

Radiolabeling, whole-body single photon emission computed tomography/computed tomography imaging, and pharmacokinetics of carbon nanohorns in mice

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Abstract: In this work, we report that the biodistribution and excretion of carbon nanohorns (CNHs) in mice are dependent on their size and functionalization. Small-sized CNHs (30–50 nm; S-CNHs) and large-sized CNHs (80–100 nm; L-CNHs) were chemically functionalized and radiolabeled with [¹¹¹In]-diethylenetriaminepentaacetic acid and intravenously injected into mice. Their tissue distribution profiles at different time points were determined by single photon emission computed tomography/computed tomography. The results showed that the S-CNHs circulated longer in blood, while the L-CNHs accumulated faster in major organs like the liver and spleen. Small amounts of S-CNHs- and L-CNHs were excreted in urine within the first few hours postinjection, followed by excretion of smaller quantities within the next 48 hours in both urine and feces. The kinetics of excretion for S-CNHs were more rapid than for L-CNHs. Both S-CNH and L-CNH material accumulated mainly in the liver and spleen; however, S-CNH accumulation in the spleen was more prominent than in the liver.

Keywords: biodistribution, excretion, functionalization, nano-carbon, nanomedicine

Introduction

Carbon nanomaterials such as carbon nanotubes (CNTs),^{1–2} carbon nanohorns (CNHs),³ and graphene-related materials^{4,5} have attracted tremendous interest in the past decade due to their unique physicochemical properties. Carbon nanomaterials can find potential applications in various fields, including medical imaging and therapeutics.^{5–11} Their large available surface area, nanoscale dimensions, and possibility of multiple surface functionalization strategies make them unique materials with a lot of promise for the design of drug delivery systems.^{12–22} In addition, they offer high conversion efficiency of near-infrared radiation energy into heat, which enables them to be agents for photothermal therapy.^{22–24} Determination of the long-term fate of these carbon nanomaterials after administration into a living body is crucially important to allow the possibility for clinical translation.

To date, intensive efforts have been devoted toward assessment of safety issues related to carbon nanomaterials. In particular, several investigations aimed to evaluate the biodistribution of various functionalized CNTs and any potential adverse reaction.^{25–31} Some of us previously reported that the surface functionalization of multiwalled CNTs determines the tissue distribution and excretion profile after intravenous administration.²⁹ The modifications with polyethylene glycol (PEG) or PEG-derived polymers



have been reported to significantly extend blood circulation time of CNTs, reducing the risk of organ accumulation.^{25–26} Adequately functionalized multiwalled CNTs radiolabeled with [¹¹¹In] are retained in the reticuloendothelial system organs, such as the liver and spleen, but are also rapidly cleared from systemic blood circulation through the renal excretion route.^{27,28} The influence of type and degree of functionalization on the fate of injected CNTs has also been evaluated.²⁹ However, the effect of other structural parameters like the particle size (ie, short versus long) and shape (ie, small versus large diameter) has not been fully understood. The main reason is likely due to the difficulties of obtaining uniform different-sized CNTs in large quantities.

CNHs are considered good candidates for drug carriers due to the fact that they have a large surface area (1,464 m²/g) but also a wide inner-tube and inter-tube space in each individual horn (0.69 mL/g) after hole-opening.³² Another advantage is that the CNHs are produced without catalysts³ and therefore they are devoid of any toxic risks associated with residual metallic impurities. Recent studies have also shown that CNHs can be separated into different controlled sizes,^{33,34} and small-sized CNHs (S-CNHs) with uniform sizes ~20–50 nm can be easily obtained in large quantity by an oxidative disaggregation method.³⁴ S-CNHs are highly hydrophilic and remarkably resistant to cellular uptake by macrophages.³⁴ Histological observations following intravenous administration have shown that S-CNHs accumulate in the liver and spleen more slowly than large-sized CNHs (L-CNHs) of 80–120 nm in diameter.³⁵ This suggested that the biodistribution of CNHs may be size-dependent and it can eventually be further controlled by chemical functionalization.

To quantitatively and dynamically study the biodistribution of CNHs in vivo, we previously used Gd₂O₃ as label.^{36,37} Unfortunately, this type of labeling is based on annealing processes at high temperature resulting in S-CNH reaggregation into larger nanoparticles. To further analyze the fate of CNHs of different sizes and to perform a more detailed quantitative investigation, we utilized radioactive indium in this study (In-111) to label CNHs and to follow their tissue distribution and whole-body excretion after intravenous administration. For this purpose, the labeling process was performed by an amidation reaction of oxidized CNHs with the chelating agent diethylenetriaminepentaacetic acid (DTPA), an approach that has been successfully used to investigate the pharmacokinetic profiles of CNTs.^{27–29} By using this functionalization strategy, we can directly visualize the dynamic distribution of CNHs in whole body using single-photon emission computed tomography/computed tomography (SPECT/CT) and quantitatively calculate the organ distribution using

gamma scintigraphy. The data allowed comparison of the differences between S-CNHs and L-CNHs in organ accumulation as well as in their excretion profiles.

Experimental

Materials

CNHs were synthesized by CO₂ laser ablation of graphite at room temperature in Ar gas without a metal catalyst.³ S- and L-CNHs were prepared by oxidation as described in the following sections.

S-CNHs

Pristine CNHs (40 mg) were dispersed in 30 mL H₂SO₄ (98%; Wako Pure Chemical Industries, Ltd., Osaka, Japan) and stirred for 4 hours at room temperature.³⁴ After cooling the suspension at 5°C, 10 mL HNO₃ solution (67%; Wako Pure Chemical Industries, Ltd.) was slowly added, followed by sonication for 4 hours in a bath-type sonicator (~100 W) at 20°C. After sonication, the suspension was filtered (membrane filter, pore size 0.2 μm), the S-CNHs on the filtration paper were washed with water and re-dispersed in water. The filtration and re-dispersion in water was repeated until the pH of the filtrate became neutral. The obtained S-CNHs were re-dispersed in water (100 mL), sonicated at approximately 20°C with a tip-type sonicator (~300 W) for 30 minutes, and centrifuged at 10,000 rpm for 30 minutes. S-CNHs were collected from the upper 80% of supernatant. The concentration of the S-CNHs in the suspension was estimated from the absorbance at 700 nm measured with a ultraviolet-visible-near-infrared radiation spectrometer (Lambda 19; PerkinElmer Inc., Waltham, MA, USA). From the volume of the supernatant (~80 mL) and the concentration of S-CNHs (~0.1 mg/mL), the yield of S-CNHs was estimated to be ~20%. The size of the S-CNHs was estimated by dynamic light scattering (FPAR-1000; Otsuka Electronic Co., Ltd., Osaka, Japan). To observe the morphologies of S-CNHs using transmission electron microscopy (TEM) (120 kV, 36 μA; 002B HRTEM; Topcon Corporation, Tokyo, Japan), one drop of S-CNH dispersion was placed on a Cu grid with ultrathin carbon film and dried at room temperature. Thermogravimetric analysis (TGA) of as-grown CNHs was performed in He using a TGA Q500 (TA Instruments, New Castle, USA) with a heating rate of 10°C·min⁻¹, while the other analyses were done using a TGA1 (Mettler Toledo, Schwerzenbach, Switzerland) apparatus from 30°C to 900°C with a ramp of 10°C·min⁻¹ under N₂ using a flow rate of 50 mL·min⁻¹ and platinum pans.

