

Running head: DEVELOPMENT OF APERIODIC ACTIVITY

# 1 The development of aperiodic neural activity in the 2 human brain

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**Abstract**

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3 The neurophysiological mechanisms supporting brain maturation are fundamental to attention and  
4 memory capacity across the lifespan. Human brain regions develop at different rates, with many  
5 regions developing into the third and fourth decades of life. Here, in this preregistered study  
6 (<https://osf.io/gsr7>), we analyzed intracranial EEG (iEEG) recordings from widespread brain  
7 regions in a large developmental cohort. Using task-based (i.e., attention to-be-remembered visual  
8 stimuli) and task-free (resting-state) data from 101 children and adults (5.93 – 54.00 years, 63 males;  $n$   
9 electrodes = 5691), we mapped aperiodic ( $1/f$ -like) activity, a proxy of excitation:inhibition (E:I)  
10 balance with steeper slopes indexing inhibition and flatter slopes indexing excitation. We reveal that  
11 aperiodic slopes flatten with age into young adulthood in both association and sensorimotor cortices,  
12 challenging models of early sensorimotor development based on brain structure. In prefrontal cortex  
13 (PFC), attentional state modulated age effects, revealing steeper task-based than task-free slopes in  
14 adults and the opposite in children, consistent with the development of cognitive control. Age-related  
15 differences in task-based slopes also explained age-related gains in memory performance, linking the  
16 development of PFC cognitive control to the development of memory. Last, with additional structural  
17 imaging measures, we reveal that age-related differences in gray matter volume are differentially  
18 associated with aperiodic slopes in association and sensorimotor cortices. Our findings establish  
19 developmental trajectories of aperiodic activity in localized brain regions and illuminate the  
20 development of PFC inhibitory control during adolescence in the development of attention and  
21 memory.

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31 **Keywords:** aperiodic  $1/f$  activity; brain development; gray matter; memory; resting-state; intracranial  
32 electroencephalography.  
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## 1 Introduction

2  
3 Human brain regions develop at different rates, with many regions developing into the third  
4 and fourth decades of life, followed by gradual declines in volume throughout adulthood (Bethlehem  
5 et al., 2022; Gogtay et al., 2004; Grydeland et al., 2019). Understanding the complexities of human  
6 brain development requires a comprehensive investigation into the intricate interplay between  
7 electrophysiological dynamics, brain structure, and behavior across the lifespan. Despite the  
8 importance of this endeavor to basic and translational neuroscience, research has been limited by a  
9 paucity of methods capable of studying human brain function with high spatial and temporal precision  
10 and focused on narrow age ranges. Further, non-oscillatory, aperiodic activity has yet to be fully  
11 characterized from a developmental perspective (cf. Favaro et al., 2023; Hill et al., 2022;  
12 Schaworonkow & Voytek, 2021; Tröndle et al., 2022). Consequently, the manifestation of age-related  
13 differences in aperiodic activity and their relation to brain structure and cognition remains unknown.

14 The aperiodic component of the electrophysiological power spectrum, characterized by its  
15 spectral slope and offset (Donoghue et al., 2020; Wen & Liu, 2016), is hypothesized to reflect the  
16 balance between excitation and inhibition (E:I) of neuronal populations (Ahmad et al., 2022; van  
17 Nifterick et al., 2023). A flatter slope and lower offset are posited to reflect increased excitatory  
18 neuronal population spiking (Manning et al., 2009; Miller et al., 2012). Converging computational  
19 (Donoghue et al., 2020; Gao et al., 2017) and pharmacological (Irene Gonzalez-Burgos et al., 2023;  
20 Molina et al., 2020; Salvatore et al., 2024; Wiest et al., 2023) work indicates that steeper slopes reflect  
21 increased inhibitory signaling (i.e., elevated GABAergic or reduced glutamatergic activity), while flatter  
22 slopes reflect dominance of excitatory signaling.

23 The balance of excitatory and inhibitory neural activity is a fundamental property of healthy  
24 brain function (Turrigiano & Nelson, 2004). Indeed, an optimal level of E:I balance is proposed to  
25 safeguard against hyper-synchronization, with E:I imbalance implicated in neurodevelopmental  
26 disorders, such as schizophrenia and autism (Earl et al., 2024; Pani et al., 2022; Shuffrey et al., 2022)  
27 and generalized learning disabilities (Fernandez & Garner, 2007). Studies using scalp  
28 electroencephalography (EEG) during passive (i.e., task-free) states have consistently demonstrated a  
29 flattening of the slope and a downward shift in the offset with advancing age throughout adulthood  
30 (Donoghue et al., 2020; Merkin et al., 2023; Voytek et al., 2015; Waschke et al., 2017). Such age-related  
31 flattening in task-free aperiodic activity predicts declines in memory performance (Voytek et al., 2015)  
32 and alterations in stimulus-related neurophysiological responses, such as inter-trial alpha phase  
33 clustering during visual spatial discrimination in the elderly (Tran et al., 2020). By contrast, flatter task-  
34 based aperiodic slopes are associated with enhanced memory and learning in healthy young adults  
35 (Cross et al., 2022; Lendner et al., 2023), hinting at a nuanced interplay between aperiodic activity,  
36 attentional state, and age. Thus, understanding the development of aperiodic activity and its  
37 modulation by attentional states with high spatial precision is necessary to understand brain  
38 development and cognitive function across the lifespan.

39 To date, developmental studies of aperiodic activity have relied on scalp EEG (Cellier et al.,  
40 2021; Favaro et al., 2023; Hill et al., 2022; Schaworonkow & Voytek, 2021). Yet, scalp-EEG is limited  
41 in spatial resolution and cannot reliably characterize regionally precise neurophysiological activity  
42 (Ofen et al., 2019). To overcome these limitations, we analyzed rare intracranial EEG (iEEG) data  
43 from an exceptionally large developmental cohort of neurosurgical patients aged 5 to 54 years  
44 undergoing invasive monitoring for seizure management. In contrast to noninvasive neuroimaging,  
45 iEEG provides both spatially localized information and the high temporal precision needed to  
46 examine neurophysiology (Johnson et al., 2020; Johnson & Knight, 2015; Parvizi & Kastner, 2018),  
47 and is thus an invaluable tool for investigating mechanisms of cognitive and brain maturation  
48 (Johnson, Tang, et al., 2018; Johnson, Yin, et al., 2022; Johnson & Knight, 2023; Ofen et al., 2019;

1 Yin et al., 2020, 2023). iEEG provides rich and novel measures of neurophysiology including low-  
2 frequency periodic and aperiodic activity, and high-frequency broadband activity reflecting neuronal  
3 population activity (Leszczyński et al., 2020; Nir et al., 2007; Ray et al., 2008; Rich & Wallis, 2017;  
4 Watson et al., 2018). Thus, iEEG enables unique discoveries of the neurophysiological mechanisms  
5 of cognitive and brain maturation in humans.

6 In this preregistered study (<https://osf.io/gsr7>), we sought to define regionally precise, brain-  
7 wide developmental trajectories of aperiodic activity in task-based and task-free states (Figures 1A,  
8 1B). In addition to mapping aperiodic activity across development, we defined the relationship  
9 between regionally precise aperiodic activity and cortical structure (Figure 1C). Measures of regional  
10 gray matter volume (GMV) and electrophysiological activity show substantial overlap in relation to  
11 cognition, pathology (Hunt et al., 2016; Schölvink et al., 2013), and age (Doval et al., 2024; Overbye  
12 et al., 2018; Sui et al., 2014; Whitford et al., 2007), which suggests that they may be jointly explained  
13 by shared factors, such as myelination and synaptogenesis. Thus, examining structure-function  
14 coupling can provide context to understand novel electrophysiological findings, such as iEEG  
15 measures of aperiodic activity by age, based on well-documented age-related variability in regional  
16 brain structure (Bethlehem et al., 2022; Gogtay et al., 2004; Groeschel et al., 2010). Based on reports  
17 of age-related variability in global scalp EEG-derived aperiodic activity (Cellier et al., 2021; Finley et  
18 al., 2022; Hill et al., 2022; Schaworonkow & Voytek, 2021; Thuwal et al., 2021) and in brain structure  
19 demonstrating that sensorimotor regions mature earlier than association regions (Gogtay et al., 2004;  
20 Grydeland et al., 2019; Hill et al., 2010; Sydnor et al., 2021), we hypothesized that: (a) in association  
21 cortices, the aperiodic slope flattens with age into young adulthood; (b) in sensorimotor cortices, the  
22 aperiodic slope flattens with age into adolescence; (c) attentional state (task-based vs. task-free)  
23 modulates age effects observed in (a) and (b), and; (d) age-related differences in aperiodic activity are  
24 modulated by regional GMV.

25 We first reveal a gradient in aperiodic activity across the brain, suggesting heightened inhibition  
26 in inferior lateral posterior regions and heightened excitation in superior medial frontal regions. We  
27 then establish developmental trajectories of aperiodic activity, revealing a flattening of the slope and  
28 a downward shift in the offset from childhood to young adulthood in both association and  
29 sensorimotor cortices, challenging our hypothesis that aperiodic activity stabilizes before young  
30 adulthood in sensorimotor cortices. We further reveal how attentional state modulates age effects in  
31 select regions including prefrontal cortex (PFC) and establish predictive links between task-based  
32 aperiodic activity in PFC and individual memory outcomes. We last uncover novel associations  
33 between cortical structure and function, highlighting how aperiodic slopes in PFC are modulated by  
34 age-related variability in GMV. Taken together, we offer critical insights into the intricate interplay  
35 between aperiodic neural activity, cortical structure, and behavior from childhood to middle age and  
36 illuminate the development of PFC inhibitory control during adolescence in the development of  
37 attention and memory.

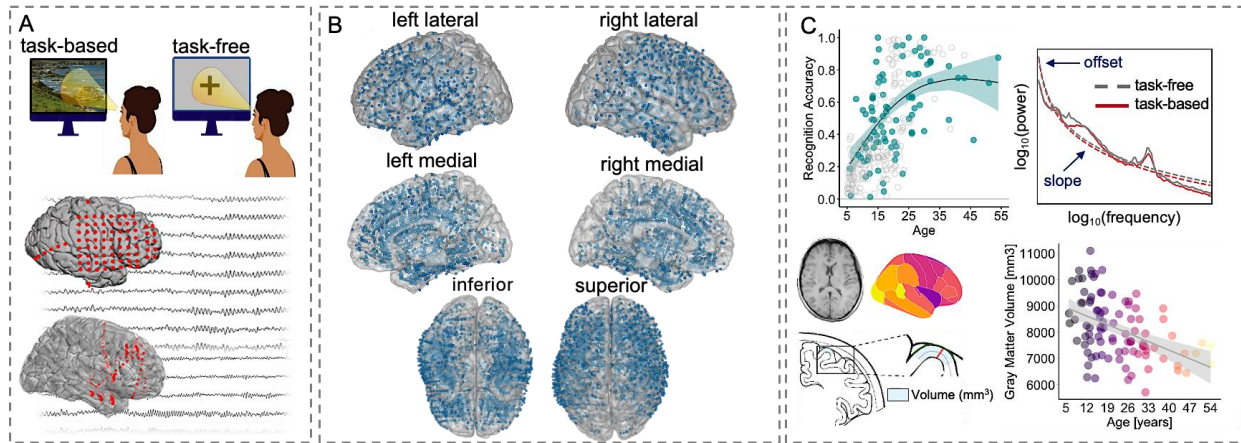
## 38 **Results**

### 39 **iEEG memory and brain volume measures generalize to healthy populations**

40 One hundred and one neurosurgical patients participated (mean age = 19.25, range = 5.93 –  
41 54.00 years; 63 males). Patients were selected based on above-chance behavioral performance on two  
42 visual memory recognition tasks (mean normalized accuracy = 0.54, SD = 0.25, range = 0.01 – 1.00;  
43  $\beta = 0.54$ , SE = 0.02,  $p = \leq .001$ ) and/or if there was a task-free recording available. Those with major  
44 lesions, prior surgical resections, noted developmental delays, or neuropsychological memory test  
45 scores <80 were considered ineligible. Analysis of recognition accuracy by age indicated a positive  
46 association ( $\beta = 0.90$ , SE = 0.16,  $p = \leq .001$ ,  $R^2 = .27$ ; see Figure 1C), indicating that iEEG patients  
47 exhibit the expected developmental trajectory of improved memory from age 5-30 years, consistent  
48  
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1 with age-matched, healthy controls (Johnson, Yin, et al., 2022, 2022; Ofen et al., 2007, 2019). Analysis  
2 of global GMV by age indicated a negative association ( $\beta = -46.56$ ,  $SE = 9.36$ ,  $p = \leq .001$ ,  $R^2 = .20$ ;  
3 Figure 1C), further demonstrating that iEEG patients show the developmental trajectory of decreased  
4 GMV from age 5 to 54 years, consistent with well-documented decreases in GMV from childhood  
5 through adulthood in healthy individuals (Bethlehem et al., 2022; Gogtay et al., 2004; Groeschel et al.,  
6 2010; Wilke et al., 2007). These demonstrations provide converging evidence that the results of our  
7 iEEG analyses generalize to healthy populations (Hill et al., 2020; Johnson & Knight, 2023).



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12 **Figure 1. Design, channel coverage, and key variables. (A)** Intracranial neurophysiological activity was recorded  
13 using electrocorticography (ECoG; middle) and stereoelectroencephalography (sEEG; bottom) during both task-  
14 based (top left) and task-free wake states (top right). **(B)** Seizure- and artifact-free intracranial channel placements ( $n$   
15 = 5691) across all patients ( $n = 101$ ) in MNI space. **(C)** Schematic of key dependent and independent variables. Top  
16 left: iEEG patients (teal;  $n = 81$ ) show the expected developmental trajectory of improved memory recognition from  
17 ~5 – 30 years of age ( $p \leq .001$ ) and fall in the range of age-matched, healthy controls (gray;  $n = 221$ ). Top right: power  
18 spectral density plot illustrating the periodic (oscillatory) components over and above the aperiodic ( $1/f$ -like)  
19 component in task-free (dashed) and task-based (solid) conditions. The offset (i.e., y-intercept) and slope (exponent)  
20 make up the aperiodic component when power (y-axis) and frequency (x-axis) are represented in log-log space.  
21 Bottom left: TI MRI obtained for each patient, parcellation of cortical regions based on the Desikan-Killiany-  
22 Tourville atlas, and GMV estimation (adapted from Bethlehem et al., 2022). Bottom right: age-related differences in  
23 global GMV ( $\text{mm}^3$ ) in our cohort, showing the expected developmental trajectory of decreased GMV from ~5 – 54  
24 years of age ( $p \leq .001$ ).

