Comparison of impact of target delineation of computed tomography- and magnetic resonance imaging-guided brachytherapy on dose distribution in cervical cancer

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Abstract

Purpose: The dose distributions obtained from three imaging approaches for target delineation in cervical cancer using high-dose-rate (HDR) brachytherapy were investigated.

Material and methods: Ten cervical cancer patients receiving four fractions of HDR brachytherapy were enrolled. Based on different imaging approaches, three brachytherapy plans were developed for each patient: with the high-risk clinical target volume (HRCTV) delineated on magnetic resonance (MRI) images for every fraction (approach A; MRIonly); on MRI for the first fraction and computed tomography (CT) images for the subsequent fractions (approach B; MRI_{1st}/CT); and on CT images for all fractions (approach C; CT-only). The volume, height, width at point A, width at maximum level, and dosimetric parameters (D_{100} , D_{98} , D_{95} , and D_{90} of the HRCTV; and $D_{0.1cc'}$, $D_{1cc'}$ and D_{2cc} of all organs at risk, or organ at risk - OAR: bladder, rectum, sigmoid colon, and bowel) provided by each approach were compared.

Results: The mean HRCTV volume, width, and height obtained from approach C (CT-only) were overestimated compared to those from approaches A (MRI-only) and B (MRI $_{1st}$ /CT). The doses to the HRCTV for approaches A and B were similar. However, the HRCTV doses for approach C were significantly lower than those for approaches A and B for all parameters (D_{95} - D_{100}). As to the OAR, the three approaches showed no differences.

Conclusions: A combination of MRI and CT is a safe alternative approach for cervical cancer HDR brachytherapy. The technique provides comparable dosimetric outcomes to MRI-based planning, while being more cost-effective.

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Key words: brachytherapy, cervix cancer, CT, MRI, target delineation.

Purpose

High-dose-rate (HDR) brachytherapy (BT) plays an essential role in the treatment of invasive cervical cancer [1,2]. With current technologies, the planning images have advanced from 2-dimensional-based planning to 3-dimensional image-guided brachytherapy (3D IGBT) [3,4,5,6]. The treatment delivery can be guided by either computed tomography (CT) or magnetic resonance imaging (MRI), but MRI has been demonstrated to provide superior soft-tissue contrast compared to CT, better image of extension of primary tumor, and its relationship with organs at risk is evidenced [7,8,9,10,11,12]. GEC-ESTRO after employment of MRI in cervix brachytherapy, with institutional series of hundreds of patients, EMBRACE study, and RetroEMBRACE study, have demonstrated better local controls and survival in these patients, when

BT treatment is defined in a volume not in point A, and with the use of MRI [13,14,15]. However, the availability of MRI-based BT is limited at some radiotherapy centers from time, labor, and resource intensive. Transition to MRI-based BT as more accessible for institutions, with safe and efficient accomplishment was described by Harkenrider et al. [16].

Given these limitations, the application of planning involving a combination of MRI and CT has been proposed (MRI_{1st}/CT). With this approach, the MRI is performed only in the first fraction of the treatment for target and organ at risk (OAR) delineation, applicator reconstruction, and dose optimization [17,18]. The contour information is then used to guide the radiation oncologist in determining the tumor target in the subsequent fraction by using CT images. The present research was therefore conducted to compare the impacts of the target

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delineation accuracies obtained using imaging with CT only, MRI only, and MRI_{1st}/CT on the dose distributions in cervical cancer brachytherapy planning.

Material and methods

Patient selection

The study was approved by the Siriraj Institutional Review Board, Faculty of Medicine, Siriraj Hospital, Mahidol University (project number 760/2560). Between August 2015 and December 2016, 10 cervical cancer patients with stage IB2 to IIIB tumors were enrolled. All patients received 50 Gy external beam radiotherapy to the whole pelvis prior to the brachytherapy. The HDR brachytherapy schedule consisted of 4 treatment fractions with prescribed dose of 7 Gy. Intracavitary radiation therapy, using MRI-compatible tandem/ring applicators with or without interstitial plastic needles (Varian Medical Systems, Palo Alto, CA, USA) was performed for each treatment application.