L-CNHs

The pristine CNHs were treated by light-assisted oxidation³⁸ to render them hydrophilic by generating oxygenated groups

such as carboxylic groups. Briefly, pristine CNHs (40 mg) were dispersed in an aqueous solution of H_2O_2 (30%, 60 mL) and heated at 70°C – 80°C for 2 hours under irradiation using an Xe lamp. The resultant dispersion was filtered (membrane filter, pore size $0.2\ \mu\text{m}$), and the L-CNHs on the filter paper were washed and re-dispersed in water. The washing and re-dispersion were repeated four times. The obtained L-CNHs were re-dispersed in water (100 mL) by sonication in a water bath for 5 minutes. Their characteristics were similarly examined using the techniques described earlier. Cu grids with holey carbon were used for TEM observation of L-CNHs.

Chemical functionalization and labeling with ^{111}In

L-CNHs or S-CNHs were first treated with an amino-DTPA derivative³⁹ (see “Supplementary materials” for description of the synthesis of amino-DTPA, Figure S1) to allow chelation of ^{111}In (Figure 1). For this purpose, the CNHs (2.8 mg) were dispersed in oxalyl chloride (10 mL) using a water bath sonicator 20 W, 40 kHz (Transsonics Digital Elma, Singen, Germany). The suspension was heated at reflux for 16 hours. After evaporation of excess oxalyl chloride under reduced pressure, the CNHs were dispersed in anhydrous tetrahydrofuran (THF) (1.9 mL) using water bath sonication. A solution of amino-DTPA (28 mg) and *N,N*-diisopropylethylamine (50 μL) in anhydrous dimethylformamide (DMF) (2.8 mL)

was added. The suspension was sonicated in a water bath for 2 minutes and then heated at 65°C for 2 days. After cooling to room temperature, the solvents were evaporated under reduced pressure. Ammonium acetate buffer (0.2 M, pH 5.5, 30 mL) was added to the residue. The suspension was dispersed using water bath sonication and centrifuged at 4,500 rpm for 10 minutes. The supernatant was discarded and the precipitate was redispersed in ammonium acetate buffer. This sequence was repeated five times with ammonium acetate buffer and three times with deionized water. The precipitate was dispersed in deionized water using water bath sonication and the suspension was dialyzed in deionized water using 12–14 kDa molecular weight cut off (MWCO) dialysis membrane (Spectrum Laboratories, Inc., CA, USA) for 2 days.

For radiolabeling of the DTPA-S-CNHs or DTPA-L-CNHs, equal volumes of 0.2 mg/mL solutions in water of each was mixed with 0.2 M ammonium acetate buffer (pH 5.5) to which 2–20 MBq of $^{111}\text{InCl}_3$ was added. The indium was left to react with the DTPA-S-CNHs or DTPA-L-CNHs for 30 minutes at room temperature. The excess ^{111}In was treated with ethylenediaminetetraacetic acid (EDTA) (0.1 M) and removed by centrifugation (13,000 rpm for 30 minutes). To determine the labeling efficiency, aliquots of each final product were diluted five times in phosphate-buffered saline (PBS), and then 1 μL of the sample was spotted on silica gel impregnated glass fiber sheets (Pall

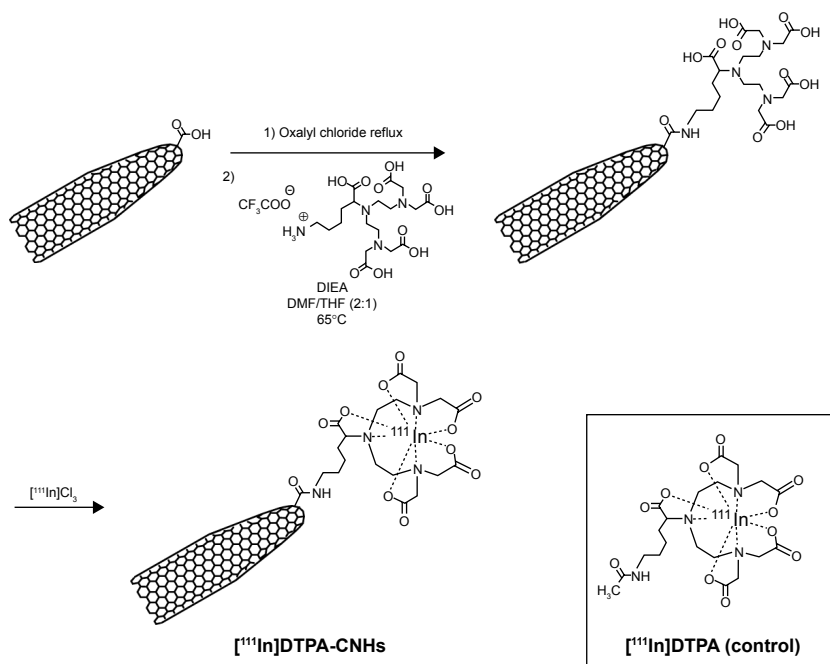


Figure 1 Synthesis of ^{111}In DTPA-CNHs (S-CNHs or L-CNHs).

Note: Inset: structure of ^{111}In DTPA derivative used as control.

Abbreviations: DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; DIEA, *N,N*-diisopropylethylamine; DMF, dimethylformamide; THF, tetrahydrofuran.

Corporation, Port Washington, NY, USA). The strips were developed with a mobile phase of 50 mM EDTA in 0.1 M ammonium acetate and allowed to dry. They were then developed for the quantitative counting of radioactivity using a Cyclone phosphor detector (PerkinElmer Inc., Waltham, MA, USA). The immobile spot on the thin-layer chromatography strips indicated the percentage of radiolabeled [^{111}In]DTPA-S-CN H or [^{111}In]DTPA-L-CN H conjugates, while [^{111}In]EDTA or [^{111}In]DTPA corresponds to the migrated spots. After centrifugation, the pellets of [^{111}In]DTPA-S-CN H s or [^{111}In]DTPA-L-CN H s were resuspended in 5% dextrose. The final concentrations of CN H s were adjusted to 0.2 mg/mL. For evaluating the radiolabeling stability of [^{111}In]DTPA-S-CN H s or [^{111}In]DTPA-L-CN H s, aliquots of each final product were diluted fivefold either in PBS or mouse serum and then incubated at 37°C over 24 hours. At different time points (0, 1, and 24 hours), 1 μL of the aliquots was spotted on silica gel impregnated glass fiber sheets and then developed, and quantified as described earlier. A control sample [^{111}In]DTPA was prepared by chelation of an acetylated DTPA ligand³⁹ with [^{111}In] (Figure 1, inset).

