



### Neural Mechanisms Involved in Mental Imagery of Slip-Perturbation While Walking: A Preliminary fMRI Study

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**Background:** Behavioral evidence for cortical involvement in reactive balance control in response to environmental perturbation is established, however, the neural correlates are not known. This study aimed to examine the neural mechanisms involved in reactive balance control for recovery from slip-like perturbations using mental imagery and to evaluate the difference in activation patterns between imagined and observed slipping.

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Bhatt T, Patel P, Dusane S, DelDonno SR and Langenecker SA (2018) Neural Mechanisms Involved in Mental Imagery of Slip-Perturbation While Walking: A Preliminary fMRI Study. Front. Behav. Neurosci. 12:203. doi: 10.3389/fnbeh.2018.00203 **Methods:** Ten healthy young participants after an exposure to regular walking and slipperturbation trial on a treadmill, performed mental imagery and observation tasks in the MR scanner. Participants received verbal instructions to imagine walking (IW), observe walking (OW), imagine slipping (IS) and observe slipping (OS) while walking.

**Results:** Analysis using general linear model showed increased activation during IS versus IW condition in precentral gyrus, middle frontal gyrus, superior, middle and transverse temporal gyrus, parahippocampal gyrus, cingulate gyrus, insula, pulvinar nucleus of the thalamus, pons, anterior and posterior cerebellar lobes. During IS versus OS condition, there was additional activation in parahippocampus, cingulate gyrus, inferior parietal lobule, superior temporal, middle and inferior frontal gyrus.

**Conclusion:** The findings of the current study support involvement of higher cortical and subcortical structures in reactive balance control. Greater activation during slipping could be attributed to the complexity of the sensorimotor task and increased demands to maintain postural stability during slipping as compared with regular walking. Furthermore, our findings suggest that mental imagery of slipping recruited greater neural substrates rather than observation of slipping, possibly due to increased sensory, cognitive and perceptual processing demands.

**New and Noteworthy:** The behavioral factors contributing to falls from external perturbations while walking are better understood than neural mechanisms underlying the behavioral response. This study examines the neural activation pattern associated with reactive balance control during slip-like perturbations while walking through an fMRI

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paradigm. This study identified specific neural mechanisms involved in complex postural movements during sudden perturbations, to particularly determine the role of cortical structures in reactive balance control. It further highlights the specific differences in neural structures involved in regular unperturbed versus perturbed walking.

Keywords: reactive balance control, locomotion, falls, imaging, neural activation

### INTRODUCTION

About 60 percent of outdoor falls sustained by community-living older adults are due to environmental perturbations in the form of a slip or a trip (Luukinen et al., 2000). Behavioral studies exposing older adults to perturbations during walking have established several biomechanical factors such as deficient limb support, inefficient compensatory stepping, reduced stability and lower hip height as predictors of falls (Pavol et al., 2004; Pavol and Pai, 2007; Yang et al., 2009, 2011). While biomechanical causes of falls are better understood, the exact neural mechanisms and substrates involved in recovering balance from sudden falls, in other words for reactive balance control, are still not known. Considering that falls are a significant health concern in the aging and neurological population, understanding the specific neural mechanisms involved in falls occurring from sudden balance loss could assist in developing targeted interventions (Luukinen et al., 2000).

Humans rely on two main strategies for balance control and fall prevention: proactive (occurring before balance disturbance) and reactive (occurring after balance disturbance) control strategies. Proactive strategies are employed to enhance stability to prevent and compensate for a loss of balance even before it occurs (Tang et al., 1998; Ferber et al., 2002; Horak, 2006; Shumway-Cook and Woollacott, 2007). For proactive adjustments, the nervous system has adequate time to predict the upcoming balance requirements and make necessary adjustments to minimize the intensity of balance loss or prevent it altogether (Massion, 1994; Aruin and Latash, 1995). A good example is early detection and avoidance of an upcoming obstacle in the walking path (Woollacott and Tang, 1997). Proactive adjustments during locomotion and functional tasks seem to involve cortical and sub-cortical structures of the CNS for planning and execution of an appropriate motor response in anticipation of a perceived threat to balance (Armstrong and Drew, 1985; Drew, 1988; Beloozerova and Sirota, 1993; Petersen et al., 2012). Indeed, a few electrophysiological studies in humans and cats have confirmed the involvement of motor cortex in regulating accurate muscle activity and modulating step cycle when a change in the environment or obstacle in the path is perceived, (Armstrong and Drew, 1985; Drew, 1988; Beloozerova and Sirota, 1993; Petersen et al., 2012).