Image acquisition

Patients with an applicator underwent T2-weighted MR imaging, with a 3 mm slice thickness using a 1.5-Tesla MRI scanner (Philips Archiva, Philips Medical Systems B.V., Eindhoven, The Netherlands) and CT imaging with a 1.25 mm slice thickness (GE Brightspeed, GE Medical Systems, Milwaukee, WI, USA) for brachytherapy planning. All patients followed the bladder filling protocol with 50-100 ml saline before the MRI and CT scans. The images were exported to brachytherapy planning system (BrachyVision version 13.6, Varian Medical Systems, Palo Alto, CA, USA). All target volumes and OAR delineations were performed on both image modalities by a same radiation oncologist.

Treatment planning

The treatment plans were generated for three different imaging schemes (Figure 1), in MRI-only approach in MRI $_{\rm 1st}$ /CT approach, and in CT-only approach. The MRI-only scheme was used as a standard approach. In MRI-only, the high-risk clinical target volume (HRCTV) and all OAR (bladder, rectum, sigmoid colon, and small bowel) on each fraction were contoured on the MRI, as recommended by GEC-ESTRO. In MRI $_{\rm 1st}$ /CT, images from the first fraction (MRI) were registered to the subsequent CT images (second to fourth fractions) using image regis-

tration software in the treatment planning system. Then, the HRCTV on the first fraction's MRI was transferred to the corresponding subsequent CT with adjustment to the CT images. In CT-only, the HRCTV and all OAR were drawn on the CT images. To avoid bias in the contouring for CT-only, the HRCTV was delineated on the CT images by a single radiation oncologist before being contoured on the MRI.

After the HRCTV and all OAR delineations were completed, treatment plans were generated. On the MRI- and CT-based plans, the applicator reconstruction and dose optimization were done via a manual technique, using the TG-43 dose calculation algorithm to compute the desired dose distribution. The dwell times and location of the radioactive source were optimized for prescribed doses 7 Gy to D_{90} of the HRCTV, with the total target dose from external beam RT and BT \geq 84 Gy, in 2 Gy equivalent (EQD2) and similar acceptable doses to the OAR in the same fraction for each planning approach to be \leq 90 EQD2 for D_{2cc} bladder, \leq 70 for D_{2cc} rectum and sigmoid as suggested by GEC-ESTRO Working Group II [19].

Data collection and statistical analyses

The volume, height, width at point A, width at the maximum level as well as the dosimetric parameters (D $_{100}$, D $_{98}$, D $_{95}$, and D $_{90}$ of the HRCTV; and D $_{0.1cc'}$ D $_{1cc'}$ and D $_{2cc}$ of all OAR) were collected from the dose-volume histogram and analyzed. The data were reported as averages (mean and SD). Repeated measure ANOVA was used to compare the differences between each fraction of parameters. Differences with a p value < 0.05 were considered to be statistically significant. All calculations were performed with SPSS Statistics for Windows, version 16.0 (SPSS Inc, Chicago, Ill, USA).

Results

HRCTV volume and dimension

The HRCTV volume from MRI of the 10 patients in this study was in the range of 11.9-30.2 cc (mean = 18.8, SD = 6.95). From Table 1, statistically significant ratios of the HRCTV CT to the MRI were 1.48 for the volume, 1.20 for the width at point A, and 1.21 for the height. Using MRI_{1st}/CT , the ratios of the overestimated volume, width, and height (fraction 2-4) were reduced to 1.11, 1.12, and 1.07, respectively. As to fraction-by-fraction comparisons, no differences were detected between MRI

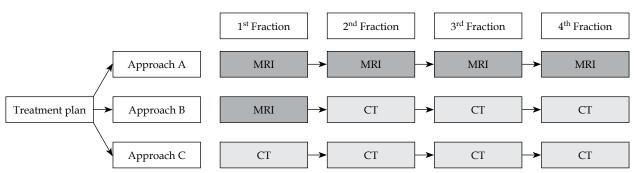


Fig. 1. Schematic workflow of the three imaging approaches

and $\mathrm{MRI}_{1\mathrm{st}}/\mathrm{CT}$ in terms of the total volume, the width at the maximum level, the width at point A, and the height (Table 2). However, the HRCTV volume, including the width at point A and the height obtained from CT, was significantly larger than that from MRI. Also, similar results of volume and height were shown for comparisons of the $\mathrm{MRI}_{1\mathrm{st}}/\mathrm{CT}$ and CT approaches.

