

# Adult mouse basal forebrain harbors two distinct cholinergic populations defined by their electrophysiology

# Cagri T. Unal<sup>1</sup>, Jorge P. Golowasch<sup>2,3</sup> and Laszlo Zaborszky<sup>1</sup>\*

<sup>1</sup> Center for Molecular and Behavioral Neuroscience, Rutgers, The State University of New Jersey, Newark, NJ, USA

<sup>2</sup> Federated Department of Biological Sciences, New Jersey Institute of Technology, Newark, NJ, USA

<sup>3</sup> Department of Mathematical Sciences, New Jersey Institute of Technology, Newark, NJ, USA

#### Edited by:

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#### \*Correspondence:

Laszlo Żaborszky, Center for Molecular and Behavioral Neuroscience, Rutgers, The State University of New Jersey, Newark, NJ 07102, USA. e-mail: laszloz@andromeda. rutgers.edu We performed whole-cell recordings from basal forebrain (BF) cholinergic neurons in transgenic mice expressing enhanced green fluorescent protein (eGFP) under the control of the choline acetyltransferase promoter. BF cholinergic neurons can be differentiated into two electrophysiologically identifiable subtypes: early and late firing neurons. Early firing neurons (~70%) are more excitable, show prominent spike frequency adaptation and are more susceptible to depolarization blockade, a phenomenon characterized by complete silencing of the neuron following initial action potentials. Late firing neurons (~30%), albeit being less excitable, could maintain a tonic discharge at low frequencies. In voltage clamp analysis, we have shown that early firing neurons have a higher density of low voltage activated (LVA) calcium currents. These two cholinergic cell populations might be involved in distinct functions: the early firing group being more suitable for phasic changes in cortical acetylcholine release associated with attention while the late firing neurons could support general arousal by maintaining tonic acetylcholine levels.

Keywords: spike frequency adaptation, tonic firing, phasic firing, calcium currents, neuromodulation

# **INTRODUCTION**

Basal forebrain (BF) areas include the medial septum, vertical, and horizontal limbs of the diagonal band, pallidal regions (ventral pallidum and globus pallidus) and the substantia innominata/extended amygdala. These areas contain a heterogeneous collection of cholinergic, GABAergic, glutamatergic, peptidergic projection neurons, and interneurons (Zaborszky and Duque, 2003; Zaborszky et al., 2012). This brain region is involved in sleep-wake regulation, motivation, learning-memory, and attention (Buzsaki et al., 1988; Saper et al., 2005; Steriade and McCarley, 2005; Datta and Maclean, 2007; Parikh and Sarter, 2008; Goard and Dan, 2009). A prominent feature of the region is the continuous collection of aggregated and non-aggregated, large, cortically projecting neurons that synthesize acetylcholine (ACh) that serves as the primary source of cholinergic input to the cerebral cortex. BF cholinergic neurons are compromised in several diseases, including Alzheimer's disease, schizophrenia, Parkinson's disease, Rett's syndrome, and autism (Bowen, 1976; Perry et al., 1978; Wenk and Mobley, 1996). Anatomically, cholinergic neurons are heterogeneous inasmuch as they have been shown to be variously colocalized with galanin (Melander and Staines, 1986), GABA (Brashear et al., 1986; Kosaka et al., 1988), N-acetyl-aspartyl-glutamate (Forloni et al., 1987), tyrosine hydroxylase (Henderson, 1987), calbindin (Chang and Kuo, 1991), and secretagogin (Gyengesi et al., 2010), among others. In addition to various neuroactive substances, cholinergic neurons are bestowed with various receptors that show differential regional distribution and species differences (for references see Harkany et al., 2003; Zaborszky et al., 2004; Hur et al., 2009; Zaborszky et al., 2012).

Single unit activity of cholinergic neurons using juxtacellular labeling in anesthetized (Duque et al., 2000; Manns et al., 2000) and in head-restrained rats (Lee et al., 2005; Hassani et al., 2009) along with cortical EEG recordings, lend support to earlier ideas suggesting an important role of BF cholinergic neurons in cortical arousal (Detari and Vanderwolf, 1987). However, the heterogeneous firing properties of cholinergic neurons (Bengtson and Osborne, 2000; Duque et al., 2000; Garrido-Sanabria et al., 2007; Hassani et al., 2009), add further complexity to understanding the specific role of cholinergic neurons in the various functions and disease states alluded to above.

Intrinsic membrane properties of cholinergic neurons have been characterized in previous studies using different approaches and species (Griffith, 1988; Markram and Segal, 1990; Alonso et al., 1996; Hedrick and Waters, 2010). To confirm the cholinergic phenotype of the recorded neurons, *post-hoc* histochemistry for acetylcholine esterase (AChE), the ACh degrading enzyme (Griffith, 1988), immunostaining for choline-acetyltransferase (ChAT), the enzyme that synthesizes ACh (Khateb et al., 1992) and single-cell PCR (Han et al., 2005) have been used. Also, *in vivo* pre-labeling before electrophysiology has been applied using an antibody against the p75 receptor (Wu et al., 2000). The various technical challenges in identifying a cholinergic phenotype in these studies can be circumvented by using mice genetically engineered to express green fluorescent protein (GFP) under the promoter of ChAT.

Using adult mice, we conducted in vitro patch clamp recordings from cholinergic cells sampled from the entire extent of the BF in transgenic ChAT-eGFP mice with the goal of obtaining a detailed knowledge of the intrinsic physiology of cholinergic neurons. Cholinergic BF neurons could be subdivided into two populations based on their firing delays in response to depolarizing current injections. Hence, we refer to them as early-(EF) and late-firing (LF) neurons. EF neurons discharged at higher frequencies in response to intracellular current injections but this was accompanied by a prominent spike frequency adaptation. In many instances, these neurons stopped firing after an initial discharge. On the other hand, LF neurons were less excitable but could maintain a tonic firing pattern even in response to longer (10s of seconds) current injections. Our results suggest that this heterogeneity is achieved through the intricate interplay among different voltage-gated calcium and potassium conductances. The mechanisms underlying these differences and their possible functional implications are discussed.

