijerph17041274

Yang, Y., Zhang, X., Luo, Z., Wang, X., Ye, D., and Fu, W. (2020). Alterations in running biomechanics after 12 Week gait retraining with minimalist shoes. *Int. J. Environ. Res. Public Health* 17 (3), 818. doi:10.3390/ijerph17030818

Yoo, W. G. (2014). Effect of the intrinsic foot muscle exercise combined with interphalangeal flexion exercise on metatarsalgia with morton's toe. J. Phys. Ther. Sci. 26 (12), 1997–1998. doi:10.1589/jpts.26.1997

Zhang, S., Fu, W., and Liu, Y. (2019). Does habitual rear-foot strike pattern with modern running shoes affect the muscle strength of the longitudinal arch? *Isokinet. Exerc. Sci.* 27 (3), 213–218. doi:10.3233/ies-192139

Zhang, X., Deng, L., Yang, Y., Xiao, S., Li, L., and Fu, W. (2021). Effects of 12-week transition training with minimalist shoes on Achilles tendon loading in habitual rearfoot strike runners. *J. Biomechanics* 128, 110807. doi:10.1016/j.jbiomech.2021. 110807

Zhang, X., Luo, Z., Wang, J., Yang, Y., and Fu, W. (2020). Ultrasound-based mechanical adaptation of Achilles tendon after 12-week running with minimalist shoes. *J. Med. Imaging Health Inf.* 10 (5), 1205–1209. doi:10. 1166/jmihi.2020.2997