In vivo experiments

All animal procedures were performed in compliance with the UK Home Office Code of Practice for the Housing and Care of Animals used in Scientific Procedures. They were conducted following approval by the Institutional Ethical Review Committee, according to the UKCCCR Guidelines (1998) and under Project License 70/7763 granted by the UK Home Office. Six to 8-week-old C57/BL/6 mice (15–20 g), were purchased from Harlan (Oxfordshire, UK). Mice were housed in groups of five with free access to water and kept at a temperature of 19°C–22°C and relative humidity of 45%–65%. Prior to performing the experiments, all animals were allowed to acclimatize for at least 7 days. The radiolabeled S-CN H s or L-CN H s (50 μg , 3–5 MBq) were injected via the tail vein of mice after anesthetization by isoflurane inhalation. Immediately after injection ($t=0.5$ hours) and at $t=3.5$ hours, $t=24$ hours, and $t=48$ hours, mice were imaged using the Nano-SPECT/CT scanner (Bioscan, Washington, D.C., USA). CT scans were performed at the beginning of each SPECT acquisition. SPECT images were obtained in 24 projections over 40–60 minutes using a four-head scanner with 1.4 mm pinhole collimators. All images were reconstructed with MEDISO software (Medical Imaging Systems, Budapest, Hungary). Fusion of SPECT and CT images was carried out using the PMOD software (PMOD Technologies, Zurich, Switzerland). For quantitative assessment of

tissue distribution of [^{111}In]DTPA-S-CN H s or [^{111}In]DTPA-L-CN H s, mice were injected via the tail vein with 250 μL containing 50 μg of [^{111}In]DTPA-S-CN H s or [^{111}In]DTPA-L-CN H s labeled with approximately 0.5–2 MBq. Mice were then sacrificed at 1, 4, and 24 hours after injection, and blood and all major organs and tissues were collected, including: heart, lungs, liver, spleen, kidneys, muscle, skin, and bone. Urine and feces were pooled and collected after 24 hours. Each sample was weighed and counted on a gamma Counter (PerkinElmer Inc.), together with a dilution of the injected dose with dead time limit below 60%. The percentage injected dose per gram tissue was calculated, using four different mice for each time point.

Results and discussion

Characterization of S-CN H s and L-CN H s, and their ^{111}In labeling

The morphologies of S-CN H s and L-CN H s were shown in Figure 2A and 2B, respectively. S-CN H s contained individual nanohorns and small-sized aggregates (Figure 2A), and their size was between 30 and 50 nm as estimated from dynamic light scattering (Figure 2C), in agreement with previous results.³⁴ L-CN H s maintain the original spherical form of aggregates (Figure 2B) with size range of ~80–120 nm (Figure 2C). TGA of as-grown CN H s, L-CN H s, and S-CN H s performed in an inert atmosphere is shown in Figure 2D. The weight loss observed for L-CN H s and S-CN H s is mainly caused by the emission of CO and CO $_2$ as a result of the thermal decomposition of oxygenated groups.⁴⁰ The concentration of carboxyl groups in the buffer solutions was estimated to be 6 μmol for S-CN H s and 2.5 μmol for L-CN H s per milligram of material, taking into account the quantities of carboxyl groups assessed from the weight loss at 400°C, which is due to the decomposition of carboxyl groups.⁴⁰ The COOH functions of both L-CN H s and S-CN H s were derivatized by amidation with the amino-DTPA derivative, via pre-activation of the carboxyl groups using oxalyl chloride. TGA performed in an inert atmosphere confirmed the successful functionalization of L-CN H s and S-CN H s with DTPA (Figure 2D). Indeed, the weight loss of DTPA-L-CN H s and DTPA-S-CN H s was higher compared to the L-CN H s and S-CN H s, respectively.

DTPA-amidated S-CN H s and L-CN H s were then labeled with ^{111}In , and the labeling efficiencies directly after the radiolabeling reaction corresponded to 64.6% and 95.2%, respectively (Figure S2). None or very little traces of free [^{111}In]DTPA molecules were confirmed by thin-layer chromatography before injecting the material in

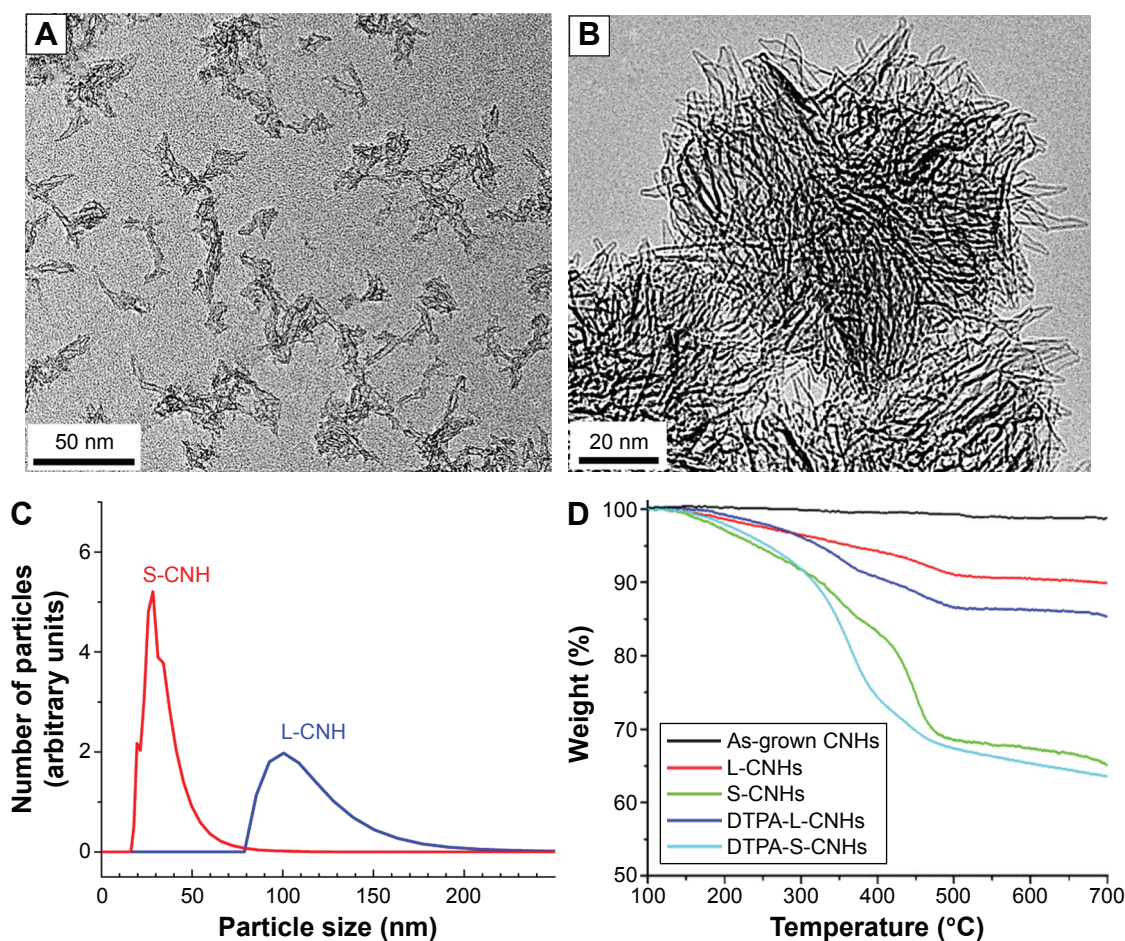


Figure 2 Characteristics of S-CNHs and L-CNHs.

Notes: (A and B) TEM images of S-CNHs and L-CNHs, respectively. (C) Dynamic light scattering results of S-CNHs and L-CNHs dispersed in water. (D) TGA of as-grown CNHs (black), L-CNHs (red), S-CNHs (green), DTPA-L-CNHs (blue), and DTPA-S-CNHs (cyan).

Abbreviations: DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; TEM, transmission electron microscopy; TGA, thermogravimetric analysis.

mice. The ^{111}In atoms were not released from the chelating function in PBS or in serum at 37°C for 24 hours (Figures S3 and S4).