### 25 26 **Aperiodic activity differs by brain region**

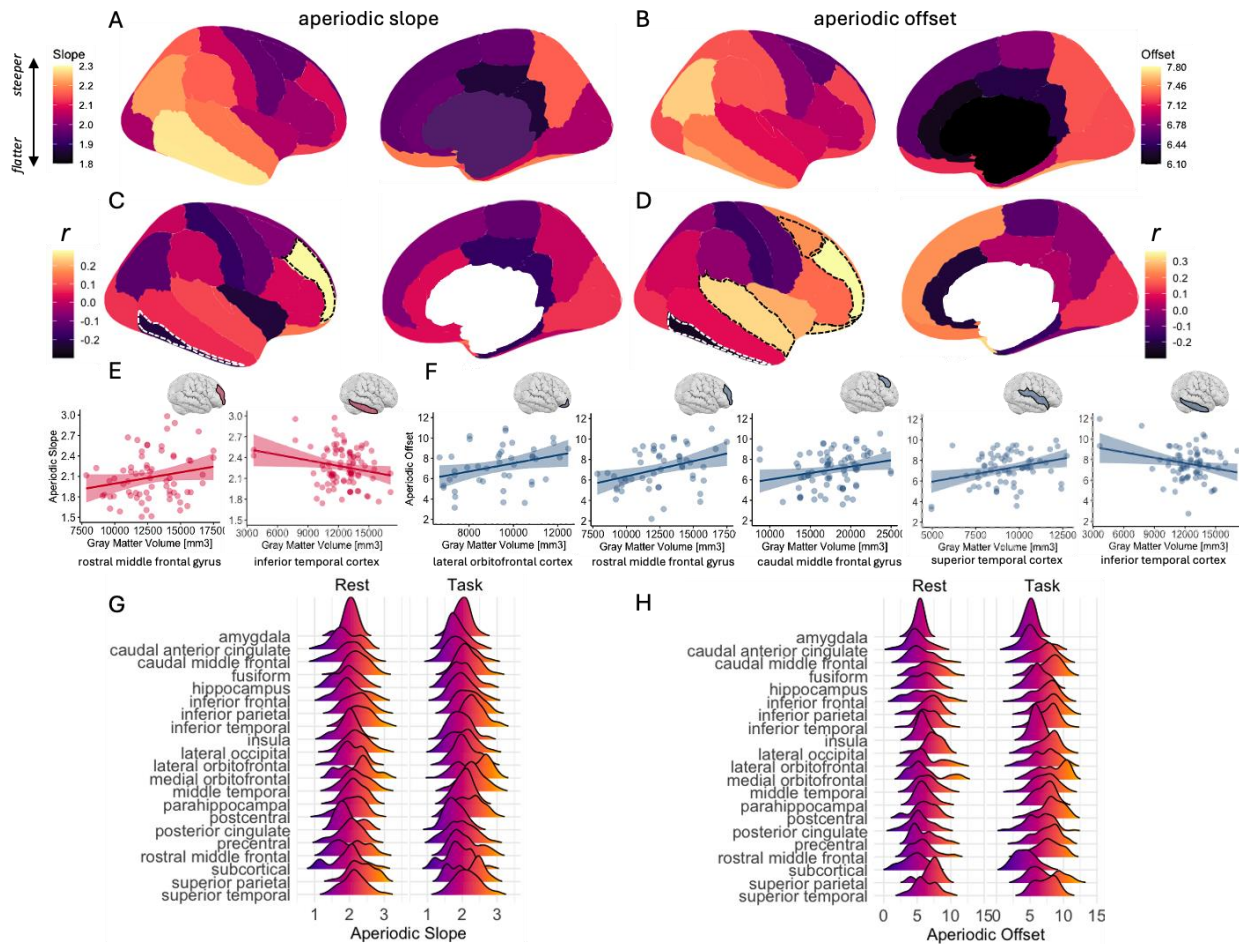
27 Prior to testing hypotheses, we first characterized regional differences in aperiodic activity by  
28 implemented linear mixed-effects models, regressing region onto the aperiodic slope and offset while  
29 regressing out attentional state (task-based, task-free) and age, treating participants and nested  
30 channels as random intercepts (Johnson & Knight, 2023). Regions of interest (ROI) were defined  
31 based on the Desikan-Killiany-Tourville (DKT) atlas (Klein & Tourville, 2012). We revealed a gradient  
32 of steeper slopes in inferior lateral posterior regions to flatter slopes in superior medial frontal regions  
33 ( $\chi^2(19) = 1038.30$ ,  $p \leq 0.001$ ; Figure 2A). The aperiodic offset exhibited a similar pattern ( $\chi^2(19) =$   
34  $484.70$ ,  $p \leq 0.001$ ; Figure 2B). These results extend previous reports of a posterior-to-anterior gradient  
35 in task-free E:I balance based on fMRI, i.e., Hurst exponent (Fotiadis et al., 2023) and  
36 magnetoencephalography (MEG) aperiodic component (Mahjoory et al., 2020). Our data demonstrate  
37 that aperiodic activity varies between localized brain regions to higher degree than previously reported.

38  
39 Second, to characterize relationships between regional GMV and aperiodic activity (i.e.,  
40 structure-function coupling), we implemented linear mixed-effects models, regressing region and  
41 GMV onto the aperiodic slope and offset while regressing out attentional state and age, treating

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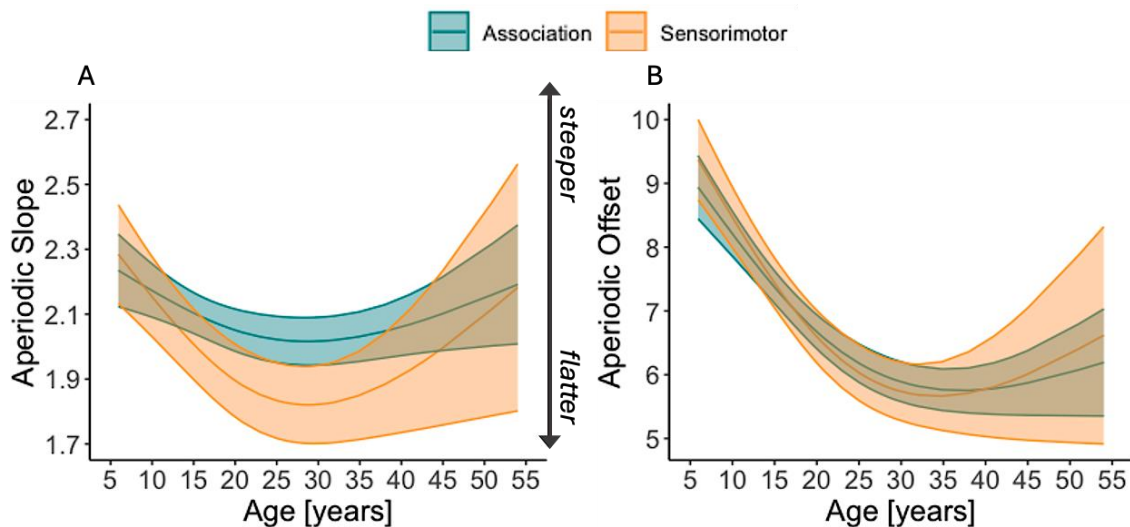
1 participants and nested channels as random intercepts (Johnson & Knight, 2023). We revealed  
 2 regionally specific relationships between aperiodic activity and GMV (Figure 2C and Figure 2D). We  
 3 observed a significant positive correlation with slope and GMV in rostral middle frontal gyrus ( $r =$   
 4  $0.27, p = 0.02, 95\% \text{ CI} = [0.04, 0.48]$ ), and a significant negative correlation in inferior temporal cortex  
 5 ( $r = -0.22, p = 0.03, 95\% \text{ CI} = [-0.40, -0.01]$ ). The offset also correlated positively with GMV in lateral  
 6 orbitofrontal cortex ( $r = 0.32, p = 0.03, 95\% \text{ CI} = [0.03, 0.57]$ ), superior temporal cortex ( $r = 0.30, p$   
 7  $= 0.01, 95\% \text{ CI} = [0.06, 0.50]$ ), and rostral ( $r = 0.36, p = 0.009, 95\% \text{ CI} = [0.09, 0.57]$ ) and caudal ( $r$   
 8  $= 0.24, p = 0.03, 95\% \text{ CI} = [0.02, 0.44]$ ) middle frontal gyri, and correlated negatively with GMV in  
 9 inferior temporal cortex ( $r = -0.25, p = 0.03, 95\% \text{ CI} = [-0.45, -0.02]$ ). These results reveal opposing  
 10 structure-function coupling between localized frontotemporal regions and indicate that there is not a  
 11 clear one-to-one mapping between GMV and aperiodic activity.



12  
 13 **Figure 2. Regional differences in the aperiodic slope and offset and their correlation with GMV.** Top row:  
 14 Brain-wide standardized means of the regional aperiodic slope (A; left) and offset (B; right). Warmer colors/higher  
 15 values indicate steeper slopes and higher offsets, respectively. Middle row: brain-wide correlations (Pearson  $r$ )  
 16 between regional GMV (mm<sup>3</sup>) and aperiodic slopes (C; left) and offsets (D; right). Warmer colors/higher values  
 17 indicate positive correlations; cooler colors/lower values indicate negative correlations. Note that the area  
 18 corresponding to subcortical space is white as no analysis of subcortical GMV was performed. Regions with  
 19 statistically significant correlations ( $p < 0.05$ ) are indicated by dashed borders. Bottom row: scatterplots illustrating  
 20 relationships between GMV (x-axis) and aperiodic slopes (E; y-axis; red) and offsets (F; y-axis; blue) in regions with  
 21 statistically significant correlations. Individual data points represent single participant data averaged across channels  
 22 for each representative ROI. Shading shows the standard error. (G) Ridgeline plot illustrating the distribution of  
 23 aperiodic slopes (x-axis; higher values denote a steeper slope) by region (y-axis) and condition (left: task-free; right:  
 24 task-based). (H) Same as (G) for the aperiodic offset (x-axis; higher values denote a higher offset).

## 1 Aperiodic activity stabilizes in young adulthood in associative and sensorimotor cortices

2 Having demonstrated that aperiodic activity differs by brain region, we sought to establish  
3 developmental trajectories of aperiodic activity between association and sensorimotor cortices. We  
4 first examined hypotheses a, that in association cortices, the aperiodic slope flattens with age into  
5 young adulthood, and b, that in sensorimotor cortices, the aperiodic slope flattens with age into  
6 adolescence (see Table S1 in the supplementary materials for a summary of association and  
7 sensorimotor regions). We implemented nonlinear mixed-effects regressions, modeling aperiodic  
8 activity as a function of age (fit with two splines) and cortex type (association, sensorimotor), treating  
9 participant and DKT region as random effects on the intercept, and channel nested under participant.  
10 For the aperiodic slope, we revealed a significant age  $\times$  cortex type interaction ( $\beta = 0.20$ , SE = 0.05,  $p$   
11  $< 0.001$ ; age:  $\beta = -0.57$ , SE = 0.18,  $p = 0.002$ ; cortex type:  $\beta = -0.02$ , SE = 0.04,  $p = 0.59$ ),  
12 demonstrating that the slope flattens with age into young adulthood, with greater flattening in  
13 sensorimotor compared to association cortices between 15 – 35 years of age ( $\beta = 0.23$ , SE = 0.11,  $p$   
14  $= 0.03$ ; Figure 3A). For the aperiodic offset, while there was no interaction between age and region ( $\beta$   
15  $= -0.16$ , SE = 0.55,  $p = .76$ ) nor a main effect of region ( $\beta = -0.21$ , SE = 0.16,  $p = 0.20$ ), we revealed  
16 a significant main effect of age, whereby the offset downshifted from 5 – 30 years of age (first spline  
17 term;  $\beta = -6.06$ , SE = 0.85,  $p \leq 0.001$ ) before stabilizing thereafter (second spline term;  $\beta = -1.15$ , SE  
18  $= 0.84$ ,  $p = 0.17$ ; Figure 3B). These results support our prediction that the aperiodic slope and offset  
19 flatten and downshift with age into young adulthood in association cortices. These results are contrary  
20 to our prediction that aperiodic activity stabilizes with age into adolescence in sensorimotor cortices;  
21 however, the difference in flattening suggests dissociable trajectories between association and  
22 sensorimotor cortices.



23  
24 **Figure 3. Age-related differences in aperiodic activity between association and sensorimotor cortices. (A)**  
25 Modeled effects for differences in the aperiodic slope (y-axis; higher values denote a steeper slope) and age (x-axis).  
26 **(B)** Modeled effects for differences in the aperiodic offset (y-axis: higher values denote a higher offset) and age (x-  
27 axis). In both **(A)** and **(B)**, association cortices are presented in teal and sensorimotor cortices in orange. Shaded  
28 regions indicate the 83% confidence interval.

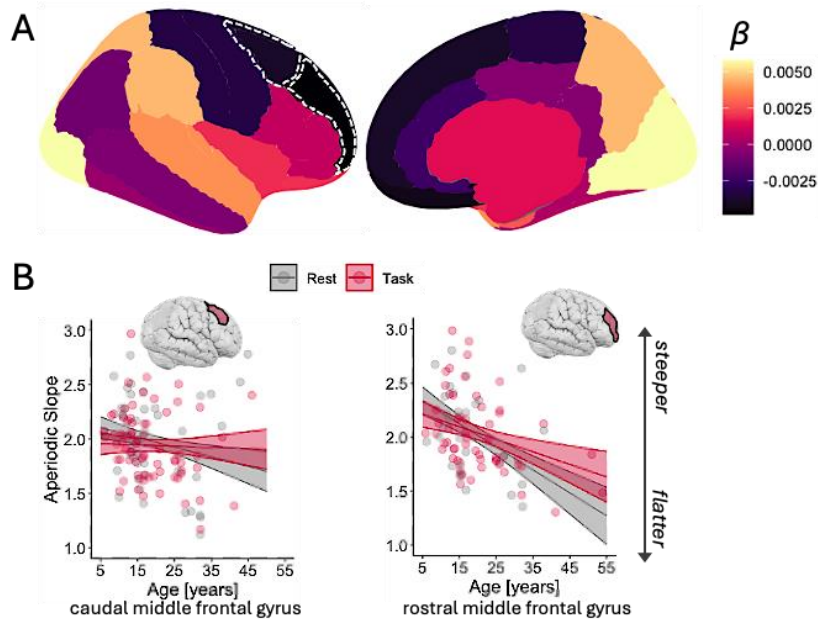
## 30 Regional aperiodic neural activity differs by age and attentional state

31 We next sought to establish developmental trajectories of aperiodic activity within localized  
32 brain regions and test hypothesis c, that age effects would differ between attentional states. To identify  
33 regional age effects in aperiodic activity and whether they differ by attentional state, we implemented  
34 separate linear mixed-effects models for each ROI. Our strategy for each analysis was to fit a model  
35 to the dependent variable of interest (i.e., aperiodic slope or offset) and regress the estimates onto age



1 (in years), attentional state (task-based, task-free), and the interaction of age and attentional state. All  
2 models were fit with by-participant and by-task random intercepts, with channel nested under  
3 participant.

4 For the aperiodic slope, we revealed a main effect of age in caudal anterior cingulate cortex ( $\beta$   
5 = -0.01, SE = 0.004,  $p_{\text{adj}} = 0.03$ ), and significant age  $\times$  attentional state interactions in caudal middle  
6 frontal gyrus (cMFG;  $\beta = -0.003$ , SE = 0.001,  $p_{\text{adj}} = 0.007$ ; age:  $\beta = -0.005$ , SE = 0.004,  $p_{\text{adj}} = 0.41$ ;  
7 task:  $\beta = 0.09$ , SE = 0.02,  $p_{\text{adj}} \leq 0.001$ ) and rostral middle frontal gyrus (rMFG;  $\beta = -0.004$ , SE = 0.001,  
8  $p_{\text{adj}} = 0.04$ ; age:  $\beta = -0.01$ , SE = 0.004,  $p_{\text{adj}} = 0.02$ ; task:  $\beta = 0.09$ , SE = 0.03,  $p_{\text{adj}} = 0.37$ ). In both cMFG  
9 and rMFG, task-free slopes are steeper than task-based slopes in children and the opposite is observed  
10 in adults; the direction of differences reverses around age 18 – 20 years (Figure 4B). If flatter slopes  
11 imply more excitation, and increased excitation in the PFC reflects activation of inhibitory cognitive  
12 control, then these results are consistent with increased inhibitory control during task engagement in  
13 adolescence (Keller et al., 2023; Larsen et al., 2023; Sydnor et al., 2021; Sydnor et al., 2023) and mirror  
14 the development of domain-general cognitive control (Tervo-Clemmens et al., 2023). These results  
15 also support our hypothesis that attentional state modulates age-related flattening of the aperiodic  
16 slope (see S1 in supplementary materials for aperiodic offset results). For visualizations of the main  
17 effects of age and condition on the aperiodic slope, see Figures S3 and S4, respectively.