Unlike proactive adjustments, reactive balance strategies are the key defense mechanisms to prevent a fall after a sudden unexpected perturbation. It involves compensatory postural adjustments initiated by feedback processes (Maki and McIlroy, 1997). Overall, it is proposed that the CNS uses an internal representation of body's mechanics to predict and identify loss of balance. Often, large postural responses displacing center of mass (COM) outside of the base of support (BOS) require changein-support i.e., stepping to prevent a fall (Maki and McIlroy, 1997; Pai and Bhatt, 2007). Several electrophysiological studies in animals and humans support that polysynaptic spinal cord reflexes (short- and long-latency) are responsible for generating the postural response to correct or restore balance during minor disturbances that do not truly pose a threat to the person (Forssberg et al., 1975; Berger et al., 1984; Dietz et al., 1986; Diener et al., 1988; Allum and Honegger, 1992; Zehr et al., 1997). Reactive responses to restore balance from a large disturbance on the other hand, are usually controlled by supra-spinal structures in the brainstem and its descending pathways (longloop reflexes)(Forssberg et al., 1975; Nashner, 1976, 1980; Eng et al., 1994), with some earlier evidence suggesting modulation from cortical structures (Forssberg et al., 1975). Specifically, cerebral cortex perhaps modifies postural response through cerebellar-cortical loop which helps in using prior experience and basal ganglia-cortical connections which incorporates sensory information based on the current context (Graydon et al., 2005; Jacobs and Horak, 2007).

Several studies have attempted to examine neural mechanisms of compensatory postural responses during stance perturbations using techniques such as electroencephalography (EEG) and functional near infrared spectroscopy (fNIRS) (Quant et al., 2004; Adkin et al., 2006; Mochizuki et al., 2009). However, neural substrates involved in maintaining/recovering balance during locomotor tasks have not been sufficiently examined. This could be partly related to the technical challenges that present with using functional neuroimaging such as fNIRS and EEG measures with walking in the form of either low spatial resolution or noise and artifact (Sipp et al., 2013). Although direct evidence via functional magnetic resonance imaging (fMRI) is difficult to obtain, mental imagery has been widely used to examine locomotor-balance tasks that cannot be performed in the MRI scanner such as walking (Jahn et al., 2004, 2008; van der Meulen et al., 2014) or obstacle crossing (Wang et al., 2009). Use of mental imagery is based on the premise that overlapping neural networks are engaged in both mental imagery and overt movements (Decety and Jeannerod, 1995; Porro et al., 1996). Similarly, action observation has also been used to elicit simulation of motor tasks during neuroimaging - especially gross whole body tasks that cannot be performed in the scanner (Dalla Volta et al., 2015). Action observation is believed to stimulate the neural presentation of the movement being observed through the mirror neuron system (Buccino, 2014). While there are a few studies directly comparing the cortical activation between action observation and actual movement performance, there is only one

study directly comparing differences in neural activation during observed versus imagined walking (Iseki et al., 2008).

Mental imagery and action observation are increasingly used as rehabilitation tools for inducing motor learning (Morganti et al., 2003; Franceschini et al., 2010; Zhu et al., 2015; Caligiore et al., 2017). Only recently these techniques have been implemented for physical rehabilitation in clinical populations (Ietswaart et al., 2011; Hong et al., 2012; Garcia Carrasco and Aboitiz Cantalapiedra, 2016; Patel et al., 2017); however, they have been widely used to improve performance in sports (Mulder, 2007). It is believed that motor imagery and action observation can prime the CNS to enhance motor learning (fewer repetitions or lesser time) when performed before the actual motor task (Edwards et al., 2003; Hardwick and Edwards, 2011; Saimpont et al., 2013). Such learning mechanisms might be beneficial for frail or neurological populations for whom tolerability of training dosage or safety might be a concern. In the context of reactive balance control, a previous study has examined if observational learning could substitute for motor learning induced via slip perturbation-training for lowering fall-risk (Bhatt and Pai, 2008). The study did demonstrate evidence of improved postural stability with observational training although not to the same extent as that induced by actual motor training. It remains to be determined if mental imagery could have produced a similar or better effect than observational learning, especially due to animation of sensory systems when performing mental imagery with eyes closed (Marx et al., 2003).