CNH tissue distribution

Three-dimensional SPECT/CT reconstruction images of mice whole-bodies after injection of ^{111}In]DTPA-S-CNHs, ^{111}In]DTPA-L-CNHs, and ^{111}In]DTPA are shown in Figures 3 and S5. The quantities are indicated with colors. ^{111}In]DTPA-S-CNHs or ^{111}In]DTPA-L-CNHs accumulated mainly in the liver and spleen. They were also observed in the kidney or bladder at early time points. After 24 hours and 48 hours postinjection, the signals were still persistent only in the liver and spleen. SPECT/CT images of S-CNHs showed relatively weaker signal intensities than those of L-CNHs because of the relatively lower labeling efficiency (Figure S2). Signals in the bladder of ^{111}In]DTPA-L-CNHs remained even after 4 hours compared to ^{111}In]DTPA-S-CNHs. The control

sample ^{111}In]DTPA was almost completely excreted within the first hour (Figure S5).

Gamma scintigraphy was then used for the quantification of S-CNHs and L-CNHs in blood and the major organs and tissues like skin, liver, spleen, kidney, heart, lung, muscle, bone, stomach, and intestine at different time points (ie, 1, 4, and 24 hours) (Figure 4 and Table 1). The control sample ^{111}In]DTPA was used for comparison (Figure S6 and Table 1). Both types of CNH signals in blood reduced rapidly within the first hour. However, low levels of the smaller ^{111}In]DTPA-S-CNHs remained constantly circulating in blood, with $2.5\ \mu\text{g}/\text{mL}$ (1.3% injected dose [ID]) remaining in blood after 24 hours. Levels of the larger ^{111}In]DTPA-L-CNHs reduced more rapidly in blood and only $0.82\ \mu\text{g}/\text{mL}$ (0.4%) remained after 24 hours (Figure 4A and B). This suggests that the smaller CNHs were able to circulate longer, and their uptake by tissues was delayed. This behavior is common in the smaller nanoparticles which tend to reenter the blood

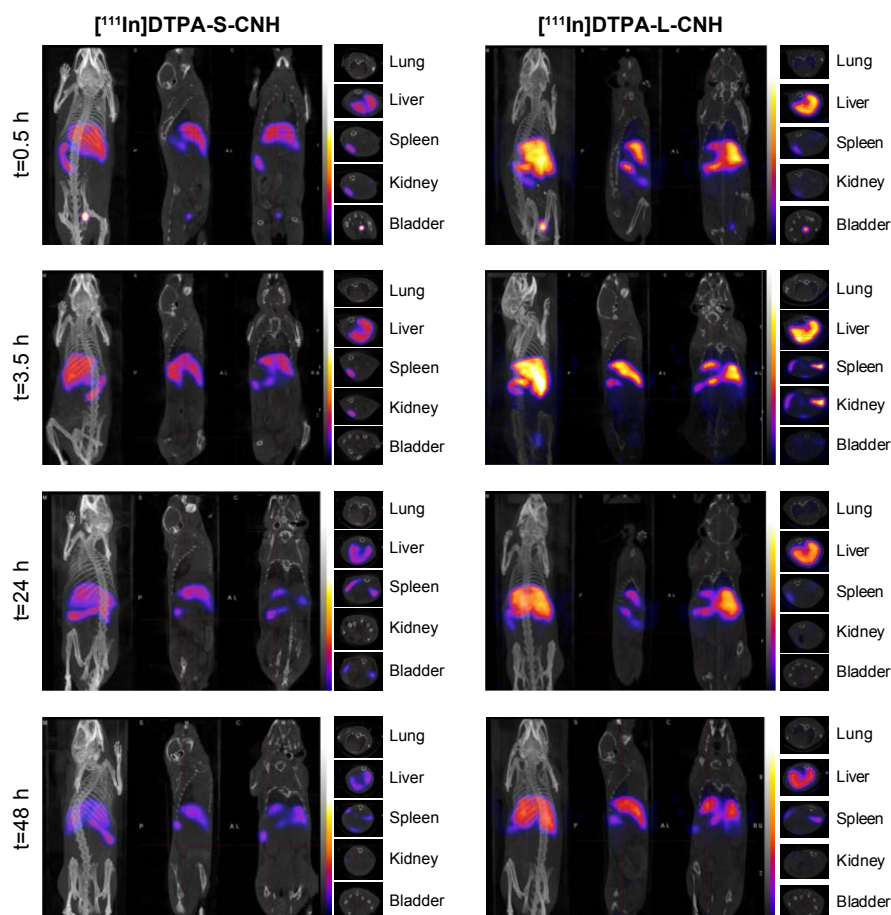


Figure 3 Whole-body SPECT/CT images of ^{111}In -labeled S-CNHs and L-CNHs after intravenous injection in C57BL/6 mice at 0.5, 3.5, 24, and 48 hours (h) postinjection. **Notes:** The bright areas indicate the accumulation of ^{111}In -labeled S-CNHs and L-CNHs. Images from left to right show whole-body, sagittal, frontal, and transverse views. The transverse cross-sectional images of spleen, liver, lung, kidney, and bladder are shown in the last columns. **Abbreviations:** DTPA, diethylenetriaminepentaacetic acid; SPECT/CT, single-photon emission computed tomography/computed tomography; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs.

stream.⁴¹ The larger ^{111}In DTPA-L-CNHs were taken up by the organs very rapidly at the first time points.

The S-CNH quantity in the liver (% ID/organ) was ~6.1% at 1 hour and increased significantly after 4 hours to 37.4%, remaining high at 24 hours (41.5%). The S-CNH quantity in the spleen was ~8.2% and increased a little with time (Figure 4C). The larger ^{111}In DTPA-L-CNHs were taken up by the organs very rapidly at the first time point. The L-CNH quantity in the liver was 73.7% (% ID/organ) at 1 hour, remaining unchanged at 4 and 24 hours (Figure 4D). The L-CNH quantity in the spleen was less than 5% at 1 hour, increasing a little with time. In other organs, quantities of S- and L-CNHs were very low, <2% (Figure 4).

A more accurate analysis of the data is given by measuring the accumulation as percentage of the injected dose per gram of tissue (% ID/gram of tissue) (Figure 4E and F), to better express the affinity of CNH material for each tissue. The preferential accumulation of CNHs in the liver and spleen was again evident. However, the accumulation of

^{111}In DTPA-S-CNHs in the spleen became more prominent, while the larger ^{111}In DTPA-L-CNHs expressed almost equal affinity to both organs. The size, sphericity, and deformability play a central role in accumulation of nanoparticles in tissues. Larger nanoparticles (150–200 nm) with spherical shapes tend to be trapped by the liver fenestra and recognized by Kupffer cells.⁴² Smaller particles (of ~100 nm in diameter) with elongated shapes may be sequestered by the spleen, unless being deformable enough to cross the spleen reticular network. The control sample ^{111}In DTPA showed rapid elimination from blood and only high kidney signals at early time points with no accumulation in other organs, with almost complete elimination after 24 hours (Figure S7, and Table 1).