Dosimetric parameters

The dosimetric parameters for the HRCTV and all OAR are presented in Tables 3 and 4. There were no differences in the doses to the HRCTV for approaches A and B. In contrast, the doses to the HRCTV for approach C were significantly lower than those for MRI-only for all parameters (D_{95} - D_{100}). Similar results were shown for the comparisons of approaches B and C. As to the OAR doses, there were no differences between the three approaches.

Discussion

It has been confirmed that 3D IGBT using MRI- or CTbased planning offers a better assessment of tumor volume than 2D-based planning. Their accuracy of the target volume and all OAR delineations effectively deliver more tumor-specific high doses, with less adverse effects on the surrounding normal tissues [3,4,20,21,22,23,24,25,26]. However, with CT, it is very difficult to identify the cervix and parametrium, and cause the tumor volume delineation to be overestimated, which results in a reduced dose coverage for the tumor volume and increased doses to OAR [7,8,9,10,26,27]. On the other hand, MRI-based planning provides better accuracy for the HRCTV and all OAR delineations. Superior treatment outcomes with impact in local control and survival from MRI-based planning have been presented by various groups [15,23,24,28,29]. However, the relative lack of availability of this superior modality is a disadvantage. Therefore, the combination of MRI_{1st}/ CT technique was introduced by Beriwal et al. [17]. The study showed that this approach is feasible and has excellent local control. A similar dose coverage to the HRCTV (especially in case of a small tumor volume) to that provided by fully MRI-based planning has also been reported by Nesvacil et al. [18].

Regarding the difference in the target volume using CT and MRI for brachytherapy for cervical cancer, Swanick *et al.* [30] studied the HRCTV volume using two image modalities, and showed that the mean HRCTV volume obtained using CT (44.1 cm³) was larger than that obtained using MRI (35.1 cm³), with statistical significance (p < 0.0001). Due to increased discrepancy in the HRCTV volume obtained with MRI, they concluded that MRI-based brachytherapy planning should be considered for the use in patients with a higher body mass index and a tumor size of 5 cm or greater, with parametrial invasion.

In the present study, the HRCTV volume obtained from fully CT-based planning was overestimated compared to the volumes acquired using full MRI-based and MRI_{1st}/CT approaches. As a consequence, the HRCTV doses obtained from CT-based planning were lower than those provided by the other two approaches in almost every fraction, and the range of dose differences were larger for the higher doses to the target (e.g., for approaches A and C: $\mathrm{D}_{\mathrm{90cc}}$ 0.69-0.83 Gy and D_{100cc} 0.75-1.20 Gy, respectively). These outcomes are very similar to those in Nesvacil study [18], and it can be concluded that the overestimations on the CT images can be overcome by using MRI in the 1st fraction to guide contouring on the subsequent fractions of the CT images. This outcome was also confirmed by the results of better the HRCTV volumes and dimensions, and improved doses for approach B than approach C, even though all were obtained from CT images. A study by Choong et al. [31] analyzed 76 cervical cancer patients who had been divided into 49 cases with CT- and MRI-guided brachytherapy (the same as approach B in the present study) and 27 cases with MRI-guided only brachytherapy (the same as MRI-only in this study). The results showed no statistically significant differences in the clinical outcomes or dosimetric analyses of the two approaches. Wang et al. [32] reviewed 13 clinical studies comprising a total of 465 patients to evaluate the accuracy of two image modalities for the brachytherapy of cervical cancer. Ten studies compared CT to MRI, while the other three compared MRI_{1st}/CT to MRI-based imaging; however, none of these studies compared all three imaging approaches on one patient (unlike the current study). Wang et al. found that, compared to MRI, the HRCTV width had been overestimated, while the height might have been underestimated when using CT. The dosimetric analyses