# **MATERIALS AND METHODS**

# ANIMALS

All experiments were performed in accordance with the US Public Health Service Policy on Humane Care and Use of Laboratory Animals, the National Institutes of Health Guidelines for the Care and Use of Animals in Research, and approved by the Rutgers University Institutional Review Board. Adult BAC transgenic mice (30-90 days old) expressing enhanced green fluorescent protein (eGFP) under the promoter of ChAT [B6.Cg-Tg(RP23-268L19-EGFP)2 Mik/J] were used (Jackson Laboratories, Bar Harbor Maine). The animals were anesthetized with i.p. injections of ketamine/xylazine mixture (150 and 30 mg/kg, respectively) and transcardially perfused with an ice cold perfusion solution containing (in mM): 248 sucrose, 2.5 KCl, 7 MgCl<sub>2</sub>, 23 NaHCO<sub>3</sub>, 1.2 NaHPO<sub>4</sub>, and 7 glucose. The brains were removed and a block containing the BF was secured on a vibratome and 250 µm coronal slices were obtained.

# ELECTROPHYSIOLOGICAL RECORDINGS

The slicing chamber in the vibratome contained the same solution used for perfusion. The slices were kept at room temperature (22-25°C) for at least 1 h in oxygenated artificial cerebrospinal fluid (ACSF) (95%  $O_2$  + 5% $CO_2$ ) containing (in mM): 124 NaCl, 2.5 KCl, 1.2 NaHPO<sub>4</sub>, 26 NaHCO<sub>3</sub>, 1.3 MgCl<sub>2</sub>, 2 CaCl<sub>2</sub>, 10 glucose. In a subset of experiments measuring whole-cell Ba<sup>2+</sup> currents, a modified ACSF (in mM) 79.5 NaCl, 2.5 KCl, 1.2 NaHPO<sub>4</sub>, 26 NaHCO<sub>3</sub>, 1.3 MgCl<sub>2</sub>, 2 CaCl<sub>2</sub>, 10 glucose, 40 TEA, and 5 BaCl<sub>2</sub> was used. 1 µM TTX was also present in the solution to block sodium channels. The slices were visualized with an Olympus BX51WI (Center Valley, PA) microscope, equipped with infrared differential contrast optics and epifluorescence setup, and superfused with oxygenated ACSF (3-5 ml/min) at room temperature. Whole-cell patch-clamp recordings were obtained from GFP+ neurons with glass pipettes  $(4-8 M\Omega \text{ tip resistance with})$ recording solutions) pulled with a horizontal puller (P-97, Sutter Instrument, Novato, CA). The intracellular solution (KMeSO<sub>4</sub>)

contained (in mM): 130 KMeSO<sub>4</sub>, 10 NaCl, 2 MgCl<sub>2</sub>, 10 HEPES, 3 Na<sub>2</sub>ATP, 0.3 GTP, 1 EGTA, pH 7.3. For Ba<sup>2+</sup> current measurements, a modified CsMeSO<sub>4</sub> intracellular containing (in mM): 125 CsMeSO<sub>4</sub>, 16 K-gluconate, 2 MgCl<sub>2</sub>, 10 HEPES, 3 Na<sub>2</sub>ATP, 0.3 Na<sub>3</sub>GTP, 1 EGTA, and 0.1 CaCl<sub>2</sub>, pH 7.3 was used (see below). The junction potential was experimentally determined to be 10  $\pm$  2 mV for all solution combinations and was not corrected for. Data acquisition started 10 min after access to the cell to allow sufficient stabilization of the recording. Specific BF subregions targeted are described in the Results.

All recordings used had stable access resistances (<10% change throughout recording) of less than 20 M $\Omega$  and were obtained only if a G $\Omega$  seal formed before whole-cell access. An Axoclamp 900A amplifier and Digidata 1440A data acquisition device (Molecular Devices, Palo Alto, CA) were used for recordings. Voltage clamp experiments were done in discontinuous mode with a sampling frequency of 10 kHz and filtered at 2 kHz. Voltage-current (V-I) relationships were generated for each neuron using 500 ms current pulses ranging from -100 to +120 pA in 20 pA increments at 0.33 Hz in bridge mode. These pulses were delivered from  $-70 \,\mathrm{mV}$  unless otherwise indicated. In some recordings, higher current amplitudes were used if necessary (see electrophysiological parameters tested). Analysis of current clamp recordings was done for data obtained from -70 mV unless otherwise stated. In all voltage clamp recordings the voltage monitor was continuously examined to ascertain sufficient return to baseline of the membrane potential prior to each voltage measurement cycle. Current densities were calculated by dividing the maximal current by whole-cell capacitance. Whole-cell capacitance was determined by injecting 5 mV hyperpolarizing voltage steps from  $-70 \,\mathrm{mV}$  and integrating the area of the associated transient. Access resistance was calculated from the linear portion of membrane hyperpolarization in response to a -20 pA current pulse from a holding potential of  $\sim -70 \,\mathrm{mV}$  in current clamp mode.

Cells were kept both at -90 and -40 mV and voltage steps of 500 ms duration were applied in 10 mV steps up to +10 mV at 0.33 Hz for the investigation of transient outward currents. In a subset (n = 6) of neurons, 1 second-long voltage steps were presented in -10 mV increments at 0.33 Hz from a holding potential of -40 mV up to -110 mV to study hyperpolarization-activated currents ( $I_h$ ).

In order to directly compare the firing properties and low voltage activated (LVA) calcium channel function, the neurons were first examined and identified in current clamp experiments carried out using the KMeSO<sub>4</sub> intracellular solution. Following the identification of the firing properties, the patch pipette was withdrawn and cells were re-patched using the CsMeSO<sub>4</sub> intracellular solution. Initial re-patching was done while the slice was still being perfused with the regular ACSF. Subsequently, we switched to the modified ACSF containing Ba<sup>2+</sup>. These procedures ensured the blockade of voltage dependent Na<sup>+</sup> and K<sup>+</sup> currents. In these experiments, the neuron was kept at -80 mV and presented with 2 second-long prepulses ranging from -110 to -50 mV in 10 mV increments followed by a 500 ms step to -40 mV unless otherwise indicated. Bridge balance and pipette capacitance neutralization was done prior to data acquisition.