CNH excretion

The values of % ID of S-CNHs or L-CNHs in the organs reported in Table 1 correspond to the quantities of materials detected in the body at different time points. The total

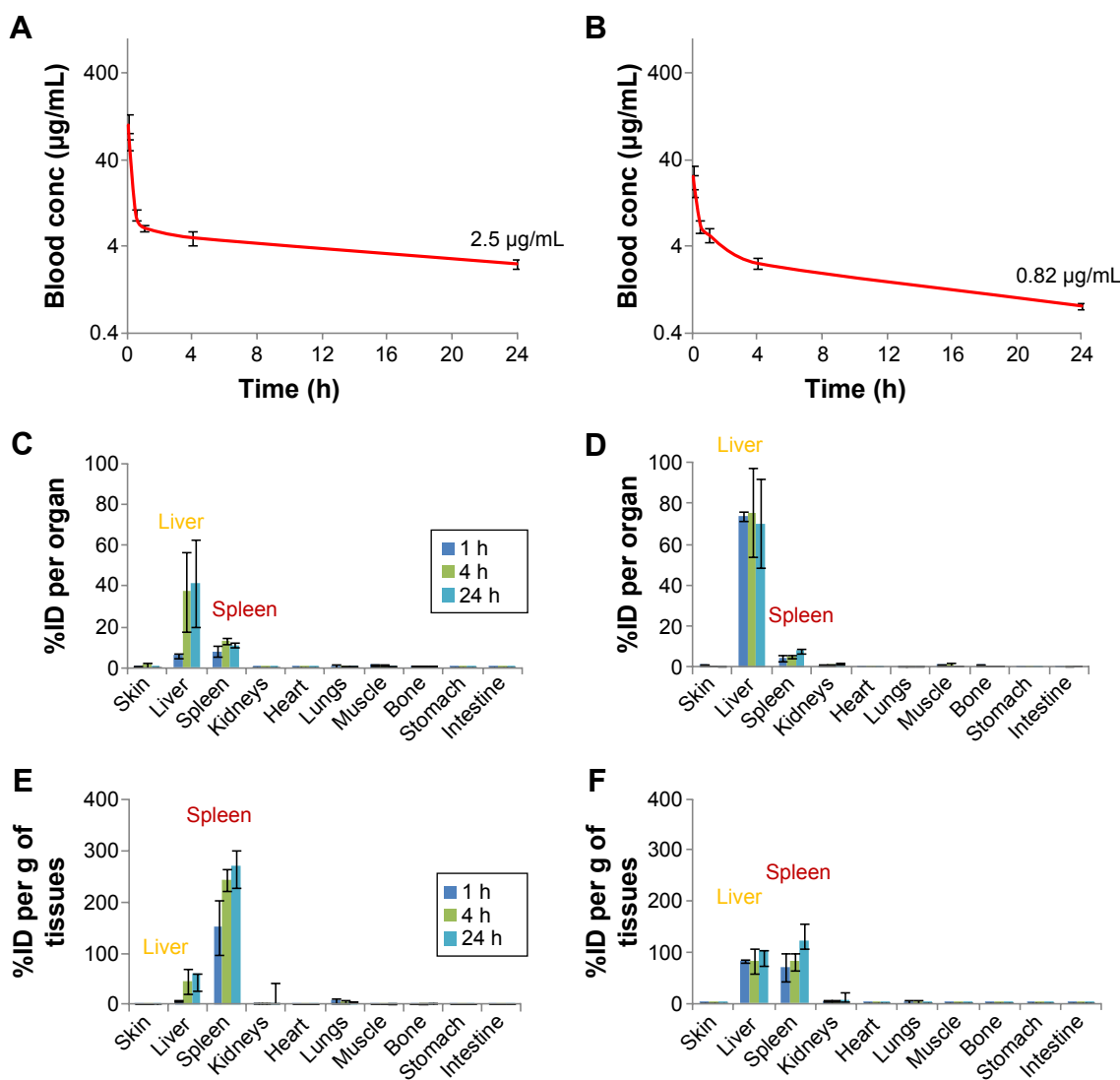


Figure 4 Quantities of [^{111}In]-labeled S-CNHs and L-CNHs in mice obtained by gamma scintigraphy up to 24 hours postinjection.

Notes: (A, B) Show concentrations detected in blood of [^{111}In]-labeled S-CNHs and L-CNHs, respectively. (C, D) Results expressed by percentages of injected dose per whole organ (% ID/organ) for S-CNHs and L-CNHs, respectively. (E, F) Present the results expressed by percentages of injected dose per gram of organs (% ID/g) for S-CNHs and L-CNHs, respectively. Data are represented as mean \pm standard error, $n=4$ mice per group.

Abbreviations: CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; h, hour(s); Conc, concentration.

amount of both S-CNHs and L-CNHs after 4 hours was 58.2% and 87.5%, respectively. Liberation of [^{111}In] atoms from S-CNHs or L-CNHs was likely not happening because no decomplexation occurred in PBS and in serum at 37°C for 24 hours (Figure S3). Thus, it is inferred that a certain amount of S-CNHs or L-CNHs was excreted mainly in

urine within the first few hours, followed by the small/trace amount excretions in urine and feces continuing for 48 hours (Figures 3 and S7). The excreted quantity of S-CNHs was more than that of L-CNHs, detected by quantities in urine, with 8% of S-CNHs excreted compared to only approximately 5% of the L-CNHs (Figure S7). This

Table I Percentage ID detected in major organs and blood by gamma quantification

Time (h)	S-CNHs			L-CNHs			DTPA		
	Major organs (%)	Blood (%)	Total (%)	Major organs (%)	Blood (%)	Total (%)	Major organs (%)	Blood (%)	Total (%)
1	19.1	3.3	22.4	83.7	2.7	86.4	4.5	6.2	10.7
4	55.7	2.5	58.2	86.2	1.3	87.5	13.5	4.2	17.6
24	56.4	1.3	57.7	83.4	0.4	83.8	1.5	0.2	1.7

Abbreviations: h, hour(s); CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; DTPA, diethylenetriaminepentaacetic acid.

may have been the case because the smaller sized S-CNHs could avoid phagocytotic uptake more effectively than the larger L-CNHs, as has been observed in a previous in vitro study.³⁵ Also, small-sized nano-carbons were able to cross the glomerular filtration slits (40 nm)²⁸ more comfortably than L-CNHs.

Urinary excretion was further confirmed by semi-quantification of the SPECT bladder signal. S- and L-CNH quantities detected in the bladder after 1 hour were ~3.50 and 2.16% of ID, respectively (Table S1). Both SPECT/CT and gamma scintigraphy data showed that overall small quantities of S-CNHs and L-CNHs (less than 10% ID) were detected in urine and feces at later time points of 24 and 48 hours (Table S1 and Figure S7). Although the preferential accumulation of S-CNHs and L-CNHs in the liver and spleen has been reported in our previous histological observations,³⁵ the results obtained in this study by SPECT quantitatively confirmed that the biodistribution of nano-carbons in vivo is size-dependent. In addition, the excretion profile of CNHs functionalized by [¹¹¹In]DTPA was different from Gd₂O₃-labeled CNHs (100 nm aggregates) coated with DSPE-PEG 1,2-distearoyl-*sn*-glycero-3-phosphoethanolamine-*N*-[amino(PEG)] (5 kDa),³⁷ that were mainly excreted via the liver–bile duct–duodenum route.³⁷ The similar results from single-wall carbon nanotubes (SWNTs) and graphene oxide also indicated that DTPA-functionalized SWNTs^{27–29} or graphene oxide⁴³ exhibited faster clearance from the body than PEG-modified CNTs or graphene.⁴⁴ Therefore, we think that the surface functionalization of CNHs with non-bulky functional groups, like DTPA, can lead to a different biodistribution and excretion kinetic profile. This is effective in avoiding the uptake by phagocytes that may further facilitate excretion via both the urinary and liver–bile duct routes.

In addition, we did not find any signs of weakness, illness, or weight loss by visual inspection of the mouse and their organs after imaging.