Table 1. Overall results of the HRCTV volume and dimensions for the ten patients

HRCTV	Fr	MRI (A)	MRI _{1st} /CT (B)	CT (C)		Ra	tio	
		Mean ± SD	Mean ± SD	Mean ± SD	A vs. B	<i>p</i> -value	A vs. C	<i>p</i> -value
Volume	1-4	18.8 ±6.7	-	27.7 ±10.1	-	-	1.48	0.00*
	2-4	18.6 ±6.8	20.8 ±6.8	26.7 ±9.3	1.11	0.02*	1.47	0.00*
Width	1-4	4.2 ±0.4	-	4.4 ±0.6	-	-	1.06	0.04
(maximum)	2-4	4.1 ±0.4	4.1 ±0.5	4.3 ±0.4	0.98	0.78	1.05	0.09
Width	1	2.7 ±0.7	-	3.2 ±0.7	-	-	1.20	0.01*
(point A)	2-4	2.5 ±0.7	2.8 ±0.7	3.1 ±0.7	1.12	0.08	1.18	0.05*
Height	1	2.7 ±0.7	_	3.3 ±0.4	-	_	1.21	0.01*
	2-4	2.8 ±0.7	2.9 ±0.6	3.3 ±0.4	1.07	0.48	1.22	0.02*

HRCTV - high-risk clinical target volume; MRI - magnetic resonance imaging; CT - computed tomography; Fr - fraction; SD - standard deviation; *statistically significant (p < 0.05)

 Table 2. HRCTV volume and dimensions for fractions 2-4 for the three imaging approaches

HRCTV	占	MRI (A)	MRI _{1st} /CT (B)	CT (C)	App	Approach A vs. B	В	App	Approach A vs. C	O	App	Approach B vs. C	O.
		Mean ± SD	Mean ± SD	Mean ± SD	Mean diff	SE	<i>p</i> -value	Mean diff	SE	<i>p</i> -value	Mean diff	SE	<i>p</i> -value
Volume	2	19.0 ±7.3	20.5 ±7.0	27.7 ±9.6	-1.53	0.95	0.42	-8.70	1.33	*00.0	-7.17	1.35	*00.0
	3	18.8 ±6.9	20.7 ±6.9	26.7 ±8.8	-1.86	0.58	0.31	-7.93	1.32	*00.0	90.9-	1.31	*00.0
	4	18.4 ±6.7	21.8 ±6.9	26.3 ±10.1	-3.41	1.04	0.03*	-7.92	0.74	*00.0	-4.51	1.71	0.03*
Width	2	4.1 ±0.4	4.1 ±0.6	4.3 ±0.6	-0.03	0.11	1.00	-0.25	0.12	0.07	-0.23	0.10	90.0
(maximum)	3	4.2 ±0.5	4.1 ± 0.5	4.3 ±0.3	0.11	0.10	0.83	-0.11	0.21	09.0	-0.20	0.19	0.33
	4	4.1 ±0.4	4.2 ±0.5	4.4 ±0.6	-0.06	0.11	1.00	-0.30	0.14	90.0	-0.28	0.09	0.02*
Width	2	2.7 ±0.8	3.0 ±0.8	3.2 ±0.6	-0.27	0.22	0.74	-0.55	0.21	0.03*	-0.27	0.17	0.15
(point A)	3	2.6 ±0.6	2.8 ±0.7	3.2 ±0.8	-0.25	0.17	0.54	-0.76	0.24	0.01*	-0.49	0.15	0.01*
	4	2.6 ±0.6	2.8 ±0.5	3.1 ±0.9	-0.26	0.14	0.32	-0.56	0.17	0.01*	-0.29	0.16	0.10
Height	2	2.7 ±0.7	2.8 ±0.6	3.2 ±0.4	-0.13	0.11	0.84	-0.53	0.18	0.02*	-0.40	0.20	0.08
	3	2.9 ±0.7	2.9 ±0.6	3.3 ±0.5	0.01	60.0	1.00	-0.46	0.16	0.02*	-0.47	0.14	0.01*
	4	2.7 ±0.7	2.8 ±0.6	3.3 ±0.4	-0.10	0.15	1.00	-0.62	0.23	0.03*	-0.52	0.15	0.01*