#### DATA ANALYSIS

Statistical analysis was performed using SPSS.19 (Chicago, IL). Averages are represented as means  $\pm$  SD and compared with *t*-Student tests for independent samples. Pearson productmoment correlation coefficients ( $\rho$ ) were calculated to reveal correlations between different variables. The Kolmogorov–Smirnov test was used to determine the normality of distributions. A repeated measures analysis of variance (RM-ANOVA) was performed for comparing the transient potassium current amplitudes at different command voltages. Additional analysis involving paired *t*-tests were carried out to compare within-neuron effects. The half-maximal activation of currents was studied by applying a sigmoidal fit to the current-voltage (I-V) curves where current responses were normalized to the maximum recorded current.

See **Table 1** for a detailed explanation for some of the physiological parameters being measured.

#### CHEMICALS

All ingredients in the ACSF and perfusion solution except CaCl<sub>2</sub> (Sigma) were purchased from Fisher Scientific.  $I_{\rm h}$  measurements were done with regular ACSF. Outward currents were measured in the presence of 1  $\mu$ M tetrodotoxin (TTX) (Tocris) and 350  $\mu$ M CdCl<sub>2</sub> (Sigma) to block contamination of responses by voltage gated sodium and calcium channels, respectively. As alluded to above, Ba<sup>2+</sup> currents were measured using a CsMeSO<sub>4</sub> intracellular solution in modified ACSF containing 40 mM tetraethyl ammonium (TEA). In a subset of experiments, 100 nM Apamin (Sigma) and 5  $\mu$ M NiCl<sub>2</sub> (Sigma) were used.

#### MORPHOLOGY

In some recordings, 0.2% biocytin was included in the pipette for subsequent visualization. Following recordings with biocytin

in the pipette, slices were transferred to 4% paraformaldehyde for at least 24 h for fixation. For biocytin imaging, slices were incubated in Cy3-conjugated streptavidin or Texas Red conjugated streptavidin (Invitrogen, Carlsbad, CA) for 20–24 h (1:200, Jackson ImmunoResearch Laboratories, West Grove PA). Slices were then transferred to a slide and mounted with Vectashield wet mounting medium (Vector Labs Inc., Burlingame, CA). For the acquisition of digital images Adobe Photoshop was used with an AxioCam camera attached to a Zeiss microscope.

For ChAT immunocytochemistry, animals (n = 3) were perfused with saline followed by 4% paraformaldehyde. The brain was removed and placed into the same solution for overnight fixation. The next day, the brains were placed into sucrose solution (30%). Three days later, 50 µm thick BF sections were cut using a freezing microtome. Sections were placed into 0.1 M phosphate buffer (PB) for  $\sim$ 24 h. Every third section was taken for immunocytochemistry in order to obtain a series at 150 µ intervals. Sections were washed 3X in 0.1 M PB and incubated with Goat-anti-ChAT (1:500; Millipore, Temecula, CA) antibody with 1% normal donkey serum and 0.5% Triton-X in 0.1 M PB for overnight incubation at room temperature under dark. The next day, sections were washed 3X in 0.1 M PB and transferred into Donkey-anti-Goat Cy3 IgG (1:100) with 1% normal donkey serum and 0.5% Triton-X in 0.1 M PB for  $\sim$ 3 h at incubation at room temperature under dark. Following incubation, sections were washed 3X in 0.1 M PB and mounted using Vectashield wet mounting medium.

The GFP+ and ChAT immunopositive somata in BF areas were mapped using the Neurolucida<sup>®</sup> software (Micro-BrightField, Inc, Williston, VT) from six sections separated 150  $\mu$  apart. The analyzed sections were obtained from a single animal (1 out of 3) where fiber systems demarcating BF regions were fully preserved.

Table 1   Physiological properties examined in this study and their operational definitions.					
Rheobase current	The current pulse that first elicits an action potential from a holding potential of -70 mV (see V-I measurements in Materials and Methods section).				
RMP	Voltage value in the absence of DC injections 10 min after patching.				
R <sub>in</sub>	Calculated from $-70\text{mV}$ in response to a $-20\text{pA}$ current injection.				
Membrane time constant	Measure obtained by fitting a single exponential to the voltage response from -70 mV to a -20 pA current injection.				
First AP threshold	The point where the rising slope first exceeds 10 mV/ms at rheobase current.				
First AP amplitude	The voltage difference between threshold and peak.				
First AP half-width	The AP duration at half-maximal amplitude of the first action potential.				
First AP delay	The time between the onset of rheobase current and the threshold of the first action potential.				
AHP amplitude	The voltage difference between the first action potential threshold and the most negative voltage associated with the slower AHP following that action potential.				
AHP time to peak	The time it takes from the action potential threshold to the most negative potential associated with the AHP.				
Adaptation ratio	1(Last ISI/First ISI) in a recording that contains the first trace with 4 action potentials (elicited from -70 mV).				
I-F slope	The slope of the action potential frequency vs. current injection graph.				
Sag ratio	Minimum membrane response (around –100 mV for each neuron)/steady state potential. A 10 ms region was averaged for both time points in order to obtain a more reliable value.				
Depolarization block	Time between the end of the last AHP (which is marked by the abrupt change in the slope of the rising phase of the AHP or the onset of ripple oscillations) to the end of a 500 msec, 120 pA current pulse without an action potential.				

#### RESULTS

#### CO-LOCALIZATION OF GFP SIGNAL AND ChAT IMMUNOCYTOCHEMISTRY IN BF

In the sections processed for ChAT immunocytochemistry we counted a total of 739 GFP+ neurons, 640 (86%) of which were also immunopositive for the ChAT antibody (**Figure 1**). We did not observe any ChAT-immunopositive neurons that were negative for GFP. Given the substantial overlap in this prerequisite anatomical analysis, the recorded cells will be referred to as cholinergic cells.