Due to lack of literature comparing motor imagery and action observation directly, there is limited understanding of the neural structures underlying these paradigms. In the present pilot study, a novel paradigm using imagined slipping during walking was used to identify neural correlates of modulating locomotor-balance control during environmental perturbations. Our primary objective was to identify the neural networks involved in reactive balance control in response to large sliplike perturbations during walking as compared with regular walking through metal imagery. Considering that slipping while walking demands greater postural control to regain balance, we postulate that during imagined slipping while walking there will be higher activation in the frontal, parietal regions and cerebellum as compared with imagined walking. We also aimed to examine whether or not imagination of slipping while walking results in activation of different brain areas as compared to observation of the same movement. This understanding of neural correlates involved in falls may provide insights for designing observational learning or mental imagery paradigms for fall prevention, especially for populations that might not be able to directly withstand the actual task-specific perturbation training.

### MATERIALS AND METHODS

#### **Subjects**

Ten young healthy adults (26.90  $\pm$  4.25 years) participated in the study after providing an informed consent approved by the Institutional Review Board. The subjects were screened for any systemic disorders and *fMRI* safety, and had normal vision and

hearing. All the subjects then performed the experimental tasks outside and then in the MRI scanner as described below.

### Walking and Slipping on Treadmill

All subjects were initially exposed to walking on the treadmill at a self-selected pace and then were exposed to a single slip-like perturbation with an acceleration of 12.00 m/s<sup>2</sup>, displacement 0.25 m and duration of 0.25 s. For these tasks, subject stood on the ActiveStep treadmill (Simbex, NH) with a comfortable stance. A harness suspended from the overhead arch was donned to prevent individuals from falling (Figure 1A). The treadmill belt speed was increased slowly until the individual perceived the speed to be similar to his/her regular walking speed. At this speed, the individual walked for a minute. Following regular walking, the individual performed another walking trial. During this trial individuals were warned that they may experience a sliplike perturbation after a few steps of walking, however, they were unaware of the exact instance of slip occurrence. Upon a sliplike perturbation, individuals were asked to execute their natural response to recover balance and prevent themselves from falling. The subjects were exposed to the treadmill slip before the fMRI experiment to provide them with an experience of how a reallife slip would feel like, especially for those people who might not have experienced a slip in recent times. Such experience could also aid in reducing within-subject variance of the observation or imagination tasks, and hence, enhance ability of the subjects to better relate to the conditions.

### **Observed and Imagined fMRI Conditions**

After the initial walking and slip exposure, and prior to the MRI scans, subjects underwent a practice session involving motor imagery and observation tasks. The motor imagery task comprised of (a) imagining themselves walking on the treadmill (IW) and (b) imagining themselves slipping on the treadmill while walking, similar to that experienced during initial exposure (IS). Similarly, the observation tasks consisted of (a) observing a video of another person walking on the treadmill (OW) and (b) observing a video of another person slipping while walking on the treadmill (OS) (Figure 1A). During the experiments, the subjects lied down supine in the scanner and the stimuli were projected on the screen in front of them through a mirror with an angle of 9° from the vertical. For the imagined conditions, subjects received clear instructions to close their eyes and that they should imagine themselves slipping where the leg suddenly slides/moves forward with respect to their body, similar to what they experienced on the treadmill. Such experimental design was purposefully chosen based on the practical realities of the research question, for example if eyes are open for imagined condition this would not be representative of a real life task (challenge to ecological validity). Furthermore, eyes closed during imagination has shown increased cortical activation of various sensory systems as the subjects recall their sensory experience from the perception of the actual activity (Marx et al., 2003). For the observed condition, subjects were instructed to observe the video of a person either walking on the treadmill or slipping while walking on the treadmill, a situation similar to what they had experienced in the laboratory. To ensure subjects engaged themselves during



observation from the first person perspective, they were shown videos of back view of walking and slipping, compared with a side view. This was based on the results from a pilot study conducted on a separate set of ten young subjects, which concluded that 90% of subjects found the back view to be most engaging to view themselves slipping as compared with the side view. The mental imagery of tasks was assessed using the Vividness of Visual Imagery Questionnaire. Following familiarization to the observed and motor imagery tasks, subjects performed these tasks in the MRI scanner. All subjects reported no difficulty in performing mental imagery as indicated by their median score of 4.5/5 on the vividness of visual imagery questionnaire.