18 **Figure 4. Regions with a significant interaction between age and attentional state on aperiodic activity. (A)**  
19 **Brain-wide age and condition interactions on regional aperiodic slopes. Regions with statistically significant**  
20 **interactions between age and attentional state ( $FDR < 0.05$ ) are indicated by dashed borders. (B) Scatterplots**  
21 **illustrating interactions between age (x-axis; in years) and attentional state (red = task-based; gray = task-free) on the**  
22 **aperiodic slope (y-axis; higher values denote a steeper slope) in regions with statistically significant interactions.**  
23 **Individual data points represent single participant data averaged across channels for each representative ROI.**  
24 **Shading shows 83% CIs.**

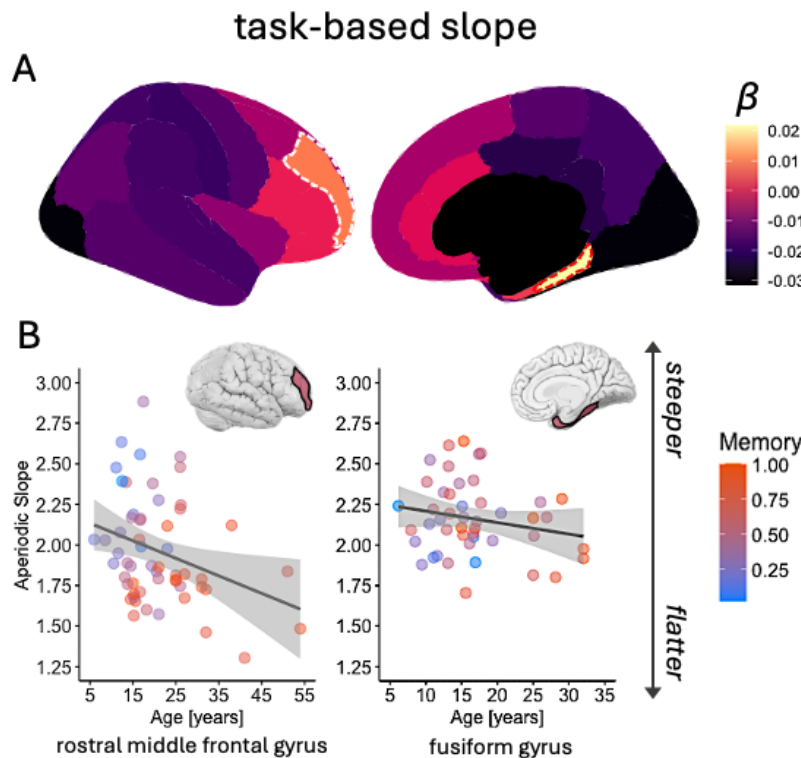
### 27 **Task-based aperiodic activity in association cortices predicts individual memory outcomes**

28 Having demonstrated that memory performance improves with age, with marked variability  
29 among adolescents (Figure 1C), we examined whether age interacts with regionally specific task-based  
30 and task-free aperiodic slopes, respectively, to predict memory performance. For each analysis, we fit  
31 a general linear model to recognition accuracy and regressed the estimates onto age (in years) and  
32 aperiodic slopes (task-based or task-free), and the interaction of age and slope. For task-based slopes,



1 we observed age  $\times$  slope interactions in rMFG ( $\beta = 0.02$ , SE = 0.01,  $p = 0.03$ ; age:  $\beta = -0.02$ , SE =  
2 0.01,  $p = 0.14$ ; slope:  $\beta = -0.76$ , SE = 0.23,  $p = 0.001$ ; Figure 5A left) and fusiform gyrus ( $\beta = -0.03$ ,  
3 SE = 0.01,  $p = 0.005$ ; age:  $\beta = 0.08$ , SE = 0.02,  $p = 0.001$ ; slope:  $\beta = 0.64$ , SE = 0.27,  $p = 0.02$ ; Figure  
4 5A right). In rMFG, memory performance increased with age and an age-related flattening of the  
5 aperiodic slope. Although overall steeper slopes were observed in children, relatively flatter slopes in  
6 children and adolescents were associated with relatively superior memory. By contrast, in fusiform  
7 gyrus, flatter slopes were associated with inferior memory in children but superior memory in  
8 adolescents and adults. There were no significant main effects of the task-free slope or interactions  
9 between the task-free slope and age on memory performance (all  $p > .05$ ). For visualization of main  
10 effects of task-based and task-free slopes on memory, see Figure S7 and Figure S9, respectively. For  
11 aperiodic offset results, see S2 in the supplementary material.

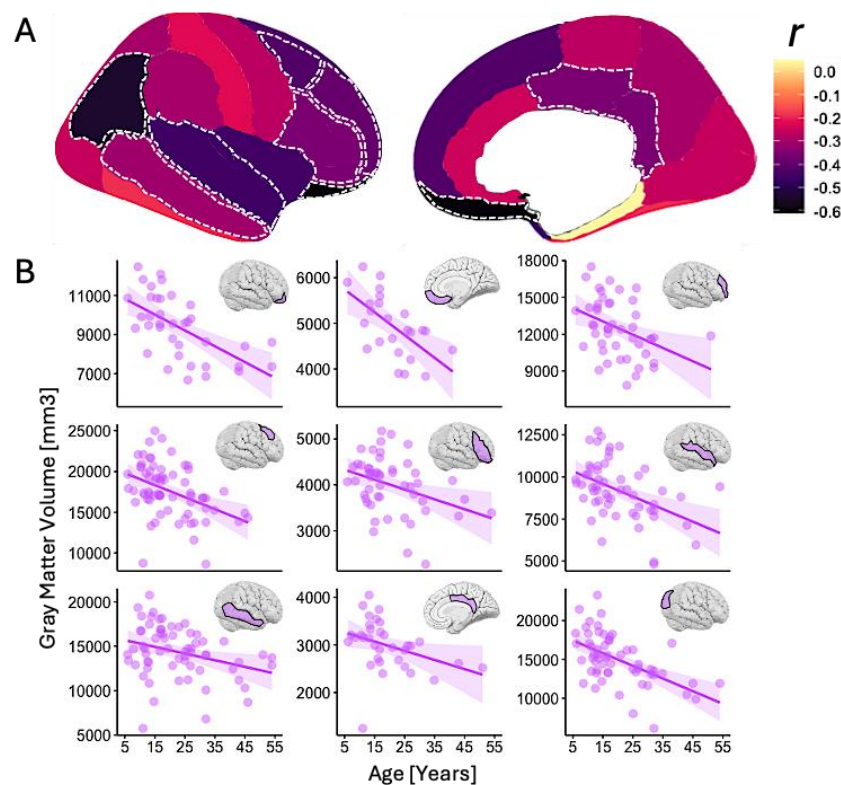
12 Taken together, our results elucidate how age-dependent effects on aperiodic slopes in PFC  
13 and fusiform gyrus, and age-invariant effects on aperiodic offsets in PFC and inferior parietal cortex  
14 predict individual memory performance (S2 and Figure S2). These effects were evident exclusively  
15 during task-based states, thus linking aperiodic activity during attention to to-be-remembered visual  
16 information to an individual's memory for that information. From this perspective, the aperiodic slope  
17 may serve as a key marker of typical and atypical memory development, while the offset may reflect  
18 an age-invariant neural marker of successful memory encoding (Figure S2).



20  
21 **Figure 5. Regions with a significant effect of task-based aperiodic activity on memory performance. (A)**  
22 Brain-wide slope and age interactions on memory. Regions with statistically significant interactions between the task-  
23 based slope and age ( $p < 0.05$ ) are indicated by dashed borders. **(B)** Scatterplots illustrating interactions between  
24 task-based slopes (y-axis; higher values denote a steeper slope) and age (x-axis; in years) on memory (z-scale; warmer  
25 colors denote higher memory recognition accuracy) in regions with statistically significant interactions. Individual  
26 data points represent single participant data averaged across channels for each representative ROI. Shading shows  
27 the standard error.

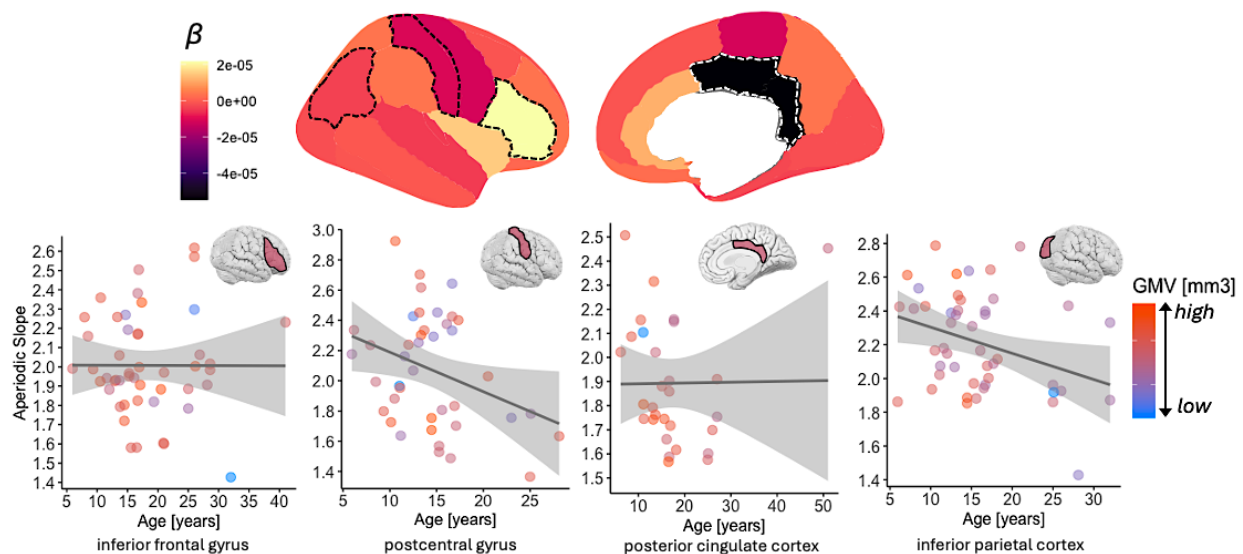
## 1 Gray matter volume and age interact to predict aperiodic activity in select brain regions

2 Thus far, we have established that aperiodic slopes in PFC differ by age and attentional state  
3 and predict age-related variability in memory outcomes, whereas slopes in sensorimotor regions do  
4 not differ by attentional state or predict age-related variability in memory outcomes. Last, we focus  
5 on structure-function relationships. Before testing hypothesis d, that age-related differences in  
6 aperiodic activity are modulated by regional GMV, we sought to replicate previous reports of age-  
7 related reductions in regional GMV (Bethlehem et al., 2022; Gogtay et al., 2004; Groeschel et al.,  
8 2010). Having demonstrated that global GMV decreases with age in our cohort (Figure 1C), we  
9 examined GMV by ROI. We implemented a linear mixed-effects model, regressing region and age  
10 onto GMV, treating participants as random intercepts. Our model confirmed a significant main effect  
11 of region ( $\chi^2(19) = 11081.98, p \leq 0.001$ ) and revealed an age  $\times$  region interaction ( $\chi^2(19) = 92.05, p$   
12  $\leq 0.001$ ; Figure 5). Gray matter volume was reduced with age in lateral orbitofrontal cortex ( $r = -0.61,$   
13  $p < 0.001, 95\% \text{ CI} = [-0.77, -0.35]$ ), mOFC ( $r = -0.60, p = 0.001, 95\% \text{ CI} = [-0.81, -0.27]$ ), rMFG ( $r =$   
14  $-0.38, p = 0.007, 95\% \text{ CI} = [-0.61, -0.11]$ ), cMFG ( $r = -0.42, p < .001, 95\% \text{ CI} = [-0.60, -0.20]$ ),  
15 inferior frontal gyrus ( $r = -0.35, p = 0.01, 95\% \text{ CI} = [-0.57, -0.09]$ ), superior temporal cortex ( $r = -$   
16  $0.45, p < 0.001, 95\% \text{ CI} = [-0.64, -0.22]$ ), middle temporal cortex ( $r = -0.31, p = 0.01, 95\% \text{ CI} = [-$   
17  $0.51, -0.07]$ ), posterior cingulate cortex ( $r = -0.36, p = 0.04, 95\% \text{ CI} = [-0.62, -0.02]$ ), and inferior  
18 parietal cortex ( $r = -0.54, p < 0.001, 95\% \text{ CI} = [-0.70, -0.33]$ ; Figure 6A and 6B). These results replicate  
19 previous reports of age-related reductions in GMV in association cortices starting in childhood  
20 (Bethlehem et al., 2022; Gogtay et al., 2004; Groeschel et al., 2010).



21 **Figure 6. Regions with a significant effect of age on GMV. (A)** Brain-wide correlations (Pearson  $r$ ) between  
22 regional GMV (mm<sup>3</sup>) and age (in years). Warmer colors/higher values indicate positive correlations and cooler  
23 colors/lower values indicate negative correlations. Note that the area corresponding to subcortical space is white as  
24 no analysis of subcortical GMV was performed. Regions with statistically significant correlations ( $p < 0.05$ ) are  
25 indicated by dashed borders. **(B)** Scatterplots illustrating relationships between GMV (y-axis) and age (x-axis) in  
26 regions with statistically significant correlations.  
27

1  
2 To test whether age-related differences in aperiodic activity are modulated by regional GMV,  
3 we fit mixed-effects models to task-based aperiodic activity (slope or offset) and regressed these  
4 estimates onto age (in years), GMV, and the interaction between age and GMV. All models were fit  
5 with by-participant and by-task random intercepts, with channel nested under participant. We revealed  
6 age  $\times$  GMV interactions on task-based aperiodic slopes in inferior frontal gyrus ( $\beta = 2.15 \times 10^{-5}$ , SE  
7  $= 9.77 \times 10^{-6}$ ,  $p = 0.03$ ; age:  $\beta = -0.09$ , SE = 0.04,  $p = 0.02$ ; GMV:  $\beta = -0.0004$ , SE = 0.0002,  $p = 0.03$ ),  
8 posterior cingulate cortex ( $\beta = -5.44 \times 10^{-5}$ , SE =  $1.71 \times 10^{-5}$ ,  $p = 0.003$ ; age:  $\beta = 0.14$ , SE = 0.04,  $p =$   
9 0.004; GMV:  $\beta = 0.0007$ , SE = 0.0002,  $p = 0.01$ ), and inferior parietal cortex ( $\beta = -3.93 \times 10^{-6}$ , SE =  
10  $1.50 \times 10^{-6}$ ,  $p = 0.01$ ; age:  $\beta = 0.04$ , SE = 0.02,  $p = 0.02$ ; GMV:  $\beta = 6.24 \times 10^{-5}$ , SE =  $2.90 \times 10^{-5}$ ,  $p =$   
11 0.03), three of the regions where GMV was reduced with age (see Figure 6), as well as postcentral  
12 gyrus ( $\beta = -1.07 \times 10^{-5}$ , SE =  $3.78 \times 10^{-6}$ ,  $p = 0.007$ ; age:  $\beta = 0.10$ , SE = 0.03,  $p = 0.007$ ; GMV:  $\beta =$   
13 0.0001, SE =  $6.30 \times 10^{-5}$ ,  $p = 0.03$ ; Figure 7). In inferior frontal gyrus, task-based aperiodic slopes  
14 flattened with age and reductions in GMV; flatter slopes were associated with higher GMV in children  
15 and lower GMV in adults. In posterior cingulate cortex, inferior parietal cortex, and postcentral gyrus,  
16 while there was no relationship between task-based slopes and GMV in children, flatter slopes were  
17 associated with higher GMV in adults (for visualizations of the main effects of age and GMV on  
18 aperiodic slopes, see Figure S9 and S10, respectively). There were no significant age  $\times$  GMV  
19 interactions on task-based aperiodic offsets (all  $p > .05$ ; for visualizations of the non-significant main  
20 effects of age and GMV on aperiodic offsets, see Figure S13 and S14, respectively).  
21  
22



23  
24 **Figure 7. Regions with a significant interaction between age and GMV on the aperiodic slope. (A)** Top row:  
25 Brain-wide GMV and age interactions on regional aperiodic slopes. Regions with statistically significant interactions  
26 between age and GMV ( $FDR < 0.05$ ) are indicated by dashed borders. Bottom row: scatterplots illustrating  
27 interactions between age (x-axis; in years) and GMV (z-scale; warmer colors denote higher GMV) on the aperiodic  
28 slopes (y-axis; higher values denote a steeper slope) in regions with statistically significant interactions. Individual  
29 data points represent single participant data averaged across channels for each representative ROI. Shading shows  
30 the standard error.