Conclusion

We have studied the size-/shape-effect of CNHs on the biodistribution and excretion profile by using two types of CNHs (S-CNH: 30 nm and L-CNH: 100 nm). These CNHs were covalently functionalized with [¹¹¹In]DTPA and intravenously injected in mice. Their whole-body biodistribution profiles and excretion rates were studied by SPECT/CT and gamma scintigraphy. Both S-CNHs and L-CNHs accumulated mainly in the liver and spleen; however, S-CNHs exhibited higher affinity for the spleen. The larger, spherical L-CNHs accumulated in the liver and spleen to the same extent. A small

amount of S-CNHs and L-CNHs was excreted within the first few hours after injection, followed by much slower excretion rates obtained after 48 hours. The excretion of S-CNHs was slightly faster than L-CNHs. Compared with the previous results for CNHs coated with phospholipid-PEG, the tissue distribution profile and kinetics of excretion determined for CNHs here were significantly different, most likely due to the differences in the material surface functionalization.

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Disclosure

The authors report no conflicts of interest in this work.

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Supplementary materials

Materials and methods

All reagents and solvents were purchased from different commercial suppliers and used as received. ^1H and ^{13}C nuclear magnetic resonance (NMR) spectra were recorded on a Bruker 300 MHz instrument (Bruker Corporation, Billerica, MA, USA). The peak values were obtained as ppm (δ) and referenced to the solvent. The resonance multiplicity is indicated as s (singlet), t (triplet), m (multiplet), and br (broad). Liquid chromatography–mass spectrometry analyses were performed on a Thermo Fisher Finnigan LCQ Advantage

Max system (Thermo Fisher Scientific, Waltham, MA, USA). Thermogravimetric analysis was performed using a Thermogravimetric analysis 1 (Mettler Toledo, Schwerzenbach, Switzerland) apparatus from 100°C to 900°C with a ramp of 10°C min⁻¹ under N₂ (flow rate of 50 mL·min⁻¹) and platinum pans.

The amino-diethylenetriaminepentaacetic acid derivative was synthesized from the *t*-Bu-protected diethylenetriaminepentaacetic acid ligand reported in Marangon et al.¹ The latter (665 mg) was stirred in trifluoroacetic acid (TFA) (8 mL) and deionized water (0.89 mL) for 17 hours.

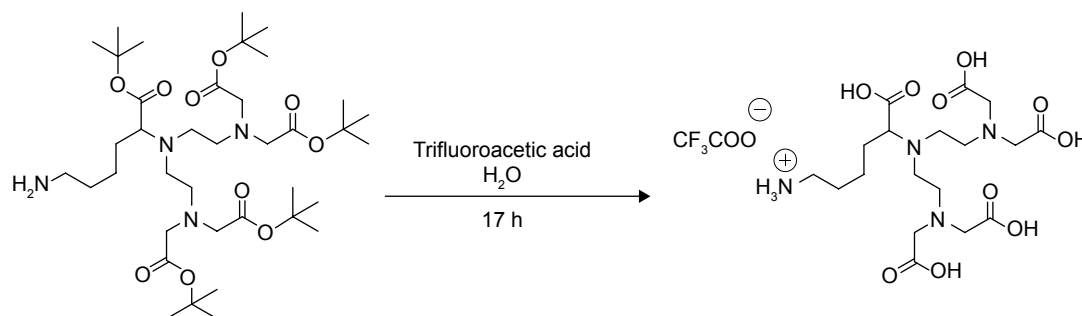


Figure S1 Preparation of amino-DTPA.

Abbreviations: DTPA, diethylenetriaminepentaacetic acid; h, hours.

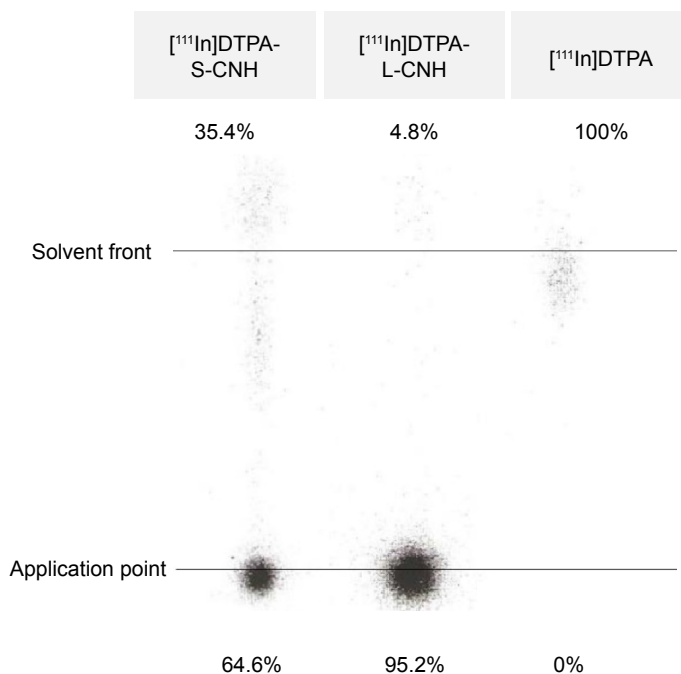


Figure S2 Radiolabeling efficiency of [¹¹¹In]DTPA-S-CNHs and [¹¹¹In]DTPA-L-CNHs compared to control [¹¹¹In]DTPA, measured directly after radiolabeling reaction.

Abbreviations: DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs.

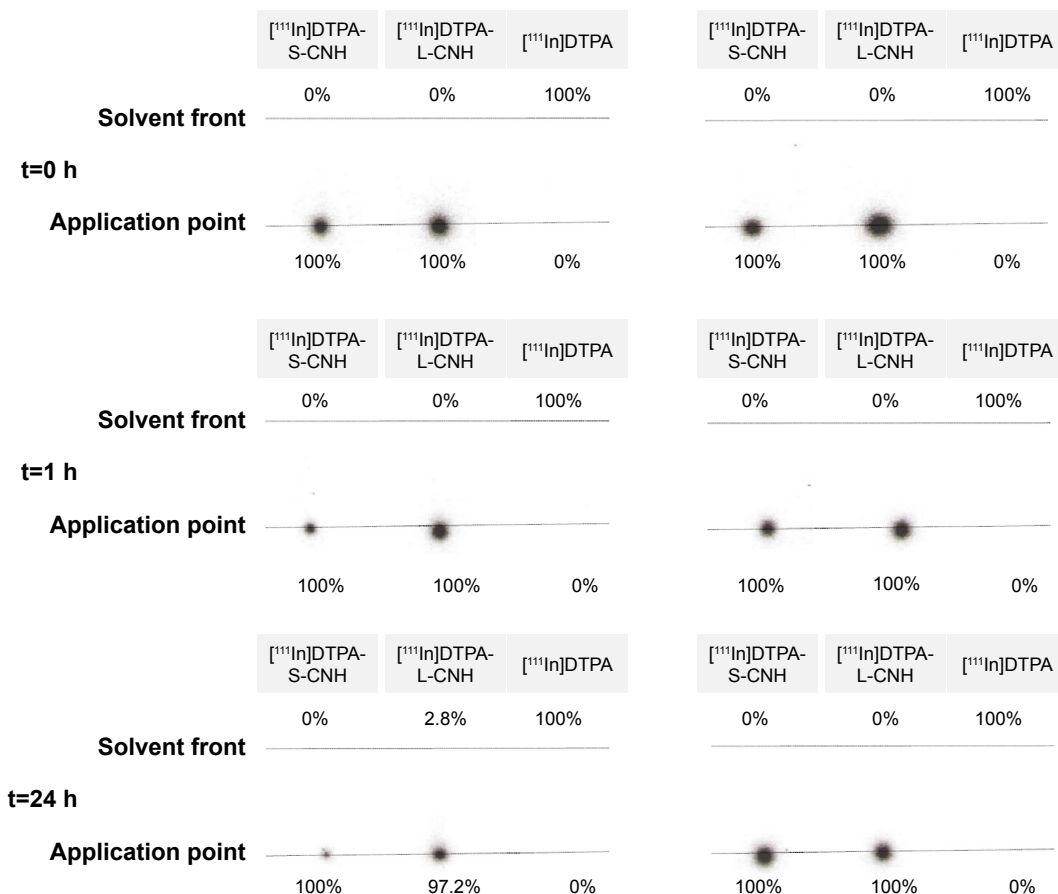


Figure S3 TLC papers showing the radiolabeling stability of $[^{111}\text{In}]\text{DTPA-S-CNHs}$ and $[^{111}\text{In}]\text{DTPA-L-CNHs}$ in mouse serum (left column) and PBS (right column) over 24 hours (h).