### **Experimental Protocol**

During the MRI scan, subjects were provided with a headset to listen to the instructions and were asked to lie still. Subjects received instructions for the imagined tasks through the headset and a screen in front of them in the scanner projecting the videos during the observed conditions. Four trials for each of the imagined and observed conditions (IW, IS, OW, and OS) were performed in the scanner. The duration of each trial was 30 s. The experimental tasks were interspersed with four trials of "Rest" condition. During the Rest condition, the screen projected the letter "X" on a black background and subjects were instructed to focus on the letter on the screen, trying not to think about anything else. The Rest condition was included to record the resting brain activity in the absence of observed or imagined tasks. The observed, imagined and rest trials were presented in a randomized order (Figure 1B). All subjects performed the trials in the same randomized order. Two blocks of two trials each were presented for each condition.

### **Data Acquisition**

Whole brain imaging was performed with a 3.0 T GE Discovery scanner (Milwaukee, WI, United States) using a standard radio frequency coil and T2\*-weighted pulse sequence. BOLD functional images were collected using a gradient-echo axial echo planar imaging sequence (Glover and Thomason, 2004) at UIC. The following parameters were used: repetition time = 2,000 m, echo time = 22.2 ms, flip angle = 90 degree, field of view = 22 cm, 64 by 64 matrix, slice thickness = 3 mm, 44 slices. An axial T1 SPGR structural image was obtained for each using 182 axial images 1 mm in thickness for spatial normalization [minimum TR/TE (9.292 ms/3.77 ms) TI = 450 ms]. During scanning, subjects completed the observed and imagined tasks. Prior to scanning, the importance of remaining motionless was conveyed to each subject. There were two runs of the experimental tasks, each lasting 5 min and 20 s, and acquiring 120 volumes. Each condition was averaged across both runs, prior to the creation of subtraction contrast analyses. The same scanner and acquisition sequence was used for all subjects and there was no relationship between the year the fMRI was performed and extracted activation of the BOLD signal.

### **Data Processing**

Preprocessing of fMRI data was conducted using SPM8<sup>1</sup>, FSL, and AFNI<sup>2</sup>. Data were despiked using AFNI. All data was then slice-time corrected in SPM8 and realigned in FSL<sup>3</sup> using MCFLIRT (Jenkinson et al., 2002). Anatomical and functional images were coregistered and normalized to Montreal

<sup>&</sup>lt;sup>1</sup>http://www.fil.ion.ucl.ac.uk/spm/

<sup>&</sup>lt;sup>2</sup>http://afni.nimh.nih.gov/afni/

<sup>&</sup>lt;sup>3</sup>http://fsl.fmrib.ox.ac.uk/fsl/fslwiki/

Neurological Institute (MNI) space using SPM8. Smoothing was completed with a full width at half maximum filter of 5 mm. First level models were built in SPM8 using x, y, and z translation realignment movement regressors from FSL for each run. The subtraction method was used to create contrast images and second level models were built in SPM8.

### **Statistical Analysis**

A gray matter mask was applied and whole brain correction was achieved for the multiple regression model at p = 0.01by conducting 1000 Monte Carlo simulations in 3dClustSim to determine a joint threshold of height and extent (p < 0.005, extent of 440 mm<sup>3</sup> or K = 55 voxels). The Monte Carlo approach was intended to balance Type I and Type II error and cluster extent was determined using the bug-fixed 3dClustSim tool (Cox et al., 2017). Further, the fMRI data was evaluated with planned t-test contrasts between selected conditions. Given the above rationales, the *p*-value was not further adjusted for multiple comparisons. We first built contrasts for each active condition by subtracting rest activation from the condition, for example: IW-minus-rest. Then, we compared activation between different conditions using contrasts created relative to the rest condition. For example, we subtracted IW-minus-rest activation from ISminus-rest activation. In total, the following planned contrasts were used: IW-rest, IS-Rest, IS-IW, IW-OW, IS-OS.

### RESULTS

### Mental Imagery of Walking and Slipping Versus Rest

As compared with rest condition (baseline), the cerebral activity was greater in both mental imagery conditions (walking and slipping) (**Tables 1, 2**). Mental imagery of walking showed increased activity in the frontal lobe within the left supplementary motor area (BA 32). The imagined slipping condition resulted in a significantly greater activity in both cortical and subcortical regions as compared with the rest condition. The cortical areas included left supplementary motor areas (BA6), left superior frontal gyrus, right pars opercularis (BA45), left inferior parietal lobule (BA 40), right parahippocampal gyrus, left cingulate gyrus and right frontal inferior operculum (BA45). Among the sub-cortical structures, bilateral posterior cerebellum showed increased activation during imagined slipping.