## 32 Discussion

33 We mapped aperiodic activity – a proposed marker of E:I balance – from childhood to late  
34 middle adulthood. Our findings demonstrate: (I) a gradient of slopes from inferior lateral to superior  
35 medial regions, suggesting heightened inhibition in inferior lateral temporal regions and heightened

1 excitation in superior medial frontal regions (Figure 2); (II) a U-shaped relationship in slopes by age,  
2 suggesting heightening excitation into young adulthood followed by heightening inhibition into middle  
3 adulthood (Figure 3); (III) a flattening of PFC slopes with advancing age, with more pronounced  
4 flattening in task-free states, suggesting that age-related increases in excitation are task-dependent  
5 (Figure 4); (IV) PFC-derived aperiodic slopes during task-based states predict age-related variability in  
6 memory (Figure 5); and (V) higher GMV that is associated with steeper slopes across age in PFC, but  
7 flatter slopes in sensorimotor cortices (Figure 7). In sum, these findings reveal regional and attentional  
8 differences in E:I balance from early childhood to late middle adulthood and establish E:I balance in  
9 PFC as a mechanism of memory development (for a schematic summary of the main results, see  
10 Figure 8).

### 11 **E:I balance stabilizes in association and sensorimotor cortices in adulthood**

12 The spatiotemporal patterning of cortical maturation progresses from sensorimotor to higher-  
13 order association cortices, characterized by heightened plasticity in late-maturing association regions,  
14 potentially influencing higher-order cognition in adulthood (Sydnor et al., 2021). Based on these  
15 observations, we hypothesized that aperiodic activity would follow similar developmental trajectories,  
16 such that it would stabilize during adolescence in sensorimotor cortices and during young adulthood  
17 in association cortices. Indeed, we revealed that the aperiodic slope and offset flatten and downshift  
18 from childhood to young adulthood in association cortices. However, contrary to dominant models  
19 of brain development based on structural measures (Gogtay et al., 2004; Grydeland et al., 2019; Sydnor  
20 et al., 2021), we found that aperiodic activity in sensorimotor cortices does not stabilize until young  
21 adulthood. We further revealed that the magnitude of flattening is greater in sensorimotor than  
22 association cortices during adolescence and young adulthood. Our findings establish that the  
23 development of aperiodic activity in sensorimotor regions does not mirror the development of cortical  
24 structure and suggest that the development of E:I balance in sensorimotor regions follows a protracted  
25 trajectory into adulthood.  
26

### 27 **Attention modulates E:I balance by age in prefrontal cortex**

28 Scalp-EEG studies have consistently demonstrated an age-related flattening and downshifting  
29 of the aperiodic slope and offset, respectively, often with a frontal-central distribution (Bornkessel-  
30 Schlesewsky, Alday, et al., 2022; Favaro et al., 2023; McSweeney et al., 2023; Merkin et al., 2023;  
31 Ouyang et al., 2020; Schaworonkow & Voytek, 2021; Thuwal et al., 2021). To our knowledge, only  
32 one iEEG study has examined age-related aperiodic slope variability, demonstrating an age-related  
33 flattening of the slope in the visual cortex of 15 patients aged 15 – 53 years (Voytek et al., 2015). Little  
34 is known regarding regional differences in the slope and offset. We found that subregions of PFC,  
35 namely caudal and rostral MFG, exhibit a flattening of the aperiodic slope across age. We further  
36 reveal that the age-related flattening of the slope is modulated by attentional state, with less  
37 pronounced flattening for task-based relative to task-free states. This finding can be interpreted in the  
38 context of PFC inhibitory control: a central role of the PFC is to exert cognitive control in the service  
39 of behavior, partially by modulating activity in regions further upstream, such as visual cortex and  
40 MTL (Gazit et al., 2020; Miller & Cohen, 2001; Noudoost & Moore, 2011). The difference between  
41 task-states also emerges at roughly 18 to 20 years of age, revealing the aperiodic slope as a potential  
42 marker of the development of cognitive control in adolescence. Functionally, steeper on-task slopes,  
43 suggesting increased inhibition, have been proposed to reflect the maintenance of top-down  
44 predictions (Cross et al., 2022; Dave et al., 2018) and support information integration (Bornkessel-  
45 Schlesewsky, Sharrad, et al., 2022; Sheehan et al., 2018). By contrast, flatter slopes have been associated  
46 with slower processing speed (Ouyang et al., 2020), and poorer visual working (Donoghue et al., 2020)  
47 and visuomotor (Immink, Cross et al., 2021) memory, albeit these studies analyzed task-free slopes.  
48



1 Our findings suggest that the PFC gains flexibility in inhibitory control with age, exerting increased  
2 inhibition during the processing of external, task-relevant information.

3  
4 Our exploratory analyses of the aperiodic offset revealed a decrease with age, with task-free  
5 offsets showing a more pronounced decline than task-based offsets in more anterior regions, and the  
6 reverse in more posterior regions. Lower offsets are hypothesized to reflect increased neuronal  
7 population activity (Manning et al., 2009; Miller et al., 2012). Accordingly, previous work has  
8 demonstrated that the offset is higher in task-free states (e.g., during sleep; Favaro et al., 2023; Lendner  
9 et al., 2023) and downshifts from ages 2 – 17 years in an anterior-to-posterior gradient (Favaro et al.,  
10 2023). Here, we extend previous reports by demonstrating a broad-band voltage reduction from  
11 childhood to middle late adulthood in frontal, MTL and occipital regions. Reductions in the offset,  
12 and thus overall power reductions, may covary with synaptic pruning, as lower synaptic density is likely  
13 related to lower EEG power (Larsen et al., 2022; McKeon et al., 2024). From this perspective, region-  
14 specific age-related reductions in the offset may indicate synaptic refinement, with overall power  
15 differing as a function of task-state.

### 16 **E:I balance during memory encoding predicts subsequent memory performance**

17 Do age-related differences in aperiodic activity predict age-related differences in memory?  
18 Prior work on aperiodic activity has reported mixed findings in relating the slope and offset to various  
19 aspects of cognition. Steeper task-free slopes have been associated with faster reaction times in young  
20 adults and improved recognition accuracy during initial learning (Immink, Cross et al., 2021).  
21 However, in the same study, flatter slopes and higher offsets were associated with improved  
22 recognition with increasing task exposure. In a similar study with young adults, flatter task-free slopes  
23 and higher offsets were associated with improved decision-making performance (Dziego et al., 2023).  
24 Of the studies examining task-based aperiodic activity, flatter slopes have been associated with  
25 improved learning of an artificial language in young adults aged 18 – 40 years (Cross et al., 2022), but  
26 lower working memory performance with age from 15 – 53 years (Voytek et al., 2015). Critically, past  
27 work has either focused on task-based or task-free aperiodic activity and cognition without accounting  
28 for differences between task-states, and it is unknown how task-based differences in localized brain  
29 regions relate to behavior by age.

30 Here, we overcame this limitation by mapping task-based and task-free aperiodic slopes and  
31 offsets by age to behavior on a region-by-region basis. We observed opposing age-dependent  
32 relationships between aperiodic slopes and memory in MFG and fusiform gyrus, which likely stems  
33 from their distinct functional roles and development (Rosen et al., 2018; Tang et al., 2018). In MFG  
34 – a region core to executive functions and cognitive control and which undergoes protracted  
35 development (Fuster, 2002; Ridderinkhof et al., 2004) – children with steeper slopes exhibited worse  
36 memory performance. This finding suggests that excessive neural inhibition (Donoghue et al., 2020;  
37 Voytek et al., 2015) in MFG during childhood may hinder attentional control. Indeed, ADHD-  
38 diagnosed, medication naïve children exhibit steeper slopes than their typically developing  
39 counterparts (Robertson et al., 2019), as do individuals with schizophrenia (Molina et al., 2020;  
40 Peterson et al., 2023), suggesting that underdeveloped inhibition in childhood results in inefficient  
41 neural communication and disrupted coordination, manifesting in poorer memory outcomes.

42 As individuals age, structural and functional changes in MFG (i.e., synaptic pruning, changes  
43 in neurotransmitter levels [GABAergic interneurons, glutamate]; Kolk & Rakic, 2022), likely lead to a  
44 flattening of aperiodic slopes (McKeon et al., 2024; Sukenik et al., 2021). Flatter slopes have been  
45 likened to increased neural “noise” (Bornkessel-Schlesewsky, Alday, et al., 2022; Bornkessel-  
46 Schlesewsky, Sharrad, et al., 2022; Dave et al., 2018; Voytek et al., 2015), due to increased levels of  
47 aberrant neural firing in the absence of a slower modulatory oscillation (Voytek et al., 2015; Voytek &  
48 Knight, 2015). We observed that flatter slopes in MFG during adulthood were less related to memory  
49

1 outcomes than in children, likely due to the emergence of compensatory neural recruitment and altered  
2 cognitive strategies (Braver et al., 2009; Cabeza et al., 2018; Spreng & Turner, 2019). Conversely, in  
3 fusiform gyrus, a higher-order visual region that supports detailed visual memory encoding (Ofen et  
4 al., 2007; Rosen et al., 2018), children with steeper slopes had superior memory. Enhanced inhibition  
5 in fusiform gyrus during childhood may be advantageous for the rapid encoding of detailed visual  
6 information, consistent with theoretical models positing that increased inhibition provides  
7 homeostatic control to restore network stability and helps to protect overlapping memories from  
8 interference (Barron, 2021), thus facilitating successful episodic memory formation (Axmacher et al.,  
9 2008). Inversely, during adulthood, age-related declines in synaptic density and myelination may result  
10 in flatter slopes, increased neural noise, and decreased inhibition. This shift towards increased neural  
11 “noise” could be an adaptive response to maintain visual memory performance. Indeed, flatter slopes  
12 have been proposed to index greater “complexity” within biological systems (Amigó et al., 2004; Medel  
13 et al., 2023), likely indicating informationally-rich neural processing (Sheehan et al., 2018). By contrast,  
14 steeper slopes have been argued to support faster information processing (Cross et al., 2022; Dziego  
15 et al., 2023), which may not always be advantageous in processing complex sensory information,  
16 particularly with advancing age.

17 Interestingly, we did not observe significant relationships between task-free slopes and  
18 memory performance. This apparent discrepancy with past findings can likely be explained by  
19 differences in experimental task designs and inter-regional source mixing inherent to scalp-EEG,  
20 where signals from multiple cortical areas are mixed due to volume conduction (Musall et al., 2014;  
21 Palva et al., 2018). Scalp-EEG, with its relatively low spatial resolution, could mask region-specific  
22 relationships between aperiodic slopes and behavior, explaining discrepancies with previous findings.  
23 Although source localization techniques can help mitigate these issues, they are limited in resolving  
24 precise cortical sources (Buzsaki, 2006; Nunez & Srinivasan, 2006). Further, previous work has  
25 focused on mapping intrinsic, task-free aperiodic activity onto trait-like measures of cognition (e.g.,  
26 processing speed, verbal ability; Euler et al., 2024; Montemurro et al., 2024; Pi et al., 2024) or tasks  
27 that do not measure episodic or working memory (Bornkessel-Schlesewsky, Sharrad, et al., 2022;  
28 Dziego et al., 2023; Immink et al., 2021). Our findings demonstrate that aperiodic activity during the  
29 encoding of visual stimuli predicts recognition of those stimuli, a direct relationship that did not  
30 survive on a region-by-region basis with intrinsic (i.e., task-free) activity.  
31

32 We further observed that lower task-based offsets were associated with better memory after  
33 accounting for the effect of age (Figure S2). In MFG and inferior parietal cortex, lower offsets were  
34 associated with improved recognition accuracy. This is in apparent contrast with previous work,  
35 wherein higher task-free offsets are associated with better behavioral performance (Immink et al.,  
36 2021) and better decision-making outcomes (Dziego et al., 2023). From this perspective, task-based  
37 offsets may facilitate memory independent of age, reflecting more stable basal neural activity. This  
38 stability may reflect better regulation of neural resources, allowing for more efficient processing of  
39 incoming information, and a brain state conducive to optimal cognitive functioning. Indeed, the two  
40 regions with negative associations between the offset and memory performance are key nodes in the  
41 frontoparietal network, a system at the interface of memory processes and attentional orientation to  
42 task-relevant information (Fischer et al., 2021).  
43

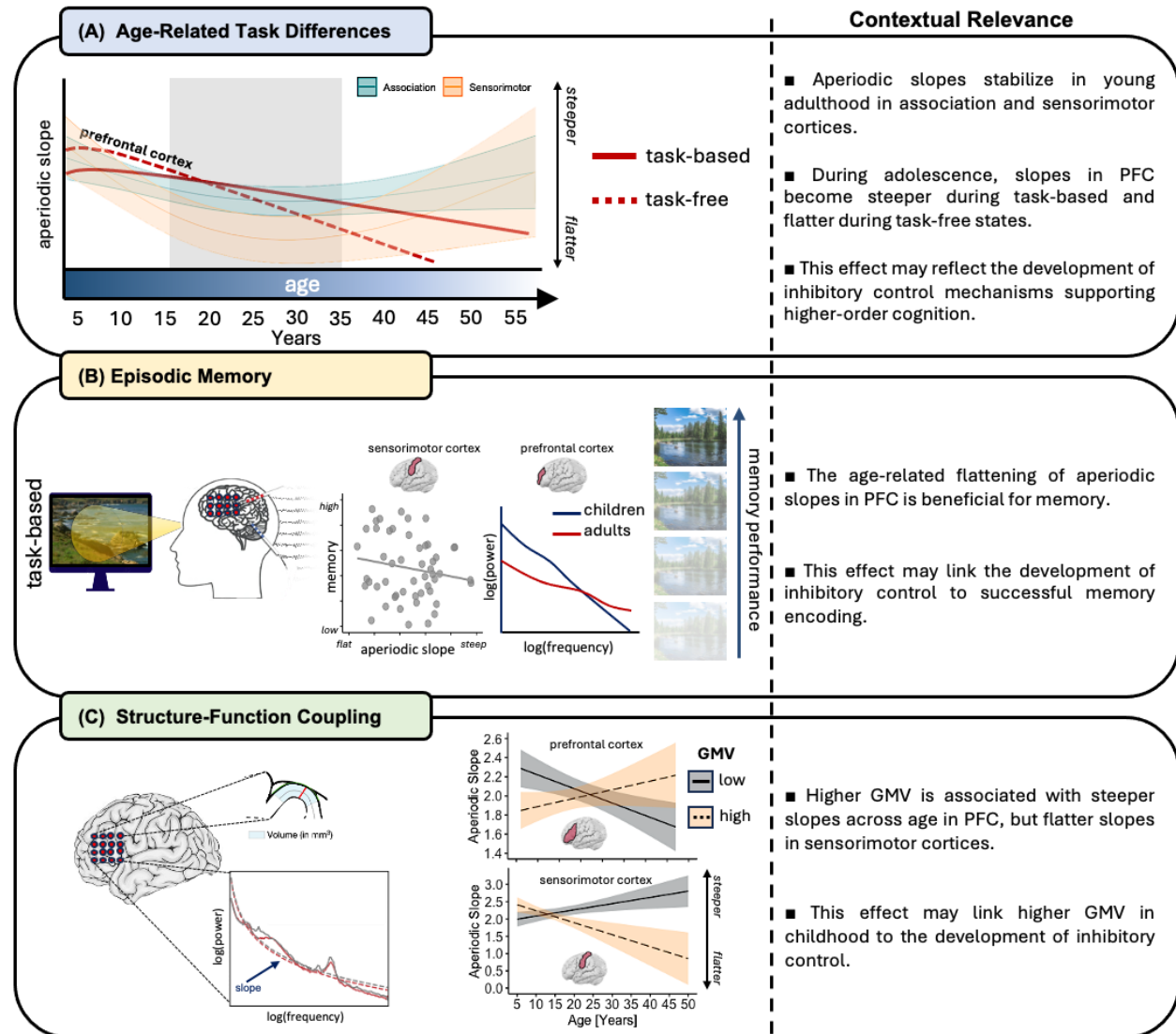
#### 44 **E:I balance is associated with age-related variability in gray matter volume**

45 Finally, having established that aperiodic activity differs by age and attentional state and that  
46 activity during task performance predicts memory outcomes, we mapped task-based aperiodic activity  
47 onto GMV across age. We reveal that in inferior frontal gyrus (IFG), lower GMV is associated with  
48 steeper aperiodic slopes during childhood, whereas the inverse relationship is observed during

1 adulthood. This suggests that premature cortical GMV pruning may precipitate an early steepening of  
2 aperiodic slopes, potentially leading to premature inhibitory processes and poorer memory outcomes.