#### DISTRIBUTION OF RECORDED NEURONS

We recorded GFP+ cholinergic neurons from the entire extent of the cholinergic BF as exemplified in (Figure 2). Nineteen neurons were located in the horizontal limb of the diagonal band (HDB). The rest of the neurons were localized in different areas including the lateral hypothalamus (n = 1), ventral pallidum (VP, n = 1), medial septum (n = 1), vertical diagonal band (VDB, n = 1), lateral preoptic area (LPO) (n = 2), substantia innominata (SI, n = 3), and anterior amygdaloid area (n = 1); areas containing the bulk of cholinergic corticopetal neurons. One neuron was localized in the bed nucleus of the stria terminalis (BNST) and two neurons were found in the interstitial nucleus of the anterior commissure, posterior component (IPAC). These latter three neurons shared similar physiological properties with neurons in the aforementioned BF regions. A subset of neurons was found at the border of BNST/VP/LPO (n = 1), hDB/VP border (n = 1), VDB/hDB border (n = 1) hDB/SI border and IPAC/VP border (n = 1). Figure 2A shows the localization (A1–A3) and structure (A4) of the neuron recorded from the medial septum. Figure 2B shows a neuron located in the hDB (B1, B2) and its morphology (B3). Finally, Figure 2C shows the localization (C1-C3) and structure (C4) of a neuron in the medial forebrain bundle (mfb).

# **GENERAL PHYSIOLOGICAL PROPERTIES OF CHOLINERGIC BF NEURONS**

Cells included (n = 103) in the initial analysis satisfied the following criteria: stable access resistance of less than 20 MΩ, less than 10% change in access resistance throughout recording, and were eGFP+ as visualized online (see Figure 3A). We characterized BF neurons according to several physiological attributes (definitions for each in Table 1). Because no physiological parameter exhibited a significant alteration due to filling with biocytin (not shown) we pooled all the data together. An additional number of neurons (n = 24) were recorded in further experiments (see below). In agreement with previous findings (e.g., Griffith and Matthews, 1986), most cholinergic cells exhibited a time independent anomalous rectification and a prominent after-hyperpolarization (AHP) (Figure 3B), outward rectification (Figure 3C), and wide spikes (Figure 3D, compare solid vs. dashed lines). In addition, many BF neurons exhibited a voltage hump (Figure 3C, arrow) after the onset of a depolarizing pulse. Because this is observed only if the cell is hyperpolarized (-80 mV in this case) it suggests the activation of a transient K current.

We found that two groups of BF neurons could clearly be distinguished based on large and significant differences in firing delay at rheobase current injections: LF neurons (LF, **Figure 4A**,



FIGURE 1 | Colocalization of GFP expression and ChAT immunocytochemistry in the substantia innominata. (A) GFP expression, (B) ChAT immunostaining, (C) Overlay of (A) and (B) shows that all GFP expressing cells are stained with an antibody against ChAT. Bar scale:  $50 \mu$ .

blue trace) and EF neurons (EF, **Figure 4A**, red trace). LF neurons had a mean firing latency of  $343 \pm 76 \text{ ms}$  (n = 33, range: 240–499 ms, ~32% of total sample) whereas EF neurons had a mean firing latency of  $107 \pm 53 \text{ ms}$  (n = 70, range: 18-206 ms,



~68% of total sample) (**Table 2**). The AP delay distributions are shown in **Figure 4B** in the form of cumulative probability plots. Each of the distributions was normally distributed within itself (Kolmogorov–Smirnov, LF: p = 0.200, n = 32; EF: p = 0.183, n = 69) while the entire data set differed significantly from a normal distribution [Kolmogorov–Smirnov, (102) 0.155 p = 0.00].

These neurons could be differentiated further by several attributes of their activity (statistical comparisons are all listed in **Table 2**): the linear slope of the current-frequency relationship of EF cells is steeper than LF cells (**Table 2**). This is also reflected by significantly higher firing rates elicited with current injections with 60 pA or higher from -70 mV [ANOVA,  $F_{(5, 96)} = 2.762$ , p < 0.05, **Figure 4C**). Moreover, EF neurons had lower AHP amplitudes (**Table 2**, **Figure 4D**).

EF and LF neurons also differ in their spike frequency adaptation properties with EF cells showing significantly more pronounced spike frequency adaptation (**Table 2**; **Figure 5**). The solid traces in **Figures 5A1** and **B1** illustrate the difference in spike frequency adaptation among LF and EF cells when stimulated with a strong depolarizing current pulse, while the dashed traces illustrate the basic action potential onset that characterizes the two cell types at rheobase. In line with the differences in spike frequency adaptation in these neurons, LF neurons could maintain a precise firing pattern when constant current was applied (Figure 5A2), while most EF neurons fired irregularly under similar conditions or became completely silent (4 out of 21) following a train of spikes (Figure 5B2), a phenomenon referred to as depolarization block. Such EF neurons could, however, fire regularly when hyperpolarizing pulses at a fixed frequency were superimposed on a constant depolarizing current possibly through the de-inactivation of voltagegated sodium currents (Figure 5B2). When measured with a 500 ms, 120 pA square pulse from -70 mV (see Table 1), varying degrees of depolarization block were apparent in many of the EF neurons within 500 ms, accompanied by significant statistical differences between the two populations along this dimension (Table 2). While EF neurons show a predominance and stronger level of spike frequency adaptation compared to LF neurons, LF neurons predominantly displayed a feature that is known as spike frequency acceleration characterized by an increase in frequency towards regular steady state firing after an initial gap (operational definition in Tables 1, 2 and Figure 5C1).