Abbreviations: TLC, thin-layer chromatography; DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; PBS, phosphate-buffered saline.

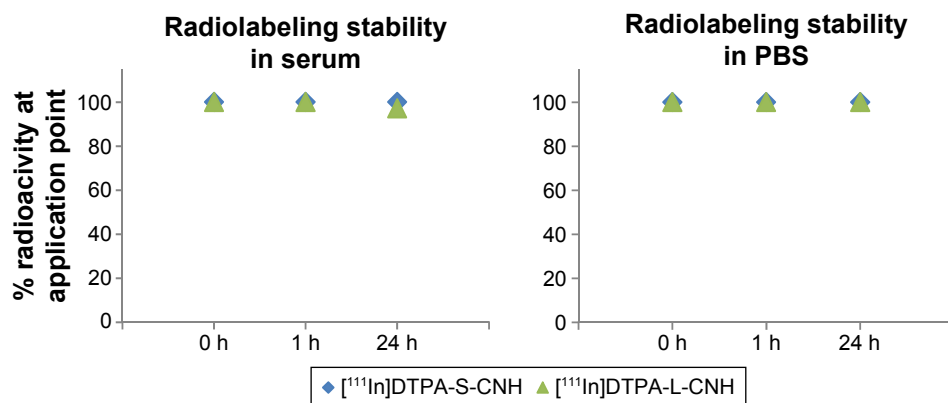


Figure S4 Radiolabeling stability of $[^{111}\text{In}]\text{DTPA-S-CNHs}$ and $[^{111}\text{In}]\text{DTPA-L-CNHs}$ in mouse serum (left) and PBS (right) over 24 hours (h).

Abbreviations: DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; PBS, phosphate-buffered saline.

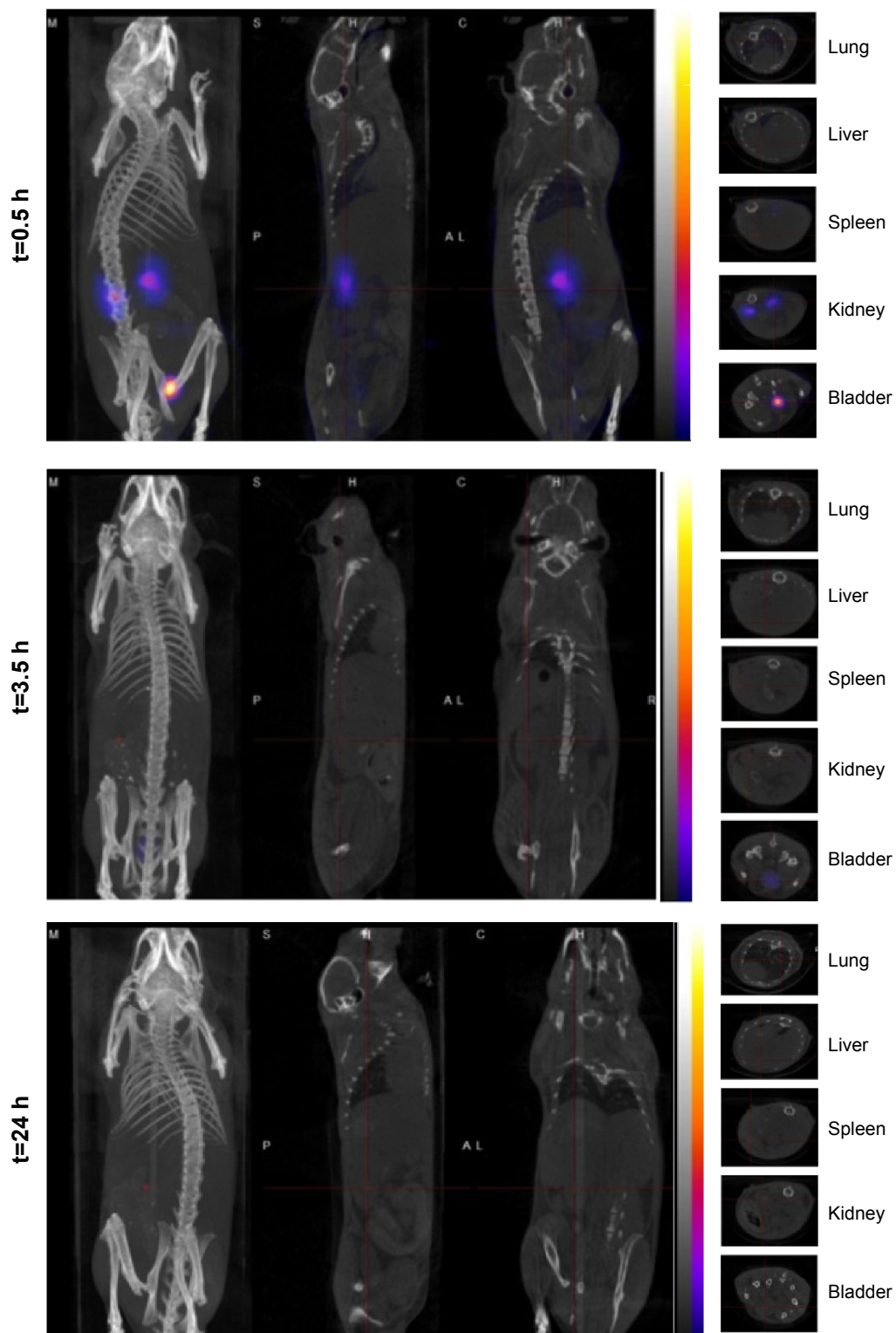


Figure S5 SPECT/CT images of $[^{111}\text{In}]\text{DTPA}$ control injected mouse at 0.5, 3.5, and 24 hours (h) postinjection.

Notes: The bright areas indicate the accumulation of $[^{111}\text{In}]\text{DTPA}$. Images from left to right show whole-body, sagittal, frontal, and transverse views. Cross-sectional images of the spleen, liver, lung, kidney, and urinary bladder are shown in the right column.

Abbreviations: SPECT/CT, single photon emission computed tomography/computed tomography; DTPA, diethylenetriaminepentaacetic acid.