3 Mechanistically, the observed relationship between GMV and aperiodic slopes in IFG can be  
4 interpreted through the lens of synaptic pruning and cortical maturation (Larsen et al., 2022; Legon et  
5 al., 2016). During childhood, accelerated pruning is posited to lead to reductions in GMV and a  
6 steepening of aperiodic slopes. This premature steepening may reflect E:I imbalance, adversely  
7 affecting cognitive functions such as memory encoding. In adulthood, however, the stabilization of  
8 synaptic networks and maintenance of GMV may facilitate flatter aperiodic slopes, indicative of a  
9 more balanced and established cortical state. Our findings suggest that E:I mechanisms may be  
10 disrupted by early reductions in regional GMV during childhood, leading to alterations in aperiodic  
11 activity.

12 By contrast, in postcentral gyrus (i.e., primary motor cortex), we observed that lower GMV is  
13 associated with flatter slopes during childhood and steeper slopes during adulthood. This is in addition  
14 to the finding that sensorimotor cortical development – as indexed by E:I balance – stabilizes during  
15 young adulthood, challenging models of early sensorimotor development based on cortical structure  
16 (Bethlehem et al., 2022; Larsen et al., 2022). The differential relationship between GMV and aperiodic  
17 slopes in association versus sensorimotor cortices by age highlights the complex interplay between  
18 structural and functional maturation. Indeed, rates of GMV development vary across brain regions  
19 (Bethlehem et al., 2022; Gogtay et al., 2004; Grydeland et al., 2019; Hill et al., 2010), as do rates of  
20 aperiodic activity development (Favaro et al., 2023; Hill et al., 2022; Schaworonkow & Voytek, 2021).  
21 Here, we identify the brain regions where these rates align and those where they diverge. Future  
22 research should further examine relationships between aperiodic activity and brain structure to  
23 elucidate the mechanisms by which structure-function development impacts the development of  
24 higher-order cognition.  
25



1  
2 **Figure 8. Aperiodic activity stabilizes in young adulthood, differs by age and attentional state, predicts age-**  
3 **related variability in episodic memory, and is associated with age-related variability in GMV. (A)** Aperiodic  
4 slopes in sensorimotor (orange) and association (teal) cortices flatten from age 5 – 25 years and steepen thereafter.  
5 Note that the flattening is more pronounced in sensorimotor than association cortices in adolescence and young  
6 adulthood (gray shading). Regarding attentional state (i.e., task-based vs. task-free) differences in aperiodic activity,  
7 in PFC, task-free (dashed red) slopes are steeper (i.e., greater inhibition) than task-based (solid red) slopes in children,  
8 and the inverse is observed in adults. Effects reverse at approximately ~18 – 20 years of age, likely reflecting the  
9 development of inhibitory control. **(B)** PFC-derived aperiodic slopes during task-based but not task-free states  
10 predicted age-related variability in memory performance, whereby the age-related flattening of aperiodic slopes was  
11 associated with age-related improvements in memory. Flatter sensorimotor cortical slopes were not associated with  
12 better memory performance after accounting for age. **(C)** Modeling the relationship between brain volume and  
13 aperiodic slopes revealed differential age-related differences in structure-function coupling. In PFC, lower GVM was  
14 associated with steeper slopes in childhood and flatter slopes in adulthood. In sensorimotor cortices, slopes were  
15 steeper in childhood regardless of GMV; in adolescence and adulthood, lower GMV was associated with steeper  
16 slopes and higher GMV was associated with flatter slopes.

17 **Limitations and future directions**

18 We have revealed regional age-related variations in aperiodic neural activity dependent upon  
19 task-state. Our findings suggest that brain development may be best understood as a diverse set of  
20



1 regionally independent trajectories, partially indexed by aperiodic activity. However, as iEEG data are  
2 cross-sectional, we were unable to follow these putative trajectories through time. A critical next step  
3 will be to establish the potential utility of aperiodic activity in elucidating longitudinal changes in  
4 regional structure-function relationships (Ofen et al., 2019). As such, future studies, focusing *a priori*  
5 on the regions we identified (e.g., MFG), could capitalize on the spatio-temporal precision and capacity  
6 to perform multi-visit longitudinal studies with, for example, MEG.

8 While our cohort is representative of typical development and the use of iEEG affords precise  
9 spatiotemporal precision, iEEG samples are comprised of pharmaco-resistant epilepsy patients,  
10 potentially limiting the generalizability of our findings (Johnson & Knight, 2023). For this reason, it is  
11 important to note that our sample demonstrated typical age-related gains in memory performance and  
12 age-related differences in global GMV (Figure 1C) that are consistent with healthy cohorts (Bethlehem  
13 et al., 2022). An additional limitation is the relatively lower representation of older individuals within  
14 our sample, a common observation in iEEG investigations, and the relatively lower representation of  
15 patients with task-free ( $n = 65$ ) compared to task-based ( $n = 81$ ) data. Nonetheless, the current results  
16 underscore maturation within MFG, and this effect was present across our entire age range of ~5 to  
17 54 years. To obtain larger samples across age, future research may seek to increase sample sizes  
18 through multi-site collaboration and data sharing (Johnson, Yin, et al., 2022; Johnson & Knight, 2023).

19 We also found no significant age-related difference in aperiodic activity in the hippocampus  
20 in relation to attentional state, or in predicting individual memory performance. Given that our study  
21 examined memory, these results may be somewhat surprising. However, it is possible that oscillatory  
22 activity in the hippocampus exhibits effects related to attentional state and memory outcomes,  
23 consistent with ample literature on hippocampal theta oscillations (Herweg et al., 2020; Lega et al.,  
24 2012). Future research should directly investigate this hypothesis. Lastly, with our task-based versus  
25 task-free contrast as a starting point, future research may also aim to examine additional attentional  
26 states, such as sleep versus wake states. The aperiodic slope and offset systematically shift as a function  
27 of sleep stage, which has recently been shown to differ across development (Favaro et al., 2023).  
28 However, it is unknown whether there are region-specific differences in sleep-based aperiodic activity,  
29 whether these regional differences relate to the development of higher-order cognition, and whether  
30 sleep-based aperiodic activity changes concomitantly with wake-related aperiodic dynamics.

### 31 **Implications**

32 Historically, neuroscientific research has predominantly focused on young adults aged 18-40  
33 years, largely overlooking the influence of age on brain dynamics. This practice has resulted in a  
34 significant knowledge gap regarding brain development. Addressing this gap is crucial due to its  
35 profound clinical implications across various domains, including neurodevelopmental disorders,  
36 traumatic brain injury, stroke, age-related cognitive decline, and neurodegenerative diseases, as well as  
37 advancements in neural prosthetics for injury, stroke, or disease management. Our study addresses  
38 this knowledge gap by elucidating the trajectory of aperiodic electrophysiological dynamics and their  
39 associations with brain structure and memory across development, from childhood into late middle  
40 adulthood. Previous attempts to characterize these dynamics have been constrained by limitations in  
41 imprecise spatiotemporal measurements and relatively small sample sizes. To overcome these  
42 challenges, we adopted a comprehensive approach. Firstly, we employed iEEG to delineate  
43 developmental neurophysiology with exceptional precision. Secondly, we applied sophisticated  
44 analyses of aperiodic components in iEEG data to establish novel connections between aperiodic  
45 activity and developmental variations in memory. Thirdly, we explored the relationship between  
46 aperiodic components and GMV. Lastly, we leveraged an exceptionally large iEEG dataset to detect  
47 subtle effects that may have been undetected in smaller cohorts.  
48

1 Understanding how cortical maturation influences memory encoding processes is also  
2 fundamental to cognitive function and daily performance, given well-documented changes in brain  
3 structure and function over the lifespan. Furthermore, elucidating the impact of brain development  
4 on memory formation across different life stages holds promise for early detection and intervention  
5 strategies targeting the emergence of both neurodevelopmental disorders and age-related memory  
6 decline. Identifying markers of healthy brain development and aging is crucial for detecting  
7 dysfunction in age-related pathologies, which often manifest gradually over many years before  
8 exhibiting overt behavioral symptoms. In this context, our findings may contribute to the prevention  
9 or delay of pathological aging, offering significant health benefits, particularly considering the  
10 limitations and risks associated with current pharmacological treatments. Additionally, our study lays  
11 the groundwork for investigating memory dysfunction in psychiatric disorders, many of which emerge  
12 during adolescence and young adulthood, and which show deviations in aperiodic activity from healthy  
13 populations (Earl et al., 2024; Fernandez & Garner, 2007; Pani et al., 2022; Shuffrey et al., 2022).

## 14 15 **Conclusions**

16 We reveal that aperiodic neural activity follows the same developmental time course across  
17 young adulthood in both sensorimotor and association cortices, challenging models of early  
18 sensorimotor development based on measures of brain structure. We also isolate attentional state and  
19 age-related differences in the aperiodic slope to PFC, demonstrating that task-based slopes are steeper,  
20 reflecting greater inhibition, and that this difference emerges during adolescence. We further establish  
21 the functional role of PFC-derived slopes in memory, revealing that age-related improvements in  
22 memory outcomes are associated with the age-related flattening of aperiodic slopes. The aperiodic  
23 offset, by contrast, which reflects overall neuronal spiking, predicts memory outcomes irrespective of  
24 age. Lastly, we characterized, for the first time, the relationship between age-related differences in  
25 aperiodic activity and brain structure, identifying region-specific trajectories in structure-function  
26 relationships during development. Taken together, our findings establish brain-wide maps in aperiodic  
27 neural activity, its relation to age-related variability in memory, and novel structure-function  
28 relationships, findings which are critical for understanding brain development and aging in both health  
29 and disease.

## 30 31 **Methods**

32  
33 **Participants.** Participants were 101 neurosurgical patients aged 5.93 – 54.00 years (63 males; mean  
34 age = 19.25) undergoing iEEG monitoring as part of clinical seizure management. Those with major  
35 lesions, prior surgical resections, noted developmental delays, or neuropsychological memory test  
36 scores <80 were considered ineligible. Patients were recruited from Northwestern Memorial Hospital,  
37 the Ann & Robert H. Lurie Children’s Hospital of Chicago, St. Louis Children’s Hospital, University  
38 of California, Irvine Medical Center, University of California, Davis Medical Center, University of  
39 California, San Francisco Benioff Children’s Hospital, Children’s Hospital of Michigan, and  
40 Nationwide Children’s Hospital, University of California, San Diego, Rady Children’s Hospital, Mount  
41 Sinai Hospital, California Pacific Medical Centre, and University of California, San Francisco Medical  
42 Centre. Written informed consent was obtained from participants aged 18 years and older and from  
43 the guardians of participants aged under 18 years. Written assent was obtained from participants aged  
44 13 – 17 years and oral assent was obtained from younger children. All procedures were approved by  
45 the Institutional Review Board at each hospital in accordance with the Declaration of Helsinki. Given  
46 that electrode positioning in these participants was based on clinical necessity rather than for  
47 experimental reasons, *a priori* power analyses were not performed. Human iEEG research is limited  
48 by the availability of neurosurgical patients. From this perspective, the majority of iEEG work has

1 been based on relatively small sample sizes and could not consider age-related or other sources of  
2 inter-individual variability (Johnson & Knight, 2023).

3  
4 **Experimental design.** Task-based iEEG data were derived from the encoding phase of two visual  
5 memory recognition tasks that have been used extensively to study memory in adults and children  
6 across neuroimaging modalities, including iEEG. In the blocked-trial paradigm, participants encode a  
7 set of 40 indoor and outdoor scenes and classify each as indoor/outdoor in preparation for a self-  
8 paced old/new recognition test of all 40 studied scenes intermixed with 20 new scenes as foils (Chai  
9 et al., 2010, 2014; Johnson, Tang, et al., 2018; Johnson, Yin, et al., 2022; Ofen et al., 2007, 2012, 2019;  
10 Tang et al., 2018; Yin et al., 2020, 2023). In the single trial paradigm, participants encode three shapes  
11 in a specific spatiotemporal sequence in preparation for a self-paced old/new recognition test of  
12 sequences that match exactly or mismatch on one dimension (i.e., shape identity, spatial position, or  
13 temporal order; cf. Davoudi et al., 2021; Dezfouli et al., 2021; Johnson, Adams, et al., 2018; Johnson,  
14 Chang, et al., 2022; Johnson et al., 2017, 2019). Both paradigms use visual stimuli to avoid potential  
15 confounds on memory with verbal material in children. The encoding phases of the two paradigms  
16 are similar because, in both paradigms, participants encode visual stimuli (3000ms, 500-1500ms inter-  
17 trial interval) in preparation for a self-paced, two-alternative forced choice recognition test. We  
18 ensured that on-task data reflected task engagement by only analyzing iEEG data during the viewing  
19 of stimuli that were attended during encoding, as indexed by a correct indoor/outdoor classification  
20 of each scene in the blocked-trial paradigm and correct old/new classification of each sequence in the  
21 single-trial paradigm (Johnson, Tang, et al., 2018; Johnson, Yin, et al., 2022; Yin et al., 2020). For a  
22 schematic of both visual memory tasks, see Figure S15. For task-free data, participants were instructed  
23 to sit quietly with their eyes open, fixating on the center of a computer monitor for five minutes. If  
24 no formal task-free task was administered, task-free data was taken from natural rest in continuous  
25 24/7 iEEG recordings.

26  
27 **Behavioral analysis.** Both visual memory tasks test memory in a two-alternative forced choice design,  
28 permitting the use of similar measures of memory performance across tasks. For both tasks, for all  
29 participants, we calculated the hit rate (i.e., number of previously studied stimuli that were correctly  
30 recognized as old/match out of all studied stimuli) and false alarm rate (number of new stimuli  
31 presented that were incorrectly identified as old/match out of all new/mismatched stimuli).  
32 Performance accuracy was calculated as hit rate minus false alarm rate to equate measures across  
33 memory tasks and correct for differences in an individual's tendency to respond old/match or  
34 new/mismatch, respectively. For a summary of behavioral performance, see Figure 1C.

35  
36 **iEEG acquisition and pre-processing.** iEEG data were recorded at a sampling rate of 200-5000  
37 Hz using Nihon Kohden JE120 Neurofax or Natus Quantum LTM recording systems interfaced with  
38 the BCI2000 software. Data acquired >1000 Hz were resampled to 1000 Hz after the fact. As  
39 described below, spectral analysis was performed up to 60 Hz. Thus, the lowest sampling rate of 200  
40 is well over the minimum Nyquist frequency required for analysis (i.e., 2 cycles/frequency = 120 Hz).  
41 For consistency, all data from both visual memory tasks and from task-free recordings were pre-  
42 processed using the same procedures. Raw electrophysiological data were filtered with 0.1-Hz high-  
43 pass and 300-Hz low-pass finite impulse response filters, and 60-Hz line noise harmonics were  
44 removed using a discrete Fourier transform. Task-based continuous data were demeaned and epoched  
45 into 3s trials (i.e., 0-3s from scene or study sequence onset). Continuous task-free data were also  
46 demeaned and transformed into 3s epochs with 25% overlap. All epoched data were manually  
47 inspected blind to electrode locations and experimental task parameters. Electrodes overlying seizure  
48 onset zones and electrodes and epochs displaying epileptiform activity or artifactual signal (from poor  
49 contact, machine noise, etc.) were excluded. Neighboring electrodes within the same anatomical  
50 structure were bipolar montage re-referenced using consistent conventions (ECoG, anterior –

1 posterior; sEEG, deep – surface). For ECoG grids, electrodes were referenced to neighboring  
2 electrodes on a row-by-row basis. An electrode was discarded if it did not have an adjacent neighbor,  
3 its neighbor was in a different anatomical structure, or both it and its neighbor were in white matter.  
4 Bipolar referencing yielded virtual channels that were located midway between the original physical  
5 electrodes. Data were then manually re-inspected to reject any trials with residual noise. Pre-processing  
6 routines used functions from the FieldTrip toolbox for MATLAB (Oostenveld et al., 2011). All results  
7 were based on analysis of non-pathologic, artifact-free channels, ensuring that data represented healthy  
8 cortical tissue (Rossini et al., 2017).