## Mental Imagery of Slipping Versus Walking

Imagined slipping resulted in greater activation compared with imagined walking (**Table 3** and **Figure 2**). As compared with imagined walking, imagined slipping showed significantly more activation in left precentral and right middle frontal gyri, bilateral inferior parietal lobule (BA 40), precuneus, bilateral insula, right superior temporal gyrus (BA 22 and 38), right middle and left transverse temporal gyri, right parahippocampal gyrus, bilateral cingulate gyrus, right pulvinar nucleus in thalamus, right cerebellum, and pons in the brainstem.

# Mental Imagery Versus Observation of Walking

The contrast comparing mental imagery of walking to observation of walking did not reveal any active voxels at the specified threshold. Thus, there was no difference in the areas of activation between mental imagery and observation of walking.

## Mental Imagery Versus Observation of Slipping

As compared with observed slipping, the mental imagery of slipping showed additional activation in left supplementary motor area (BA 6), bilateral middle frontal gyrus (BA 10), left superior temporal gyri, bilateral parahippocampal gyrus, left cingulate gyrus. (**Table 4** and **Figure 3**). Also, as opposed to observation of slipping, mental imagery of slipping yielded greater activation in the left inferior parietal lobule. Both mental imagery and observation of slipping showed similar activation in the inferior frontal gyrus and limbic regions.

### DISCUSSION

The purpose of this pilot study was to examine the neural correlates associated with slipping while walking. As hypothesized, activation of additional brain areas was seen during imagined slipping as compared with imagined walking. Our other major findings include increased activation during imagined slipping as compared with observed slipping and no additional activation in imagined walking as compared to observed walking.

## Mental Imagery of Slipping Versus Walking

The middle frontal gyrus was the common area activated between the imagined walk minus rest and imagined slip minus rest contrasts. However, imagined slip condition showed additional activation in areas such as supplementary motor area (SMA), dorsolateral prefrontal cortex, inferior parietal lobule, cerebellum, precuneus, cingulate gyrus, parahippocampal gyri and pulvinar nucleus of the thalamus over imagined walking. The brain activation pattern noted for imagined slipping was remarkably similar to previous studies which found activation in SMA, frontal cortex and cerebellum during imagery of dynamic balancing tasks (Ferraye et al., 2014; Taube et al., 2015).

The increased activation in the SMA during imagined slip condition over the imagined walk condition could be assumed as a response to perturbation causing activation of the SMA-cerebellar loop via the pontine nucleus and back to the motor cortex or association area in order to modify the ongoing movement. SMA, is mainly related to movement execution, motor planning and coordination along with dorsolateral prefrontal cortex, which help in response selection using prior associations (Eccles, 1982; Chouinard and Paus, 2006). These areas generate an appropriate motor response, including corrective motor responses, to prevent loss

#### TABLE 1 | Differences in activation between imagined slipping and rest conditions.

Contrast		Anatomical Regions	mm <sup>3</sup>	Voxels	MNI coordinates					
	Lobe	Gyrus	BA	Side			x	у	z	Z-value
IS>Rest	Frontal	Precentral Frontal inferior operculum	-	L	6,112	764	-48	8	14	3.87
		Superior frontal	6	L	1,040	130	-32	12	54	3.80
	Parietal	Frontal inferior operculum	45	R	2,608	326	56	10	22	3.92
		Inferior parietal lobule	40	L	920	115	-46	-46	46	3.48
	Limbic	Parahippocampal	-	R	640	80	14	-10	-18	3.34
		Cingulate gyrus	24	L	10,352	1294	_4	-8	50	4.07
	Cerebellum –	Declive Cerebellum and	N/A	L	904	113	-38	-60	-30	3.54
	posterior lobe	crus cerebri		R	1,016	127	28	-74	-28	3.77

IS, Imagined slipping; BA, Broadmann area.