HRCTV – high-risk clinical target volume; MR/ – magnetic resonance imaging; CT – computed tomography; Fr – fraction; SD – standard deviation; mean diff – mean difference; SE – standard error, *statistically significant (p < 0.05)

Table 3. Summary of dosimetric results for HRCTV for the three imaging approaches

HRCTV	正	MRI (A)	MRI _{1st} /CT (B)	CT (C)	App	Approach A vs. B	В.	App	Approach A vs. C	. C	App	Approach B vs. C	. C
		Mean ± SD	Mean ± SD	Mean ± SD	Mean diff	SE	<i>p</i> -value	Mean diff	SE	<i>p</i> -value	Mean diff	SE	p-value
D ₉₀	2	6.8 ±0.7	6.9 ±1.5	6.0 ±1.3	-0.10	0.39	1.00	0.83	0.36	0.14	0.92	0.33	90.0
	3	6.9 ±0.5	6.8 ±1.1	6.0 ±1.1	0.12	0.24	1.00	0.94	0.28	0.02*	0.83	0.25	0.03*
	4	6.9 ±0.3	7.0 ±0.7	6.3 ±0.7	90:0-	0.19	1.00	69.0	0.22	0.04*	0.75	0.19	0.01*
D ₉₅	2	6.2 ±0.8	6.3 ±1.5	5.3 ±1.2	-0.07	0.37	1.00	0.89	0.35	0.10	96.0	0.34	90.0
	3	6.3 ±0.6	6.2 ± 1.1	5.3 ±1.1	0.12	0.22	1.00	96.0	0.29	0.03*	0.84	0.26	0.03*
	4	6.3 ±0.4	6.4 ±0.8	5.6 ±0.7	-0.08	0.19	1.00	0.73	0.24	0.05*	0.81	0.21	0.02*
D ₉₈	2	5.7 ±0.8	5.7 ±1.4	4.7 ±1.2	90.0-	0.35	1.00	0.95	0.37	60.0	1.01	0.35	0.05
	3	5.8 ±0.7	5.6 ±1.0	4.7 ±1.1	0.17	0.18	1.00	1.06	0.29	0.02*	06.0	0.28	0.04*
	4	5.8 ±0.5	5.9 ±0.8	5.0 ±0.8	-0.07	0.19	1.00	0.76	0.24	0.04*	0.83	0.22	0.01*
D ₁₀₀	2	4.5 ±0.8	4.4 ±1.1	3.4 ±1.0	0.08	0.25	1.00	1.05	0.29	0.02*	0.97	0.29	0.03*
	8	4.7 ±0.8	4.5 ±0.9	3.5 ±0.9	0.17	0.22	1.00	1.20	0.22	*00.0	1.03	0.30	0.02*
	4	4.6 ±0.5	4.6 ±0.8	3.8 ±0.6	90.0-	0.21	1.00	0.75	0.20	0.02*	0.80	0.21	0.02*

HRCTV – high-risk clinical target volume; MRI – magnetic resonance imaging; CT – computed tomography; Fr – fraction; SD – standard deviation; mean diff – mean difference; SE – standard error; "statistically significant (p < 0.05); D₉₉, D₁₉₀ – the minimum dose to 90%, 95%, 98%, 100% of the CTV