10 **Aperiodic neural activity.** The irregular-resampling auto-spectral analysis method (Wen & Liu, 2016)  
11 (IRASA) was used to estimate the  $1/f$  power-law exponent. IRASA estimates the aperiodic (random  
12 fractal) component of neural time series data by resampling the signal at multiple non-integer factors  
13  $b$  and their reciprocals  $1/b$ . As this resampling procedure systematically shifts narrowband peaks away  
14 from their original location along the frequency spectrum, averaging the spectral densities of the  
15 resampled series attenuates peak components while preserving the  $1/f$  distribution of the fractal  
16 component. The exponent summarizing the slope of aperiodic spectral activity is then calculated by  
17 fitting a linear regression to the estimated fractal component in log-log space. Using the YASA toolbox  
18 (Vallat & Walker, 2021) v.0.6.3 implemented in MNE-Python (Gramfort et al., 2013) v.1.3.1, we fit a  
19 power-law function to each fractal estimate within the frequency range of 1 – 60 Hz. For each epoch,  
20 channel, and task, the inverse slope of the power-law function was taken as the trial-level estimate of  
21 the  $1/f$  exponent. The aperiodic offset (i.e., intercept of the power-law function) was also extracted,  
22 which reflects the initial amplitude of the power-law.

24 **iEEG localization.** Macro-electrodes were surgically implanted for extra-operative recording based  
25 solely on clinical need. The electrodes were subdural electrode grids or strips with 10 mm spacing or  
26 stereoelectroencephalography electrodes with 5-10 mm spacing. Anatomical locations were  
27 determined by co-registering post-implantation computed tomography coordinates to pre-operative  
28 magnetic resonance (MR) images, as implemented in FieldTrip (Stolk et al., 2018), FreeSurfer (Fischl,  
29 2012), iELVis (Groppe et al., 2017) or VERA (Adamek et al., 2022). Electrode locations were then  
30 projected into standard MNI space and bipolar channel locations (see preprocessing) were projected  
31 at the midpoint between their contributing electrodes. Based on these MNI coordinates, the R package  
32 *label4MRI* v1.2 (<https://github.com/yunshiuian/label4MRI>) was used to categorize each channel into  
33 its corresponding Brodmann area, which were then grouped according to the DKT atlas (Klein &  
34 Tourville, 2012).

36 **Structural imaging and regional gray matter volume.** T1-weighted MRI scans were acquired as  
37 part of routine preoperative procedures. Parcellation of cortex into regions of interest (ROI) was  
38 performed based on standard procedures implemented within FreeSurfer (Fischl, 2012). Regional  
39 GMVs were then estimated based on the DKT atlas (Klein & Tourville, 2012). GMV from each ROI  
40 was calculated using FreeSurfer (Fischl, 2012). Volumes were calculated for left and right ROIs and  
41 averaged across hemispheres for analysis.

43 **Statistical analysis.** Data were imported into R version 4.2.3 (R Core Team, 2020) with the aid of  
44 the *tidyverse* package (Wickham et al., 2019) and analyzed using linear and nonlinear mixed-effects  
45 models fit by restricted maximum likelihood (REML) using *lme4* (Bates, 2010) and *splines* (R Core  
46 Team, 2020). *P*-values were estimated using the summary function from the *lmerTest* package, which  
47 is based on Satterthwaite's degrees of freedom (Kuznetsova et al., 2017), and effects were plotted  
48 using the package *ggeffects* (Lüdtke, 2018) and *ggplot2* (Wickham & Wickham, 2016). Statistical  
49 significance was adjusted using the False Discovery Rate with an alpha threshold of .05 in analyses  
50 modeling aperiodic activity on a region-by-region basis testing hypothesis b. Task was entered as an



1 unordered factor using sum-to-zero contrast coding and age was specified as a continuous predictor.  
2 In our preregistration, we specified that we would apply cubic splines to age to model potential non-  
3 linear effects of age on aperiodic activity for each ROI, as well as a random effect of task-free recording  
4 type (eyes open vs eyes closed). However, in doing so, models indicated nonconvergence or singular  
5 fit. To reduce model complexity, we modeled age as a linear predictor and removed task-free recording  
6 type as a random effect in our analysis of each ROI. For analyses testing hypotheses a and b, where  
7 we tested differences in association and sensorimotor cortices, we had sufficient power to model  
8 nonlinear differences. Also note that when contrast coding is explicitly described, the need for post-  
9 hoc testing is eliminated (for a detailed discussion of contrast coding in linear mixed-effects  
10 regressions, please see (Brehm & Alday, 2022). Further, for modeled effects, an 83% confidence  
11 interval (CI) threshold was used given that this approach corresponds to the 5% significance level  
12 with non-overlapping estimates (Austin & Hux, 2002; MacGregor-Fors & Payton, 2013). In order to  
13 isolate outliers, we used Tukey's method (Tukey, 1977), which identifies outliers as exceeding  $\pm 1.5 \times$   
14 inter-quartile range. The packages *ggseg* (Mowinckel & Vidal-Piñero, 2020) and *ggsegDKT* were used to  
15 generate cortical plots based on DKT atlas nomenclature. Hypotheses a and b were tested using the  
16 following formula:

$$17 \quad EEG_i = \beta_0 + \beta_1 ns(age, 2)_i * \beta_2 region_i + channel/subject_{0i} + \epsilon,$$

18 where *EEG* is the aperiodic estimate; *age* is age in years modeled with two spline terms, and *region*  
19 encodes association and sensorimotor cortices; *channel* encodes region-specific channels nested under  
20 the random intercept of *participant*, and *participant* is the random intercept term of participant ID. To  
21 test hypothesis c, we employed the following model equation on a region-by-region basis:

$$22 \quad EEG_i = \beta_0 + \beta_1 condition_i * \beta_2 age_i + channel/subject_{0i} + task_{0i} + \epsilon,$$

23 where *EEG* is the aperiodic estimate; *condition* encodes task-based and task-free recordings, age is age  
24 in years as a linear predictor; *channel* encodes region-specific channels nested under *participant*, and  
25 *participant* is participant ID, while *task* is a random intercept encoding whether the recording is derived  
26 from the working memory or scene recognition tasks.

27  
28 Our exploratory analyses focused on relationships between GMV, behavioral performance, and  
29 aperiodic estimates derived from task-based and task-free recordings. Here, our primary exploratory  
30 research questions were whether:

- 31 i) regional age-related variability in aperiodic neural activity predicts variability in memory  
32 performance, and;
- 33 ii) regional age-related variability in GMV predicts regional variability in aperiodic neural  
34 activity.

35 These exploratory analyses were examined with general linear models with the following formulae:

$$36 \quad (a) \quad memory_i = \beta_0 + \beta_1 age_i * \beta_2 EEG_i + \epsilon,$$

37 where *memory* is performance on the visual memory task(s), *age* is age in years, and *EEG* is the aperiodic  
38 estimate from each ROI.

$$39 \quad (b) \quad EEG_i = \beta_0 + \beta_1 age_i * \beta_2 volume_i + channel/subject_{0i} + task_{0i} + \epsilon,$$

40 Here, *EEG* is the aperiodic estimate; *age* is age in years; *volume* is regional GMV in  $mm^3$ ; *channel* encodes  
41 ROI-specific channels; *participant* is participant ID; *task* encodes whether the task recording was from  
42 the scene recognition or working memory task. As with the other models, each ROI was applied to  
43 the model equation described above. *Participant* was modeled as a random effect on the intercept, while  
44 *channel* was nested under participant. *Task* were also specified as a random effect on the intercept.  
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1 Note that in our preregistration, we stated that we would include task (task-based, task-free) in all  
2 models examining the interaction between GMV and age on aperiodic activity. However, all models  
3 indicated nonconvergence or singular fits. To reduce model complexity, we examined aperiodic  
4 activity during task-based states only.  
5

6 A final exploratory analysis examined the aperiodic offset. Here, we submitted the aperiodic offset to  
7 the same models that we specified for the slope, with the following formulae (the description of each  
8 fixed and random effect structure is described for the model equations presented above):  
9

10 (a)  $offset_i = \beta_0 + \beta_1 condition_i * \beta_2 age_i + channel/subject_{0i} + task_{0i} + \epsilon,$

11 (b)  $memory_i = \beta_0 + \beta_1 age_i * \beta_2 offset + \epsilon,$

12 (c)  $offset = \beta_0 + \beta_1 age_i * \beta_2 volume_i + channel/subject_{0i} + task_{0i} + \epsilon,$   
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References

- 1  
2 Adamek, M., Swift, J., & Brunner, P. (2022). VERA-Versatile electrode localization Framework.  
3 *Preprint.* *Version Doi-Release*, 10.
- 4 Ahmad, J., Ellis, C., Leech, R., Voytek, B., Garces, P., Jones, E., Buitelaar, J., Loth, E., dos Santos, F.  
5 P., Amil, A. F., Verschure, P. F. M. J., Murphy, D., & McAlonan, G. (2022). From  
6 mechanisms to markers: Novel noninvasive EEG proxy markers of the neural excitation and  
7 inhibition system in humans. *Translational Psychiatry*, 12(1), 467.  
8 <https://doi.org/10.1038/s41398-022-02218-z>
- 9 Amigó, J. M., Szczepański, J., Wajnryb, E., & Sanchez-Vives, M. V. (2004). Estimating the Entropy  
10 Rate of Spike Trains via Lempel-Ziv Complexity. *Neural Computation*, 16(4), 717–736.  
11 <https://doi.org/10.1162/089976604322860677>
- 12 Austin, P. C., & Hux, J. E. (2002). A brief note on overlapping confidence intervals. *Journal of*  
13 *Vascular Surgery*, 36(1), 194–195.
- 14 Axmacher, N., Elger, C. E., & Fell, J. (2008). Memory formation by refinement of neural  
15 representations: The inhibition hypothesis. *Behavioural Brain Research*, 189(1), 1–8.  
16 <https://doi.org/10.1016/j.bbr.2007.12.018>
- 17 Barron, H. C. (2021). Neural inhibition for continual learning and memory. *Neurobiology of Learning*  
18 *and Plasticity*, 67, 85–94. <https://doi.org/10.1016/j.conb.2020.09.007>
- 19 Bates, D. M. (2010). *lme4: Mixed-effects modeling with R*.
- 20 Bethlehem, R. A. I., Seidlitz, J., White, S. R., Vogel, J. W., Anderson, K. M., Adamson, C., Adler, S.,  
21 Alexopoulos, G. S., Anagnostou, E., Areces-Gonzalez, A., Astle, D. E., Auyeung, B., Ayub,  
22 M., Bae, J., Ball, G., Baron-Cohen, S., Beare, R., Bedford, S. A., Benegal, V., ... Alexander-  
23 Bloch, A. F. (2022). Brain charts for the human lifespan. *Nature*, 604(7906), 525–533.  
24 <https://doi.org/10.1038/s41586-022-04554-y>
- 25 Bornkessel-Schlesewsky, I., Alday, P. M., Corcoran, A. W., Wilkinson, E. M., Sharrad, I., Kliegl, R.,  
26 Lewis, R. L., Small, S. L., & Schlewsky, M. (2022). Effects of neural noise on predictive  
27 model updating across the adult lifespan. *bioRxiv*, 2022–12.
- 28 Bornkessel-Schlesewsky, I., Sharrad, I., Howlett, C. A., Alday, P. M., Corcoran, A. W., Bellan, V.,  
29 Wilkinson, E., Kliegl, R., Lewis, R. L., & Small, S. L. (2022). Rapid adaptation of predictive  
30 models during language comprehension: Aperiodic EEG slope, individual alpha frequency  
31 and idea density modulate individual differences in real-time model updating. *Frontiers in*  
32 *Psychology*, 13, 817516.
- 33 Braver, T. S., Paxton, J. L., Locke, H. S., & Barch, D. M. (2009). Flexible neural mechanisms of  
34 cognitive control within human prefrontal cortex. *Proceedings of the National Academy of Sciences*,  
35 106(18), 7351–7356. <https://doi.org/10.1073/pnas.0808187106>
- 36 Brehm, L., & Alday, P. M. (2022). Contrast coding choices in a decade of mixed models. *Journal of*  
37 *Memory and Language*, 125, 104334.
- 38 Buzsáki, G. (2006). *Rhythms of the Brain*. Oxford university press.
- 39 Cabeza, R., Albert, M., Belleville, S., Craik, F. I. M., Duarte, A., Grady, C. L., Lindenberger, U.,  
40 Nyberg, L., Park, D. C., Reuter-Lorenz, P. A., Rugg, M. D., Steffener, J., & Rajah, M. N.  
41 (2018). Maintenance, reserve and compensation: The cognitive neuroscience of healthy

- 1 ageing. *Nature Reviews Neuroscience*, 19(11), 701–710. [https://doi.org/10.1038/s41583-018-](https://doi.org/10.1038/s41583-018-0068-2)  
2 0068-2
- 3 Cellier, D., Riddle, J., Petersen, I., & Hwang, K. (2021). The development of theta and alpha neural  
4 oscillations from ages 3 to 24 years. *Developmental Cognitive Neuroscience*, 50, 100969.  
5 <https://doi.org/10.1016/j.dcn.2021.100969>
- 6 Chai, X. J., Ofen, N., Gabrieli, J. D., & Whitfield-Gabrieli, S. (2014). Development of deactivation  
7 of the default-mode network during episodic memory formation. *Neuroimage*, 84, 932–938.
- 8 Chai, X. J., Ofen, N., Jacobs, L. F., & Gabrieli, J. D. (2010). Scene complexity: Influence on  
9 perception, memory, and development in the medial temporal lobe. *Frontiers in Human*  
10 *Neuroscience*, 4, 1021.
- 11 Cross, Z. R., Corcoran, A. W., Schlesewsky, M., Kohler, M. J., & Bornkessel-Schlesewsky, I. (2022).  
12 Oscillatory and aperiodic neural activity jointly predict language learning. *Journal of Cognitive*  
13 *Neuroscience*, 34(9), 1630–1649.
- 14 Dave, S., Brothers, T. A., & Swaab, T. Y. (2018). 1/f neural noise and electrophysiological indices of  
15 contextual prediction in aging. *Brain Research*, 1691, 34–43.  
16 <https://doi.org/10.1016/j.brainres.2018.04.007>
- 17 Davoudi, S., Parto Dezfouli, M., Knight, R. T., Daliri, M. R., & Johnson, E. L. (2021). Prefrontal  
18 lesions disrupt posterior alpha–gamma coordination of visual working memory  
19 representations. *Journal of Cognitive Neuroscience*, 33(9), 1798–1810.
- 20 Dezfouli, M. P., Davoudi, S., Knight, R. T., Daliri, M. R., & Johnson, E. L. (2021). Prefrontal lesions  
21 disrupt oscillatory signatures of spatiotemporal integration in working memory. *Cortex*, 138,  
22 113–126.
- 23 Donoghue, T., Haller, M., Peterson, E. J., Varma, P., Sebastian, P., Gao, R., Noto, T., Lara, A. H.,  
24 Wallis, J. D., & Knight, R. T. (2020). Parameterizing neural power spectra into periodic and  
25 aperiodic components. *Nature Neuroscience*, 23(12), 1655–1665.
- 26 Doval, S., López-Sanz, D., Bruña, R., Cuesta, P., Antón-Toro, L., Taguas, I., Torres-Simón, L.,  
27 Chino, B., & Maestú, F. (2024). When Maturation is Not Linear: Brain Oscillatory Activity in  
28 the Process of Aging as Measured by Electrophysiology. *Brain Topography*.  
29 <https://doi.org/10.1007/s10548-024-01064-0>
- 30 Dziego, C. A., Bornkessel-Schlesewsky, I., Jano, S., Chatburn, A., Schlesewsky, M., Immink, M. A.,  
31 Sinha, R., Irons, J., Schmitt, M., & Chen, S. (2023). Neural and cognitive correlates of  
32 performance in dynamic multi-modal settings. *Neuropsychologia*, 180, 108483.
- 33 Earl, R. J., Ford, T. C., Lum, J. A. G., Enticott, P. G., & Hill, A. T. (2024). Exploring aperiodic  
34 activity in first episode schizophrenia spectrum psychosis: A resting-state EEG analysis.  
35 *Brain Research*, 1840, 149052. <https://doi.org/10.1016/j.brainres.2024.149052>
- 36 Euler, M. J., Vehar, J. V., Guevara, J. E., Geiger, A. R., Deboeck, P. R., & Lohse, K. R. (2024).  
37 Associations between the resting EEG aperiodic slope and broad domains of cognitive  
38 ability. *Psychophysiology*, n/a(n/a), e14543. <https://doi.org/10.1111/psyp.14543>
- 39 Favaro, J., Colombo, M. A., Mikulan, E., Sartori, S., Nosadini, M., Pelizza, M. F., Rosanova, M.,  
40 Sarasso, S., Massimini, M., & Toldo, I. (2023). The maturation of aperiodic EEG activity