**TABLE 2** | Differences in activation between imagined walking and rest conditions.

		10115		mm <sup>s</sup>	Voxels	MNI coordinates			
Lobe	Gyrus	BA	Side			x	У	z	Z-value
Frontal	Middle frontal	32	L	808	101	-6	6	50	3.49
	Lobe Frontal	Lobe         Gyrus           Frontal         Middle frontal	Lobe     Gyrus     BA       Frontal     Middle frontal     32	LobeGyrusBASideFrontalMiddle frontal32L	Lobe     Gyrus     BA     Side       Frontal     Middle frontal     32     L     808	Lobe     Gyrus     BA     Side       Frontal     Middle frontal     32     L     808     101	Lobe         Gyrus         BA         Side         x           Frontal         Middle frontal         32         L         808         101         -6	Lobe         Gyrus         BA         Side         x         y           Frontal         Middle frontal         32         L         808         101         -6         6	Lobe         Gyrus         BA         Side         x         y         z           Frontal         Middle frontal         32         L         808         101         -6         6         50

IW, Imagined walking; BA, Broadmann area.

TABLE 3 | Differences in activation between imagined slipping and imagined walking.

Contrast		Anatomical regions					N			
	Lobe	Gyrus	BA	Side	-		x	У	z	Z-value
IS > IW	Frontal	Precentral	-	L	704	88	-52	-4	6	3.38
		Middle frontal	-	R	968	121	42	-4	48	3.33
	Parietal	Inferior parietal	40	R	1,288	161	56	-34	24	3.32
		lobule	40	L	704	88	-56	-30	24	3.41
		Precuneus	7		480	60	-8	-64	56	3.15
	Temporal	Superior temporal	38	R	440	55	36	6	-22	3.84
			22	R	720	90	46	-18	0	3.22
		Middle temporal	-	R	848	106	54	-42	0	3.79
		Transverse temporal	-	L	1,080	135	-38	-28	12	4.17
	Limbic	Parahippocampal	35	R	1,056	132	18	-30	-10	4.00
		Cingulate	31	R	984	123	8	-30	42	3.19
				L	768	96	-6	-34	42	3.25
	Insula	Insula L Rolandic	-	L	624	78	-40	0	0	3.35
		Oper Undefined		L	1,048	131	-44	4	14	4.16
				R	928	116	34	10	10	3.62
	Thalamus	Pulvinar	-	R	640	80	8	-28	2	4.01
	Brainstem	Pons	-	L	1,256	157	-8	-32	-24	3.85
	Cerebellum Anterior	Undefined Declive	_	R	600	75	18	-42	-30	3.30
	Lobe Posterior Lobe	of vermis	NA	R	984	123	2	-70	-26	3.14

IS, imagined slipping; IW, imagined walking; BA, Broadmann area.

of balance or fall. Our findings are in line with EEG studies performed during standing perturbations, which indicated the presence of N1, negative event-related potential occurring about 100 ms after onset of an unpredictable stance perturbation in the fronto-central cortical sites (Quant et al., 2004; Adkin et al., 2006; Mochizuki et al., 2009). In these studies, small magnitude perturbations were delivered which evoked feet-inplace postural responses. In addition, it was found that the



in thalamus, bilateral cerebellum, and pons in brainstem (p < 0.005).

TABLE 4	Differences in	activation between	imagined	slipping a	and observed	slipping.
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Contrast		Anatomical regions			mm <sup>3</sup>	Voxels	MNI coordinates			
	Lobe	Gyrus	BA	Side			x	У	z	Z-value
IS > OS	Frontal	Middle frontal	_	R	2,768	346	36	32	26	4.28
			10	L	1,368	171	-36	40	24	3.46
		Inferior frontal	-	L	4,280	535	-36	30	2	3.85
	Parietal	Inferior Parietal Iobule Extra Nuclear	40	R	536	67	64	-42	32	4.10
			-	L	624	78	-16	2	14	3.70
	Temporal	Superior temporal		L	9,584	1198	-52	-18	0	4.17
	Limbic	Parahippocampal	-	R	13,160	1645	36	-16	-28	4.46
				L	1,720	215	-16	-36	-12	3.95
				R	1,328	166	20	-20	-16	3.63
		Cingulate (SMA)	-	L	27,216	3402	-4	4	46	5.09

IS: Imagined slipping, OS: Observed slipping, BA: Broadmann area, SMA: Supplementary motor areas.

amplitude of the N1 response changed with the knowledge of an impending perturbation such that the N1 amplitude was greater during an unpredictable perturbation (Adkin et al., 2006). Similarly, Mihara et al. (2012) using fNIRS, examined cortical activation during anterior-posterior and medio-lateral stance perturbations in individuals with stroke. It was found that postural responses were accompanied by increased uptake of oxygenated hemoglobin in bilateral prefrontal, premotor and parietal cortex association areas. Thus, these studies suggest the role of frontal cortex in detection of balance loss and in modulating recovery responses (Dietz et al., 1984).