Table 4. Summary of dosimetric results for OAR for the three imaging approaches

OAR	占	MRI-only (A)	MRI _{1st} /CT (B)	CT-only (C)	App	Approach A vs. B	В	App	Approach A vs. C	. C	App	Approach B vs.	C
		Mean ± SD	Mean ± SD	Mean ± SD	Mean diff	SE	<i>p</i> -value	Mean diff	SE	p-value	Mean diff	SE	<i>p</i> -value
Bladder													
0.1 cc	2	6.9 ±1.0	7.4 ±2.0	7.4 ±2.0	-0.54	0.49	0.89	-0.55	0.49	0.87	-0.01	0.01	0.94
	8	6.8 ±0.7	8.2 ±2.0	8.2 ±2.0	-1.37	09.0	0.14	-1.37	0.59	0.14	0.00	0.01	1.00
	4	7.0 ±0.6	7.5 ±1.4	7.5 ±1.4	-0.49	0.55	1.00	-0.48	0.55	1.00	0.01	0.01	0.59
1 cc	2	5.5 ±0.7	6.1 ± 1.6	6.1 ±1.6	-0.56	0.36	0.46	-0.56	0.36	0.50	0.00	0.01	1.00
	3	5.6 ±0.5	6.3 ±1.0	6.3 ± 1.0	-0.64	0.36	0.31	0.65	0.36	0.31	-0.01	0.01	1.00
	4	5.7 ±0.4	5.8 ±1.1	5.7 ±1.2	-0.14	0.38	1.00	60.0-	0.41	1.00	0.04	0.04	1.00
2 cc	2	5.0 ±0.7	5.5 ±1.5	5.5 ±1.5	-0.51	0.31	0.42	-0.51	0.31	0.41	0.00	0.00	0.58
	3	5.1 ±0.4	5.7 ±0.8	5.7 ±0.8	-0.60	0.29	0.22	09:0-	0.29	0.22	0.00	0.00	1.00
	4	5.1 ±0.4	5.2 ±0.9	5.2 ±1.00	-0.12	0.31	1.00	-0.08	0.34	1.00	0.04	0.04	1.00
Rectum													
0.1 cc	7	5.0 ±0.8	5.4 ±1.1	5.4 ±1.1	-0.39	0.17	0.14	-0.40	0.17	0.13	-0.01	0.01	1.00
	3	5.2 ±0.4	6.3 ±1.9	6.3 ±1.9	-1.08	0.63	0.35	-1.09	0.63	0.36	-0.01	0.01	1.00
	4	5.2 ±0.6	5.9 ±1.0	5.8 ±1.1	-0.72	0.28	60.0	-0.64	0.32	0.23	0.08	0.08	1.00
1 cc	2	4.1 ±0.7	4.3 ±0.9	4.3 ±0.9	-0.22	0.16	0.58	-0.22	0.16	0.58	0.00	0.00	1.00
	3	4.3 ±0.4	4.9 ±1.2	4.9 ±1.2	-0.63	0.41	0.47	-0.63	0.41	0.47	0.00	0.00	1.00
	4	4.1 ±0.5	4.6 ±0.6	4.6 ±0.7	-0.54	0.24	0.16	-0.47	0.28	0.29	0.07	90.0	0.95
2 cc	2	3.6 ±0.6	3.9 ±0.9	3.9 ±0.9	-0.27	0.17	0.41	-0.27	0.17	0.40	0.00	0.00	1.00
	3	3.8 ±0.4	4.4 ±1.0	4.4 ±1.0	-0.61	0.34	0.32	-0.62	0.34	0.32	-0.01	0.01	1.00
	4	3.7 ±0.5	4.1 ±0.5	4.1 ±0.6	-0.42	0.23	0.31	-0.36	0.25	0.58	90.0	90.0	1.00
Sigmoid													
0.1 cc	2	2.9 ±1.2	4.2 ±2.1	4.2 ±2.0	-1.24	0.45	90.0	-1.25	0.44	90.0	0.00	0.01	1.00
	Ω	2.7 ±1.2	3.9 ±2.1	3.9 ±2.1	-1.15	0.53	0.17	-1.14	0.53	0.17	0.00	0.00	1.00
	4	2.9 ±1.0	4.4 ±2.3	4.3 ±2.3	-1.50	0.62	0.13	-1.45	0.63	0.15	0.04	0.04	1.00
1 cc	2	2.4 ±0.9	3.2 ±1.5	3.2 ±1.5	-0.85	0.34	0.10	-0.82	0.35	0.13	0.03	0.02	0.59
	8	2.1 ±0.9	3.0 ±1.6	3.0 ±1.6	-0.93	0.43	0.19	-0.93	0.44	0.19	0.00	0.01	1.00
	4	2.3 ±0.9	3.2 ±1.7	3.1 ±1.8	-0.93	0.43	0.19	-0.82	0.50	0.43	0.11	0.10	0.85
2 cc	2	2.1 ±0.8	2.8 ±1.3	2.8 ±1.3	-0.67	0.31	0.19	-0.67	0.31	0.18	0.00	0.00	0.50
	8	1.8 ±0.8	2.7 ±1.4	2.8 ±1.5	-0.84	0.37	0.15	-0.94	0.35	0.07	-0.10	0.10	0.99
	4	2.1 ±0.8	2.9 ±1.5	2.8 ±1.6	-0.81	0.38	0.21	-0.71	0.44	0.43	0.10	0.08	0.77