FIGURE 3 | Morphological and physiological identification of GFP expressing neurons in the BF. (A) Morphology of a typical GFP+ neuron. (A1) Image of the neuron taken with DIC. (A2) Same neuron imaged with epifluorescence illumination showing GFP fluorescence. (A3) Overlay of images in A1 and A2. Arrows in A1, A2, and A3 indicate the cell being patched. (B) A cholinergic neuron at rest responding to negative and positive square pulses ranging between -100 and 20 pA in 20 pA increments. Zero pA step not shown. Note the prominent AHP following the single spike (indicated with arrow), and anomalous inward rectification at negative voltages. (C) The same neuron recorded in the presence of  $1 \mu$ M TTX from a membrane potential of  $-80 \, \text{mV}$  in response to positive square current pulses from 20 to 120 pA in 20 pA increments. Note the voltage hump (indicated by arrow) and the outward rectification in the positive direction. (D) A representative cholinergic neuron spike (thick continuous line) and a spike from a non-cholinergic neuron (dashed line). Note the wide spike of the cholinergic neuron.

Six out of 70 EF neurons expressed a voltage sag, with a sag ratio higher than 1.05, suggestive of an h-current, whereas only 1 LF neuron expressed a voltage sag of this magnitude. Therefore, we did not pursue the h-current as an indicator of the EF vs LF distinction. The largest sag ratio observed was 1.12 and in those cells we could also measure an h-current in voltage clamp (not shown).

# POSSIBLE MECHANISMS UNDERLYING THE DIFFERENCES IN CHOLINERGIC NEURONS

In order to determine the possible mechanisms underlying the differences between EF and LF neurons we first compared the membrane time constant. EF neurons displayed significantly shorter time constants than LF neurons (**Table 2**). However, the difference is much smaller than the observed firing delay differences. On the other hand, action potential threshold for EF neurons is slightly, but statistically significantly, lower than for LF neurons (**Table 2**), which can also only partially explain the shorter delays. Hence, we measured the transient K<sup>+</sup> current expressed in these neurons, an A-type current, I<sub>A</sub>. **Figure 6A1** shows the protocol and raw currents used to determine I<sub>A</sub>-like current obtained after subtraction of non-inactivating currents from those obtained from a low, de-inactivating, voltage (-90 mV, **Figure 6A2**). Both cell types expressed I<sub>A</sub> to varying degrees, with LF neurons exhibiting

slightly higher current densities than EF neurons, but this did not reach significance [ANOVA,  $F_{(7, 24)} = 0.426$ , p = 0.43]. At a voltage of  $-40 \,\mathrm{mV}$ , the voltage closest to the spike threshold in these neurons, current densities were  $8.9 \pm 3.6 \text{ pA/pF}$  for LF neurons and  $8.3 \pm 5.1 \text{ pA/pF}$  for EF, which did not reach significance [t(31) = -0.3452, p = 0.73, Figure 6B1]. I<sub>A</sub> decay time constants measured at -40 mV were  $133.9 \pm 116 \text{ ms}$  for EF and  $137.1 \pm 65 \,\mathrm{ms}$  for LF neurons, which was also not significantly different between these two populations [t(31) =0.0796, p = 0.93, Figure 6B2]. Finally, we determined the halfmaximal activation voltages for IA by fitting a sigmoidal function to the conductance vs. voltage relationships of the two cell types. Here again we found no statistically significant difference  $[-31 \pm 7 \text{ mV} \text{ for EF} \text{ and } -28 \pm 5 \text{ mV} \text{ for LF} \text{ neurons;}$ t(31) = -1.109, p = 0.85]. Although no differences between mean values of any of these parameters of IA were found, the delay in action potential firing in individual LF neurons appears to relate to decay time of the IA they express. We observed a clear linear relationship between IA decay time constant (measured as single exponential fits to the decaying portion of IA measured at -40 mV) and action potential firing delays in LF neurons [after subtracting the membrane time constant to remove its small contribution, see Table 2, **Figure 6C1**, r(9) = 0.77, p = 0.007] but no such relationship for EF neurons was found [**Figure 6C2**, r(21) = 0.34, p = 0.090]. The general picture emerging from these correlations did not change when the absolute spike delay was considered instead of membrane time constant-subtracted spike delay (not shown). Figure 6D illustrates two LF neurons with different current densities and kinetics and the spiking delay differences in the expected direction.

Given the absence of significant differences in IA but a significant relationship between IA decay time constant with spike delay only in LF neurons, we tested the possibility of calcium currents contributing to the earlier spiking in these neurons in separate experiments. For these purposes, we compared LVA mediated Ba<sup>2+</sup> currents (I<sub>LVA</sub>) in EF and LF neurons (see Materials and Methods for details, Figure 7A1) with the prediction that  $I_{\text{LVA}}$ would be stronger in EF neurons. In line with this hypothesis, I<sub>LVA</sub> density was significantly higher in EF neurons when tested with pulses from -70 mV to -40 mV [6.4  $\pm$  3.8 pA/pF for EF and  $2.3 \pm 2.4$  pA/pF for LF neurons; t(13) = 2.467, p =0.03, Figure 7A2]. In order to confirm that these effects are due to the involvement of ILVA we also measured the inward current at -40 mV obtained with different prepulse voltages (Figure 7B1) and confirmed a statistically significant difference in I<sub>LVA</sub> between EF and LF neurons for all prepulse potential values except -50 mV [ANOVA,  $F_{(6, 8)} = 2.110$ , p < 0.05; Figure 7B2]. No statistically significant difference was observed for either the half-maximal activation  $[-71 \pm 12 \text{ mV} \text{ for LF}, -63 \pm 10 \text{ mV}$ for EF; t(13) = -1.327, p = 0.207] and decay time constant  $[16.7 \pm 10.0 \text{ ms} \text{ for LF}, 20.9 \pm 10.0 \text{ ms} \text{ for EF}; t(13) = 0.247,$ p = 0.808] between the two populations. HVA mediated currents were measured with ramp protocols (Murchison et al., 2009) and yielded no significant differences in EF and LF neurons (data not shown). To confirm these results independently in pharmacological experiments (n = 4 for each group), we investigated potential