In order to correct movement error for restoring and maintaining the COM within the BOS, the cerebellum could be activated. Since cerebellum (vermis) acts as a comparator for signals received from the proprioceptors of the moving



body segments via the spinocerebellar tract and timely modulate the response to match the intended movement, it could be involved in planning of the reactive stepping response (Pisotta and Molinari, 2014).

We found activation of areas related to visuo-spatial navigation such as the precuneus region of the parietal lobe and parahippocampal gyri. Activation in these regions could be related to the mental visualization of the slipping environment (Cavanna and Trimble, 2006) and formation of associations between visual and spatial information, thus helping in integration of the walking path (McNaughton et al., 1996). Furthermore, parahippocampal gyri could also be associated to the retrieval of past memory in order to generate the reactive balance responses (Ekstrom and Bookheimer, 2007).

Considering the unique sensory experience provided by slipping, the activation of inferior parietal lobule could be associated with the integration of somatosensory and visual stimuli (Singh-Curry and Husain, 2009). Similarly, activation of thalamus could be attributed to sensory integration, processing and maintaining erect posture while recovering balance from falls (Zwergal et al., 2009; Barra et al., 2010). Activation in insula which helps in perception, motor control and self-awareness was also noted (Sterzer and Kleinschmidt, 2010).

There was significant activation in the cingulate gyrus, which plays a role in monitoring error while performing motor tasks and could be of significance in detecting balance loss during walking (Holroyd et al., 2004; Debener et al., 2005; Anguera et al., 2009; Sipp et al., 2013). Our findings are similar to the results from a recent study, which used high-density EEG along with independent component analysis to identify cortical activity related to loss of balance (Sipp et al., 2013). The authors found that walking on a balance beam mounted on a treadmill was associated with activation of anterior cingulate, posterior cingulate, anterior parietal, sensorimotor and dorsolateral-prefrontal cortices (Sipp et al., 2013).

Despite some similarities in activations observed between imagined slipping and walking conditions, additional cortical and subcortical areas recruitment during imagined slipping suggest the involvement of different neural pathways in reactive balance control while walking than regular walking. This could be functionally or in real-life associated with the novelty of the sensorimotor stimulus and the perceived complexity of maintaining stability during a sudden slip while walking. It is established that longer-term training of a motor skill reduces the amount of cortical activation in motor areas suggesting a more efficient control of movement after sufficient practice (Jancke et al., 2000; Picard et al., 2013; Naito and Hirose, 2014). On similar lines, walking is a self-generated, anticipatory and a relatively learned (over years) task as compared with recovering balance during a sudden slip. Unlike regular walking, an unexpected disturbance during walking results in larger excursion of COM threatening postural stability. Such disturbance while walking might necessitate recruitment of a variable motor command than regular walking to control lower extremities and execute an appropriate postural response. It is thus likely that, slipping demands greater neural resources for sensory (visuospatial, perceptual, tactile, proprioceptive), cognitive and motor processing than regular walking, as that observed in our study.

## Mental Imagery Versus Observation of Walking

Neuroimaging studies have established the existence of a strong overlap in the neural areas activated during the actual task performance and its imagination and observation (Buccino et al., 2001; Grezes and Decety, 2002; Hanakawa et al., 2003). This evidence comes from studies examining brain activation during lower extremity movements (la Fougere et al., 2010; Dalla Volta et al., 2015). For example, Iseki et al. (2008) compared imagined and observed walking, and found that SMA and the dorsal premotor cortex (PMd) were activated in both the conditions (Iseki et al., 2008). Previous studies have shown that these two areas are essential for gait initiation, turning, negotiating obstacles and walking in narrow passages (Della Sala et al., 2002; Malouin et al., 2003; Nadeau, 2007). Another study examining neural activation during whole body gymnastic movements showed that similar motor areas were activated during both motor imagery and action observation (Munzert et al., 2008). Furthermore, Orr et al. (2008) observed that both imagination and observation of ankle movements was associated with common activation in inferior parietal lobule and precentral gyrus. Based on previous evidence, the fact that we did not observe any additional activation in imagined versus observed walking condition could be due to the common areas activated during these conditions.