p-value 1.00 0.68 1.00 0.59 1.00 1.00 B vs. 0.00 0.00 0.00 0.00 0.00 0.00 0.01 0.01 Approach SE 0.00 0.00 0.00 0.00 0.00 -0.01 0.00 0.01 lue 0.82 0.10 0.56 0.09 1.00 0.12 0.33 لعا Approach A vs. 0.37 0.44 0.33 0.39 0.73 0.47 0.47 ₫ -0.43-1.29-0.33 -1.88-0.84-0.63Mean ne 0.82 0.10 0.56 1.00 0.09 0.13 0.33 p-valu Approach A vs. 0.47 0.39 0.73 0.47 0.37 0.44 0.33 0.51 SE diff -0.79-0.43-1.30-0.63-0.33 -0.19-0.84-1.12SD 3.87 ±1.49 2.64 ±1.36 2.75 ± 0.67 +0.8 CT-only 3.0 ±1. $4.1 \pm 1.$ 5.7 ±2 Mean 4.1 <u>@</u> SD 2.64 ±1.36 41.49 2.75 ± 0.67 3.0 ± 1.5 5.7 ± 2.4 3.1 ± 0.8 4.4 ±1.7 MRI_{1st}/CT 4.1 ±1. 3.87 4.1 MRI-only (A) S ±0.84 3.08 ±0.90 ±0.81 2.11 ± 0.96 2.6 ±0.9 3.3 ± 1.2 2.3 ± 1.0 3.9 ± 1.2 $3.0 \pm 1.$ 2.31 Table 4. Cont 占 4 S S 0.1

· oo and · Ď *statistically significant (p < 0.05); error; – mean difference; SE diff deviation; mean - standard computed tomography; Fr – fraction; SD minimum dose to the most exposed 0.1 cm³, 1 cm³, and 2 cm atı - organ

for the HRCTV were also lower for the CT-only approach compared with at least one fraction of the MRI-based brachytherapy. These outcomes were similar to the results of the current study. However, the height of the HRCTV obtained from our CT approach was contoured at two-thirds of the uterine height, as suggested by Hegazy *et al.* [33] and was found to be significantly higher compared to the results obtained with the MRI-only and the MRI_{1st}/CT approaches. As to fraction-by-fraction comparisons, there was a significant overestimation of the volume, and the dimension was obtained from the CT modality.

With regards to doses delivered to OAR, most dosimetric parameters in the dose-volume histogram, including $D_{0.1cc'}$, $D_{1cc'}$ and D_{2cc} showed no differences for the three imaging approaches used in the present study. In comparison, the Wang study [33] demonstrated that there were no statistically significant differences between the two modalities for the dosimetric analysis of OAR conducted in 4 studies. Furthermore, the MRI-guided brachytherapy provided an improved dose to the bladder in 4 studies, to the rectum in 4 other studies, and to the sigmoid in the remaining study. However, the clinical toxicity incidence showed no statistically significant difference between the two modalities.

The results of the present study indicate that the use of MRI-guided brachytherapy for target localization in MRI_{1st}/CT approach in cervical cancer brachytherapy provides an improved accuracy and precision of the tumor volume as well as a better dose coverage to the HRCTV, when it is compared with CT exclusive-based planning. At least one MRI is required to assess the tumor extension due to the overestimation of the HRCTV volume obtained using CT images (which was similar to the findings of other studies). However, there are some limitations of this study: it included small number of patients, and the interobserver variation was not assessed.

Conclusions

 $\mathrm{MRI}_{\mathrm{1st}}/\mathrm{CT}$ approach is a safe alternative for brachytherapy in cervical cancer patients, especially in those centers with limited MRI availability. Moreover, it is more cost-effective than the MRI-based approach.

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Disclosure

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