	Early-firing Mean + SD	Late-firing Mean + SD	t	p	df
First AP delay (ms)	$107 \pm 53$	$343 \pm 76$	-16.094	<0.001	101
	(n = 70)	(n = 33)			
I-F slope (Hz/pA)	$0.06\pm0.04$	$0.03\pm0.02$	4.287	<0.001	101
Adaptation ratio	$2.74\pm2.57$	$1.33\pm0.57$	4.126	< 0.001	93
Depolarization block (ms)	$136\pm163$	$34\pm79$	4.234	<0.001	101
AHP (mV)	$18\pm10$	$24 \pm 7$	-3.576	<0.001	101
First AP threshold (mV)	$42 \pm 4$	$40 \pm 3$	2.839	0.006	101
Membrane tau (ms)	$44 \pm 18$	$52\pm16$	-2.268	0.025	101
RMP (mV)	$58.9\pm9.3$	$60.6\pm7.0$	-0.929	>0.05	101
R <sub>in</sub> (MΩ)	$610\pm301$	$641 \pm 247$	-0.512	>0.05	101
First AP amplitude (mV)	$71 \pm 9$	$72 \pm 7$	-0.395	>0.05	101
First AP half-width (ms)	$1.8\pm0.5$	$1.8\pm0.4$	0.160	>0.05	101

Ranked in order of highest-to-lowest significant difference. Differences tested using the t-Student test for independent measures.

spike onset changes under control conditions and in the presence of  $5 \,\mu$ M Ni<sup>2+</sup>, a concentration that is close to IC<sub>50</sub> values for the blockade of Ca(v) 3.2 channels (Kang et al., 2006), which is the dominant channel isoform in cholinergic BF neurons (Han et al., 2005). In EF neurons, Ni<sup>2+</sup> significantly delayed the spike onset

 $[72.8 \pm 12.1 \text{ ms without Ni}^{2+} \text{ and } 139.3 \pm 31.8 \text{ with Ni}^{2+}; t(3) = 3.6584, p < 0.0001, paired t-test] suggesting an important contribution of I<sub>LVA</sub> to AP delay. Contrary to this, Ni<sup>2+</sup> application did not produce a change in action potential delay in LF neurons <math>[315.5 \pm 89.3 \text{ ms without Ni}^{2+} \text{ and } 315.0 \pm 81.9 \text{ with Ni}^{2+};$ 



t(3) = 0.092, p = 0.932, paired *t*-test; **Figure 7C1**]. A representative effect of Ni<sup>2+</sup> application on AP delay in EF neurons is shown in **Figure 7C2**.

Spike frequency adaptation in LF neurons was increased when their AHP amplitude was reduced following application of 100 nM apamin, a selective SK channel inhibitor (n = 3; **Figure 5A1** *inset*) suggesting the participation of SK channels in determining the firing adaptation properties of LF neurons.

Finally, we analyzed whether the physiological differences observed had an anatomical correlate in morphologically well preserved sections with biocytin filled neurons. Due to the small number of samples from each area, we made hDB vs. non-hDB comparisons and none of the physiological parameters tested revealed any differences (data not shown) suggesting that cholinergic neurons with putatively different functions are intermixed across different BF regions. No BF area recorded contained bursting cholinergic neurons (see Discussion).

# DISCUSSION

Given the significance of the BF cholinergic system in diverse cognitive and physiological functions, characterizing the physiological properties of its constituent neurons is essential for a proper understanding of the mechanisms whereby these neurons exert their effects on cortical processing. Using adult transgenic mice expressing eGFP in cholinergic neurons, sampling from the entire BF and applying systematic physiological criteria, we have obtained evidence for the existence of two electrophysiologically distinct cholinergic cell populations in the mature BF, characterized by more than three-fold difference in spike onset latencies and two-fold difference in spike frequency adaptation rates; with EF cells exhibiting a more excitable and adapting profile. As evidenced by voltage-clamp analysis, the EF neurons exhibited higher expression of LVA calcium currents compared to the LF neurons. The variability of action potential delay in each group seems to be related to different mechanisms: IA-like



**FIGURE 6 | I<sub>A</sub> properties in BF neurons. (A)** Voltage dependence. **(A1)** Voltage clamp protocols (top left) used to isolate I<sub>A</sub>. Currents were measured in the presence of 1  $\mu$ M TTX and 350  $\mu$ M CdCl<sub>2</sub>. Examples of current responses to these two protocols are shown below. The currents shown on the right (V<sub>hold</sub> = -40 mV, dashed red line, steps: -60 to + 10 mV) were subtracted from the currents shown on the left (V<sub>hold</sub> = -90 mV, dashed red line). **(A2)** The net I<sub>A</sub> obtained after the subtraction described in **A1. (B)** I<sub>A</sub> density **(B1)** and I<sub>A</sub> decay at -40 mV **(B2)**. LF and EF neurons shown in blue and red, respectively. The box sizes indicate the standard error of the mean while whiskers indicate standard deviation. Circles indicate individual data points while the filled square shows the group means. **(C)** Spike onset correlations with I<sub>A</sub> decay time constants and membrane tau-corrected spike delays in LF **(C1)** and EF **(C2)** neurons. **(D)** Representative I<sub>A</sub> recordings from two LF neurons along with their current clamp recording of spiking activity (inset). The cell indicated by a darker trace has a slower inactivating I<sub>A</sub> along with a more pronounced spike delay.