## Mental Imagery Versus Observation of Slipping

Contrary to that seen for regular walking, for the slipping condition, our results suggest that there was additional activation noted during imagined versus the observed condition. Although motor imagery and observation could be driven by similar neural pathways (Grafton et al., 1996; Grezes and Decety, 2001; Jeannerod, 2001), it can be argued that first person motor imagery involves a more conscious brain engagement in an attempt to simulate the actual motor experience. This may be particularly important during tasks posing significant threat to balance and the CNS relies on activation of necessary visualperceptual and motor systems to select an appropriate response. In our study, imagined slipping showed additional activation in SMA (BA 6) and bilateral middle frontal gyrus, which are involved in movement planning and initiation (Eccles, 1982; Chouinard and Paus, 2006); cingulate gyrus, which monitors motor error and detects balance loss during walking (Holroyd et al., 2004; Debener et al., 2005; Anguera et al., 2009; Sipp et al., 2013) and inferior frontal gyrus, which is involved in

regulating excessive trunk movement to prevent loss of balance via response suppression (Sharp et al., 2010). Furthermore, there was recruitment of sensory and visual processing areas such as superior temporal gyri, bilateral parahippocampal gyrus and cingulate gyrus, (McNaughton et al., 1996; Yang et al., 2015) and areas related to perception and internal awareness such as inferior parietal lobule, resulting in increased activation (Singh-Curry and Husain, 2009). These findings clearly suggest greater engagement of neural structures while imagining a challenging locomotor-balance task like slipping. Our findings are also in agreement with the study by Taube et al. (2015) showing increased activation in SMA and the middle frontal gyrus during imagery over observation of maintaining standing balance on a wobble board which continuously disturbs balance. Thus, current and previous findings highlight that the extent of neural activation during motor imagery might also be influenced by task complexity, uniqueness or prior motor experience with the task.

### CLINICAL APPLICATION AND LIMITATION

Considering that mental imagery showed greater activation of brain areas, it can be used to better examine the neural correlates than action observation for activities which cannot be overtly performed in the scanner. While a mental imagery paradigm is beneficial to evaluate gait related activities, the findings of this study should be interpreted in light of few limitations of this approach. There could be individual differences in the ability of the subjects to imagine even though no difference was noted on the scoring of the Vividness of motor and visual imagery questionnaire, which can alter the areas and the extent of clusters activated, as supported by van der Meulen et al. (2014). Furthermore, the quality of the imagined movement is dependent on the attentiveness during imagination (De Beni et al., 2007; Gregg et al., 2010). The elimination of action of gravity on the otherwise weight bearing activities of walking and slipping may have some effect on the overall activation pattern. Also, the observed differences between activations during mental imagery and rest or observed conditions could be due to the fact that the eyes were closed in the imagined condition and open during rest and observed conditions.

Since our study is a pilot study, the study may be underpowered owing to a smaller sample size. However, this pilot study does provide a proof of feasibility, and estimates of effect sizes, so that larger studies, needed to rule out type I error can be planned. To evaluate potential future clinical application of our results in other population, a larger sample size with variable hand dominance would be recommended. Further, examining those with known gait disturbances can also provide convergent validity for these results. In spite of these limitations, we had the advantage of better spatial resolution as compared with other imaging techniques provided by use of *fMRI* (Chen and Ugurbil, 1999). The results of this study suggest that a network of cortical and subcortical areas somewhat different from regular walking is associated with the act of balancing in response to a novel slip. It further corroborates the view that specific cortical regions play a role in reactive balance control which has been proposed by several behavioral (Rankin et al., 2000; Brauer et al., 2002; Adkin et al., 2006) and animal studies (Beloozerova and Sirota, 1993; Deliagina et al., 2007). This study elucidates the neural structures associated with slipping in a young healthy nervous system. Future studies should investigate the brain activation patterns in elderly and in populations with balance deficits to further inform neural mechanisms of reactive balance control and potential causes of falls in these individuals.

### DISCLOSURE

No commercial party having a direct financial interest in the research findings reported here has conferred or will confer a benefit on the authors or on any organization with which the authors are associated.

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### **ETHICS STATEMENT**

A written informed consent was obtained from all research participants. The study protocol was approved by the Institutional Review at University of Illinois at Chicago.

### **AUTHOR CONTRIBUTIONS**

TB provided the conceptual framework and experimental design, facilities, funding, and assistance with manuscript preparation. SL has contributed toward experimental design, data processing and analysis, consultation and reviewing of manuscript. PP and SD assisted with experimental design, data collection, analysis, and manuscript preparation. SRD has assisted with data processing, analysis, and manuscript review.

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**Conflict of Interest Statement:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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