- 1 across development reveals a progressive differentiation of wakefulness from sleep.  
2 *NeuroImage*, 277, 120264. <https://doi.org/10.1016/j.neuroimage.2023.120264>
- 3 Fernandez, F., & Garner, C. C. (2007). Over-inhibition: A model for developmental intellectual  
4 disability. *Trends in Neurosciences*, 30(10), 497–503.
- 5 Finley, A. J., Angus, D. J., Van Reekum, C. M., Davidson, R. J., & Schaefer, S. M. (2022). Periodic  
6 and aperiodic contributions to theta-beta ratios across adulthood. *Psychophysiology*, 59(11),  
7 e14113.
- 8 Fischer, M., Moscovitch, M., & Alain, C. (2021). A systematic review and meta-analysis of memory-  
9 guided attention: Frontal and parietal activation suggests involvement of fronto-parietal  
10 networks. *Wiley Interdisciplinary Reviews: Cognitive Science*, 12(1), e1546.
- 11 Fischl, B. (2012). FreeSurfer. *Neuroimage*, 62(2), 774–781.
- 12 Fotiadis, P., Cieslak, M., He, X., Caciagli, L., Ouellet, M., Satterthwaite, T. D., Shinohara, R. T., &  
13 Bassett, D. S. (2023). Myelination and excitation-inhibition balance synergistically shape  
14 structure-function coupling across the human cortex. *Nature Communications*, 14(1), 6115.  
15 <https://doi.org/10.1038/s41467-023-41686-9>
- 16 Fuster, J. M. (2002). Frontal lobe and cognitive development. *Journal of Neurocytology*, 31(3), 373–385.  
17 <https://doi.org/10.1023/A:1024190429920>
- 18 Gao, R., Peterson, E. J., & Voytek, B. (2017). Inferring synaptic excitation/inhibition balance from  
19 field potentials. *NeuroImage*, 158, 70–78. <https://doi.org/10.1016/j.neuroimage.2017.06.078>
- 20 Gazit, T., Gonen, T., Gurevitch, G., Cohen, N., Strauss, I., Zeevi, Y., Yamin, H., Fahoum, F.,  
21 Hendler, T., & Fried, I. (2020). The role of mPFC and MTL neurons in human choice under  
22 goal-conflict. *Nature Communications*, 11(1), 3192. [https://doi.org/10.1038/s41467-020-](https://doi.org/10.1038/s41467-020-16908-z)  
23 [16908-z](https://doi.org/10.1038/s41467-020-16908-z)
- 24 Gogtay, N., Giedd, J. N., Lusk, L., Hayashi, K. M., Greenstein, D., Vaituzis, A. C., Nugent, T. F.,  
25 Herman, D. H., Clasen, L. S., Toga, A. W., Rapoport, J. L., & Thompson, P. M. (2004).  
26 Dynamic mapping of human cortical development during childhood through early  
27 adulthood. *Proceedings of the National Academy of Sciences*, 101(21), 8174–8179.  
28 <https://doi.org/10.1073/pnas.0402680101>
- 29 Gramfort, A., Luessi, M., Larson, E., Engemann, D. A., Strohmeier, D., Brodbeck, C., Goj, R., Jas,  
30 M., Brooks, T., & Parkkonen, L. (2013). MEG and EEG data analysis with MNE-Python.  
31 *Frontiers in Neuroscience*, 267.
- 32 Groeschel, S., Vollmer, B., King, M., & Connelly, A. (2010). Developmental changes in cerebral grey  
33 and white matter volume from infancy to adulthood. *International Journal of Developmental*  
34 *Neuroscience*, 28(6), 481–489.
- 35 Groppe, D. M., Bickel, S., Dykstra, A. R., Wang, X., Mégevand, P., Mercier, M. R., Lado, F. A.,  
36 Mehta, A. D., & Honey, C. J. (2017). iELVis: An open source MATLAB toolbox for  
37 localizing and visualizing human intracranial electrode data. *Journal of Neuroscience Methods*,  
38 281, 40–48.
- 39 Grydeland, H., Vértes, P. E., Váša, F., Romero-Garcia, R., Whitaker, K., Alexander-Bloch, A. F.,  
40 Bjørnerud, A., Patel, A. X., Sederevičius, D., & Tamnes, C. K. (2019). Waves of maturation

- 1 and senescence in micro-structural MRI markers of human cortical myelination over the  
2 lifespan. *Cerebral Cortex*, 29(3), 1369–1381.
- 3 Herweg, N. A., Solomon, E. A., & Kahana, M. J. (2020). Theta Oscillations in Human Memory.  
4 *Trends in Cognitive Sciences*, 24(3), 208–227. <https://doi.org/10.1016/j.tics.2019.12.006>
- 5 Hill, A. T., Clark, G. M., Bigelow, F. J., Lum, J. A. G., & Enticott, P. G. (2022). Periodic and  
6 aperiodic neural activity displays age-dependent changes across early-to-middle childhood.  
7 *Developmental Cognitive Neuroscience*, 54, 101076. <https://doi.org/10.1016/j.dcn.2022.101076>
- 8 Hill, J., Inder, T., Neil, J., Dierker, D., Harwell, J., & Van Essen, D. (2010). Similar patterns of  
9 cortical expansion during human development and evolution. *Proceedings of the National  
10 Academy of Sciences*, 107(29), 13135–13140.
- 11 Hill, P. F., King, D. R., Lega, B. C., & Rugg, M. D. (2020). Comparison of fMRI correlates of  
12 successful episodic memory encoding in temporal lobe epilepsy patients and healthy  
13 controls. *NeuroImage*, 207, 116397.
- 14 Hunt, B. A., Tewarie, P. K., Mougín, O. E., Geades, N., Jones, D. K., Singh, K. D., Morris, P. G.,  
15 Gowland, P. A., & Brookes, M. J. (2016). Relationships between cortical myeloarchitecture  
16 and electrophysiological networks. *Proceedings of the National Academy of Sciences*, 113(47),  
17 13510–13515.
- 18 Immink, M. A., Cross, Z. R., Chatburn, A., Baumeister, J., Schlesewsky, M., & Bornkessel-  
19 Schlesewsky, I. (2021). Resting-state aperiodic neural dynamics predict individual differences  
20 in visuomotor performance and learning. *Human Movement Science*, 78, 102829.
- 21 Irene Gonzalez-Burgos, Marie Bainier, Simon Gross, Philipp Schoenenberger, José A. Ochoa,  
22 Miguel Valencia, & Roger L. Redondo. (2023). Glutamatergic and GABAergic Receptor  
23 Modulation Present Unique Electrophysiological Fingerprints in a Concentration-Dependent  
24 and Region-Specific Manner. *Eneuro*, 10(4), ENEURO.0406-22.2023.  
25 <https://doi.org/10.1523/ENEURO.0406-22.2023>
- 26 Johnson, E. L., Adams, J. N., Solbakk, A.-K., Endestad, T., Larsson, P. G., Ivanovic, J., Meling, T.  
27 R., Lin, J. J., & Knight, R. T. (2018). Dynamic frontotemporal systems process space and  
28 time in working memory. *PLoS Biology*, 16(3), e2004274.
- 29 Johnson, E. L., Chang, W. K., Dewar, C. D., Sorensen, D., Lin, J. J., Solbakk, A.-K., Endestad, T.,  
30 Larsson, P. G., Ivanovic, J., & Meling, T. R. (2022). Orbitofrontal cortex governs working  
31 memory for temporal order. *Current Biology*, 32(9), R410–R411.
- 32 Johnson, E. L., Dewar, C. D., Solbakk, A.-K., Endestad, T., Meling, T. R., & Knight, R. T. (2017).  
33 Bidirectional frontoparietal oscillatory systems support working memory. *Current Biology*,  
34 27(12), 1829–1835.
- 35 Johnson, E. L., Kam, J. W., Tzovara, A., & Knight, R. T. (2020). Insights into human cognition  
36 from intracranial EEG: a review of audition, memory, internal cognition, and causality.  
37 *Journal of Neural Engineering*, 17(5), 051001.
- 38 Johnson, E. L., King-Stephens, D., Weber, P. B., Laxer, K. D., Lin, J. J., & Knight, R. T. (2019).  
39 Spectral imprints of working memory for everyday associations in the frontoparietal  
40 network. *Frontiers in Systems Neuroscience*, 12, 65.

- 1 Johnson, E. L., & Knight, R. T. (2015). Intracranial recordings and human memory. *Current Opinion*
- 2 *in Neurobiology*, *31*, 18–25. <https://doi.org/10.1016/j.conb.2014.07.021>
- 3 Johnson, E. L., & Knight, R. T. (2023). How Can iEEG Be Used to Study Inter-Individual and
- 4 Developmental Differences? In *Intracranial EEG: A Guide for Cognitive Neuroscientists* (pp. 143–
- 5 154). Springer.
- 6 Johnson, E. L., Tang, L., Yin, Q., Asano, E., & Ofen, N. (2018). Direct brain recordings reveal
- 7 prefrontal cortex dynamics of memory development. *Science Advances*, *4*(12), eaat3702.
- 8 <https://doi.org/10.1126/sciadv.aat3702>
- 9 Johnson, E. L., Yin, Q., O’Hara, N. B., Tang, L., Jeong, J.-W., Asano, E., & Ofen, N. (2022).
- 10 Dissociable oscillatory theta signatures of memory formation in the developing brain. *Current*
- 11 *Biology*, *32*(7), 1457-1469.e4. <https://doi.org/10.1016/j.cub.2022.01.053>
- 12 Klein, A., & Tourville, J. (2012). 101 Labeled Brain Images and a Consistent Human Cortical
- 13 Labeling Protocol. *Frontiers in Neuroscience*, *6*.
- 14 <https://www.frontiersin.org/journals/neuroscience/articles/10.3389/fnins.2012.00171>
- 15 Kolk, S. M., & Rakic, P. (2022). Development of prefrontal cortex. *Neuropsychopharmacology*, *47*(1),
- 16 41–57. <https://doi.org/10.1038/s41386-021-01137-9>
- 17 Kuznetsova, A., Brockhoff, P. B., & Christensen, R. H. (2017). lmerTest package: Tests in linear
- 18 mixed effects models. *Journal of Statistical Software*, *82*, 1–26.
- 19 Larsen, B., Cui, Z., Adebimpe, A., Pines, A., Alexander-Bloch, A., Bertolero, M., Calkins, M. E.,
- 20 Gur, R. E., Gur, R. C., Mahadevan, A. S., Moore, T. M., Roalf, D. R., Seidlitz, J., Sydnor, V.
- 21 J., Wolf, D. H., & Satterthwaite, T. D. (2022). A developmental reduction of the
- 22 excitation:inhibition ratio in association cortex during adolescence. *Science Advances*, *8*(5),
- 23 eabj8750. <https://doi.org/10.1126/sciadv.abj8750>
- 24 Lega, B. C., Jacobs, J., & Kahana, M. (2012). Human hippocampal theta oscillations and the
- 25 formation of episodic memories. *Hippocampus*, *22*(4), 748–761.
- 26 <https://doi.org/10.1002/hipo.20937>
- 27 Legon, W., Punzell, S., Dowlati, E., Adams, S. E., Stiles, A. B., & Moran, R. J. (2016). Altered
- 28 Prefrontal Excitation/Inhibition Balance and Prefrontal Output: Markers of Aging in
- 29 Human Memory Networks. *Cerebral Cortex*, *26*(11), 4315–4326.
- 30 <https://doi.org/10.1093/cercor/bhv200>
- 31 Lendner, J. D., Harler, U., Daume, J., Engel, A. K., Zöllner, C., Schneider, T. R., & Fischer, M.
- 32 (2023). Oscillatory and aperiodic neuronal activity in working memory following anesthesia.
- 33 *Clinical Neurophysiology*, *150*, 79–88. <https://doi.org/10.1016/j.clinph.2023.03.005>
- 34 Lendner, J. D., Niethard, N., Mander, B. A., van Schalkwijk, F. J., Schuh-Hofer, S., Schmidt, H.,
- 35 Knight, R. T., Born, J., Walker, M. P., Lin, J. J., & Helfrich, R. F. (2023). Human REM sleep
- 36 recalibrates neural activity in support of memory formation. *Science Advances*, *9*(34), eadj1895.
- 37 <https://doi.org/10.1126/sciadv.adj1895>
- 38 Leszczyński, M., Barczak, A., Kajikawa, Y., Ulbert, I., Falchier, A. Y., Tal, I., Haegens, S., Melloni,
- 39 L., Knight, R. T., & Schroeder, C. E. (2020). Dissociation of broadband high-frequency
- 40 activity and neuronal firing in the neocortex. *Science Advances*, *6*(33), eabb0977.

- 1 Lüdecke, D. (2018). ggeffects: Tidy data frames of marginal effects from regression models. *Journal of*  
2 *Open Source Software*, 3(26), 772.
- 3 MacGregor-Fors, I., & Payton, M. E. (2013). Contrasting diversity values: Statistical inferences based  
4 on overlapping confidence intervals. *PLoS One*, 8(2), e56794.
- 5 Mahjoory, K., Schoffelen, J.-M., Keitel, A., & Gross, J. (2020). The frequency gradient of human  
6 resting-state brain oscillations follows cortical hierarchies. *eLife*, 9, e53715.  
7 <https://doi.org/10.7554/eLife.53715>
- 8 Manning, J. R., Jacobs, J., Fried, I., & Kahana, M. J. (2009). Broadband shifts in local field potential  
9 power spectra are correlated with single-neuron spiking in humans. *Journal of Neuroscience*,  
10 29(43), 13613–13620.
- 11 McKeon, S. D., Perica, M. I., Parr, A. C., Calabro, F. J., Foran, W., Hetherington, H., Moon, C.-H.,  
12 & Luna, B. (2024). Aperiodic EEG and 7T MRSI evidence for maturation of E/I balance  
13 supporting the development of working memory through adolescence. *Developmental Cognitive*  
14 *Neuroscience*, 66, 101373.
- 15 McSweeney, M., Morales, S., Valadez, E. A., Buzzell, G. A., Yoder, L., Fifer, W. P., Pini, N.,  
16 Shuffrey, L. C., Elliott, A. J., Isler, J. R., & Fox, N. A. (2023). Age-related trends in aperiodic  
17 EEG activity and alpha oscillations during early- to middle-childhood. *NeuroImage*, 269,  
18 119925. <https://doi.org/10.1016/j.neuroimage.2023.119925>
- 19 Medel, V., Irani, M., Crossley, N., Ossandón, T., & Boncompte, G. (2023). Complexity and 1/f  
20 slope jointly reflect brain states. *Scientific Reports*, 13(1), 21700.  
21 <https://doi.org/10.1038/s41598-023-47316-0>
- 22 Merkin, A., Sghirripa, S., Graetz, L., Smith, A. E., Hordacre, B., Harris, R., Pitcher, J., Semmler, J.,  
23 Rogasch, N. C., & Goldsworthy, M. (2023). Do age-related differences in aperiodic neural  
24 activity explain differences in resting EEG alpha? *Neurobiology of Aging*, 121, 78–87.  
25 <https://doi.org/10.1016/j.neurobiolaging.2022.09.003>
- 26 Miller, E. K., & Cohen, J. D. (2001). An Integrative Theory of Prefrontal Cortex Function. In  
27 *Annual Review of Neuroscience* (Vol. 24, Issue Volume 24, 2001, pp. 167–202). Annual Reviews.  
28 <https://doi.org/10.1146/annurev.neuro.24.1.167>
- 29 Miller, K. J., Hermes, D., Honey, C. J., Hebb, A. O., Ramsey, N. F., Knight, R. T., Ojemann, J. G.,  
30 & Fetz, E. E. (2012). *Human motor cortical activity is selectively phase-entrained on underlying rhythms*.
- 31 Molina, J. L., Voytek, B., Thomas, M. L., Joshi, Y. B., Bhakta, S. G., Talledo, J. A., Swerdlow, N. R.,  
32 & Light, G. A. (2020). Memantine Effects on Electroencephalographic Measures of Putative  
33 Excitatory/Inhibitory Balance in Schizophrenia. *Biological Psychiatry: Cognitive Neuroscience and*  
34 *Neuroimaging*, 5(6), 562–568. <https://doi.org/10.1016/j.bpsc.2020.02.004>
- 35 Montemurro, S., Borek, D., Marinazzo, D., Zago, S., Masina, F., Napoli, E., Filippini, N., & Arcara,  
36 G. (2024). Aperiodic component of EEG power spectrum and cognitive performance are  
37 modulated by education in aging. *Scientific Reports*, 14(1), 15111.  
38 <https://doi.org/10.1038/s41598-024-66049-2>
- 39 Mowinckel, A. M., & Vidal-Piñeiro, D. (2020). Visualization of brain statistics with R packages ggseg  
40 and ggseg3d. *Advances in Methods and Practices in Psychological Science*, 3(4), 466–483.