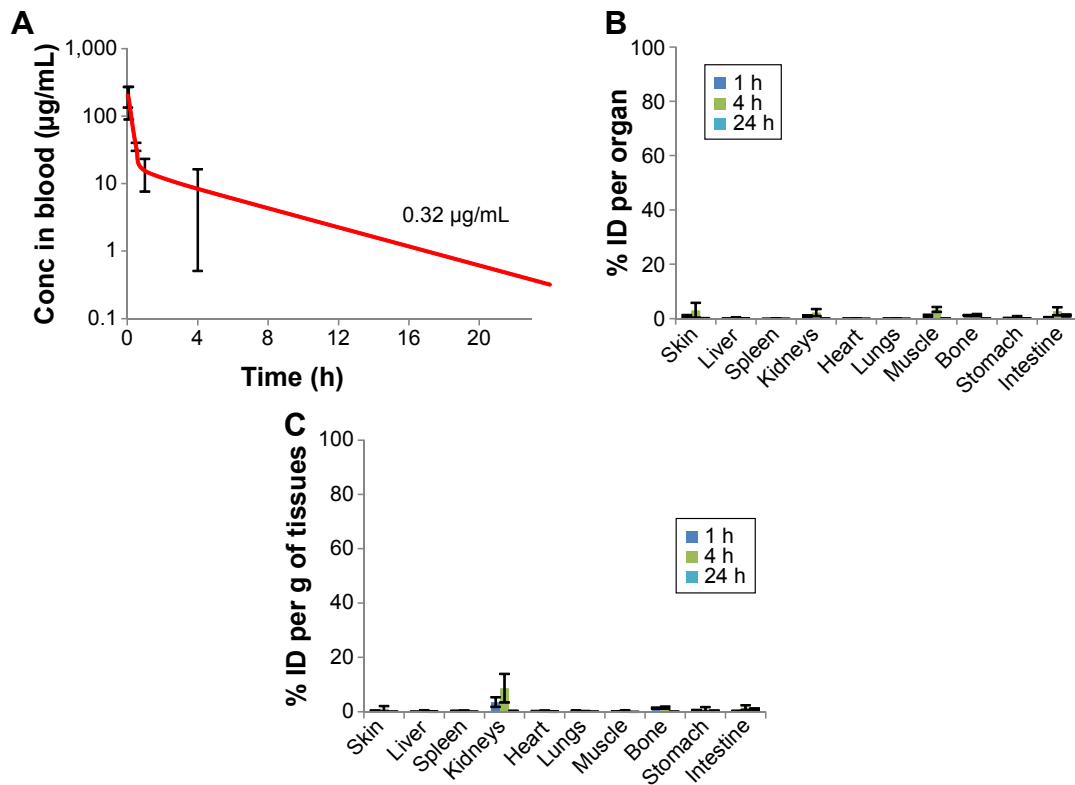


Figure S6 Quantities of ^{111}In DTPA control injected intravenously in mice detected by gamma scintigraphy up to 24 hours (h) postinjection. **Notes:** (A) Detected in whole blood by concentration ($\mu\text{g/mL}$). (B) Percentage ID per whole organ, and (C) expressed by % ID per gram of tissues. Data are represented as mean \pm standard error, $n=4$ mice per group. **Abbreviations:** DTPA, diethylenetriaminepentaacetic acid; conc, concentration.

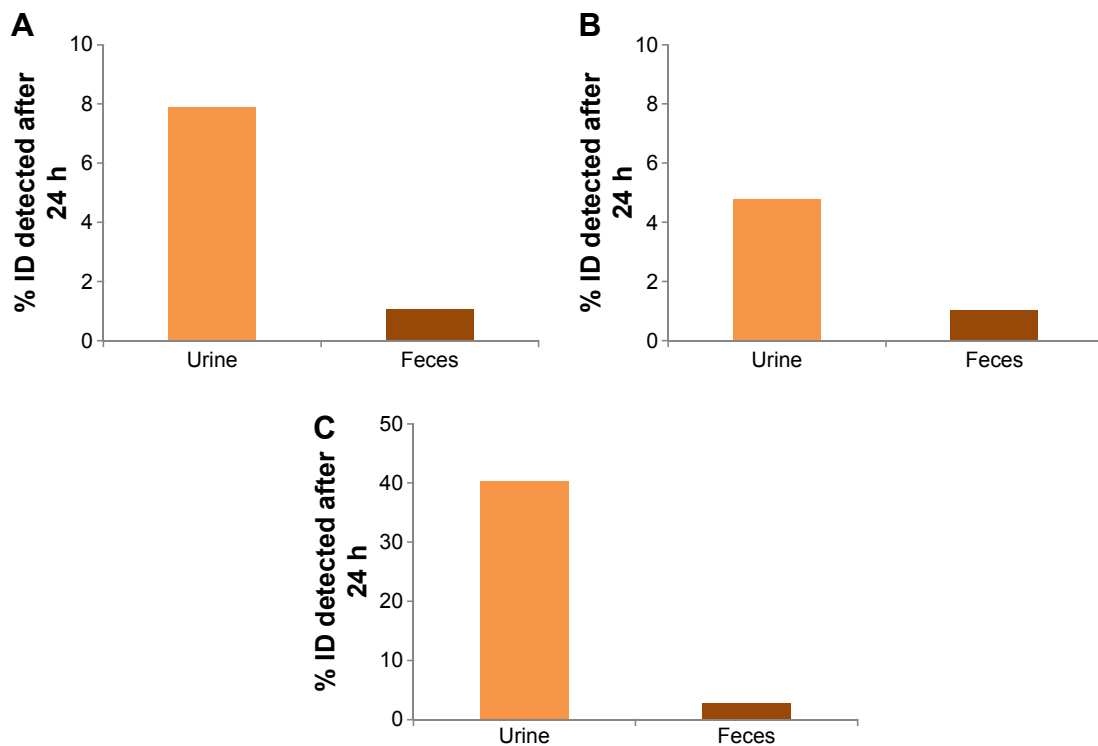


Figure S7 Metabolic profile represented by amounts of ^{111}In labeled S- or L-CNHs (% ID) detected in urine and feces 24 hours postinjection. **Notes:** (A) ^{111}In DTPA-S-CNHs, (B) ^{111}In DTPA-L-CNHs, and (C) ^{111}In DTPA control. **Abbreviations:** DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs; h, hours.

Table S1 Percentage ID detected in bladder by single-photon emission computed tomography/computed tomography semi-quantification

Time (h)	DTPA (%)	S-CNHs (%)	L-CNHs (%)
0.5	3.9	3.5	2.2
3.5	1.3	0.2	1.0
24	0.1	0.3	0.4
48	0.0	0.5	0.2
Total	5.3	4.4	3.8

Abbreviations: h, hour(s); DTPA, diethylenetriaminepentaacetic acid; CNHs, carbon nanohorns; S-CNHs, small-sized CNHs; L-CNHs, large-sized CNHs.

Then, the reaction mixture was evaporated under vacuum to give a beige solid in a quantitative yield. ^1H NMR (300 MHz, dimethyl sulfoxide- d_6 as a TFA salt, the signal of TFA was not included) δ =1.42–1.64 (m, 4 H), 1.74–1.92 (m, 2 H),

2.72–2.85 (m, 2 H), 2.98–3.15 (m, 4 H), 3.25–3.40 (m, 4 H), 3.60 (s, 8 H), 4.45 ppm (t, J =6.5 Hz, 1 H), 7.84 (br s, 3 H). ^{13}C NMR (75 MHz, dimethyl sulfoxide- d_6 as a TFA salt, the signal of TFA was not included) δ =23.1, 26.3, 26.9, 38.3, 49.9, 50.1, 54.1, 63.7, 170.5, 172.2 ppm. Liquid chromatography–mass spectrometry [molecular weight (ammonium) 465]: m/z 465 $[\text{M}]^+$.

Reference

1. Marangon I, Ménard-Moyon C, Kolosnjaj-Tabi J, et al. Covalent functionalization of multi-walled carbon nanotubes with a gadolinium chelate for efficient T1-weighted magnetic resonance imaging. *Adv Funct Mater.* 2014;24(45):7173–7186.

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