FIGURE 7 | Low voltage activated calcium current ( $I_{LVA}$ ) properties in BF neurons. (A1) LF neuron (top blue traces) and EF neuron (bottom red traces) in current clamp (top trace in each case) showing the characteristic AP delay in response to a rheobase current injection (60 pA in this case). Bottom trace in each case shows  $I_{LVA}$  in response to a voltage clamp step from -70 mV to -40 mV upon re-patching the same cells with Cs-Meth intracellular solution and in Ba<sup>2+</sup>-containing ACSF (see Materials and Methods). Scale bars apply to both neurons. (A2) Box plot for  $I_{LVA}$  densities measured as described in A1. Box size indicates standard error of the mean. Square and whiskers have been displaced for clarity and indicate mean and standard deviation, respectively. Empty circles indicate individual data points (n = 7 LF; n = 8 EF). **(B1)** I<sub>LVA</sub>measured at -40mV with a de-inactivation protocol (see inset) for an LF (blue) and EF (red) neuron. Inset shows the protocol used to elicit the currents (2000 ms long prepulses from -100 to -50 mV, and 500 ms long test voltage at -40 mV all from a holding voltage of -80 mV). Scale bars apply to the current traces. **(B2)** I-V curve for the protocol in **B1. (C1)** Bar graph illustrating the selective effect of  $5\,\mu$ M nickel on firing delay in EF but not in LF neurons (n = 4 for each group). **(C2)** demonstrates the effect of Ni<sup>++</sup> application (light red trace) on firing delay in an EF neuron.

potassium currents, which have been shown to have important roles in determining spike onset latency in diverse systems (Tierney and Harris-Warrick, 1992; Gerber and Jakobsson, 1993; Tell and Bradley, 1994; Magarinos-Ascone et al., 1999; MacLean et al., 2005), seem to be related to spike delay only in LF neurons. On the other hand, the contribution of  $I_A$  is masked by LVA calcium current effects in EF neurons.

Previous results on cholinergic cell physiology in different BF subregions [e.g., (Momiyama and Zaborszky, 2006; Hedrick and Waters, 2010)] converge with our observations on some basic principles. In short, cholinergic BF neurons fire at lower frequencies compared to non-cholinergic BF neurons and therefore, they are usually referred to as slow firing BF neurons (Griffith and Matthews, 1986). Moreover, their action potentials are wider and commonly followed by prominent SK channel mediated medium afterhyperpolarizations (mAHPs) (Williams et al., 1997). In addition, anomalous rectification and outward rectification are among the other defining properties of cholinergic BF neurons (Bengtson and Osborne, 2000). However, we were unable to observe burst firing in any of the BF cholinergic neurons in our study compared with reports of bursting in cholinergic neurons of the substantia innominata (Khateb et al., 1992, 1995; Alonso et al., 1996). These discrepancies may arise from differences in the protocols used to record from these cells. Studies reporting bursting behavior were carried out with ACSF containing higher Ca<sup>2+</sup> concentration than our study (2.5 mM vs. 2 mM). In our conditions, calcium entry might not have been sufficient to counteract outward currents and generate bursting, a notion suggested before (Gorelova and Reiner, 1996; Sim and Allen, 1998). Finally, in some experiments we observed GFP negative neurons firing spike doublets similar to those reported as bursts in cholinergic neurons [e.g., (Khateb et al., 1992)]. Thus, bursting does not seem to be a universal property of cholinergic neurons in any BF region and cannot be used as an electrophysiological criterion to identify cholinergic neurons in vitro. However, these results do not negate the possibility of burst firing of cholinergic neurons in vivo [e.g., (Nunez, 1996; Manns et al., 2000)] and in vitro under specific experimental conditions or species differences (guinea pig vs. rat/mouse) (Khateb et al., 1997, 1998). For instance, EF neurons, with their strong calcium currents (see below) may correspond to burst firing cholinergic neurons recorded *in vivo* in the full presence of ascending neuromodulatory influences.

In summary, using direct comparison of current and voltage clamp data in the same cells and sampling from the entire BF, our study suggests the existence of two distinct types of cholinergic neurons. Ectopic expression of GFP might be a potential source of error in studies using transgenic animals. Likewise, we observed a slightly higher number of GFP+ neurons than the number of ChAT-immunoreactive (86% of the neurons were both GFP and immunopositive). However, immunocytochemistry likely has lower sensitivity than GFP expression, which could explain some of these differences. Further, the expression of general electrophysiological characteristics of cholinergic neurons in both EF and LF populations, mitigate against a significant contamination of our analysis by the small percentage of non-cholinergic neurons expressing GFP in a non-specific manner.

#### MECHANISMS UNDERLYING THE DIFFERENCES BETWEEN EF AND LF NEURONS TRANSIENT POTASSIUM CURRENTS

Transient potassium currents activate when neurons are depolarized from hyperpolarized potentials (Coetzee et al., 1999; Birnbaum et al., 2004) and have been shown to delay firing and regulate firing frequency (Storm, 1988; Tierney and Harris-Warrick, 1992; Gerber and Jakobsson, 1993; Tell and Bradley, 1994; Del Negro and Chandler, 1997; Kanold and Manis, 1999; Magarinos-Ascone et al., 1999; MacLean et al., 2005). Previous studies have reported the existence of transient potassium currents in cholinergic neurons in BF cultures but without reference to firing delay and other functional properties (Sim and Allen, 1998; Tkatch et al., 2000) while Eggermann et al. (2001) reported the presence of this current in voltage recordings and defines it as a set criterion for cholinergic BF neurons. The decay time constants of the current we identified resemble the slowly inactivating I<sub>A</sub> current which is also referred to as the I<sub>D</sub> current. However, in dissociated culture, IA currents identified in cholinergic neurons had faster inactivation kinetics (Sim and Allen, 1998; Tkatch et al., 2000). A recent study (Garrido-Sanabria et al., 2011) in slices also reported fast inactivating IA currents in slow firing putative cholinergic neurons in BF slices. The differences in the decay kinetics of this current might reflect differences in preparation and/or the age of animals used. Indeed, various potassium channels have been shown to be developmentally regulated in different cell types like cortical parvalbumin neurons (Okaty et al., 2009). Whether such alterations also occur in BF cholinergic neurons and their functional implications remain to be tested. Finally, the preponderance of cholinergic neurons with spike frequency acceleration along with the long decay time constant of the measured currents is suggestive for the presence of a Kv1 mediated ID current (Miller et al., 2008).