- 1 Musall, S., von Pföstel, V., Rauch, A., Logothetis, N. K., & Whittingstall, K. (2014). Effects of Neural  
2 Synchrony on Surface EEG. *Cerebral Cortex*, *24*(4), 1045–1053.  
3 <https://doi.org/10.1093/cercor/bhs389>
- 4 Nir, Y., Fisch, L., Mukamel, R., Gelbard-Sagiv, H., Arieli, A., Fried, I., & Malach, R. (2007).  
5 Coupling between neuronal firing rate, gamma LFP, and BOLD fMRI is related to  
6 interneuronal correlations. *Current Biology*, *17*(15), 1275–1285.
- 7 Noudoost, B., & Moore, T. (2011). Control of visual cortical signals by prefrontal dopamine. *Nature*,  
8 *474*(7351), 372–375. <https://doi.org/10.1038/nature09995>
- 9 Nunez, P. L., & Srinivasan, R. (2006). Recording strategies, reference issues, and dipole localization.  
10 *Nunez PL, Srinivasan R: Electric Fields of the Brain: The Neurophysics of EEG, Ed, 2, 275–312.*
- 11 Ofen, N., Chai, X. J., Schuil, K. D., Whitfield-Gabrieli, S., & Gabrieli, J. D. (2012). The development  
12 of brain systems associated with successful memory retrieval of scenes. *Journal of Neuroscience*,  
13 *32*(29), 10012–10020.
- 14 Ofen, N., Kao, Y.-C., Sokol-Hessner, P., Kim, H., Whitfield-Gabrieli, S., & Gabrieli, J. D. (2007).  
15 Development of the declarative memory system in the human brain. *Nature Neuroscience*,  
16 *10*(9), 1198–1205.
- 17 Ofen, N., Tang, L., Yu, Q., & Johnson, E. L. (2019). Memory and the developing brain: From  
18 description to explanation with innovation in methods. *Developmental Cognitive Neuroscience*, *36*,  
19 100613. <https://doi.org/10.1016/j.dcn.2018.12.011>
- 20 Oostenveld, R., Fries, P., Maris, E., & Schoffelen, J.-M. (2011). FieldTrip: Open source software for  
21 advanced analysis of MEG, EEG, and invasive electrophysiological data. *Computational*  
22 *Intelligence and Neuroscience*, *2011*, 1–9.
- 23 Ouyang, G., Hildebrandt, A., Schmitz, F., & Herrmann, C. S. (2020). Decomposing alpha and 1/f  
24 brain activities reveals their differential associations with cognitive processing speed.  
25 *NeuroImage*, *205*, 116304.
- 26 Overbye, K., Huster, R. J., Walhovd, K. B., Fjell, A. M., & Tamnes, C. K. (2018). Development of  
27 the P300 from childhood to adulthood: A multimodal EEG and MRI study. *Brain Structure*  
28 *and Function*, *223*, 4337–4349.
- 29 Palva, J. M., Wang, S. H., Palva, S., Zhigalov, A., Monto, S., Brookes, M. J., Schoffelen, J.-M., &  
30 Jerbi, K. (2018). Ghost interactions in MEG/EEG source space: A note of caution on inter-  
31 areal coupling measures. *NeuroImage*, *173*, 632–643.  
32 <https://doi.org/10.1016/j.neuroimage.2018.02.032>
- 33 Pani, S. M., Saba, L., & Fraschini, M. (2022). Clinical applications of EEG power spectra aperiodic  
34 component analysis: A mini-review. *Clinical Neurophysiology*, *143*, 1–13.  
35 <https://doi.org/10.1016/j.clinph.2022.08.010>
- 36 Parvizi, J., & Kastner, S. (2018). Promises and limitations of human intracranial  
37 electroencephalography. *Nature Neuroscience*, *21*(4), 474–483.
- 38 Peterson, E. J., Rosen, B. Q., Belger, A., Voytek, B., & Campbell, A. M. (2023). Aperiodic Neural  
39 Activity is a Better Predictor of Schizophrenia than Neural Oscillations. *Clinical EEG and*  
40 *Neuroscience*, *54*(4), 434–445. <https://doi.org/10.1177/15500594231165589>

- 1 Pi, Y., Yan, J., Pscherer, C., Gao, S., Mückschel, M., Colzato, L., Hommel, B., & Beste, C. (2024).
- 2 Interindividual aperiodic resting-state EEG activity predicts cognitive-control styles.
- 3 *Psychophysiology*, 61(8), e14576. <https://doi.org/10.1111/psyp.14576>
- 4 Ray, S., Crone, N. E., Niebur, E., Franaszczuk, P. J., & Hsiao, S. S. (2008). Neural correlates of high-
- 5 gamma oscillations (60–200 Hz) in macaque local field potentials and their potential
- 6 implications in electrocorticography. *Journal of Neuroscience*, 28(45), 11526–11536.
- 7 Rich, E. L., & Wallis, J. D. (2017). Spatiotemporal dynamics of information encoding revealed in
- 8 orbitofrontal high-gamma. *Nature Communications*, 8(1), 1139.
- 9 Ridderinkhof, K. R., Ullsperger, M., Crone, E. A., & Nieuwenhuis, S. (2004). The Role of the Medial
- 10 Frontal Cortex in Cognitive Control. *Science*, 306(5695), 443–447.
- 11 <https://doi.org/10.1126/science.1100301>
- 12 Robertson, M. M., Furlong, S., Voytek, B., Donoghue, T., Boettiger, C. A., & Sheridan, M. A.
- 13 (2019). EEG power spectral slope differs by ADHD status and stimulant medication
- 14 exposure in early childhood. *Journal of Neurophysiology*, 122(6), 2427–2437.
- 15 Rosen, M. L., Sheridan, M. A., Sambrook, K. A., Peverill, M. R., Meltzoff, A. N., & McLaughlin, K.
- 16 A. (2018). The Role of Visual Association Cortex in Associative Memory Formation across
- 17 Development. *Journal of Cognitive Neuroscience*, 30(3), 365–380.
- 18 [https://doi.org/10.1162/jocn\\_a\\_01202](https://doi.org/10.1162/jocn_a_01202)
- 19 Rossini, L., Garbelli, R., Gnatkovsky, V., Didato, G., Villani, F., Spreafico, R., Deleo, F., Lo Russo,
- 20 G., Tringali, G., & Gozzo, F. (2017). Seizure activity per se does not induce tissue damage
- 21 markers in human neocortical focal epilepsy. *Annals of Neurology*, 82(3), 331–341.
- 22 Salvatore, S. V., Lambert, P. M., Benz, A., Rensing, N. R., Wong, M., Zorumski, C. F., & Mennerick,
- 23 S. J. (2024). Periodic and aperiodic changes to cortical EEG in response to pharmacological
- 24 manipulation. *Journal of Neurophysiology*. <https://doi.org/10.1152/jn.00445.2023>
- 25 Schaworonkow, N., & Voytek, B. (2021). Longitudinal changes in aperiodic and periodic activity in
- 26 electrophysiological recordings in the first seven months of life. *Developmental Cognitive*
- 27 *Neuroscience*, 47, 100895. <https://doi.org/10.1016/j.dcn.2020.100895>
- 28 Schölvinck, M. L., Leopold, D. A., Brookes, M. J., & Khader, P. H. (2013). The contribution of
- 29 electrophysiology to functional connectivity mapping. *Neuroimage*, 80, 297–306.
- 30 Sheehan, T. C., Sreekumar, V., Inati, S. K., & Zaghoul, K. A. (2018). Signal Complexity of Human
- 31 Intracranial EEG Tracks Successful Associative-Memory Formation across Individuals. *The*
- 32 *Journal of Neuroscience*, 38(7), 1744. <https://doi.org/10.1523/JNEUROSCI.2389-17.2017>
- 33 Shuffrey, L. C., Pini, N., Potter, M., Springer, P., Lucchini, M., Rayport, Y., Sania, A., Firestein, M.,
- 34 Brink, L., Isler, J. R., Odendaal, H., & Fifer, W. P. (2022). Aperiodic electrophysiological
- 35 activity in preterm infants is linked to subsequent autism risk. *Developmental Psychobiology*,
- 36 64(4), e22271. <https://doi.org/10.1002/dev.22271>
- 37 Spreng, R. N., & Turner, G. R. (2019). The Shifting Architecture of Cognition and Brain Function in
- 38 Older Adulthood. *Perspectives on Psychological Science*, 14(4), 523–542.
- 39 <https://doi.org/10.1177/1745691619827511>
- 40 Stolk, A., Griffin, S., van der Meij, R., Dewar, C., Saez, I., Lin, J. J., Piantoni, G., Schoffelen, J.-M.,
- 41 Knight, R. T., & Oostenveld, R. (2018). Integrated analysis of anatomical and

- 1           electrophysiological human intracranial data. *Nature Protocols*, 13(7), 1699–1723.  
2           <https://doi.org/10.1038/s41596-018-0009-6>
- 3   Sui, J., Huster, R., Yu, Q., Segall, J., & Calhoun, V. (2014). *Function-structure associations of the brain:*  
4       *Evidence from multimodal connectivity and covariance studies. Neuroimage 102P1*, 11–23.
- 5   Sukenik, N., Vinogradov, O., Weinreb, E., Segal, M., Levina, A., & Moses, E. (2021). Neuronal  
6       circuits overcome imbalance in excitation and inhibition by adjusting connection numbers.  
7       *Proceedings of the National Academy of Sciences*, 118(12), e2018459118.
- 8   Sydnor, V. J., Larsen, B., Bassett, D. S., Alexander-Bloch, A., Fair, D. A., Liston, C., Mackey, A. P.,  
9       Milham, M. P., Pines, A., Roalf, D. R., Seidlitz, J., Xu, T., Raznahan, A., & Satterthwaite, T.  
10      D. (2021). Neurodevelopment of the association cortices: Patterns, mechanisms, and  
11      implications for psychopathology. *Neuron*, 109(18), 2820–2846.  
12      <https://doi.org/10.1016/j.neuron.2021.06.016>
- 13   Tang, L., Shafer, A. T., & Ofen, N. (2018). Prefrontal Cortex Contributions to the Development of  
14      Memory Formation. *Cerebral Cortex*, 28(9), 3295–3308.  
15      <https://doi.org/10.1093/cercor/bhx200>
- 16   Thuwal, K., Banerjee, A., & Roy, D. (2021). Aperiodic and periodic components of ongoing  
17      oscillatory brain dynamics link distinct functional aspects of cognition across adult lifespan.  
18      *Eneuro*, 8(5).
- 19   Tran, T. T., Rolle, C. E., Gazzaley, A., & Voytek, B. (2020). Linked sources of neural noise  
20      contribute to age-related cognitive decline. *Journal of Cognitive Neuroscience*, 32(9), 1813–1822.
- 21   Tröndle, M., Popov, T., Dziemian, S., & Langer, N. (2022). Decomposing the role of alpha  
22      oscillations during brain maturation. *eLife*, 11, e77571. <https://doi.org/10.7554/eLife.77571>
- 23   Tukey, J. W. (1977). *Exploratory data analysis* (Vol. 2). Reading, MA.
- 24   Turrigiano, G. G., & Nelson, S. B. (2004). Homeostatic plasticity in the developing nervous system.  
25      *Nature Reviews Neuroscience*, 5(2), 97–107. <https://doi.org/10.1038/nrn1327>
- 26   Vallat, R., & Walker, M. P. (2021). An open-source, high-performance tool for automated sleep  
27      staging. *Elife*, 10, e70092.
- 28   van Nifterick, A. M., Mulder, D., Duineveld, D. J., Diachenko, M., Scheltens, P., Stam, C. J., van  
29      Kesteren, R. E., Linkenkaer-Hansen, K., Hillebrand, A., & Gouw, A. A. (2023). Resting-state  
30      oscillations reveal disturbed excitation–inhibition ratio in Alzheimer’s disease patients.  
31      *Scientific Reports*, 13(1), 7419. <https://doi.org/10.1038/s41598-023-33973-8>
- 32   Voytek, B., Kramer, M. A., Case, J., Lepage, K. Q., Tempesta, Z. R., Knight, R. T., & Gazzaley, A.  
33      (2015). Age-related changes in 1/f neural electrophysiological noise. *Journal of Neuroscience*,  
34      35(38), 13257–13265.
- 35   Waschke, L., Wöstmann, M., & Obleser, J. (2017). States and traits of neural irregularity in the age-  
36      varying human brain. *Scientific Reports*, 7(1), 17381.
- 37   Watson, B. O., Ding, M., & Buzsáki, G. (2018). Temporal coupling of field potentials and action  
38      potentials in the neocortex. *European Journal of Neuroscience*, 48(7), 2482–2497.
- 39   Wen, H., & Liu, Z. (2016). Separating fractal and oscillatory components in the power spectrum of  
40      neurophysiological signal. *Brain Topography*, 29, 13–26.

- 1 Whitford, T. J., Rennie, C. J., Grieve, S. M., Clark, C. R., Gordon, E., & Williams, L. M. (2007).  
2 Brain maturation in adolescence: Concurrent changes in neuroanatomy and  
3 neurophysiology. *Human Brain Mapping*, 28(3), 228–237.  
4 <https://doi.org/10.1002/hbm.20273>
- 5 Wickham, H., Averick, M., Bryan, J., Chang, W., McGowan, L. D., François, R., Grolemund, G.,  
6 Hayes, A., Henry, L., & Hester, J. (2019). Welcome to the Tidyverse. *Journal of Open Source*  
7 *Software*, 4(43), 1686.
- 8 Wickham, H., & Wickham, H. (2016). Data analysis. *Ggplot2: Elegant Graphics for Data Analysis*, 189–  
9 201.
- 10 Wiest, C., Torrecillos, F., Pogosyan, A., Bange, M., Muthuraman, M., Groppa, S., Hulse, N.,  
11 Hasegawa, H., Ashkan, K., Baig, F., Morgante, F., Pereira, E. A., Mallet, N., Magill, P. J.,  
12 Brown, P., Sharott, A., & Tan, H. (2023). The aperiodic exponent of subthalamic field  
13 potentials reflects excitation/inhibition balance in Parkinsonism. *eLife*, 12, e82467.  
14 <https://doi.org/10.7554/eLife.82467>
- 15 Wilke, M., Krägeloh-Mann, I., & Holland, S. K. (2007). Global and local development of gray and  
16 white matter volume in normal children and adolescents. *Experimental Brain Research*, 178,  
17 296–307.
- 18 Yin, Q., Johnson, E. L., & Ofen, N. (2023). Neurophysiological mechanisms of cognition in the  
19 developing brain: Insights from intracranial EEG studies. *Developmental Cognitive Neuroscience*,  
20 64, 101312. <https://doi.org/10.1016/j.dcn.2023.101312>
- 21 Yin, Q., Johnson, E. L., Tang, L., Auguste, K. I., Knight, R. T., Asano, E., & Ofen, N. (2020).  
22 Direct brain recordings reveal occipital cortex involvement in memory development.  
23 *Neuropsychologia*, 148, 107625. <https://doi.org/10.1016/j.neuropsychologia.2020.107625>