To our surprise, EF and LF neurons did not differ with respect to the average transient potassium current density or decay time constant. Interestingly, we observed a decay time constant to spike onset latency correlation, which can help to explain the spike delay variability of LF neurons, but clearly not that of EF neurons. This led us to consider other possibilities. While the shorter membrane time constant of EF neurons could explain the differences in spike latency to some extent, it is likely not an important factor since the transient potassium current decay time constant's relationship to spike onset latency in both groups remained unchanged after the membrane time constant was subtracted from the spike onset delay. Also, the slight but significant differences in spike thresholds between EF and LF neurons constitute another source for spike onset delay. These differences, although potentially important, are however, unlikely to explain differences measured in the order of tens of milliseconds.

# LOW VOLTAGE ACTIVATED CALCIUM CURRENTS

Voltage-gated ion channels are expressed in different neurons in different proportions, and the interplay between them has been shown to be critical in determining a neuron's behavior. Indeed, compensatory actions of different ion channels have been demonstrated in other systems (Linsdell and Moody, 1994; Pape et al., 1994; Del Negro et al., 2002; MacLean et al., 2003, 2005; Molineux et al., 2005; Hudson and Prinz, 2010). Given these possibilities, we predicted the presence of an inward current in EF neurons that counteract transient potassium currents. Due to their reliable expression profile in these neurons the most plausible candidate in cholinergic BF neurons is the Ca<sup>2+</sup> channels that mediate LVA currents (Allen et al., 1993). Indeed, it has been reported that different cholinergic neurons can be distinguished based on their LVA current density (Han et al., 2005). Moreover, interplay between transient potassium currents and LVA currents has been demonstrated to play an important role in determining spike latency in cerebellar stellate neurons (Molineux et al., 2005). Consistent with our predictions, EF neurons exhibited higher LVA current densities than LF neurons and blockade of channels mediating LVA currents in cholinergic neurons with nickel delayed spike onset latency in these neurons. Thus, it appears that the differences in firing delay between EF and LF neurons are probably due to interplay between membrane currents with different polarities. These findings might also explain the lower spike thresholds observed in EF neurons. Unfortunately, accurately measuring Ca<sup>2+</sup> and K<sup>+</sup> currents in the same neurons to determine their possible functional interactions is not possible given the combinations of blocking agents required and thus, establishing a definitive relationship between these currents remains a challenge.

Various types of voltage-gated ion channels can have different functions depending on their cellular localization (Brew and Forsythe, 1995; Hoffman et al., 1997; Magee, 1998; Migliore et al., 1999; Johnston et al., 2000; Gu et al., 2005; Burkhalter et al., 2006; Kollo et al., 2006, 2008). Our study is limited to the somatic current measurements due to problems associated with voltage clamping dendrites and therefore does not address the degree of involvements of these currents in the electrotonically distal portions of the neurons.

#### MECHANISMS UNDERLYING DIFFERENCES IN SPIKE FREQUENCY ADAPTATION

SK channels mediated AHPs have been shown to enhance the uniformity of the inter-spike interval in cholinergic BF neurons (Gorelova and Reiner, 1996) and in other systems, such as the non-cholinergic neurons of the globus pallidus (Deister et al., 2009). Our data are in line with this suggestion where LF neurons are shown to have higher AHP amplitudes and minimal spike frequency adaptation. Thus, SK channel-mediated AHPs may be important in recruiting Na<sup>+</sup> channels (via de-inactivation) for action potential generation and contribute to the determination of the electrophysiological properties that distinguish BF neuron cell types. The I<sub>A</sub> current is also known to facilitate Na<sup>+</sup> channel recovery from inactivation (Hess and El Manira, 2001). Therefore, in LF neurons mAHP and I<sub>A</sub> may in concert help sustain the repetitive firing.

The calcium channel that provides the calcium source for the activation of medium duration AHPs following single spikes show neuronal type-specific differences in many systems. In BF cholinergic neurons, calcium entry through the LVA channels have been shown to determine AHP amplitude (Williams et al., 1997). Curiously, our data show a

higher LVA density in EF neurons, which we have shown to exhibit smaller AHP amplitudes. It is possible that EF neurons have lower levels of SK channel expression and/or different localization of this channels compared to LF neurons where they might serve other functions [e.g. (Gu et al., 2005)].

#### **FUNCTIONAL IMPLICATIONS**

This study provides evidence for the existence of two subtypes of BF cholinergic neurons based on spike onset latency in the mature BF. EF neurons with their initial high frequency discharge followed by pronounced spike frequency adaptation could lead to a different acetylcholine release profile than that of LF neurons, which show little spike frequency adaptation when depolarized. Recent amperometric studies suggest that acetylcholine release can be tonic (measured in minutes) or phasic (measured in seconds) depending on attentional demands (Parikh et al., 2007; Parikh and Sarter, 2008; Hasselmo and Sarter, 2011), an observation that may relate to the existence of two functionally distinct cholinergic neuronal populations described in our study. Moreover, the delay to spiking, the main feature distinguishing cholinergic BF neurons, may be involved in different aspects of synaptic plasticity given the novel finding regarding the temporal requirements of cholinergic activation for different forms of hippocampal plasticity (Gu and Yakel, 2011).

Another interesting possibility relates to the complex architecture of cholinergic space in the BF. Statistical analysis of anatomical data based on nearest neighbor density determined that cholinergic neurons in rats are either found in dense clusters or diffusely located in the background (Nadasdy et al., 2010). Since the projection target of the clusters and the low density locations are different (Zaborszky et al., unpublished observations) it would be functionally important to test in future studies to what extent EF/LF neurons in mice fit into this anatomical scheme.

Further studies combining circuitry analysis, membrane physiology, and behavior will be instrumental in establishing of how this *in vitro* functional distinction relates to anatomical subtypes or *in vivo* behavior of cholinergic BF neurons.

# **AUTHOR CONTRIBUTIONS**

The work was done in Laszlo Zaborszky laboratory. Cagri T. Unal, Jorge P. Golowasch, and Laszlo Zaborszky conceptualized and designed the experiments. Cagri T. Unal performed all the experiments and analyzed the data. Jorge P. Golowasch and Laszlo Zaborszky assisted in the analysis of the data. Cagri T. Unal, Jorge P. Golowasch, and Laszlo Zaborszky interpreted the data and wrote the paper.

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